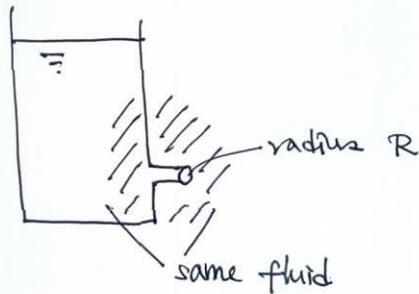


§ Flow through circular apertures (submerged)



$$Re < 3 : Q = \frac{R^3 \Delta P}{3\mu}$$

$$\text{higher } Re : Q = C \pi R^2 \left(\frac{2 \Delta P}{\rho} \right)^{1/2}$$

C : orifice coefficient = $f_n(R_d)$

Chap. 14. Internal flows in organisms

- most circulatory systems of animals
- ~ pulsatile flow of non-Newtonian fluids in pipes of time varying cross-sectional areas and shapes

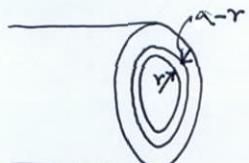
§ Circumventing the parabolic profile



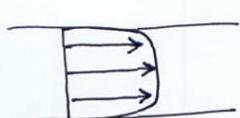
- (1) How far is flow from a wall?

- distance index

$$D_i = \frac{1}{\pi a^2 \bar{u}} \int_0^a u(a-r) \cdot 2\pi r dr / a$$

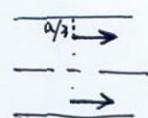


① plug flow (slug flow)



$$\bar{u} = u = \text{const.}$$

$$\begin{aligned} D_i &= \frac{2\pi}{\pi a^2 \bar{u}} u \int_0^a (ar - r^2) dr \\ &= \frac{2}{a^2} \cdot \left(\frac{a^3}{2} - \frac{a^3}{3} \right) = \frac{1}{3} \end{aligned}$$



② fully developed laminar flow (parabolic)

$$D_i = \frac{2}{a^3 \bar{u}} \int_0^a \frac{\Delta P}{4\mu L} (a^2 - r^2) (ar - r^2) dr.$$

$$= \frac{7}{15} = 0.467$$

$\bar{u} = \frac{\Delta P \cdot a^2}{L \cdot 8\mu}$

$\overbrace{\quad \quad \quad}^{0.467a}$

③ reversed parabolic profile : wall forcing the flow (cilia)



- $D_i \downarrow$ - exchange of material/heat \uparrow

(2) Using noncircular cross sections

- circular cross section :

good - mechanical robustness
cost of construction
wont - exchange

- large pipes through which exchange takes place

~ closer to parallel plates than to circles

e.g. internal gills of fish

nasal passages

Intestine of earthworm

Fig. 14.2

(3) Making the pipes very small

$a \downarrow$ - D_i the same

-  total cross-sectional area \uparrow (good for exchange)

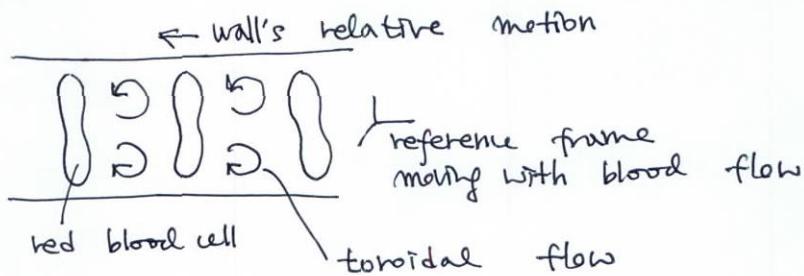
\sim rel. \downarrow

\sim time for exchange \uparrow

(4) Eddies and turbulence

- turbulence : $\overrightarrow{v}_{rel.}$: greatly enhance exchange
but Re of biological pipes too low
- eddies $\overline{\text{_____}}$
 $Re > 30.$

(5) Periodic boluses



* Peclet number

$$Pe = \frac{UL}{D} = \frac{\text{convection}}{\text{diffusion}}$$

D : diffusion coefficient of the dissolved substance

(6) Pumping at the wall

- cilia / flagella coatings on the walls
- steep velocity gradient \rightarrow efficiency of exchange \uparrow
but cost of operation high
- e.g. oviducts
gastroderm of coelenterates
gills of mollusks

S Effluent branching arrays of pipes

(1) Murray's law

- optimal design of a circulatory system based on minimization of cost factors

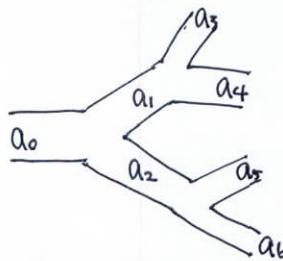
* cost factors

① keeping the blood going against the pressure losses consequent to Hagen-Poiseuille eq.

② construction and maintenance cost proportional to the volume of the system.

$$Q = k a^3$$

e.g. branching tubes



$$\text{by continuity, } A_0^3 = A_1^3 + A_2^3 = A_3^3 + A_4^3 + A_5^3 + A_6^3$$

- consequences

$$\textcircled{1} \quad \text{if } A_1 = A_2, \quad \therefore A_1^3 = A_0^3 \quad ; \quad A_1^3 = \frac{1}{2} A_0^3$$

$$\text{cross-sectional area: } A_1^2 = \left(\frac{1}{2}\right)^{\frac{2}{3}} A_0^2 = 0.63 A_0^2$$

$$\textcircled{2} \quad U_0 A_0^2 = U_1 A_1^2$$

$$= 1.26 U_1 A_0^2$$

$$U_1 = \frac{1}{1.26} U_0 = 0.79 U_0$$

$$\textcircled{3} \quad Q = A^2 U = k a^3$$

$$U \sim a$$



$$\textcircled{4} \quad \text{same specific parabolic profile } \left(\frac{U}{a}\right)$$

for every vessel

$\textcircled{5}$ same velocity gradient at the wall

$$\frac{du}{dr} \Big|_{r=a}$$

$$\textcircled{6} \quad \text{same shear stress } \sim \mu \frac{du}{dr} \Big|_{\text{wall}}$$

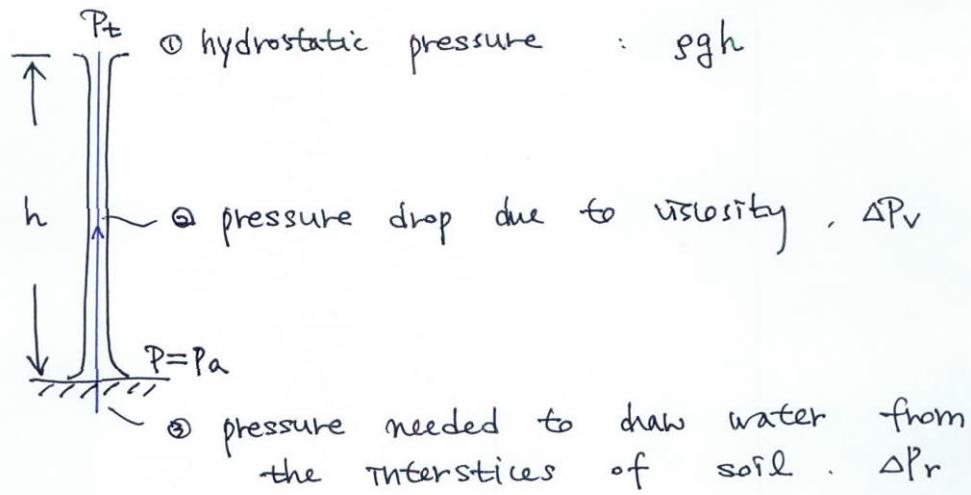
(2) Do real systems really follow Murray's law?

almost yes. Table 14.1

except arterioles and capillaries
(flow profile not parabolic)

§ The ascent of sap in trees

- sap : liquid that rises in the xylem from roots to leaves
- \leftrightarrow fluid in phloem (汁液)



$$P_t = P_a - \rho gh - \Delta P_v - \Delta P_r$$

for tall trees ($h = 100\text{m}$)

$$P_a = 1 \text{ atm}$$

$$\rho gh = 10 \text{ atm}$$

$$P_t \approx -80 \text{ atm} \quad (\text{absolute})$$

- driving pressure : $P_a - P_t \approx 80 \text{ atm}$
 \leftarrow evaporation of water in the interstices of leaves

if $U_{\text{say}} = 0.1 \text{ m/s}$

$d_{\text{xylem}} = 0.25 \text{ mm}$

$$\frac{\Delta p_{\text{ideal}}}{L} = \frac{8\mu U}{a^2} = \frac{8(10^{-3})(0.1)}{(0.125 \times 10^{-3})^2} = 51.2 \text{ kPa/m}$$

$$\frac{\Delta p_{\text{real}}}{L} = (0.7)^{-1} \frac{\Delta p_{\text{ideal}}}{L} = 73 \text{ kPa/m} \neq 7.3 \text{ kPa/m} \quad (\text{in textbook})$$

Chap. 15. Flow at very low Reynolds numbers

- creeping flow

N.-S. eq.

$$0 = -\nabla p + \mu \nabla^2 \bar{u} : \text{Stokes eq}$$

e.g. microscopic organisms
proteins, cells, DNA, ...

- characteristics

- ① reversible
- ② mixing extremely difficult
- ③ significant wall effect

- propulsion slow

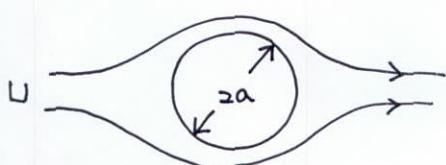
$$\text{Drag} \sim L^2$$

$$\text{Thrust} \sim \text{volume} \sim L^3 \quad (\text{engine size})$$

$$\frac{T}{D} \sim L \quad \downarrow \text{as } L \downarrow$$

§ Drag

(1) Spheres



$$D = 6\pi\mu U a \quad (Re < 1)$$

Stokes' law