

# Micro Electro Mechanical Systems for mechanical engineering applications

## Lecture 8: Introduction to BioMEMS: from historical background to current research

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# Definition of BioMEMS

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- **From a systemic aspect:**

BioMEMS usually contains sensors, actuators, mechanical structures and electronics. Such systems are being developed as diagnostic and analytical devices.

- Suzanne Berry, TRENDS in Biotechnology (2002)

- **From a component aspect:**

BioMEMS is the research of microfabricated devices for biological applications.

- Tejal A. Desai, Biomolecular Engineering (2000)

- MEMS technology is an engineering solution for biomedical problems.



# BioMEMS in Biomedical Field

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BioMEMS encompasses all interfaces and intersections of the **life sciences** and **clinical disciplines** with **microsystems** and **nanotechnology**.

Related area:

- Micro & nanotechnology for drug delivery,
- Tissue engineering, harvesting, manipulation
- Biomolecular amplification,
- Sequencing of nucleic acids
- Proteomics
- Microfluidics and miniaturized total analysis systems (microTAS)
- Biosensors
- Molecular assembly,
- Nano-scale imaging, and integrated systems

Adapted from Cambridge Healthtech Institute  
<http://www.genomicglossaries.com>

# MEMS vs. BioMEMS

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## MEMS

- Silicon based Material
- Electrical & Mechanical interface integration
- Moving part in micromachining system  
-active component

## BioMEMS

- Biocompatible Material
- Biomolecular & physical parameter (electrical, mechanical, optical ) transducer integration
- Motion medium in passive  
Moving ∴  
-microfluidic driving force

*A quite different thinking process from MEMS to BioMEMS*

# Applications in Bioscience

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- Exploit size match between cells and MEMS
- Utilize physical microscale phenomena
- Miniature, multi-component instruments
  - sensors
    - potential, pressure, force, pH, chemistry
  - actuators
    - pumps, valves, probes, grippers, ...
  - systems
    - Integrated microfluidic platforms
    - Lab-on-a-chip systems



# Actuation Mechanisms of BioMEMS

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Typical MEMS actuation mechanisms for pumping:

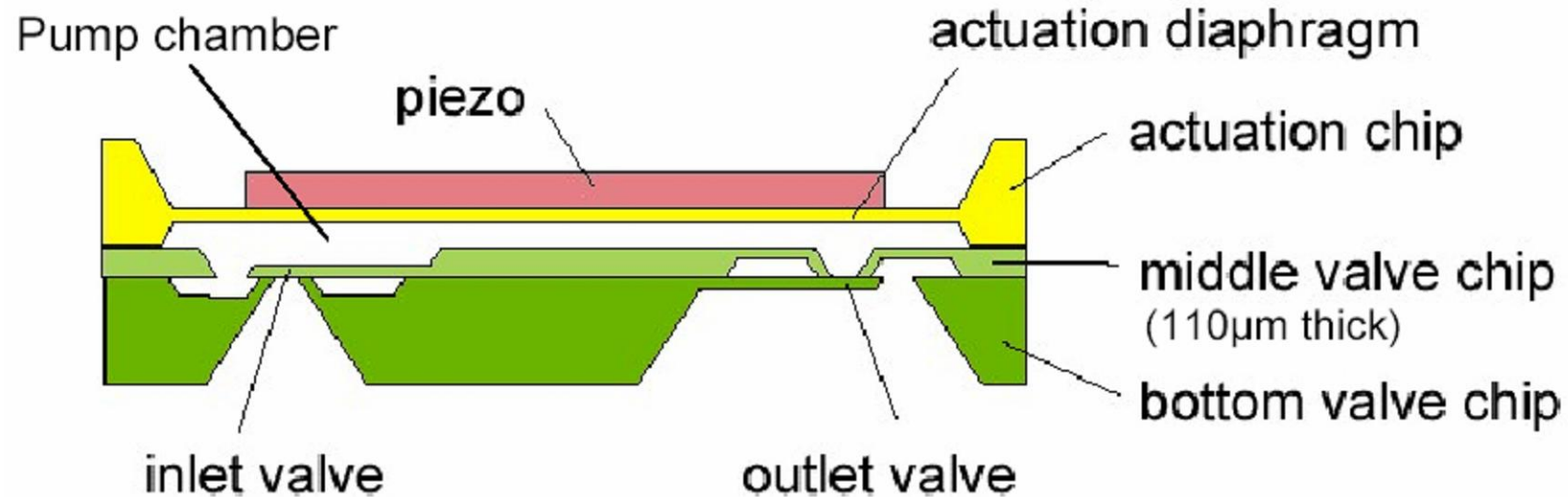
- Electrostatic
- Thermal
- Magnetic
- Pneumatic
- Piezoelectric
- Ultrasonic

Direct fluidic actuation mechanisms:

- Fluidic phase change
- Electrohydrodynamic (EOF, electrophoresis, etc)



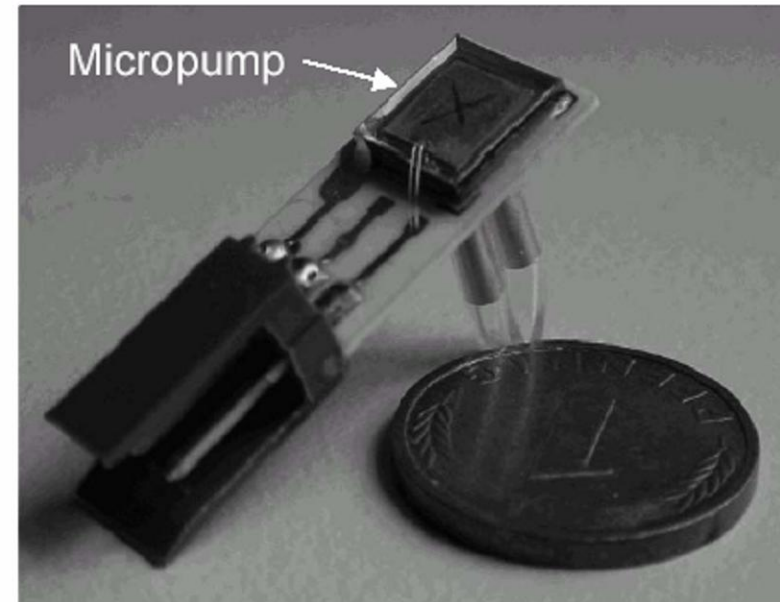
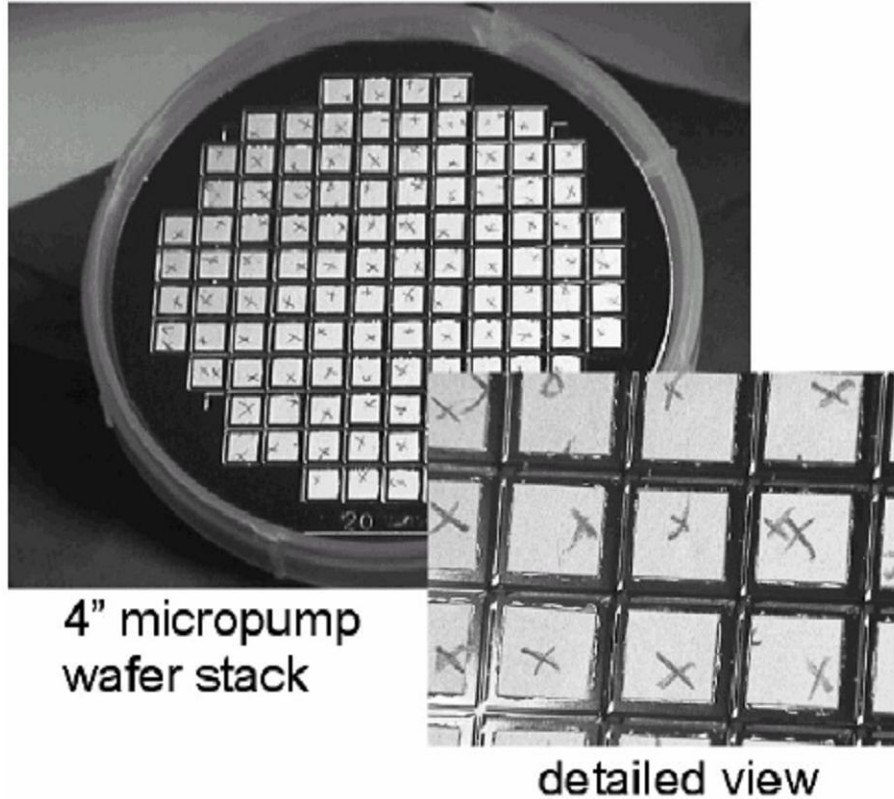
# Piezoelectric Pump (1)



- Optimized pump is “bubble tolerant” and “self-priming.”
- Lower 2 wafers bonded via silicon fusion bonding. Top wafer later glued.
- Piezo ceramic driven by high voltage (-40V, +90V)
- At 100Hz, no back pressure, average flow rate  $\approx 1600\mu\text{l}/\text{min}$ .
- Dead volume = pump chamber volume  $\approx 800\text{nl}$ .
- Average stroke volume = 260nl.

# Piezoelectric Pump (1)

- Packaging and Production

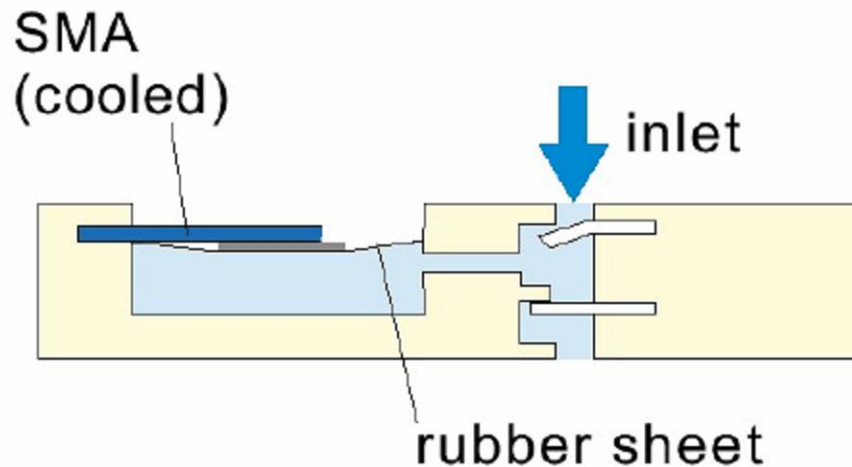
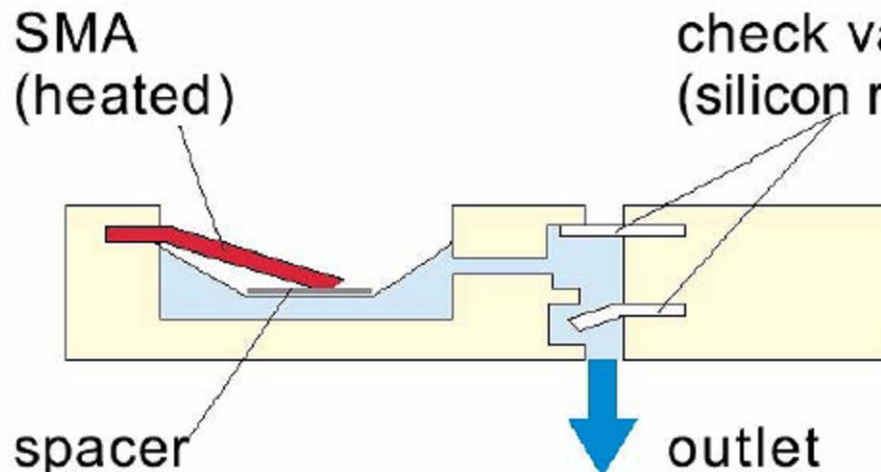


*Micropump (7mm x 7mm) is glued on a carrier with electrical and fluidic interconnects attached.*

Piezoelectric crystals are attached to all die simultaneously via glue and assembly aids.

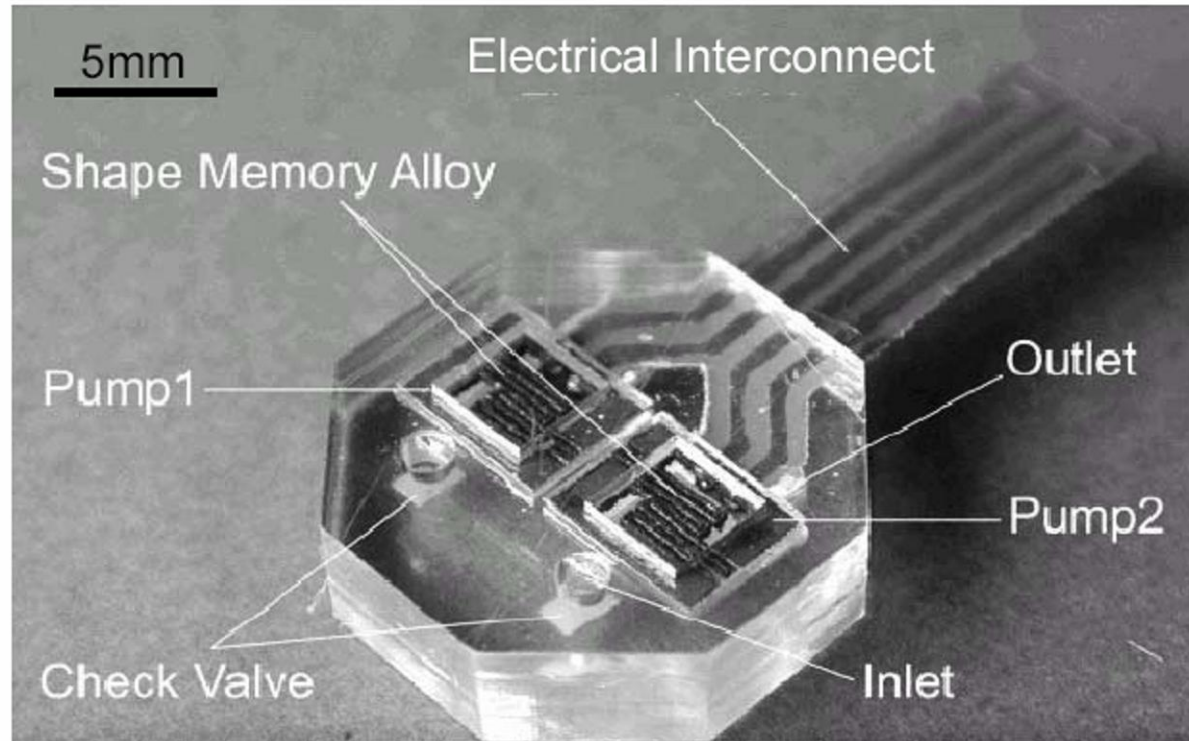


# Shape Memory Alloy Pump (1)



- Also bubble tolerant and self-priming.
- Fabrication via custom UV polymerization process (micro stereo lithography).
- SMA, silicone rubber, ICs, and spacers are inserted during polymerization – No bonding needed and leak proof packaging created easily.

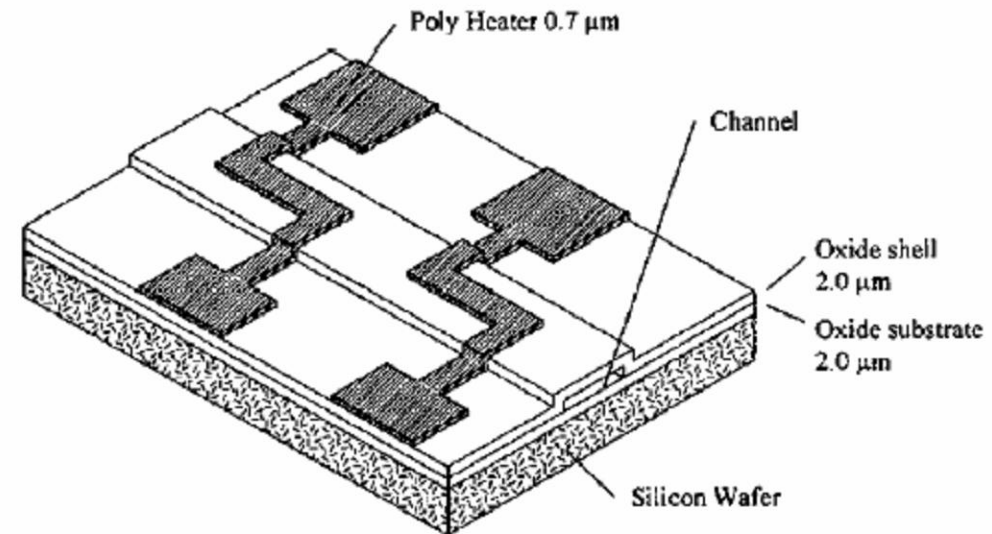
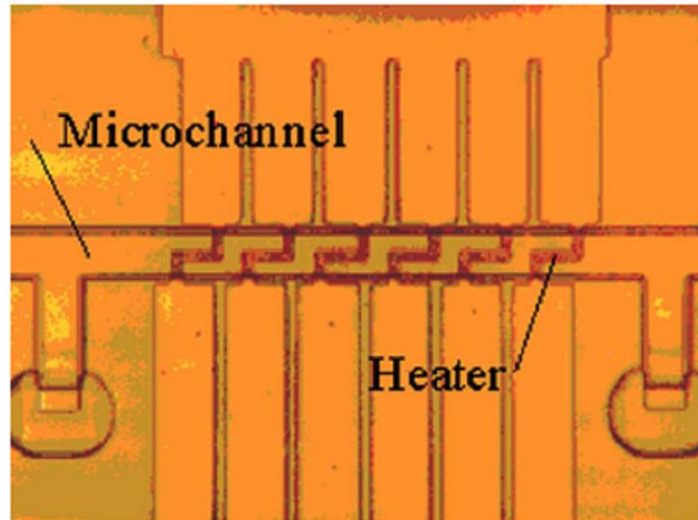
# Shape Memory Alloy Pump (2)



	Maximum Flow	Maximum Pressure
Liquid (water)	12.3 $\mu\text{l}/\text{min}$	25 kPa
Gas (air)	11.0 $\mu\text{l}/\text{min}$	5 kPa

K. Ikuta, T. Adachi, Nakoya University

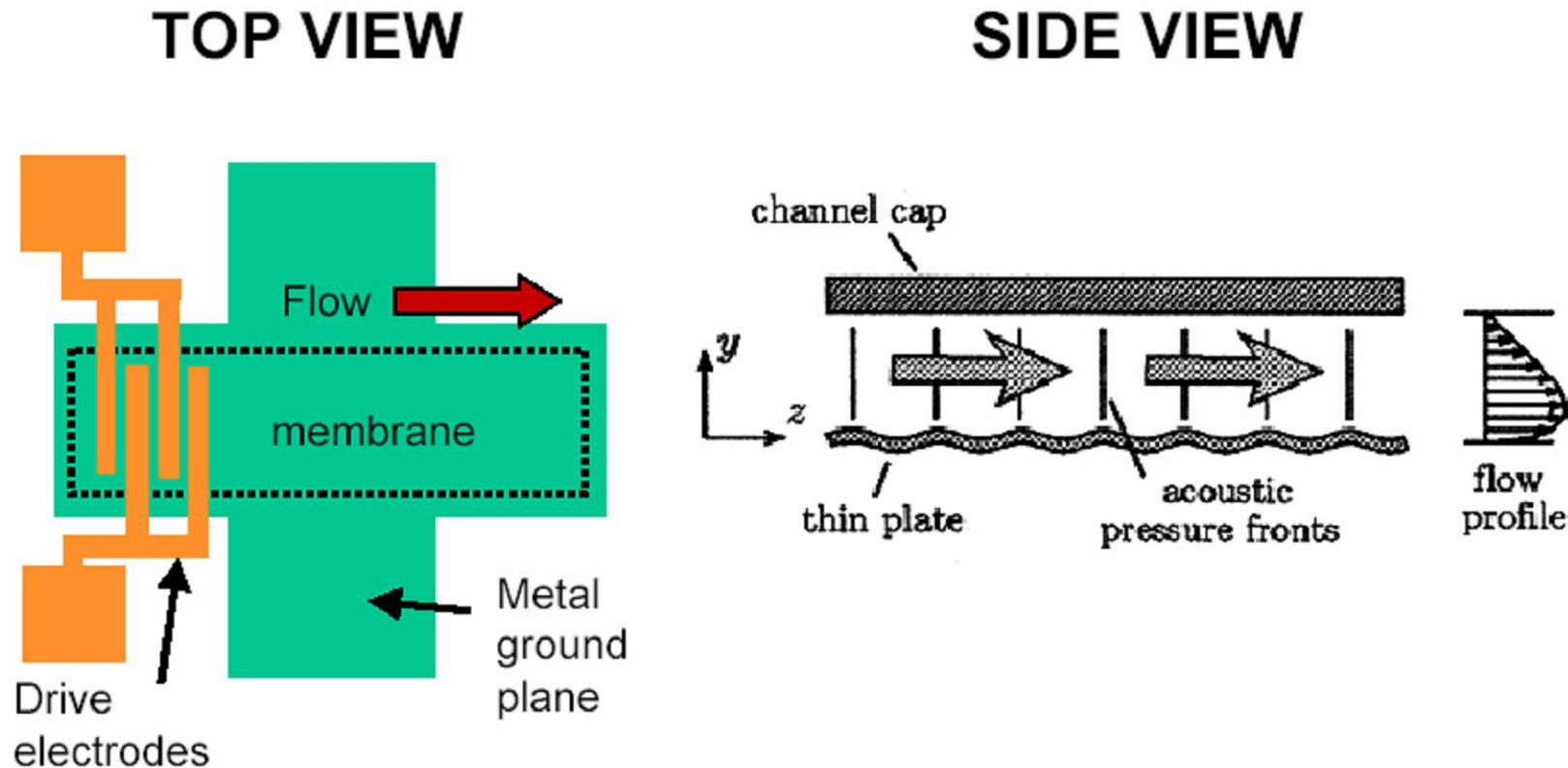
# Bubble-driven Micropump



- Bubble formation induced in heater pushes fluid in the channel.
- Maximum flow rate = 0.5nl/min
- Maximum pressure head = 800Pa

T. K. Jun and C. J. Kim, UCLA/MAE

# Acoustic Pumping

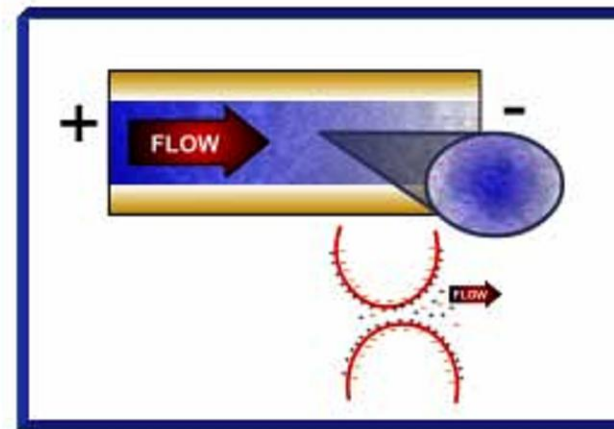
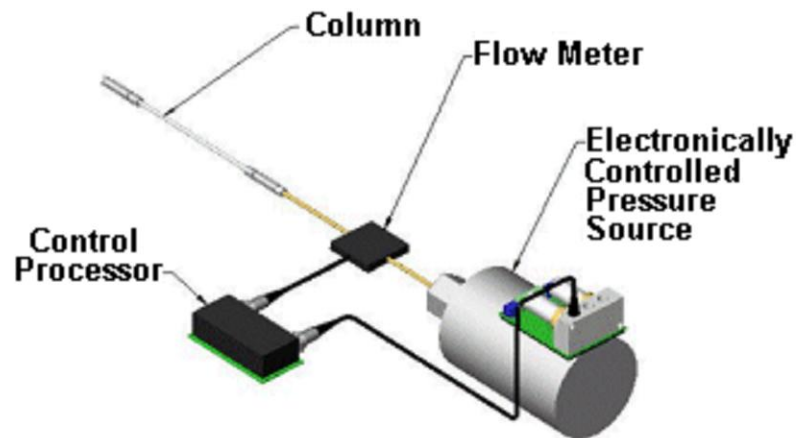


Acoustic streaming causes micron-size particles to be channeled by ultrasonic standing waves.

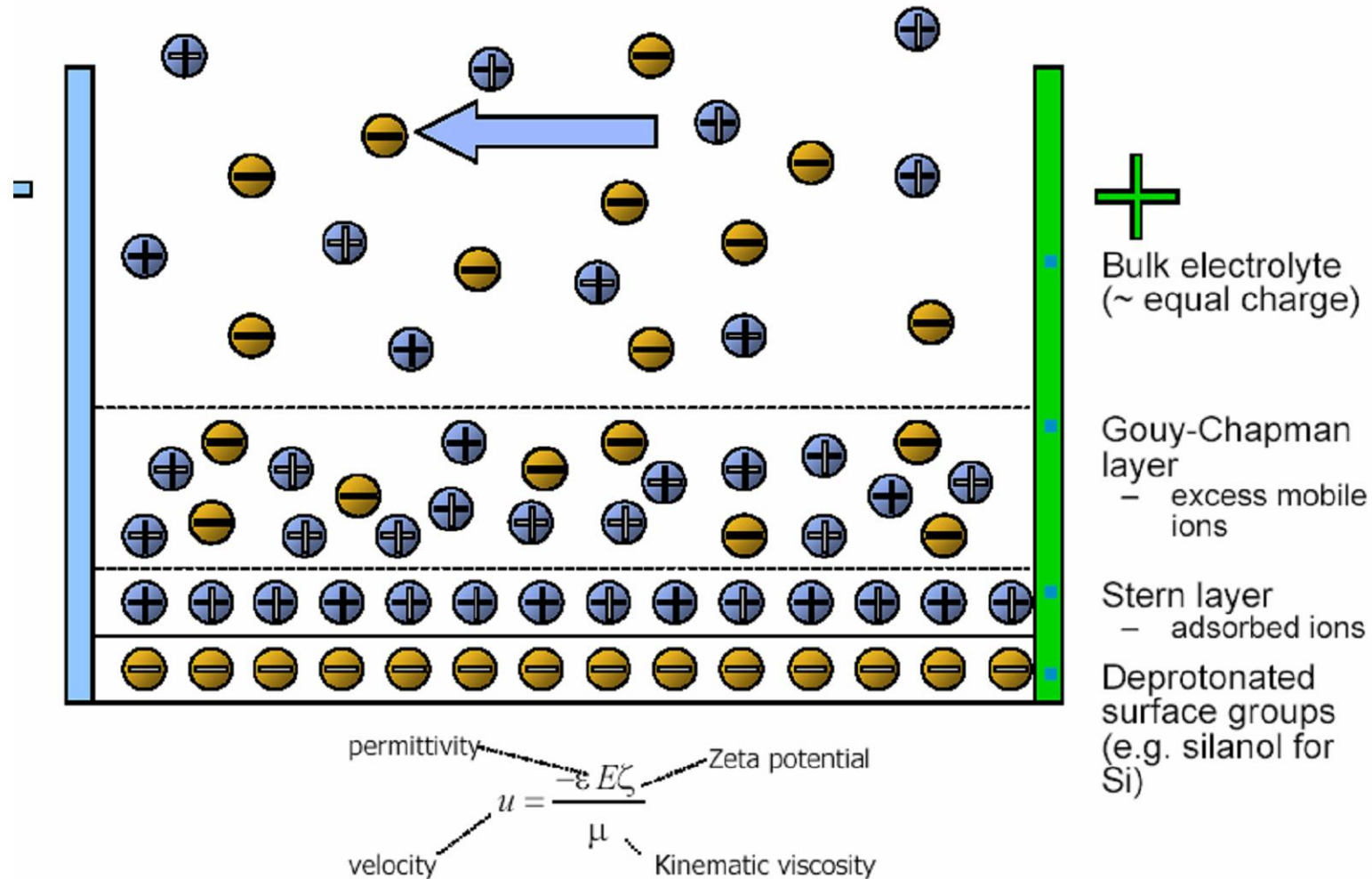
# Electrokinetic Pump

- Precise control of flow rate
- Ability to pump against substantial back pressures
- Active feedback for identification -and prediction- of leaks or blockages
- Virtually instantaneous response to step changes in flow rate setpoint

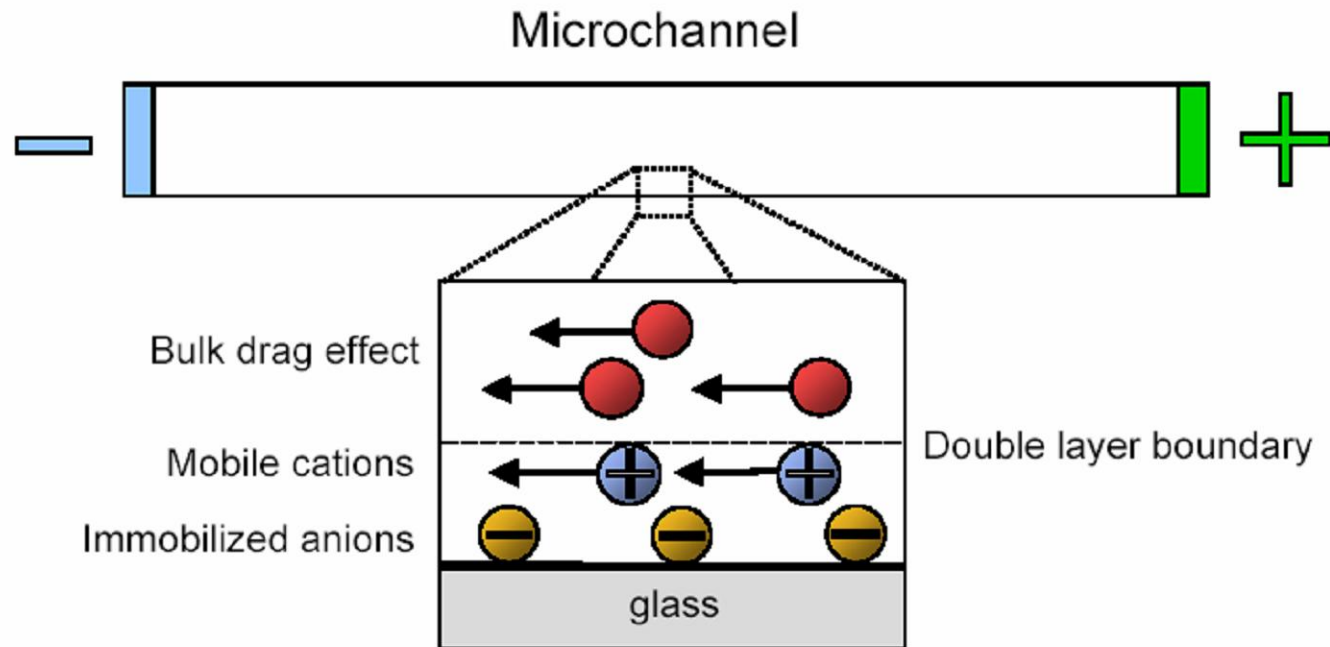
Animation: [http://www.eksigent.com/tech\\_ekpump.htm](http://www.eksigent.com/tech_ekpump.htm)



# Electro-Osmotic Pump (1)



# Electro-Osmotic Pump (2)

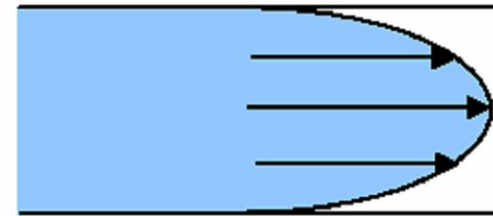


- Immobilized charges on the walls of the channels or capillary contribute to formation of double layer of opposite charges.
- The mobile charges move under the influence of the external electric field, causing bulk drag effects (flow rate is linear w/applied potential).
- Packed capillaries can generate 20atm with 2kV.  
(D = 530 $\mu$ m, L = 5.4cm)

# EOF Flow Profile



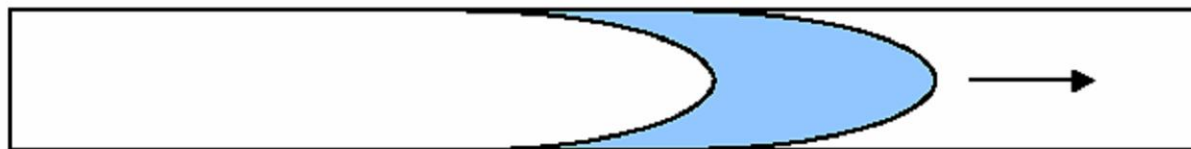
Electroosmotic flow



Pressure-driven flow



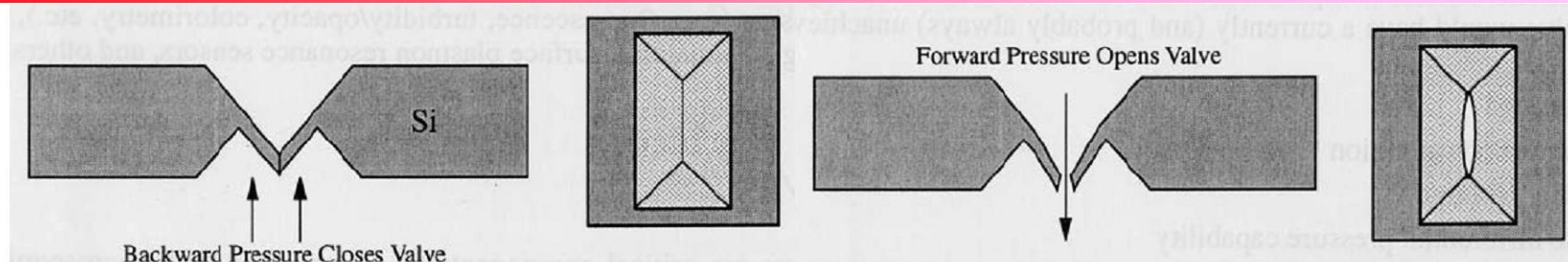
Electroosmotic flow



Pressure-driven flow

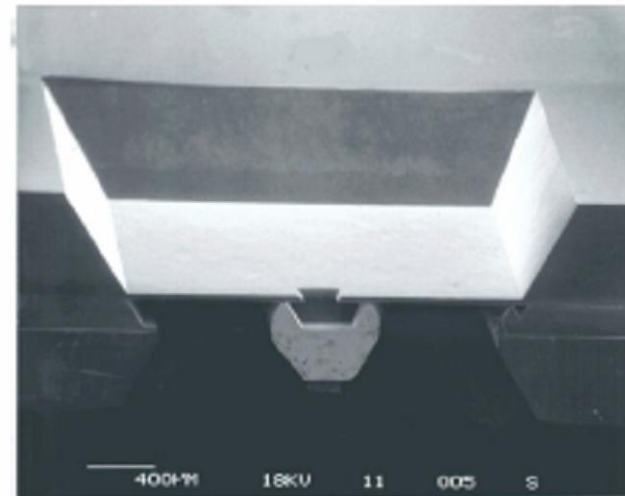
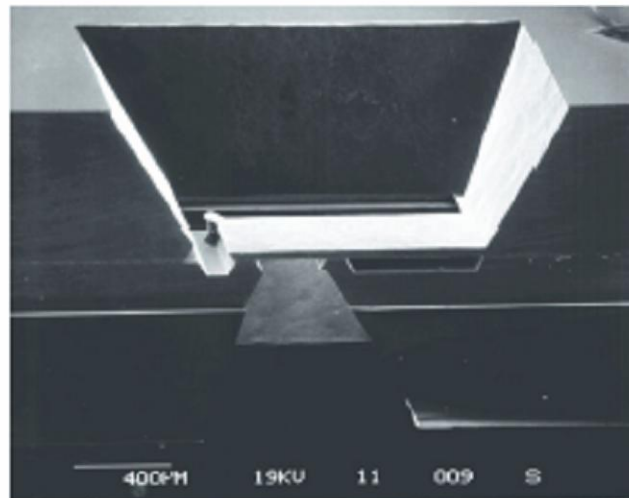
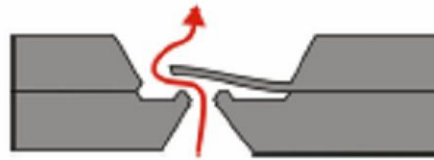


# Passive Valve

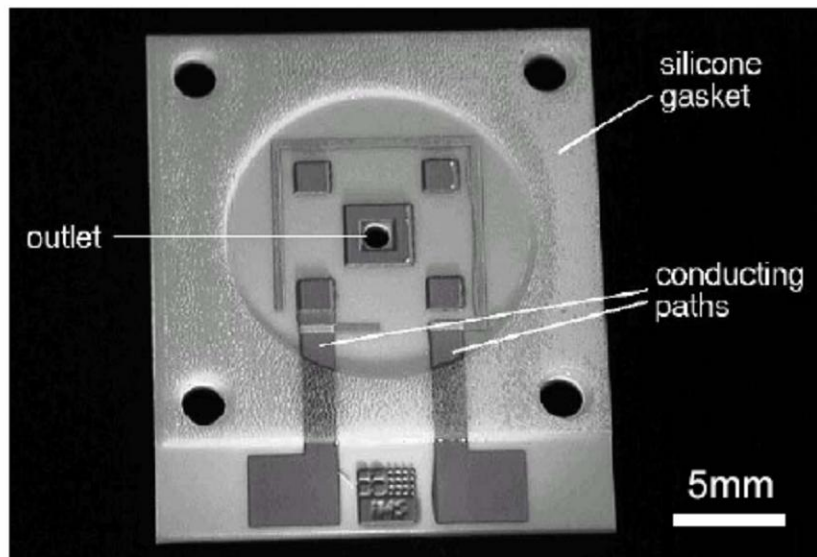
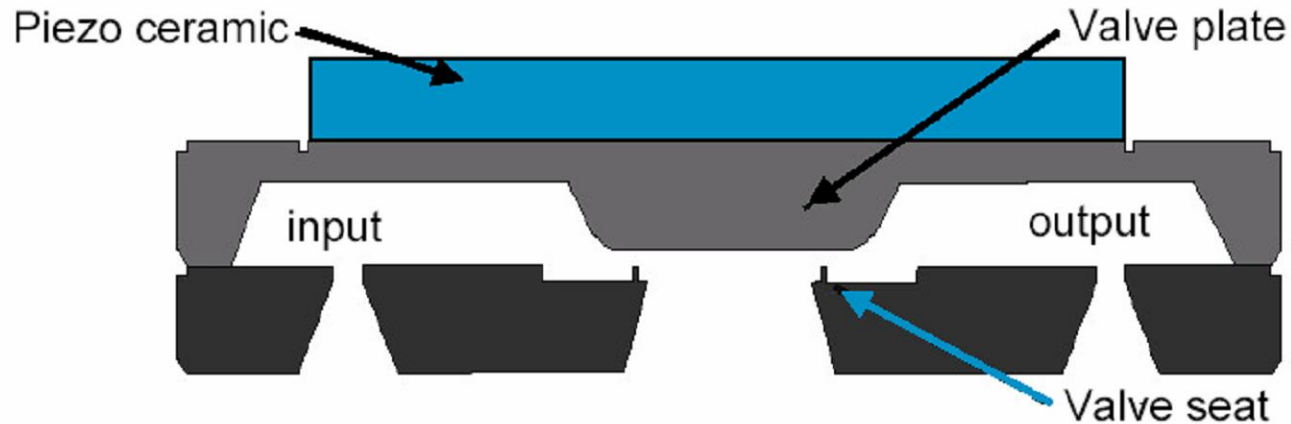


flap valve

membrane valve



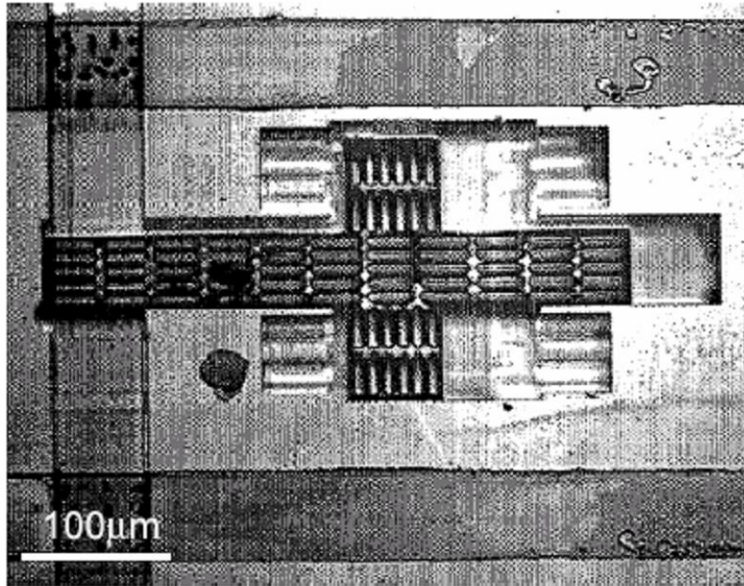
# Piezoelectric Valve



- Valve stroke = 17 $\mu$ m (high pressure configuration)
- Leakage = 7ml/min, with 270V applied and a pressure drop of 6bar across valve.
- Valve packaged on ceramic chip carrier with silicone gasket.

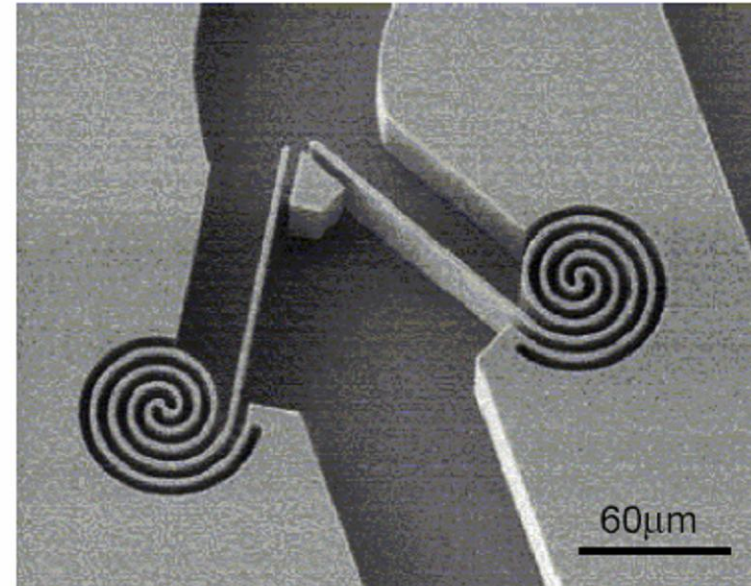
S. Kluge, Fraunhofer Institute

# Planar Mechanical Valve



*A. Papavasiliou (BSAC/UCB)*

- Electrolysis bubble-actuated gate valve

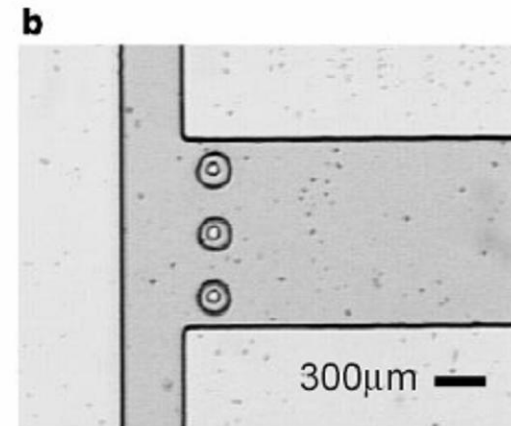
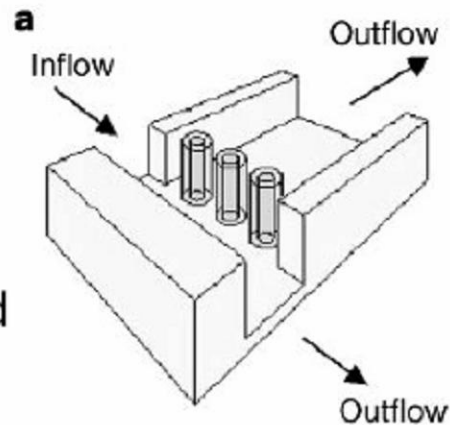


*J. Evans (BSAC/UCB)*

- Spring loaded check valve

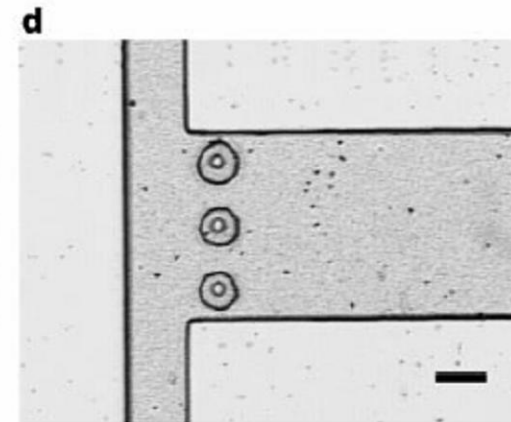
# Hydrogel Microfluidic Valve (1)

Integrated within the channel, photopatterned



As fabricated

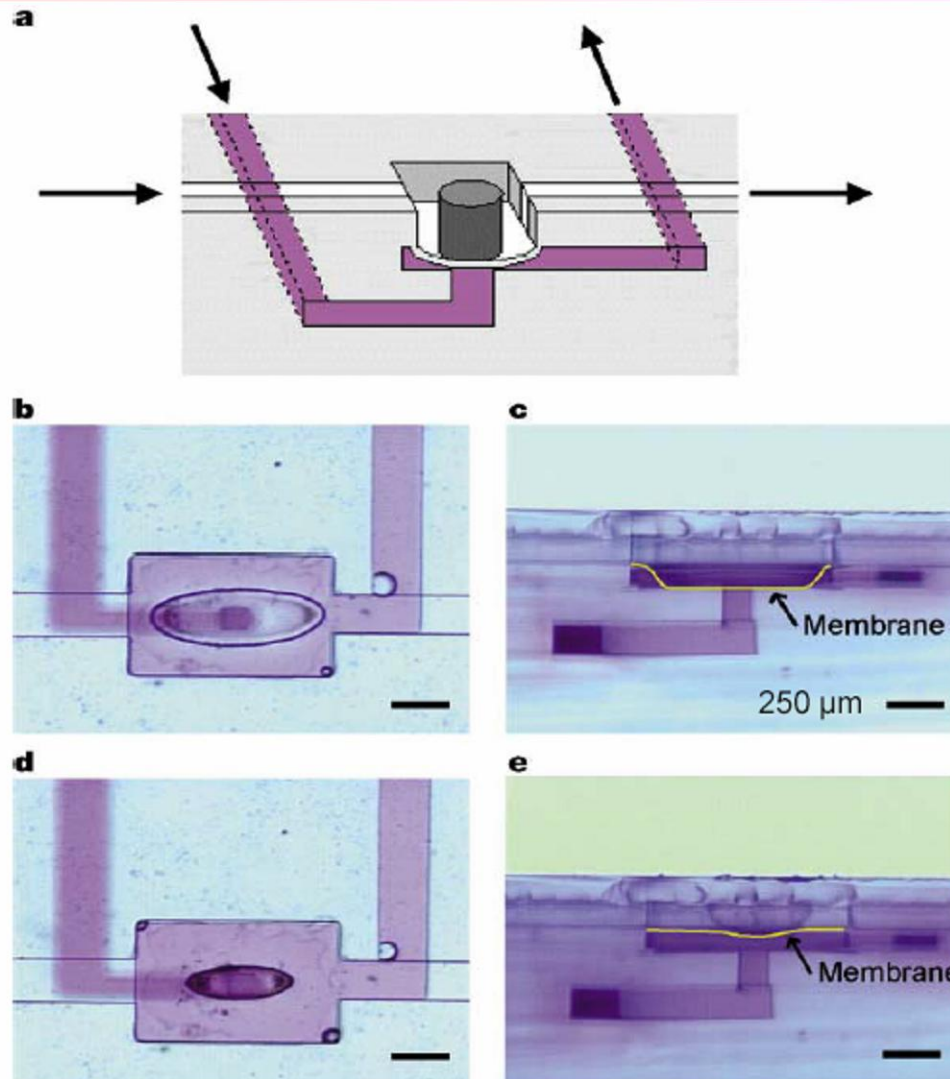
Activated in response to pH – flow is blocked



Contracted in response to pH – flow resumes

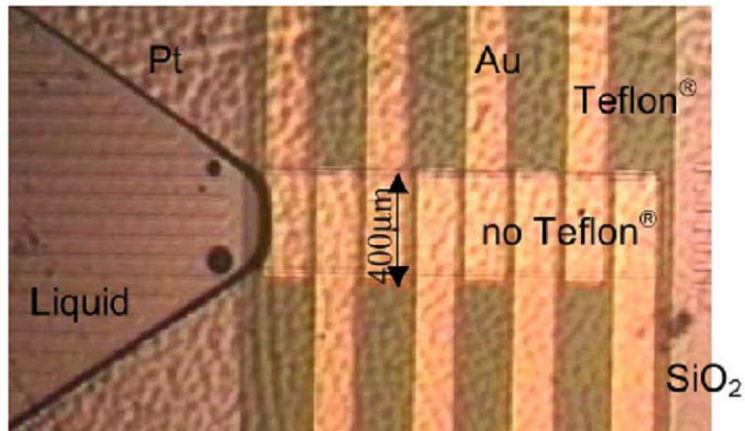
Beebe et. al., *Nature*, vol. 404, pp. 588 – 590, April 6, 2000.

# Hydrogel Microfluidic Valve (2)

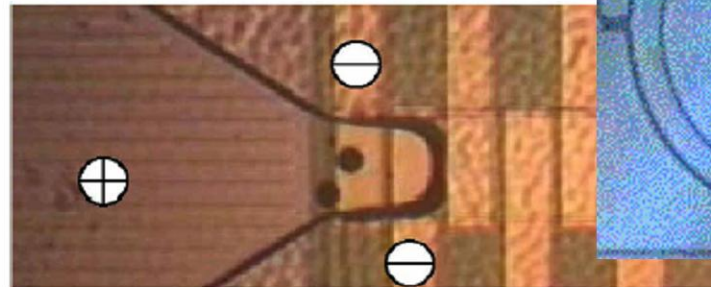


- In response to pH, the hydrogel structure in upper channel expands
- The membrane deforms, blocking flow in the lower channel.
- Hydrogel functions as sensor and actuator
- Stimulus can also be antigens  $\Rightarrow$  self regulated drug delivery, biosensing

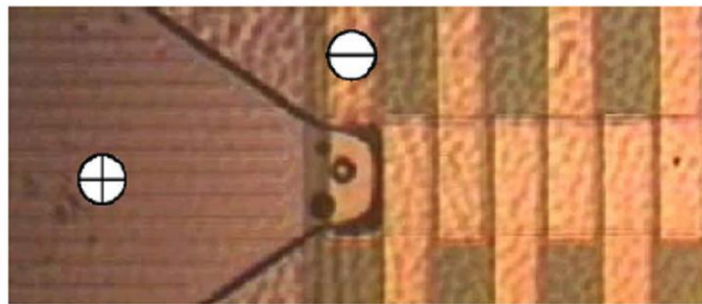
# Surface tension-based Fluid Control



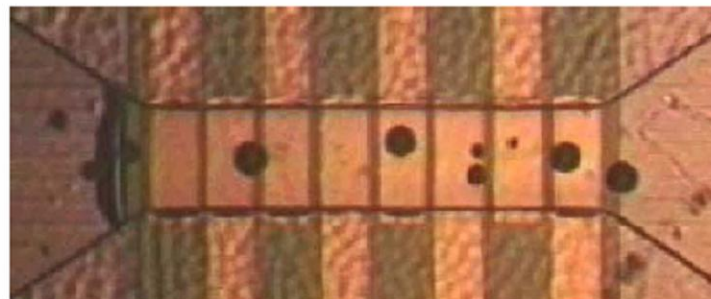
(a) Liquid introduced



(c) 1<sup>st</sup> and 2<sup>nd</sup> electrodes biased



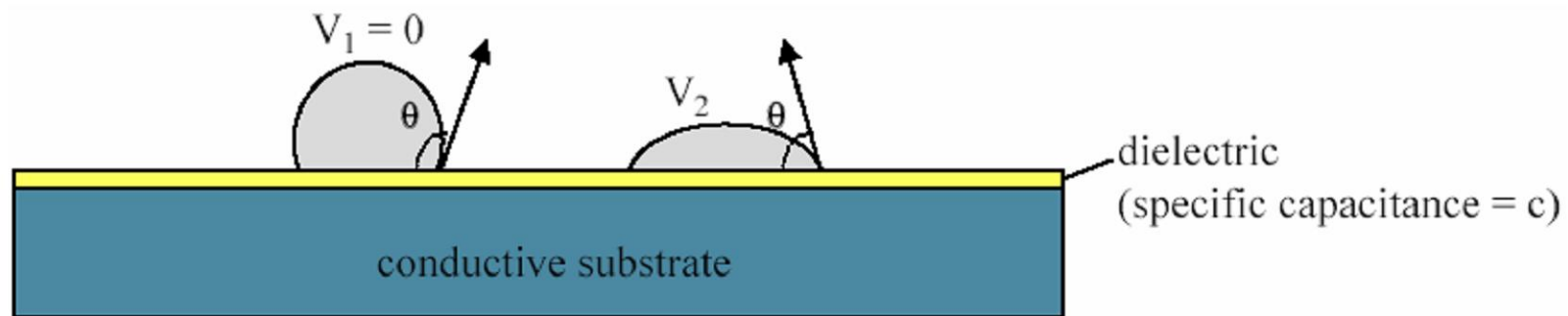
(b) First electrode biased



(d) All electrodes biased

J. Lee and C. J. Kim, UCLA/MAE

# Electrochemical Wetting Principle



$$\cos(\theta) = \cos(\theta_0) + (1/2\gamma_{LG})cV^2$$

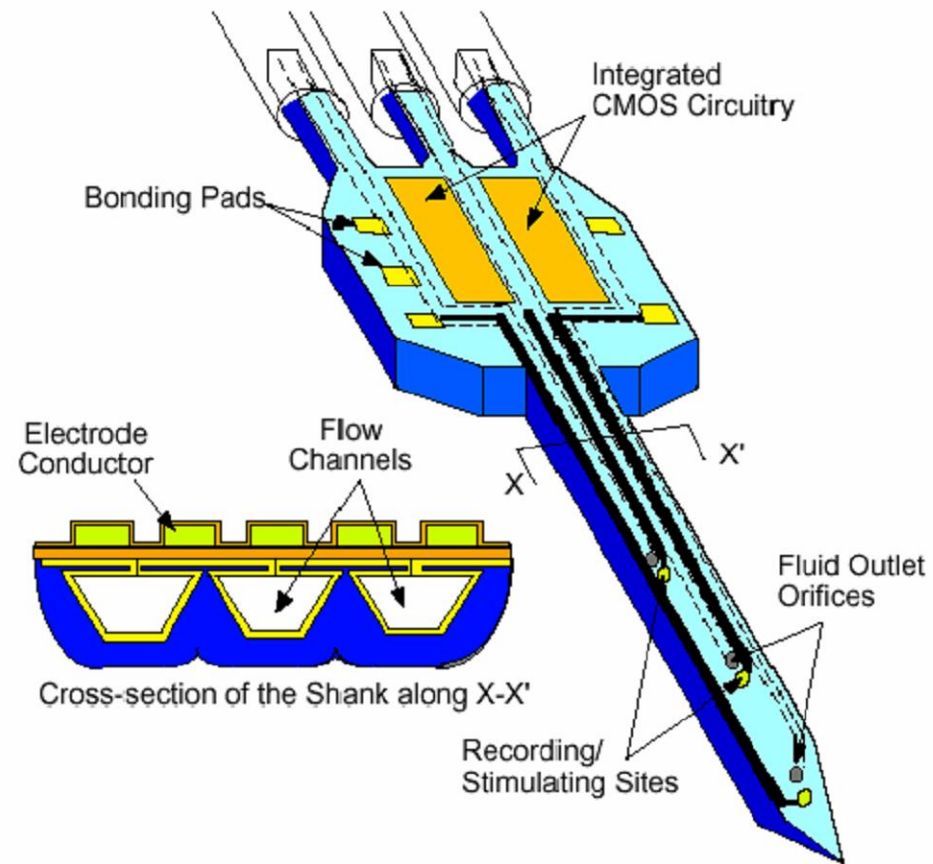
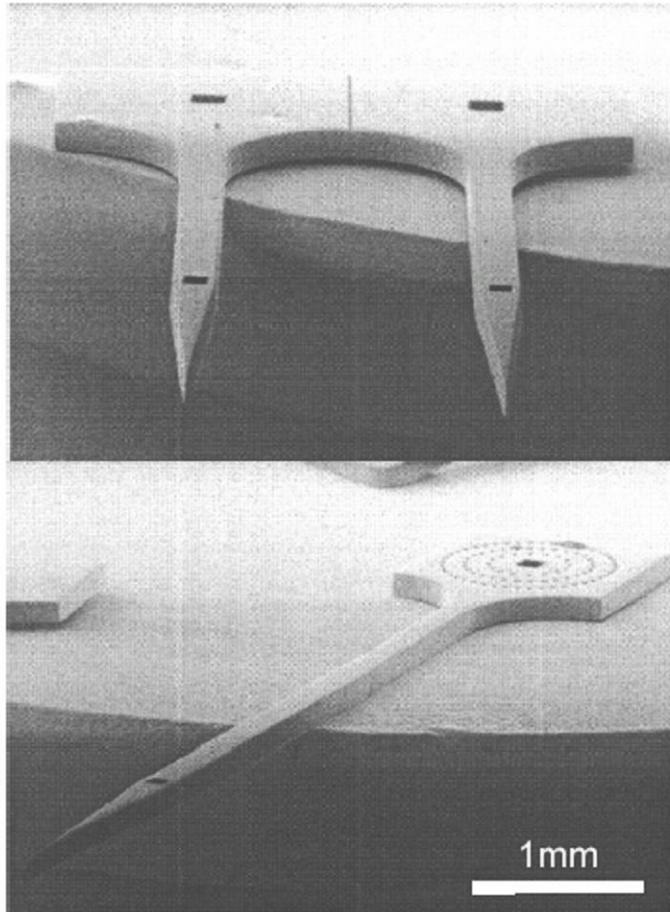
$\theta$  is contact angle

$\gamma_{LG}$  is liquid-gas surface tension

$c$  is specific capacitance of dielectric

$V$  is applied voltage

# Drug Delivery Platforms

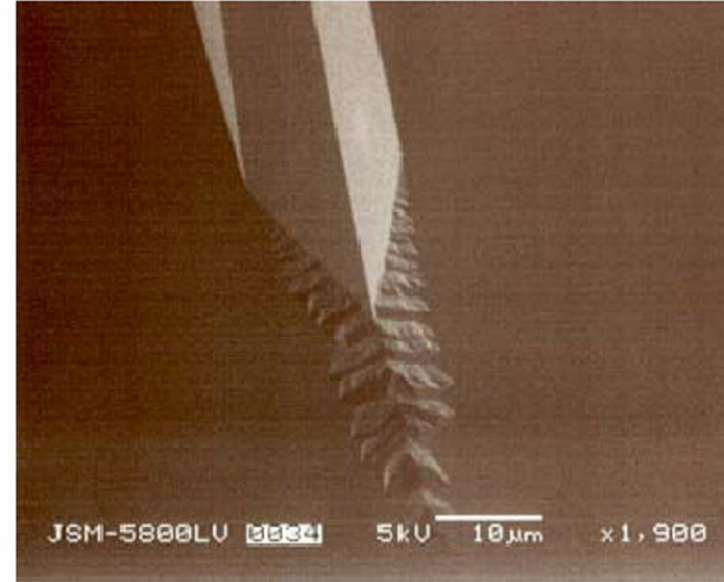
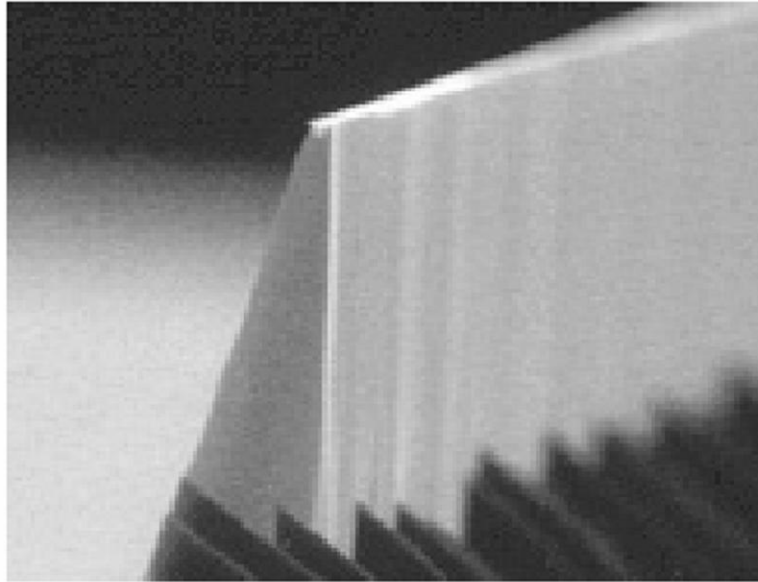


Photos courtesy of N. Talbot and A. Pisano, UC Berkeley  
Diagram courtesy of K. Wise, U. Michigan.



# MEMS Microblades

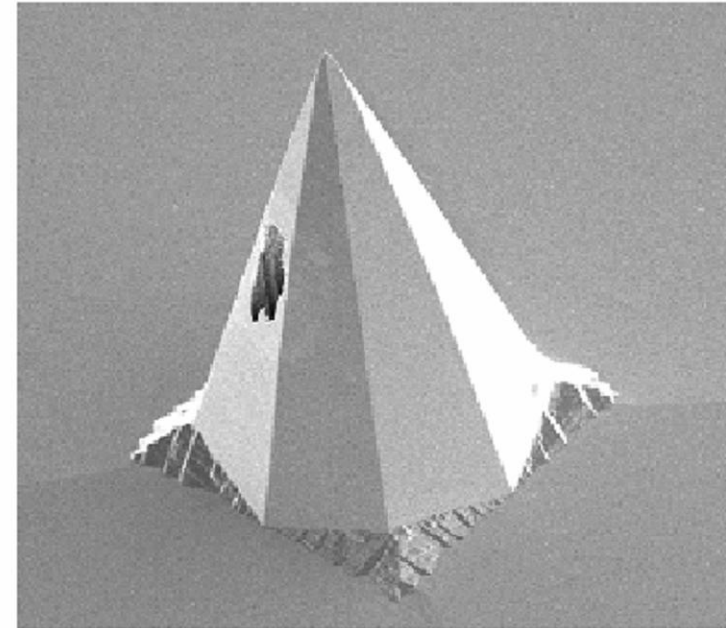
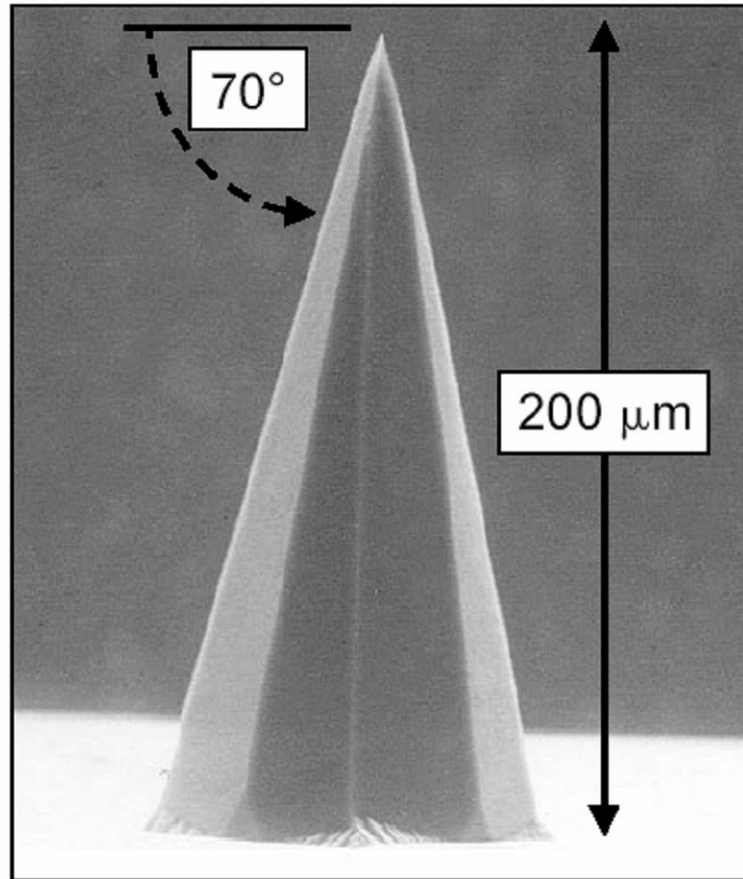
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- Silicon micro-blades etched via chemical etching
- May be used for delicate microsurgery
- Microneedles fabricated in a similar fashion

Fabricated at Standard MEMS, Inc.

# Drug Delivery Microneedles



- Single crystal silicon
- Bulk micromachined
- Higher order planes exposed
- Laser drilled hole

Fabricated at Standard MEMS, Inc.