

NanoBio Integration for Medical Innovation

-Targeting Therapy by Supramolecular Nanodevices-

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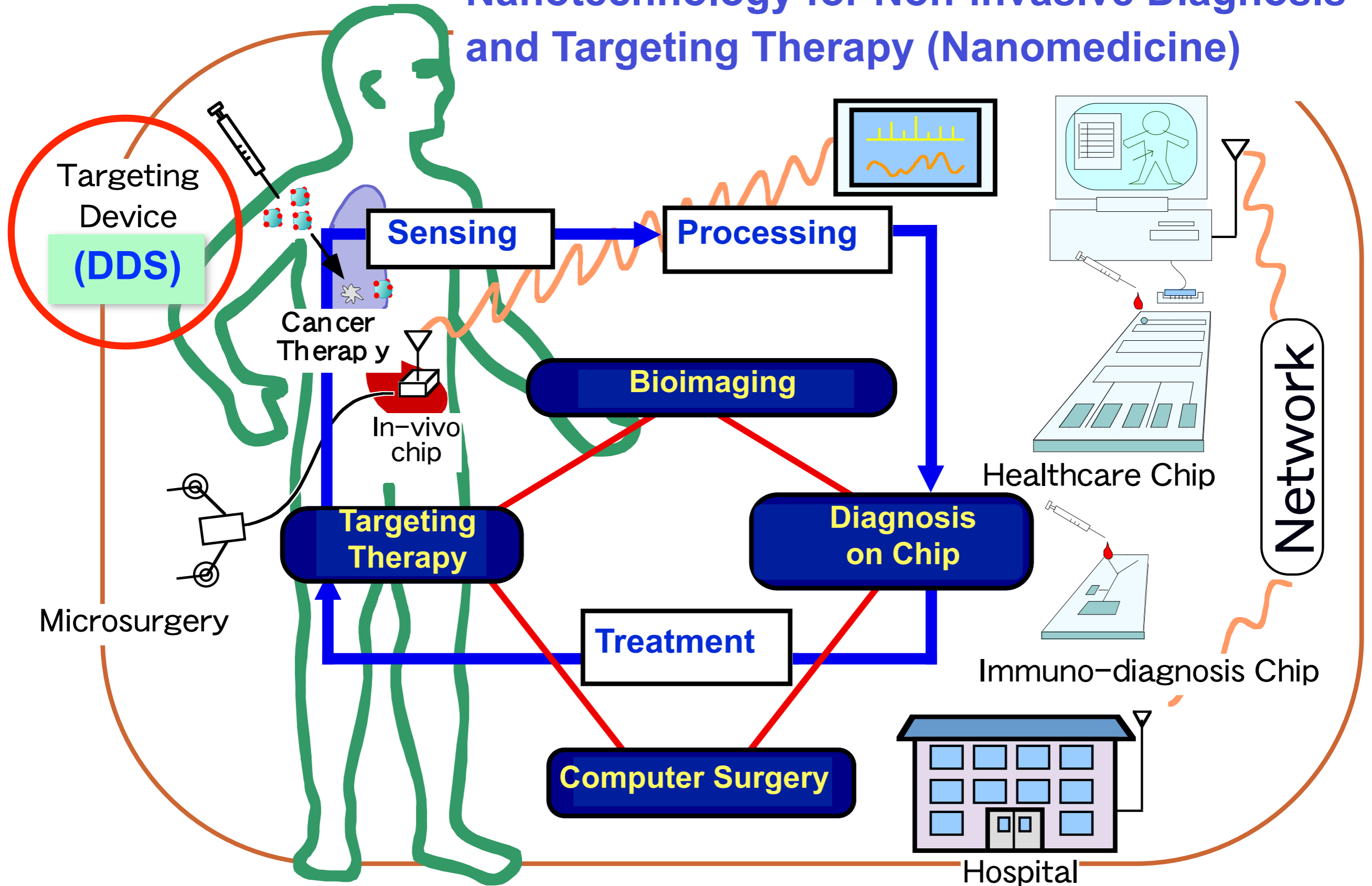
November 25, 2009

UT-SNU Exchange Lecture Course

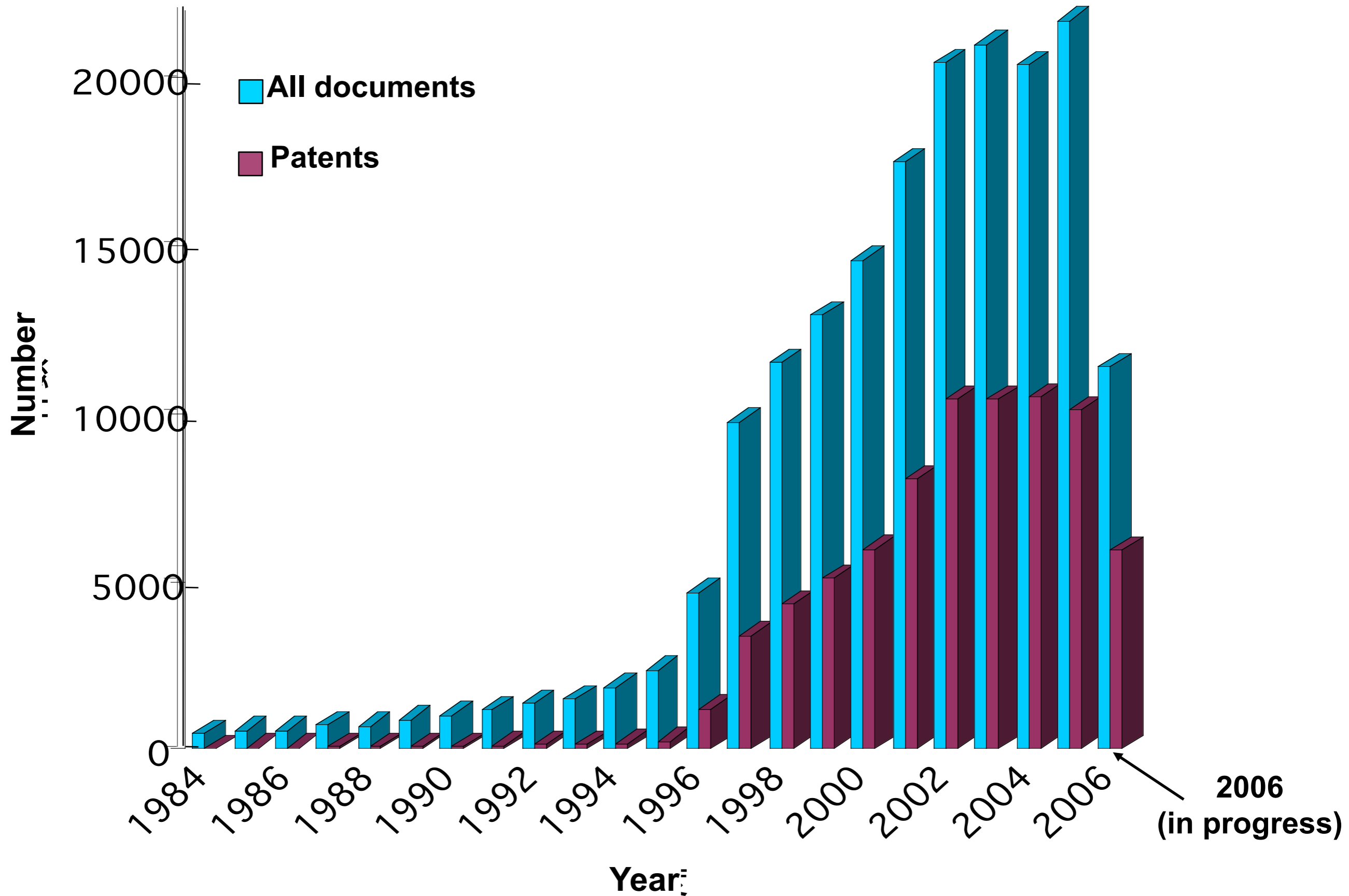
Introduction to Bioengineering



Nanotechnology for Non-invasive Diagnosis and Targeting Therapy (Nanomedicine)

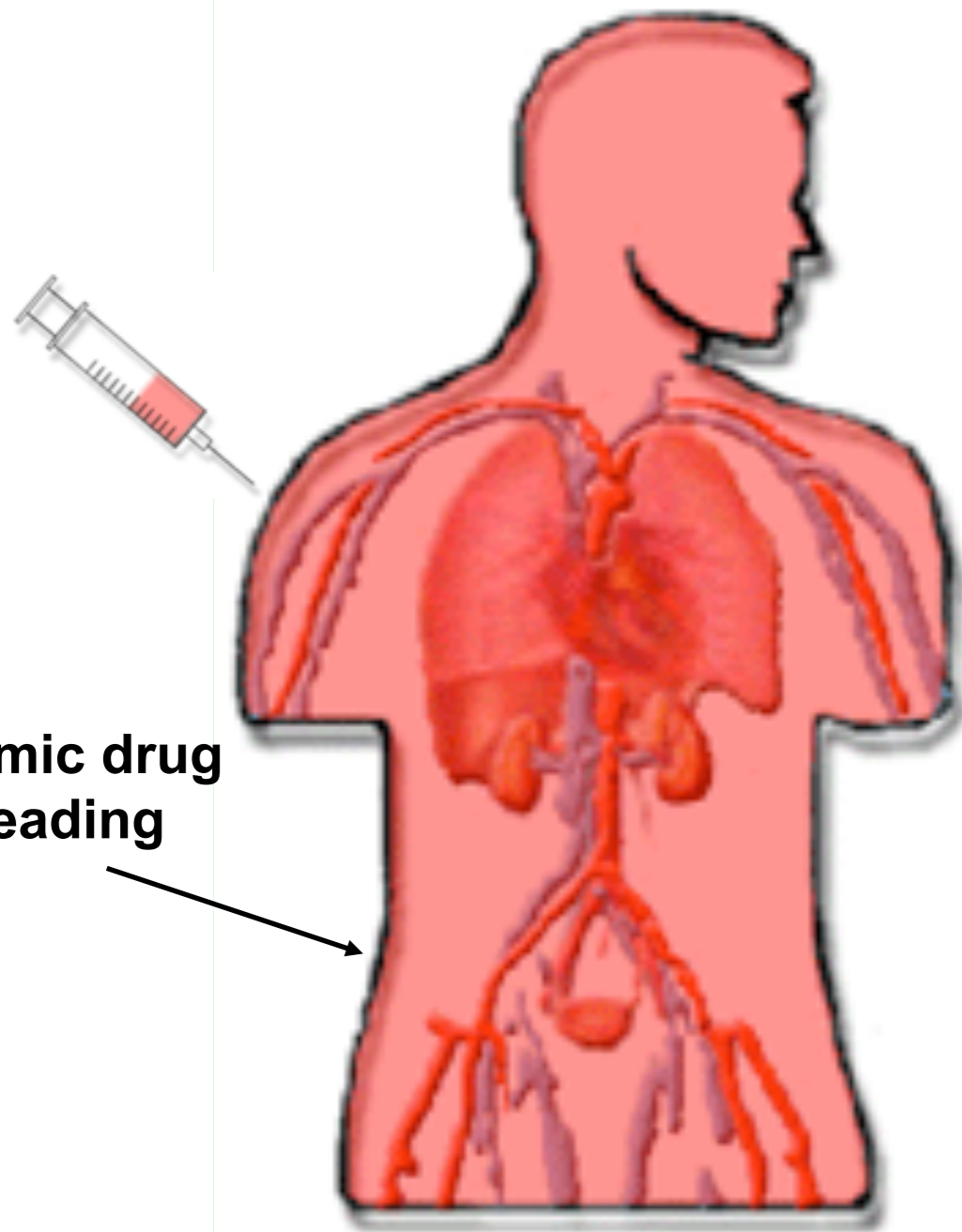


Number of scientific papers and patents related to DDS



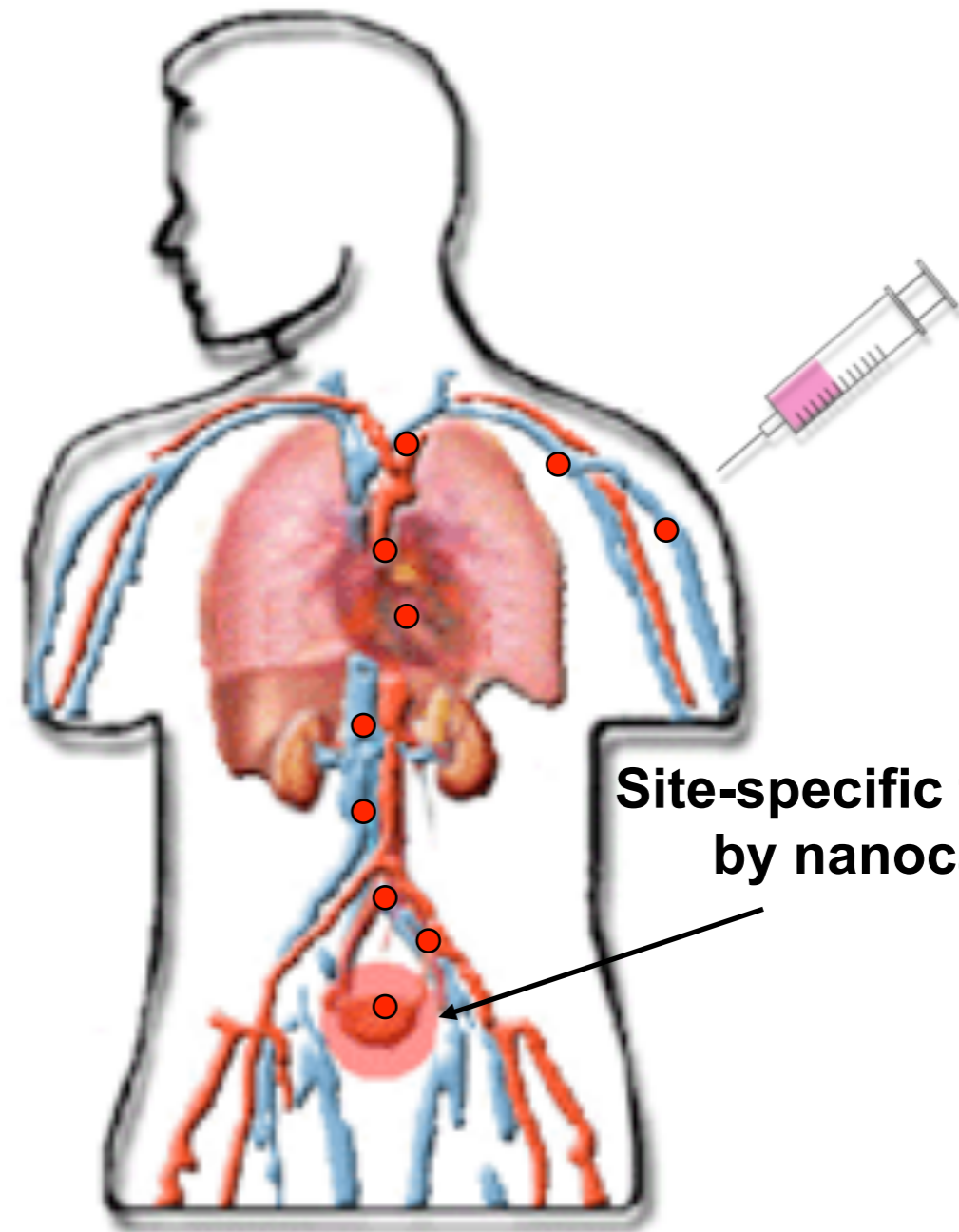
*Source: SciFinder

Targeting Therapy by Nanotechnology-based Medicine



Systemic drug spreading

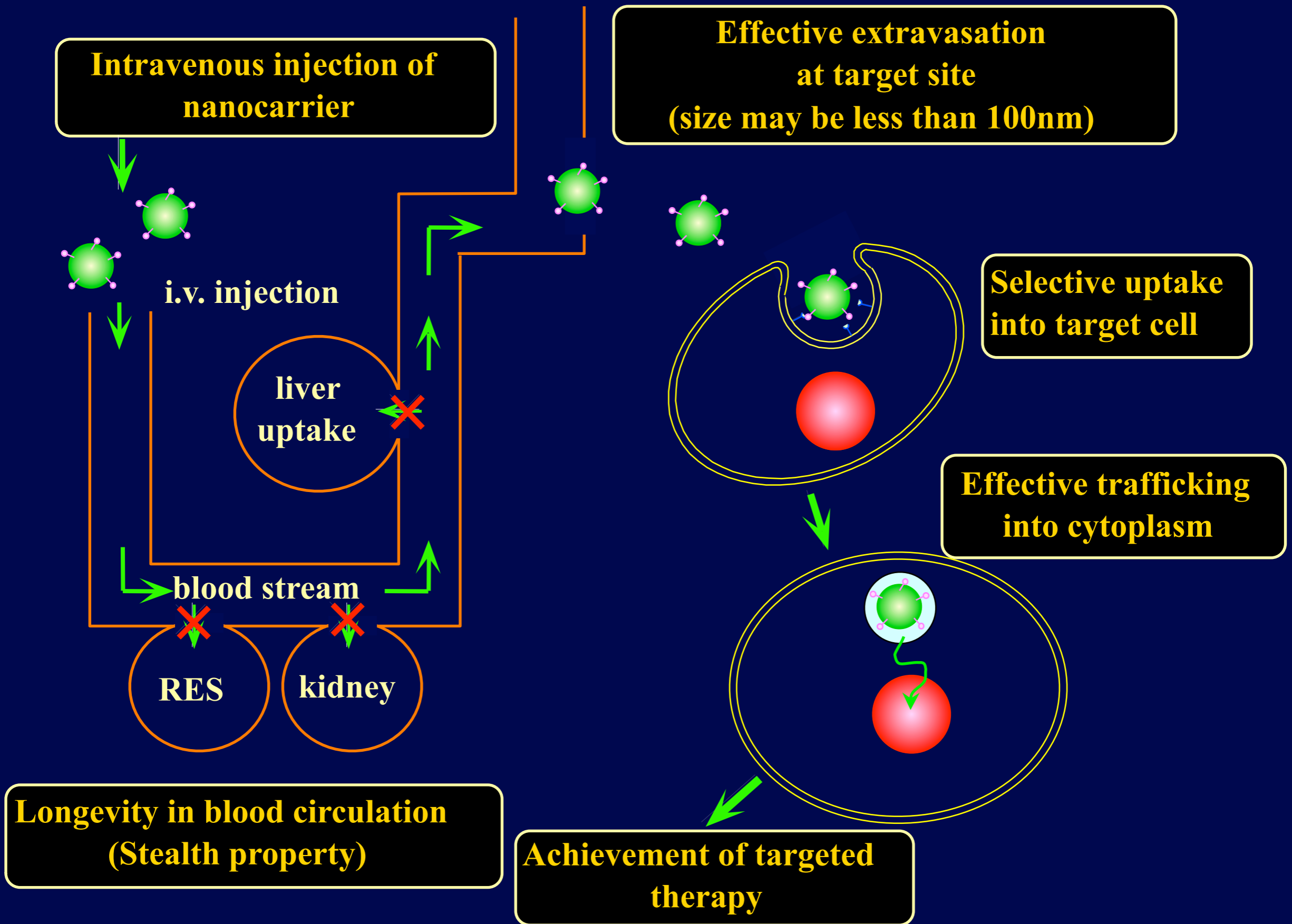
General Chemotherapy



Site-specific targeting by nanocarrier

Targeting Therapy

Itinerary of intravenously-injected nanocarriers



Structural Design of Polymeric Micelles for DDS

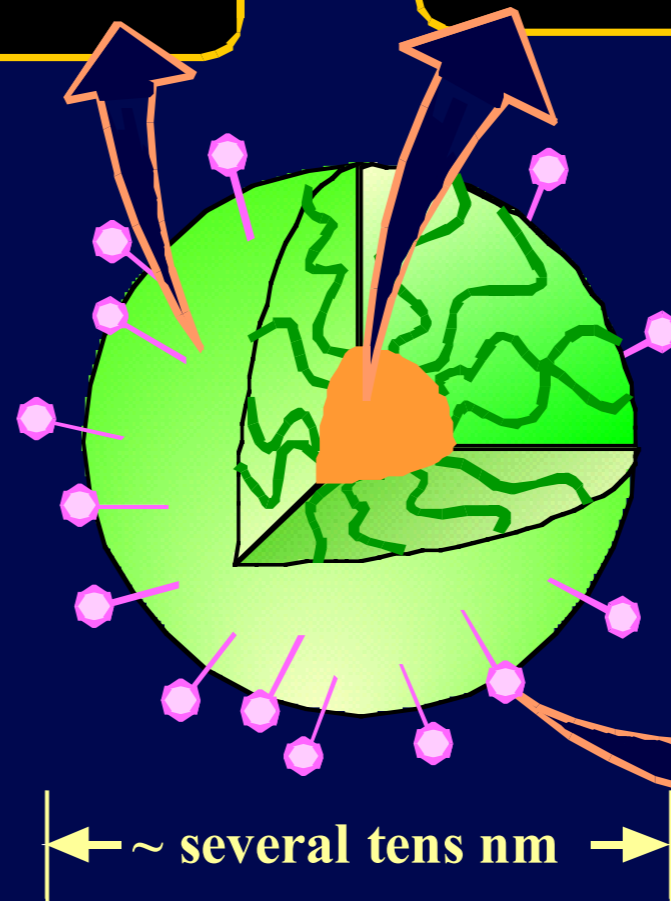
Hydrophilic outer shell composed of flexible tethered polymer strands
→ **Biocompatibility**

Core segregated from outer environment
→ **Drug reservoir**

Multi-molecular association in aqueous milieu
(association number: $\sim 10^2$)

Formation of polymeric micelle with core-shell architecture

Amphiphilic block copolymer



Introduction of multi-ligands on micelle periphery
→ **Targetability**

Uniform size with a range comparable to viruses
→ **High extravasating ability**

Structural Design of Polymeric Micelles for DDS

Hydrophilic outer shell composed of flexible tethered polymer strands
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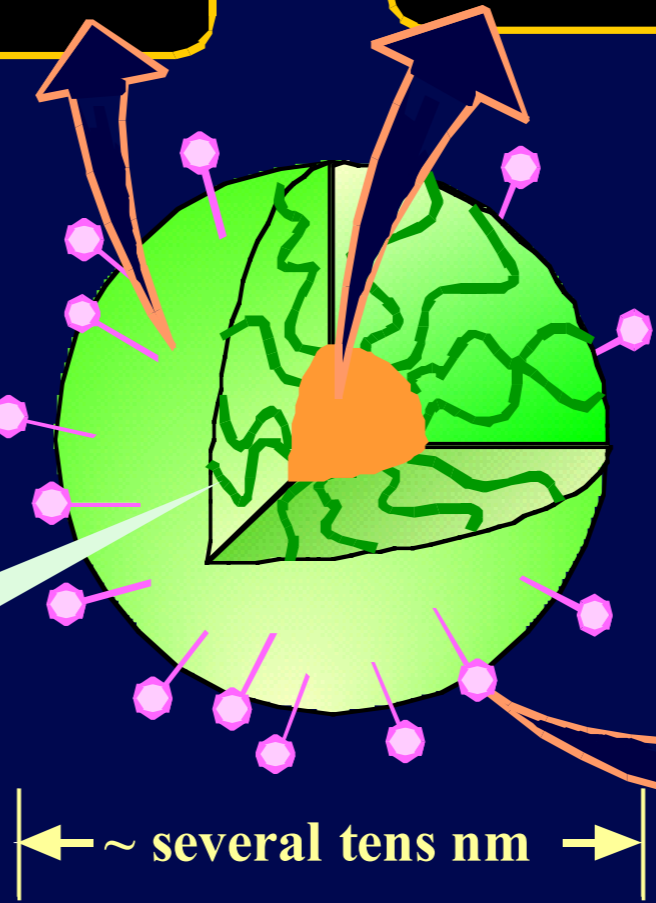
Formation of polymeric micelle with core-shell architecture

$-(\text{CH}_2\text{CH}_2\text{O})_n-$
Poly(ethylene glycol)

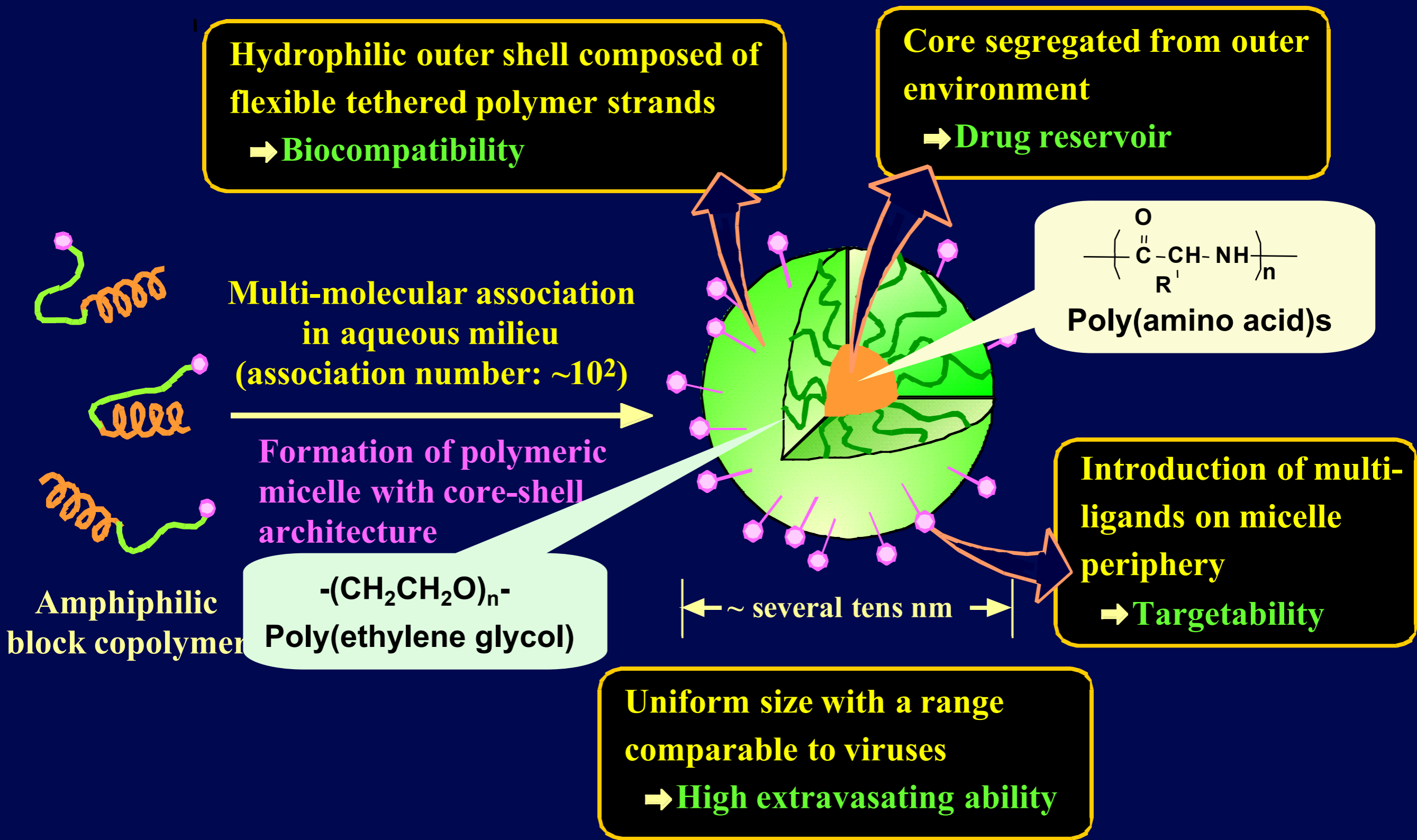
Amphiphilic block copolymer

Uniform size with a range comparable to viruses
→ **High extravasating ability**

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→ **Targetability**

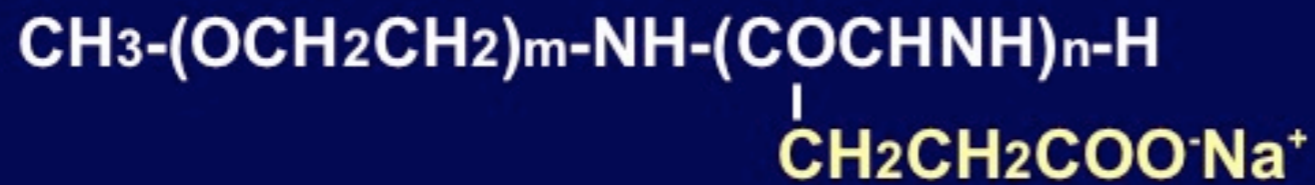


Structural Design of Polymeric Micelles for DDS

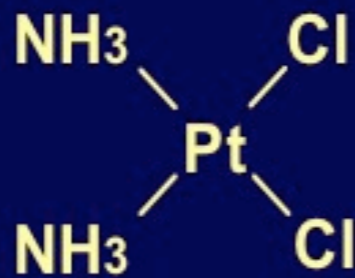


M. Yokoyama, K. Kataoka, et al, *J. Contrl. Rel.* 11, 269 (1990); K. Kataoka, G. S. Kwon et al, *J. Contrl. Rel.* 24, 119 (1993); G. S. Kwon, K. Kataoka, et al, *J. Contrl. Rel.* 29, 17 (1994); A. Harada, K. Kataoka, *Science* 283, 65 (1999)

Preparation of cisplatin (CDDP)-incorporated polymeric micelles

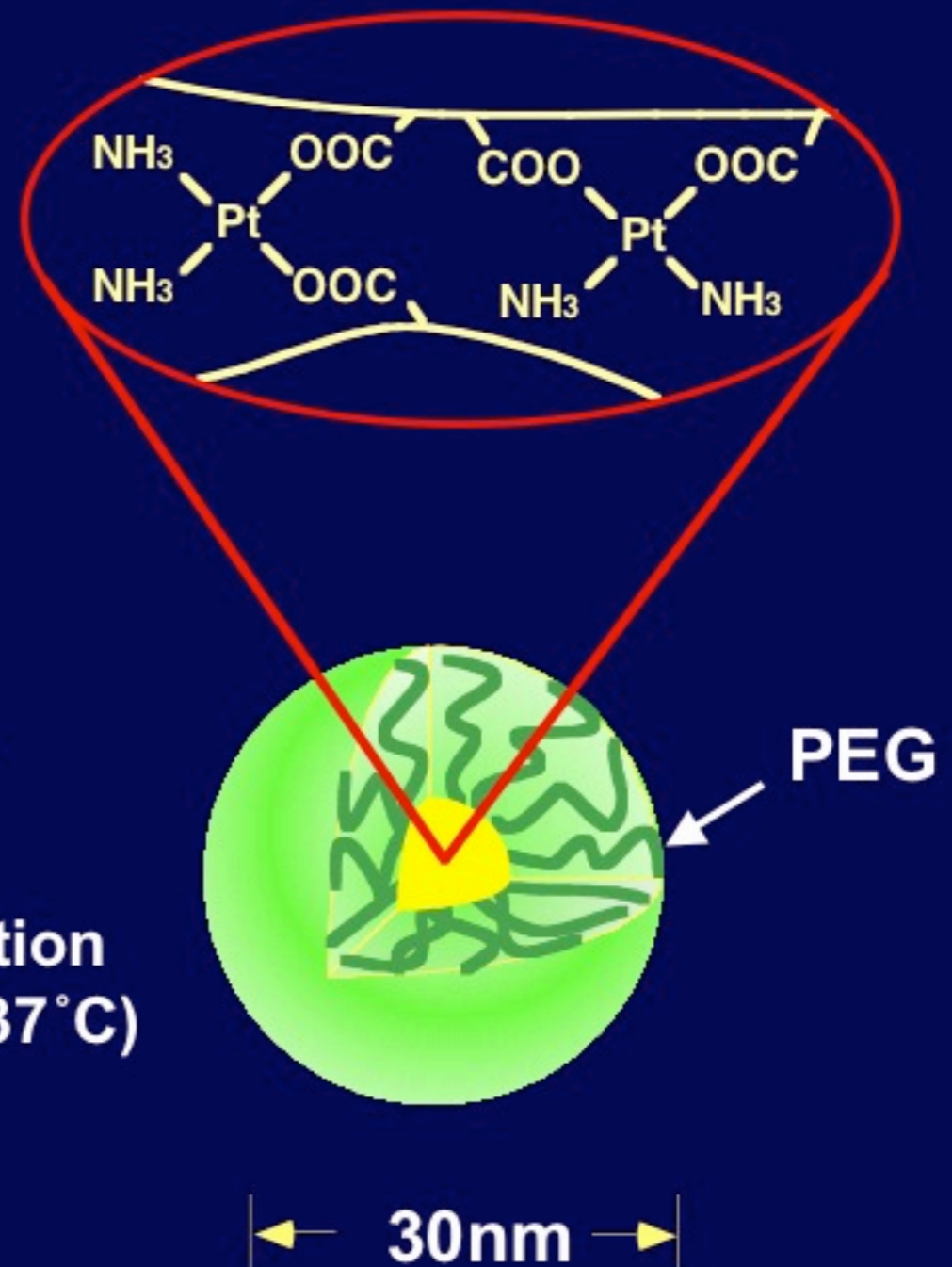


PEG-P(Glu)



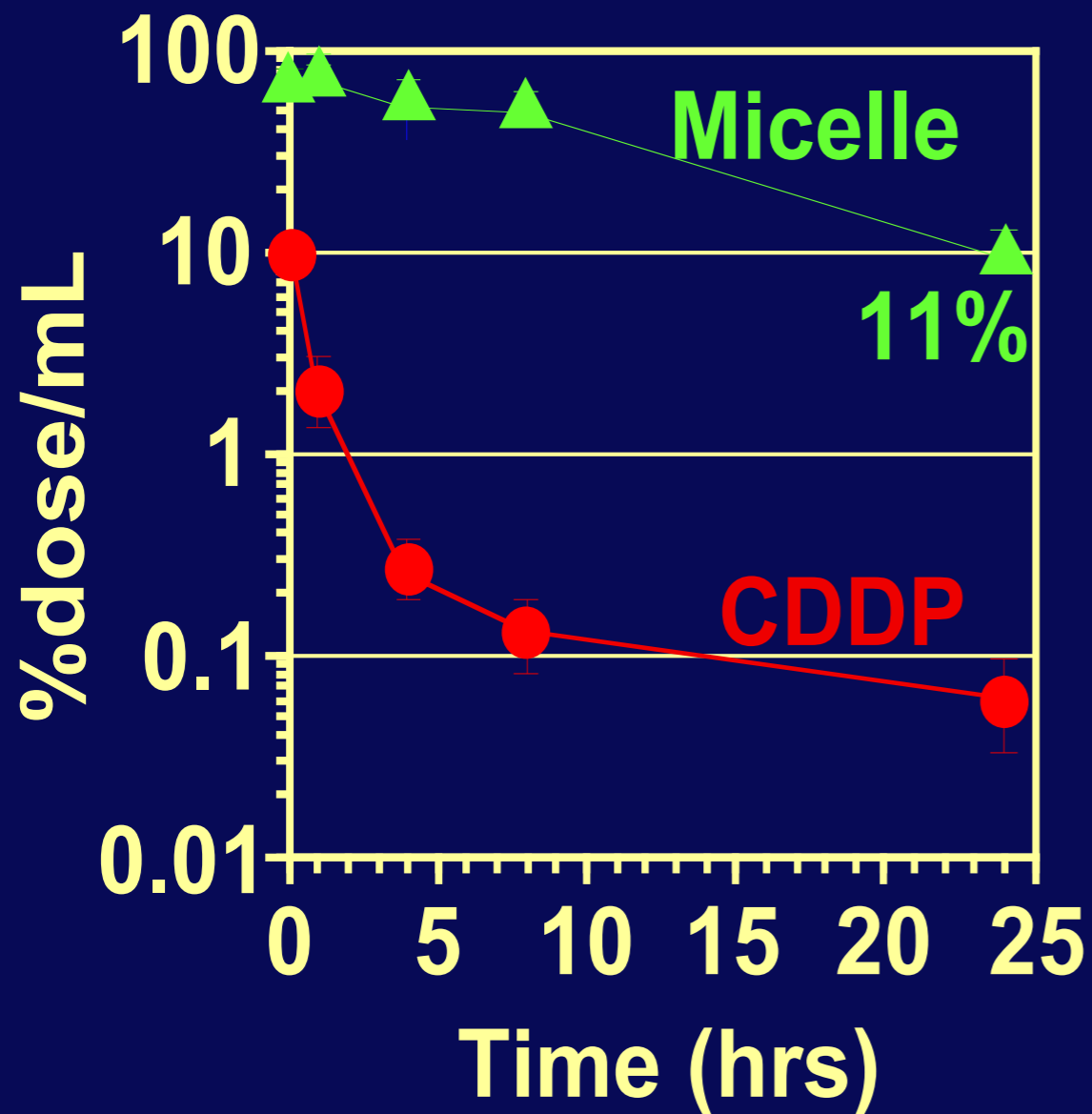
CDDP

self-association
(in water at 37 °C)

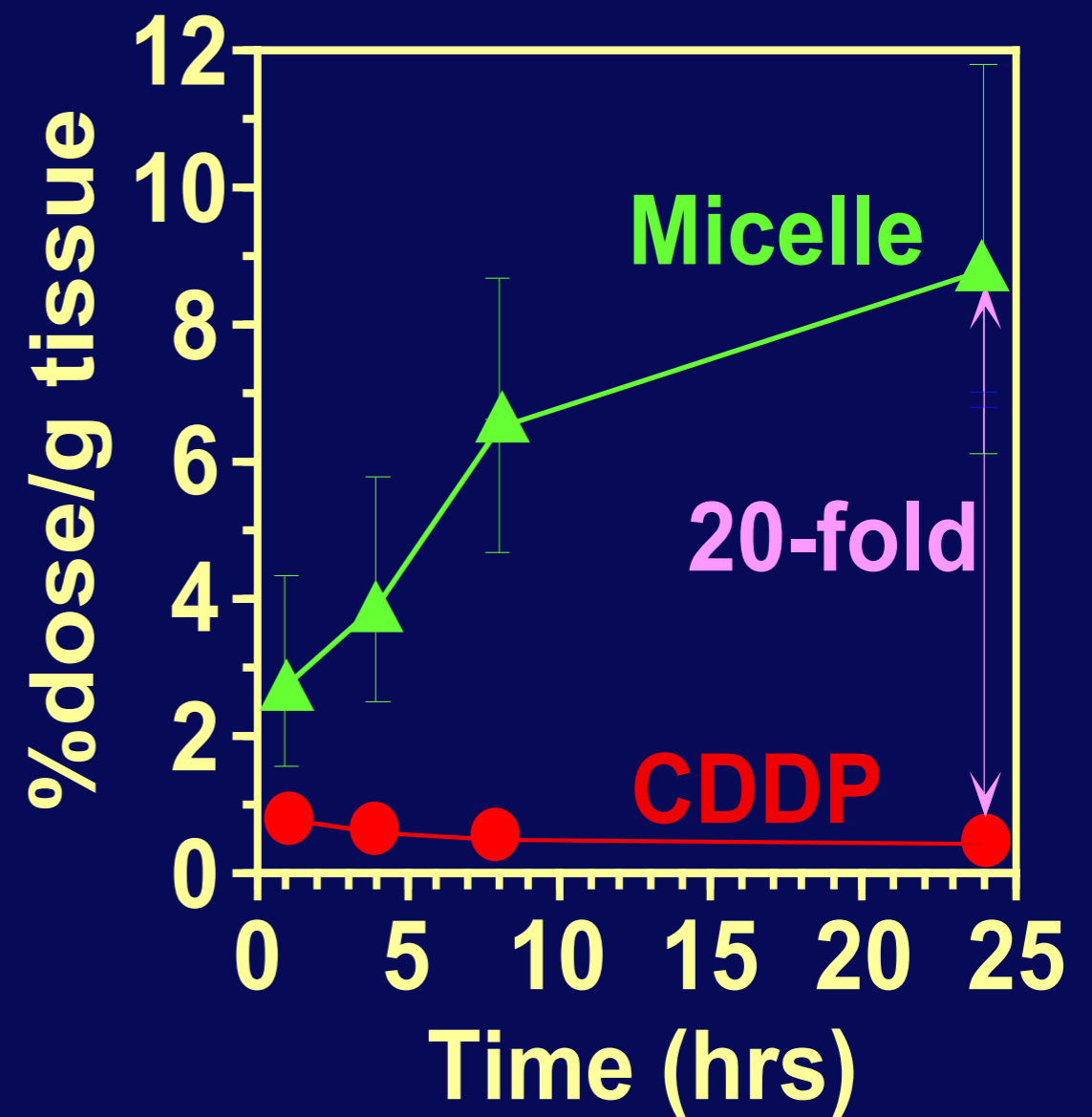


Biodistribution of CDDP-incorporated micelles

Plasma Pt concentration

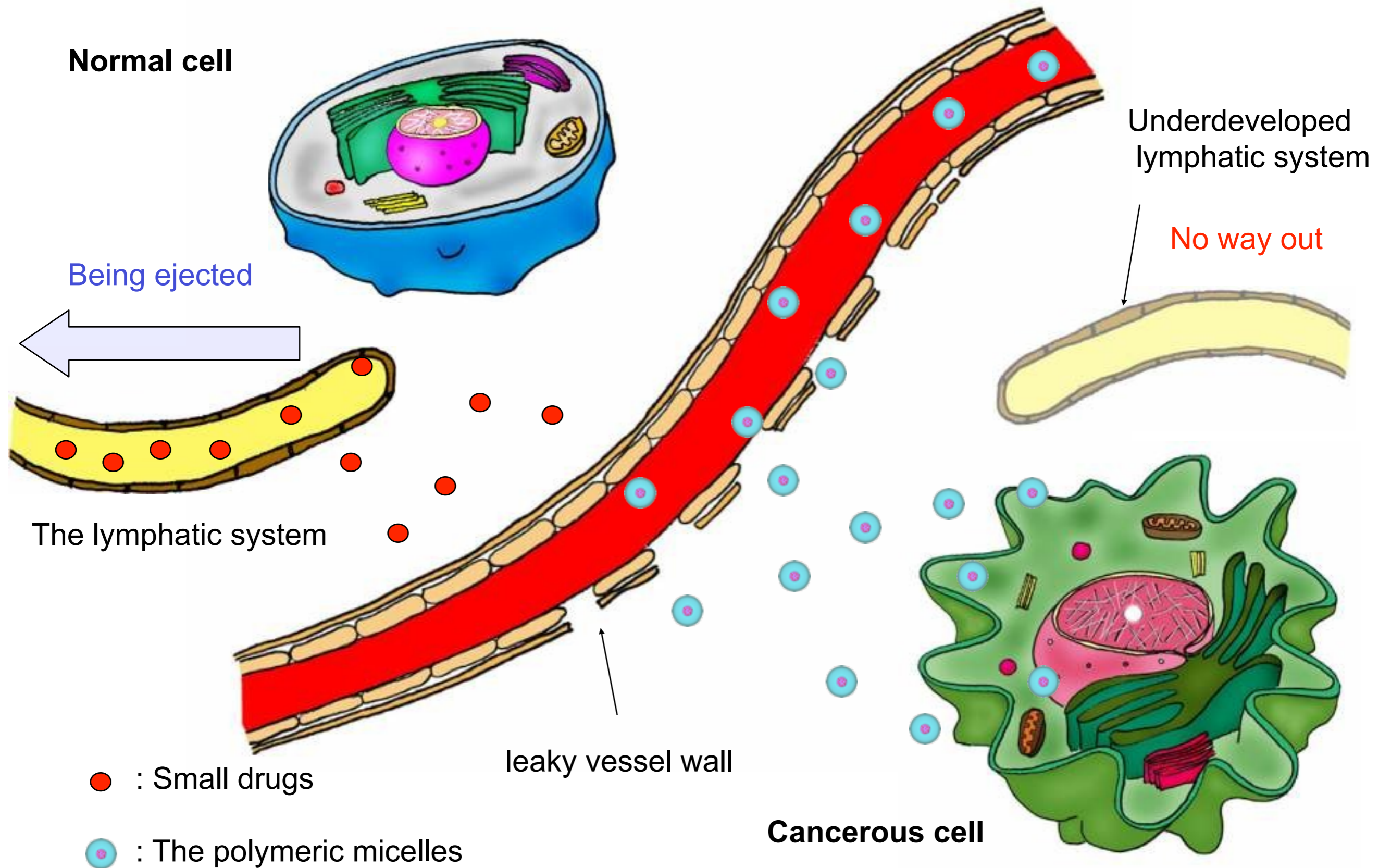


Tumor accumulation



CDDP and CDDP-incorporated micelles were administered i.v. to Lewis lung carcinoma (LLC)-bearing C57BL6N mice (male, 6 week old, n=4)

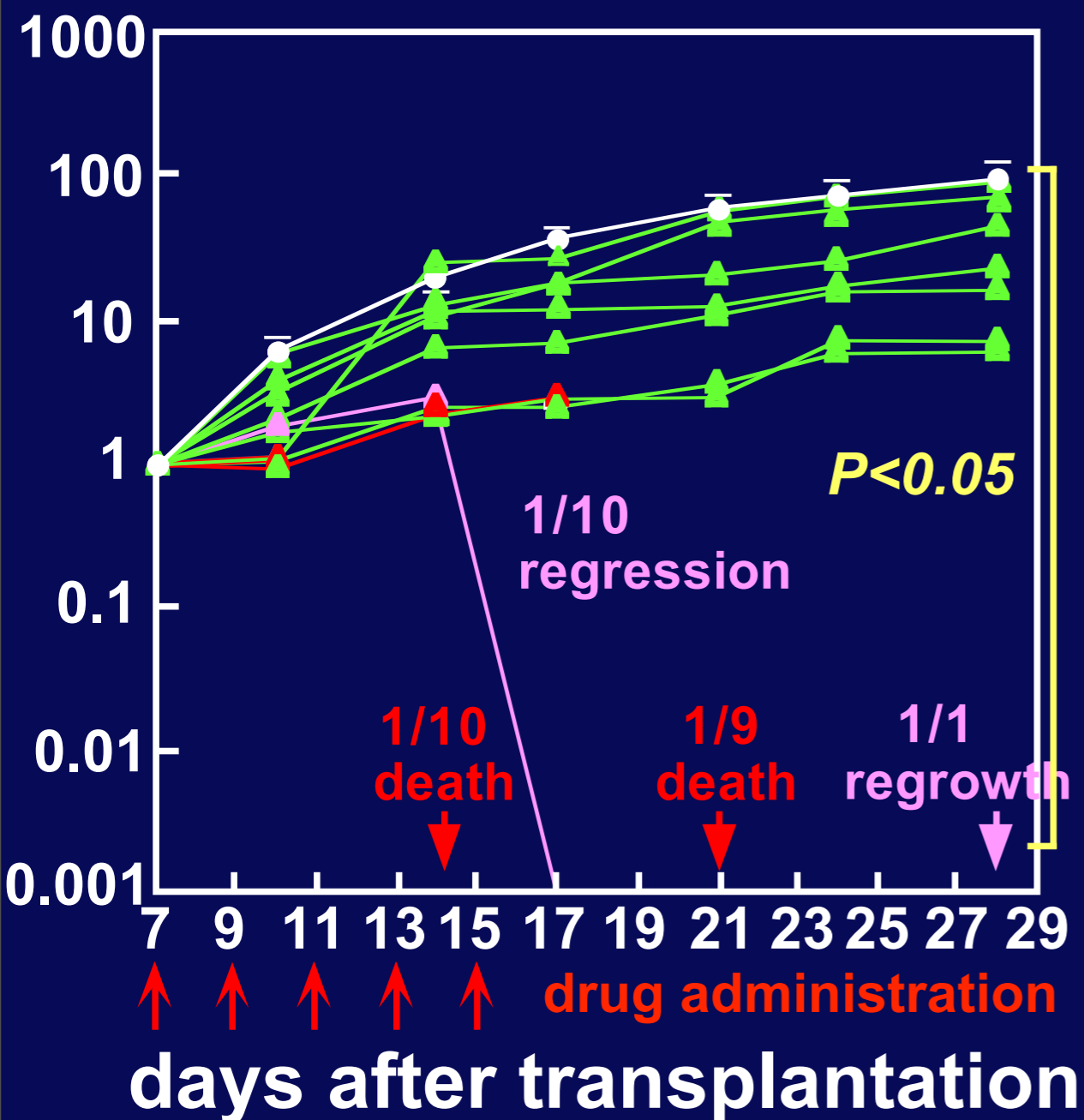
Enhanced Permeability and Retention(EPR) Effect



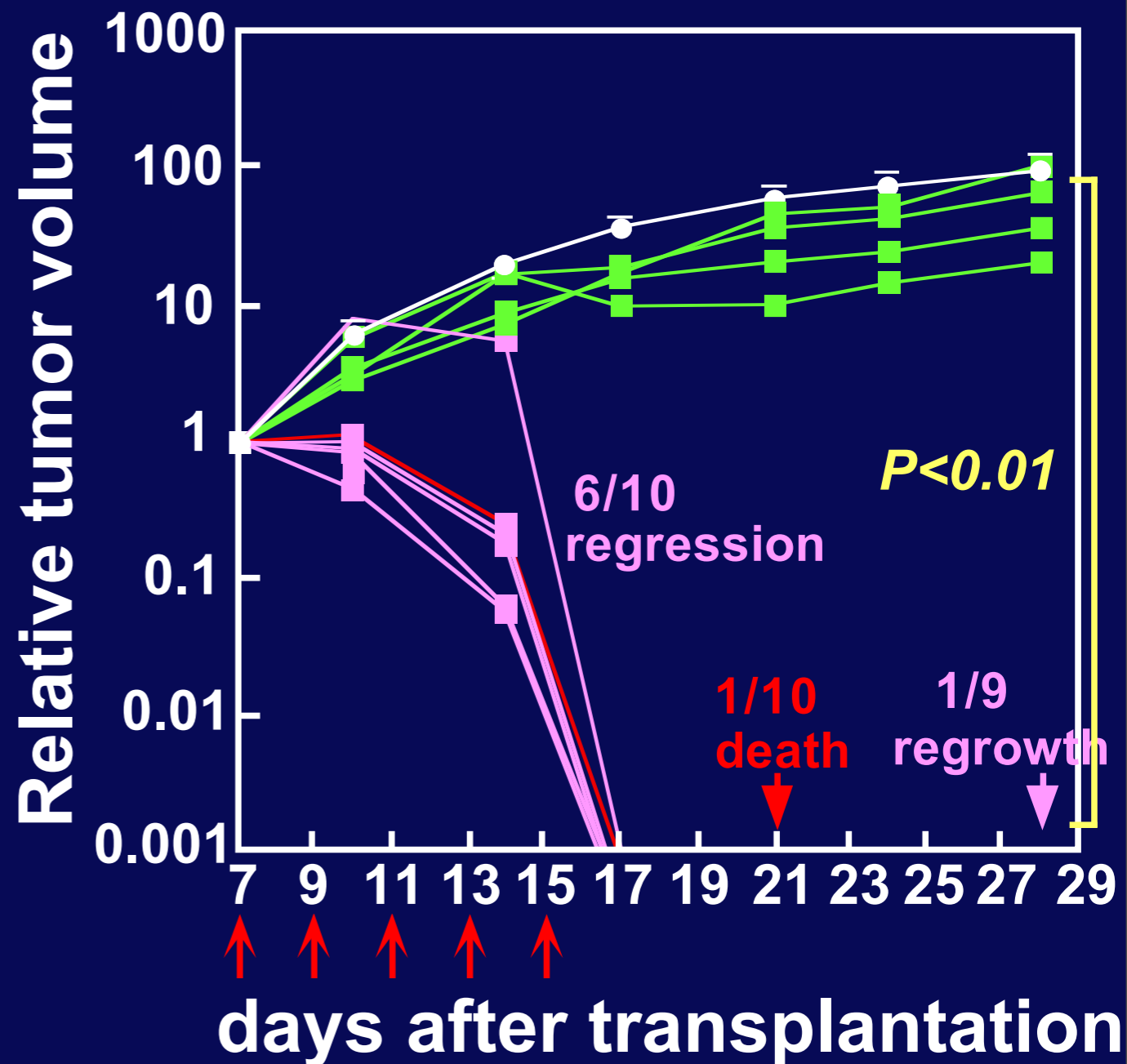
Anti-tumor activity of CDDP-incorporated micelles

Colon 26-bearing CDF₁ mice (female, 6 week old, n=10) were treated 5 times with CDDP and CDDP-incorporated micelle (4mg/kg/day).

CDDP 4mg/kg/day

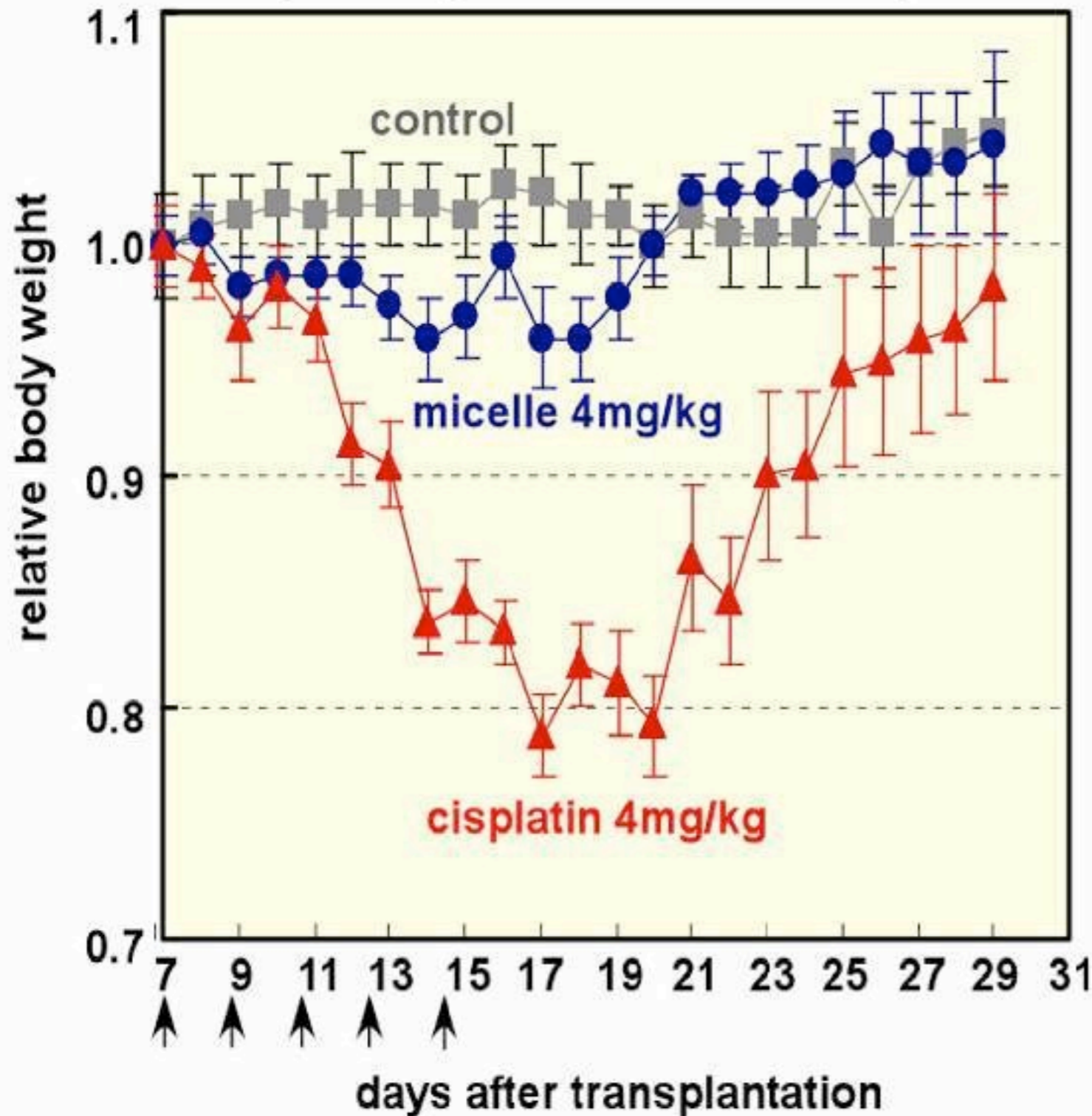


Micelles 4mg/kg/day



Change in body weight of mice treated with cisplatin and PEG-P(Glu(CDDP)) (12-60) micelles

(Data are presented as mean \pm SE.)



Decrease in body weight

cisplatin 20%

micelle 5%

Disappearance of primary tumor

control 0/10

cisplatin 0/8

micelle 4/9

PEG-P(Glu(CDDP)) (12-60) micelles achieved lower toxicity and higher antitumor activity than same dose of cisplatin.

Polymeric Micelles from PEG-poly(amino acid) Block Copolymers in Clinical Development

Adriamycin (NK911:Nippon Kayaku Co.) :

Phase II Clinical Trial

Paclitaxel (NK105:NanoCarrier Co./Nippon Kayaku Co.) :

Phase II Clinical Trial

Cisplatin (NC6004:NanoCarrier Co.) :

Phase I/II Clinical Trial

Camptothecine derivative (SN-38) (NK012:Nippon Kayaku Co.) :

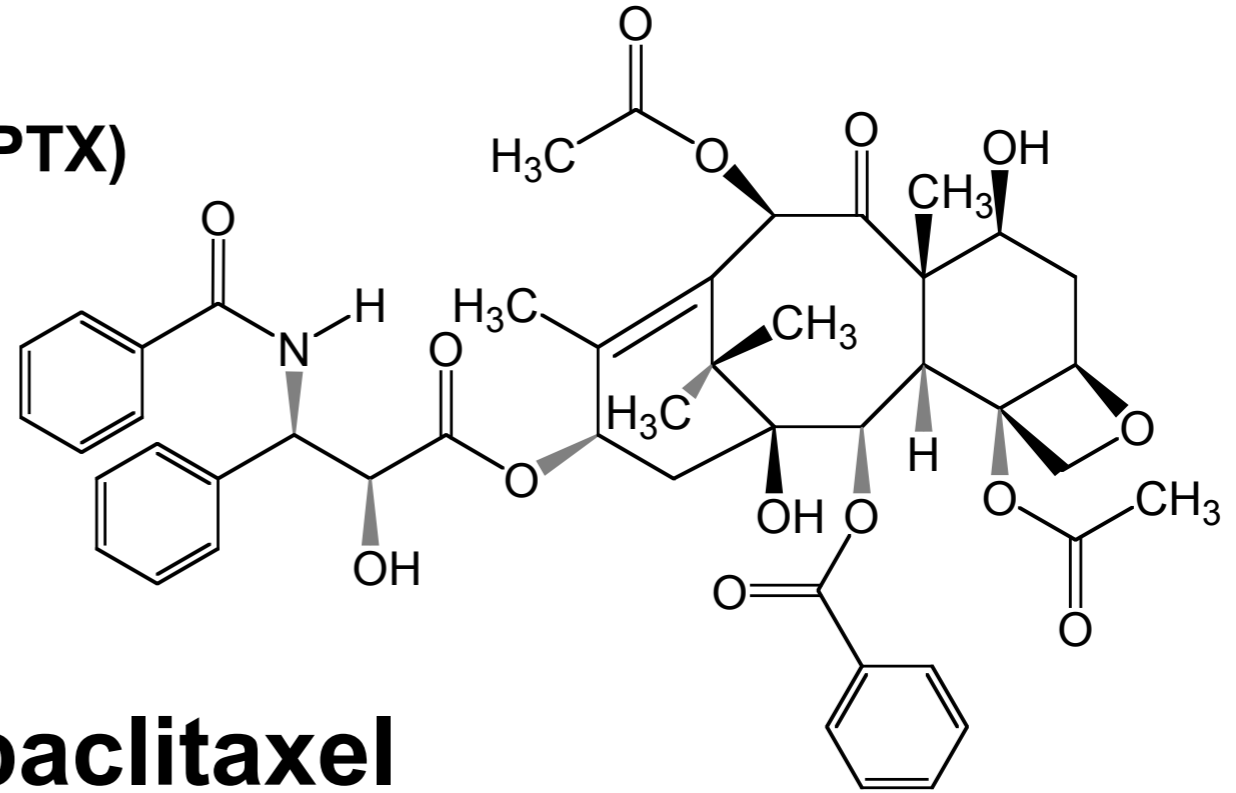
Phase I Clinical Trial

Dachplatin (NC4016/ND-1:NanoCarrier Co./Debio Pharm Co.) :

Phase I Clinical Trial

Preparation of Paclitaxel-loaded Polymeric Micelle (NK105)

Structure of paclitaxel (PTX)



Preparation of the micellar paclitaxel

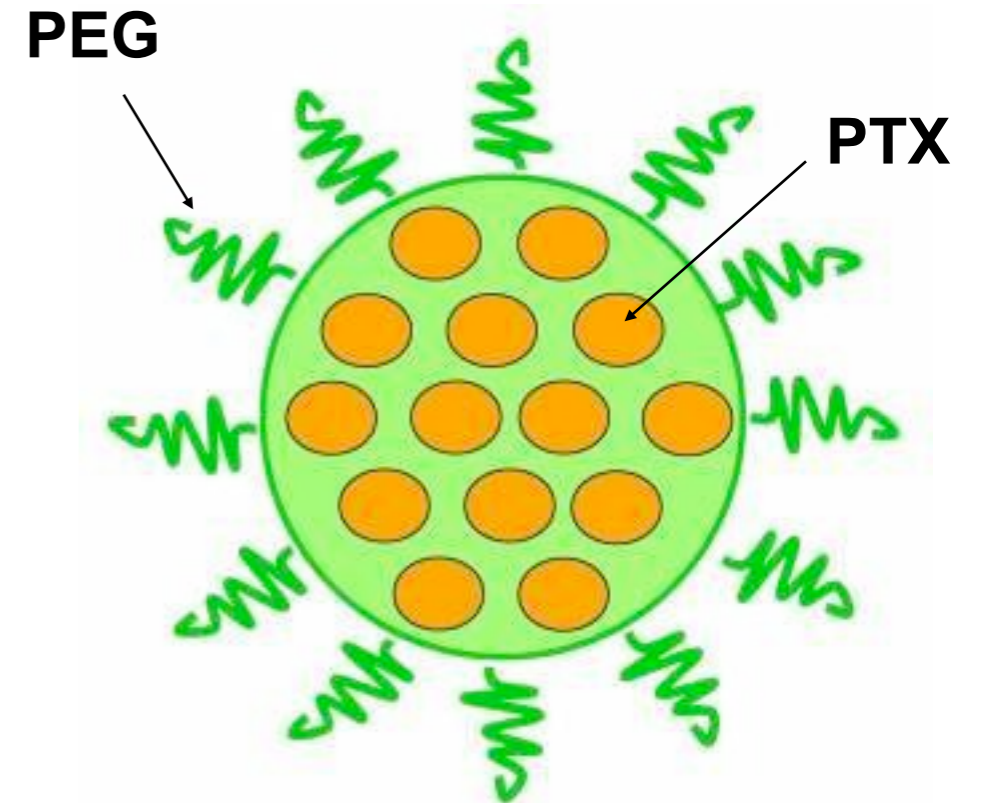
PEG-Hydrophobically modified poly(amino acid)
block copolymer

+ (Mixed in dichloromethane)

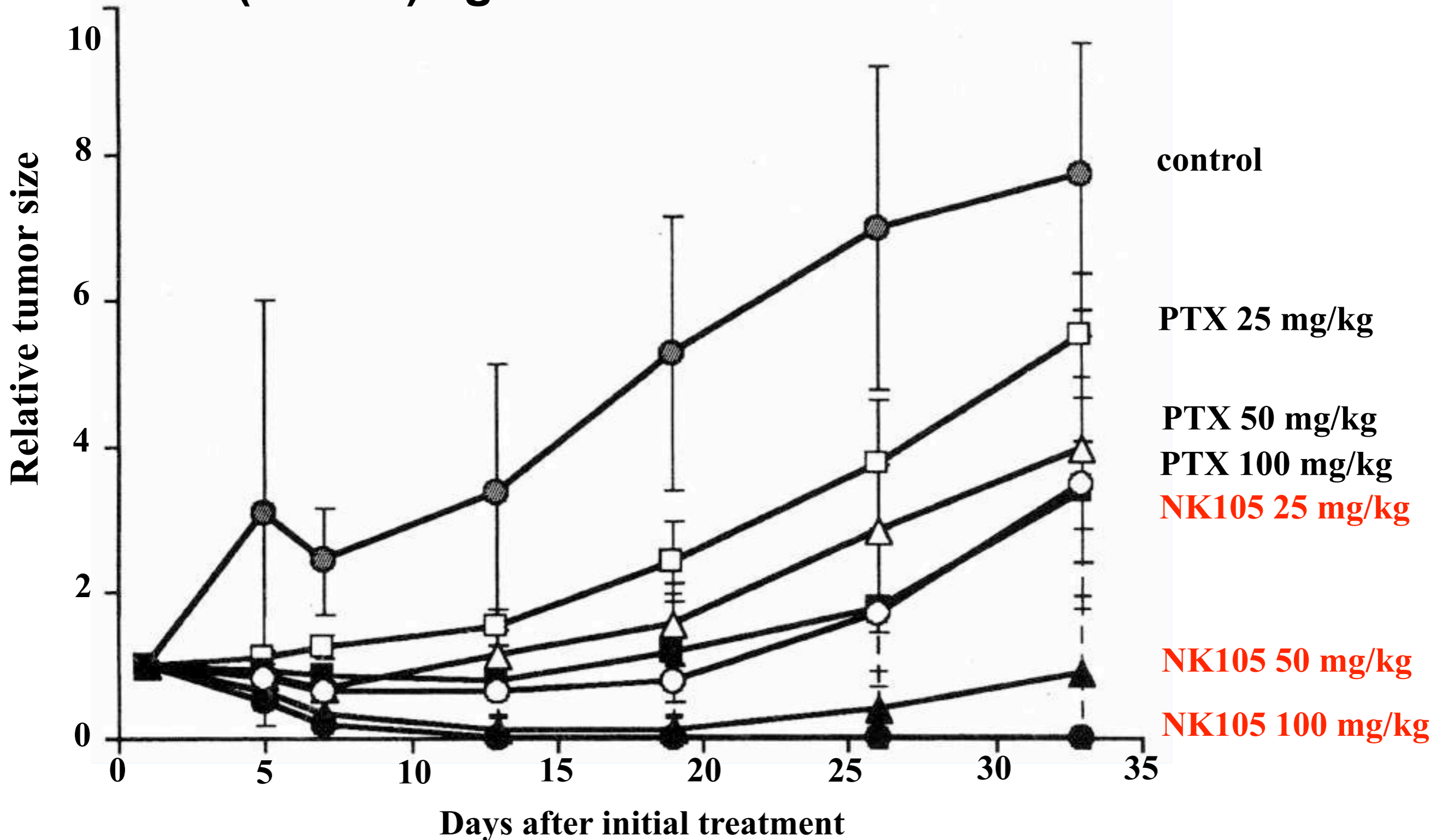
paclitaxel

↓ Emulsification
Evaporation

Micellar paclitaxel (NK105)

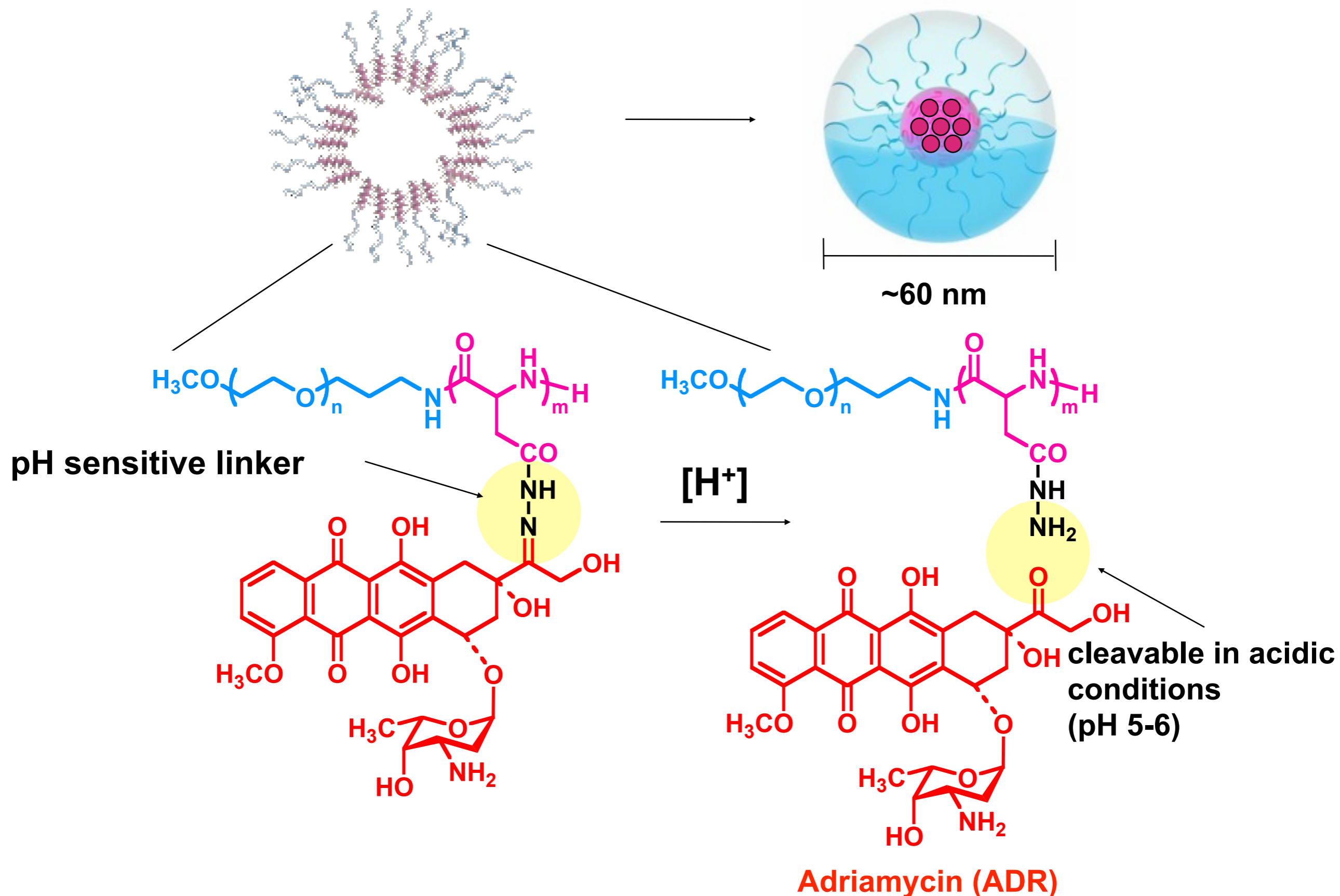


Anti-tumor activity of paclitaxel-loaded polymeric micelles (NK105) against HT-29 tumor in nude mice

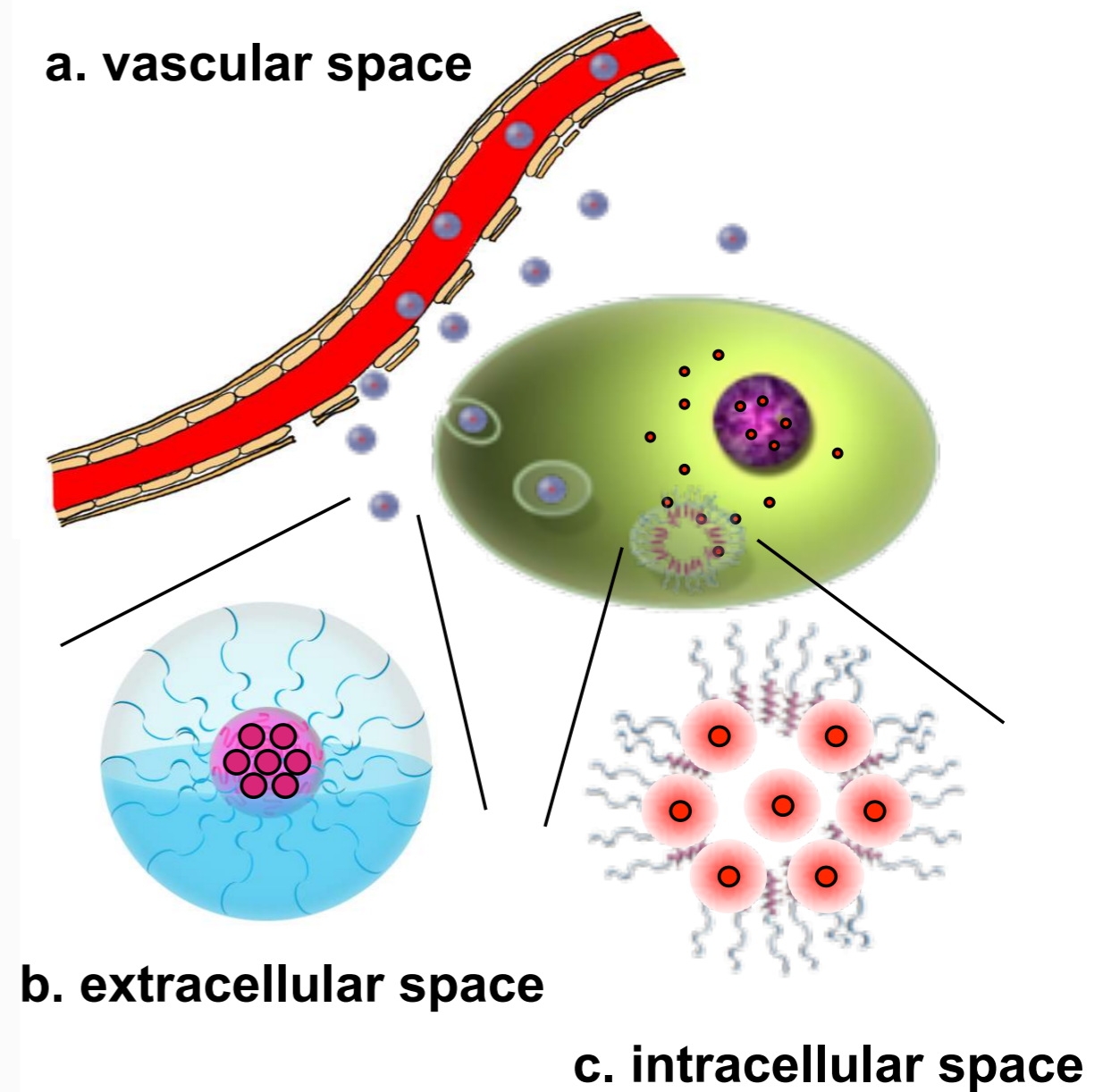
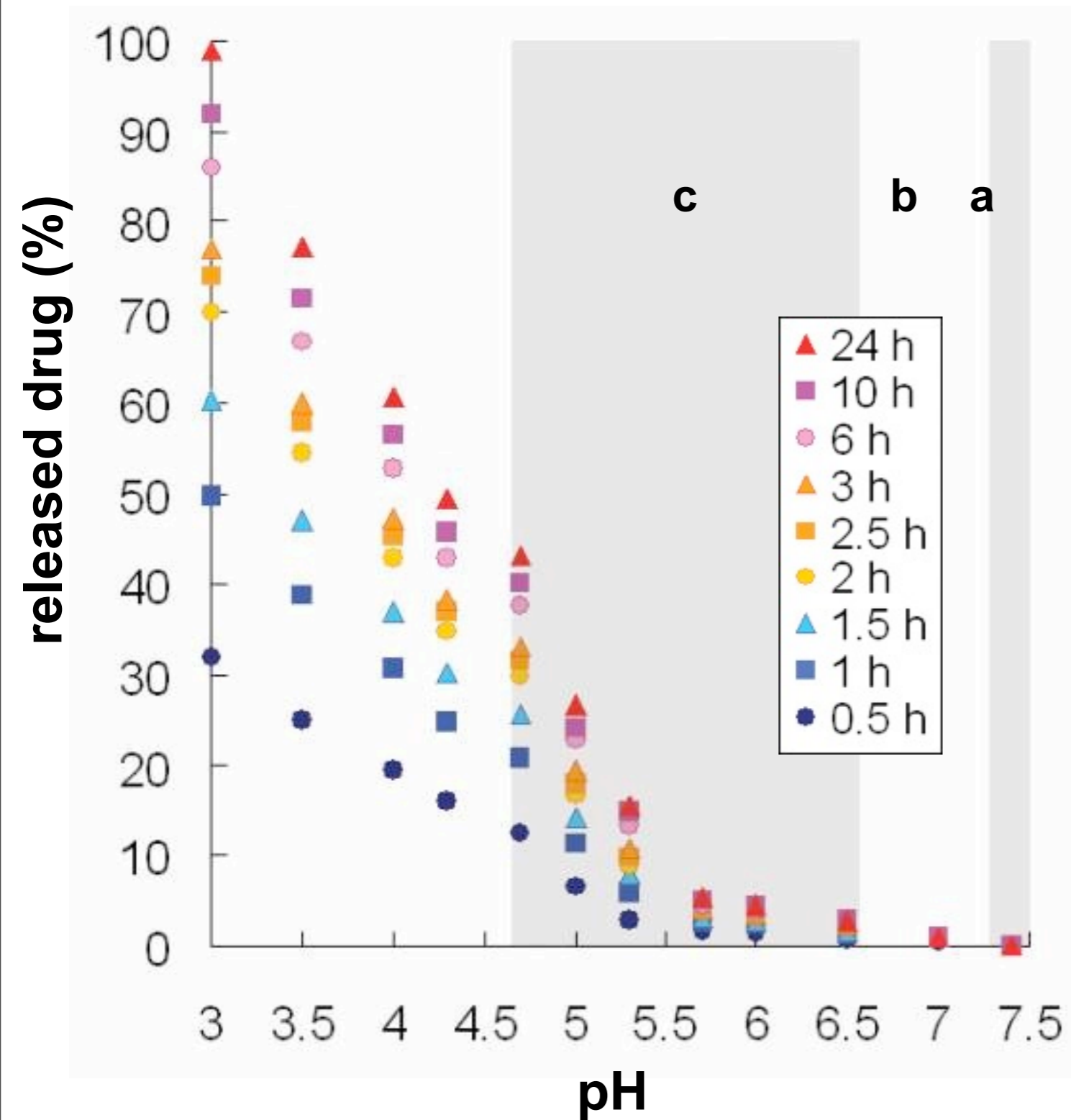


PTX (open) and NK105 (closed) were injected intravenously once weekly for 3 weeks at PTX-equivalent doses of 25, 50, and 100 mg/kg.

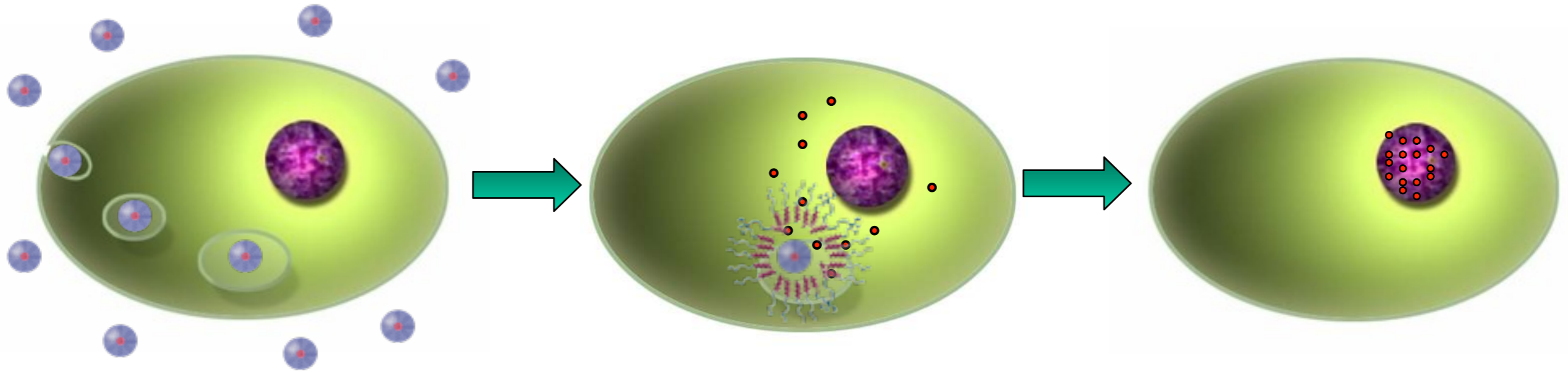
The pH-sensitive polymeric micelles



pH-sensitivity adjusted to intracellular endosomal space



Observation of intracellular drug release by fluorescence

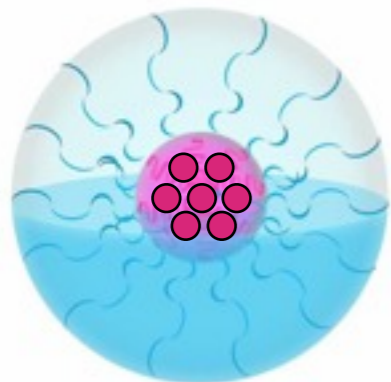


FL remains quenched as long as the micelles are stable

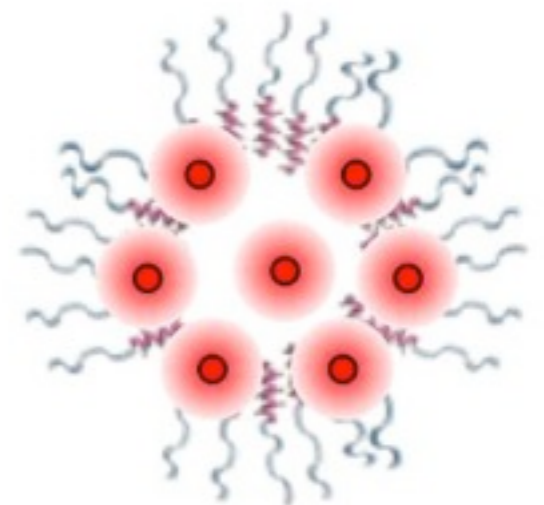
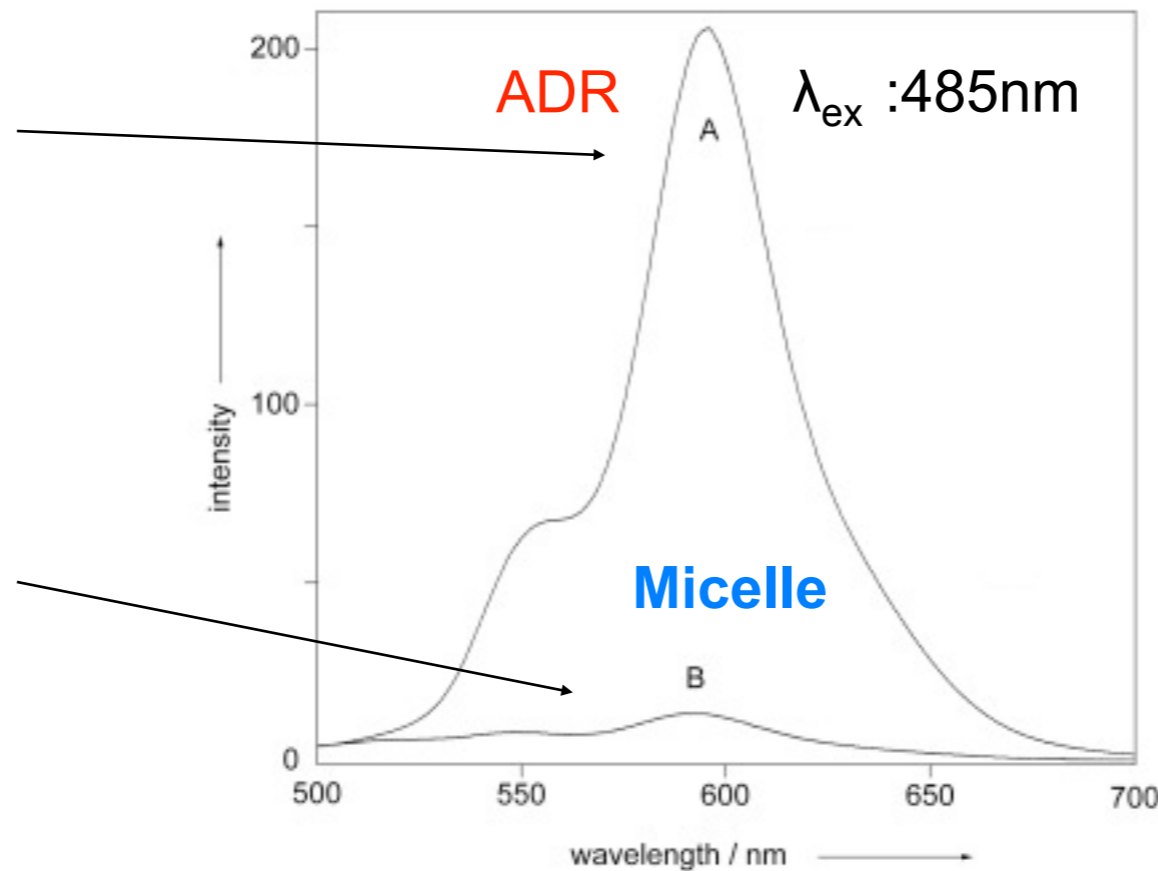
Intracellular localization and drug release of the micelles are detectable

We can expect fate of released drugs in the cell

ADR has intense FL

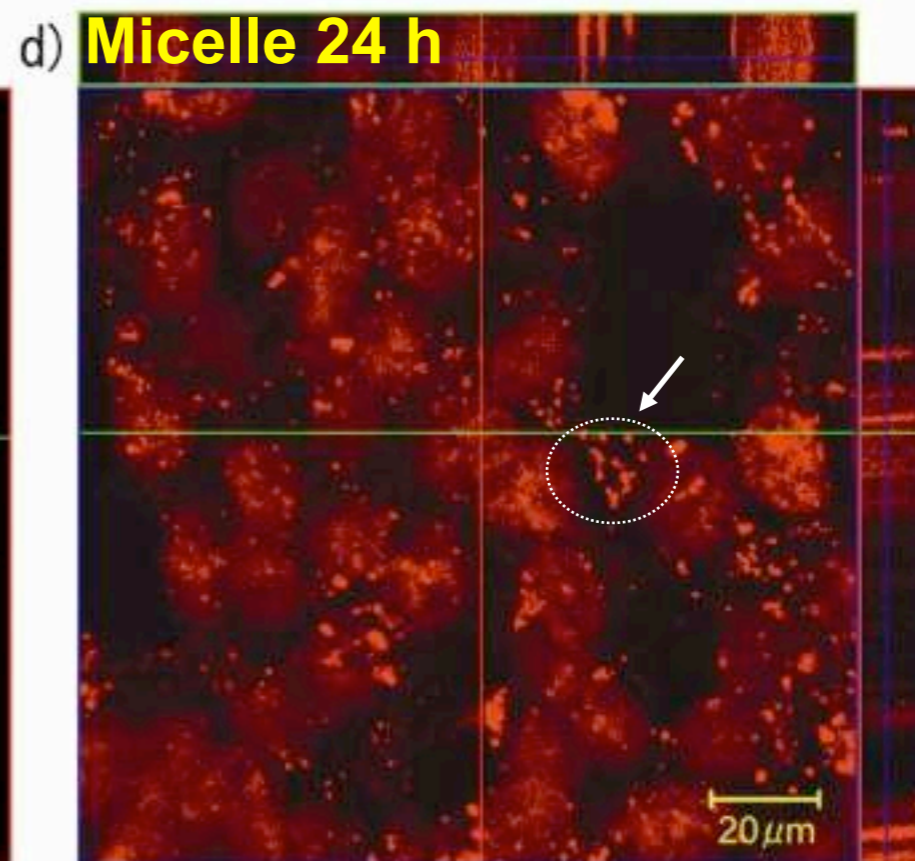
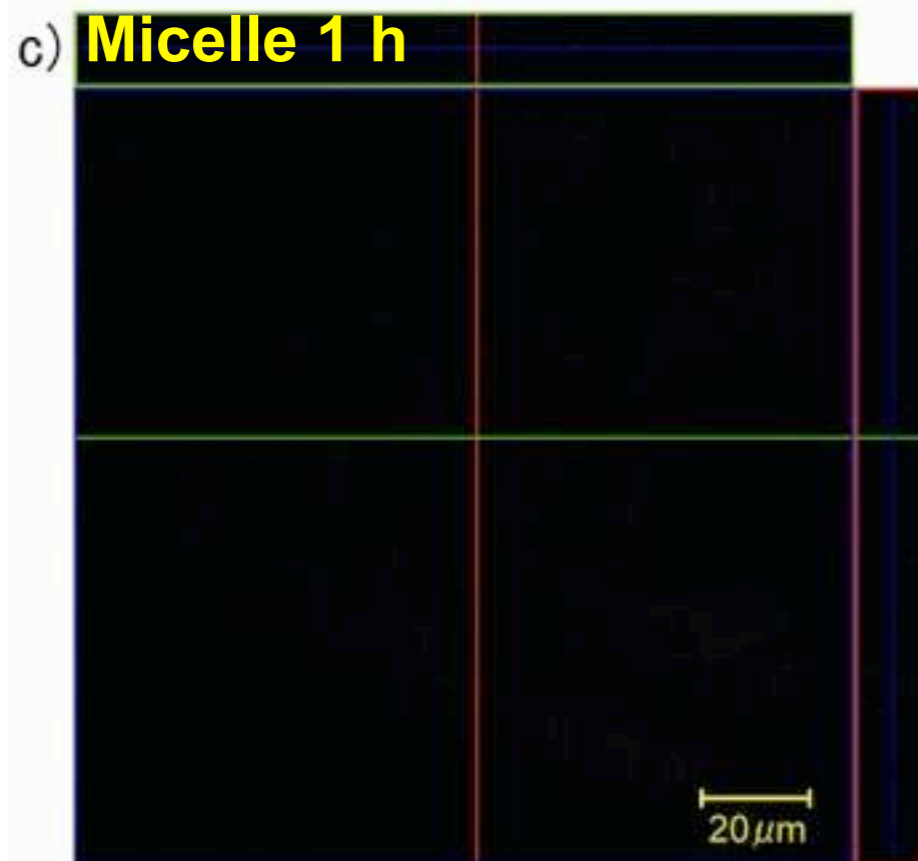
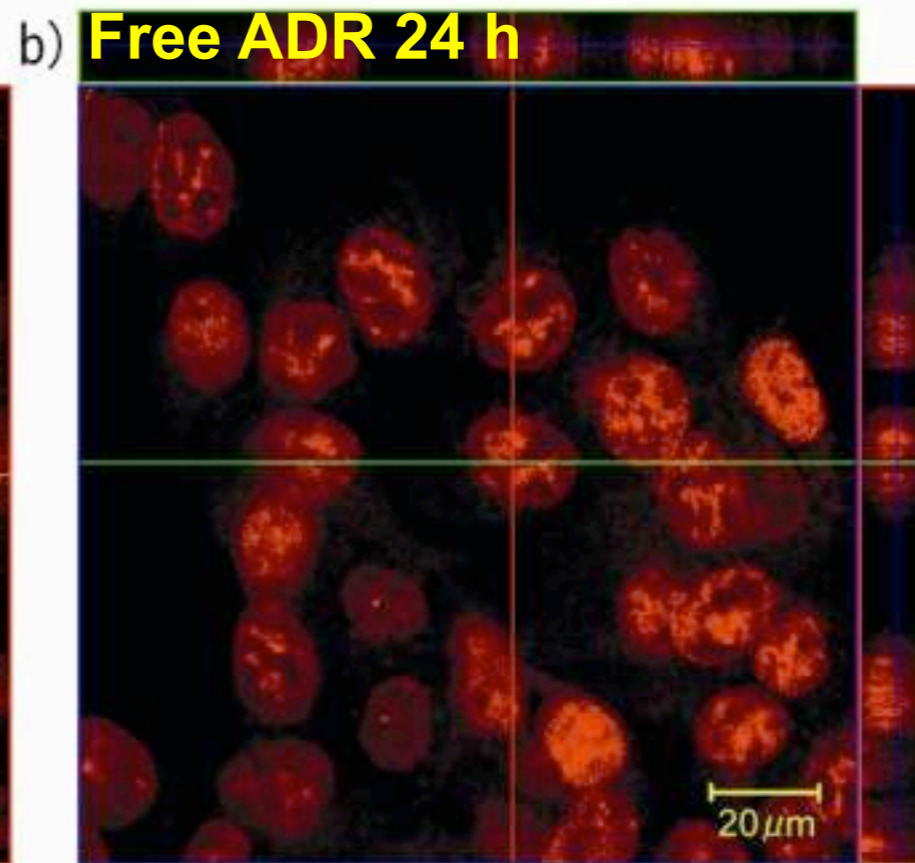
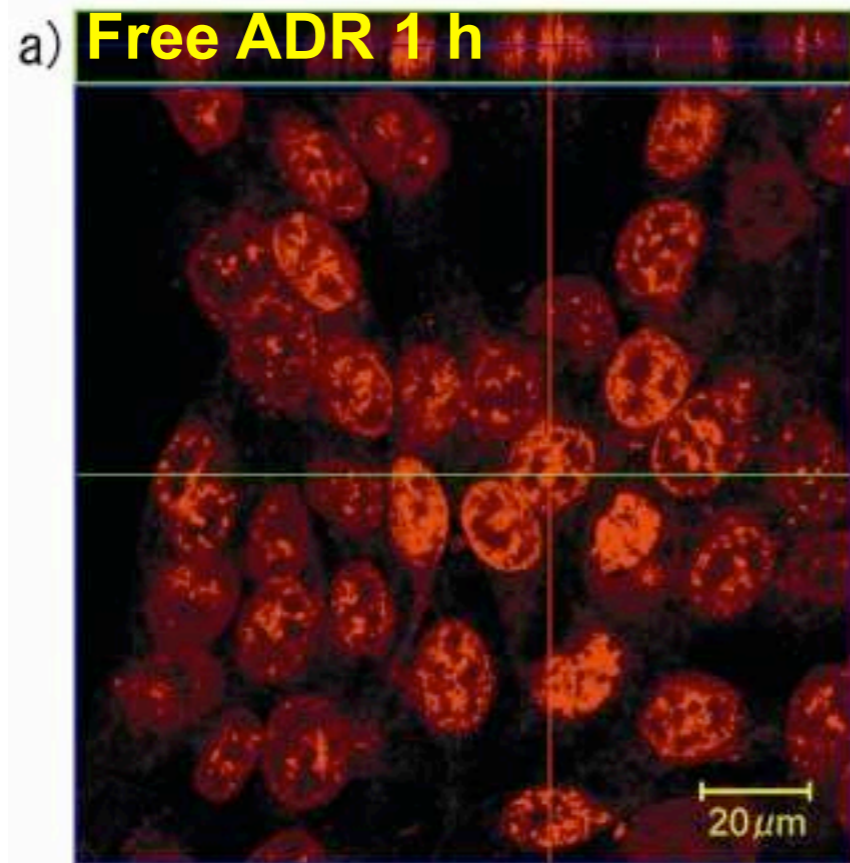


FL is quenched in the micelle core

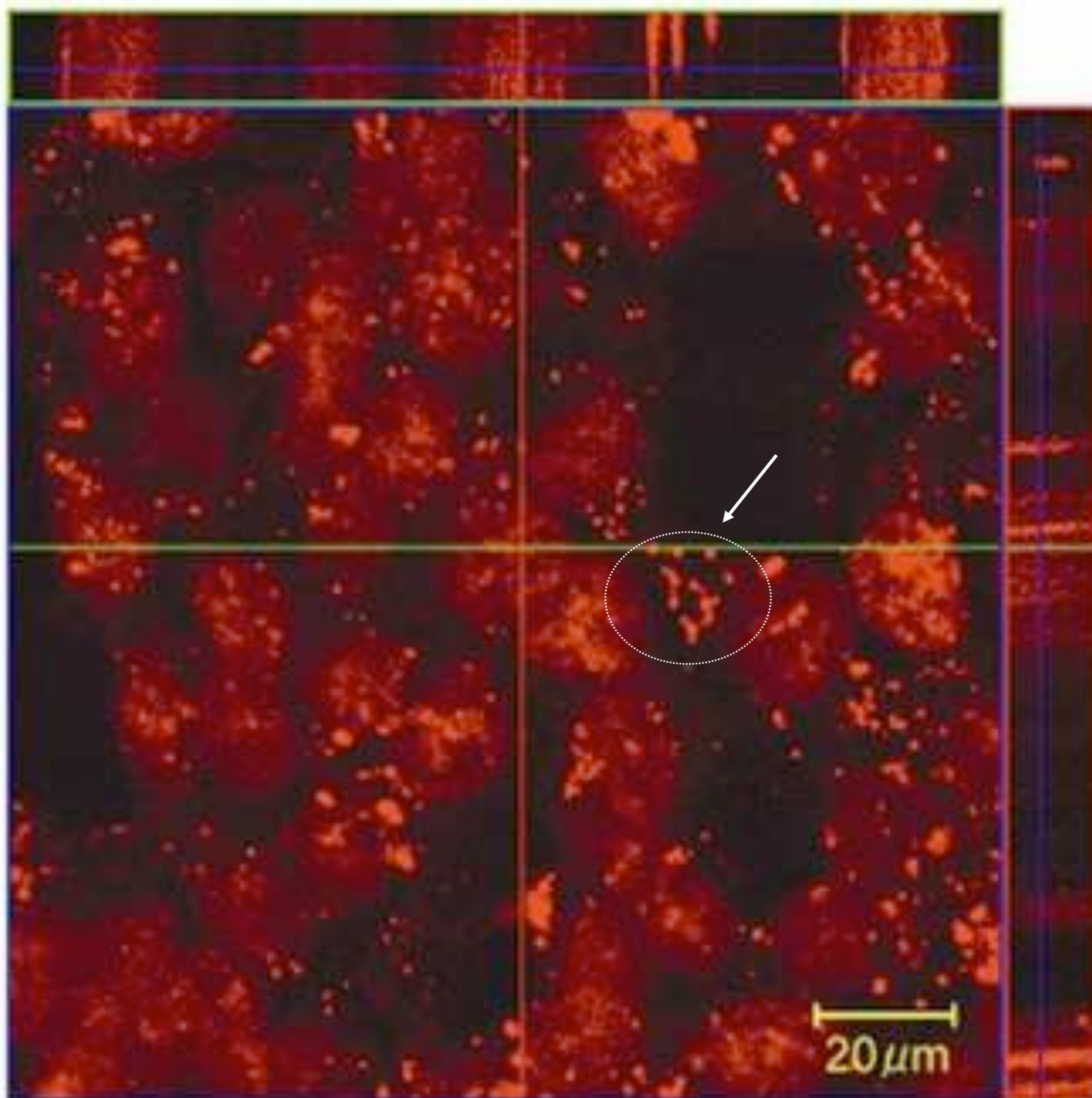


FL becomes detectable with drug release

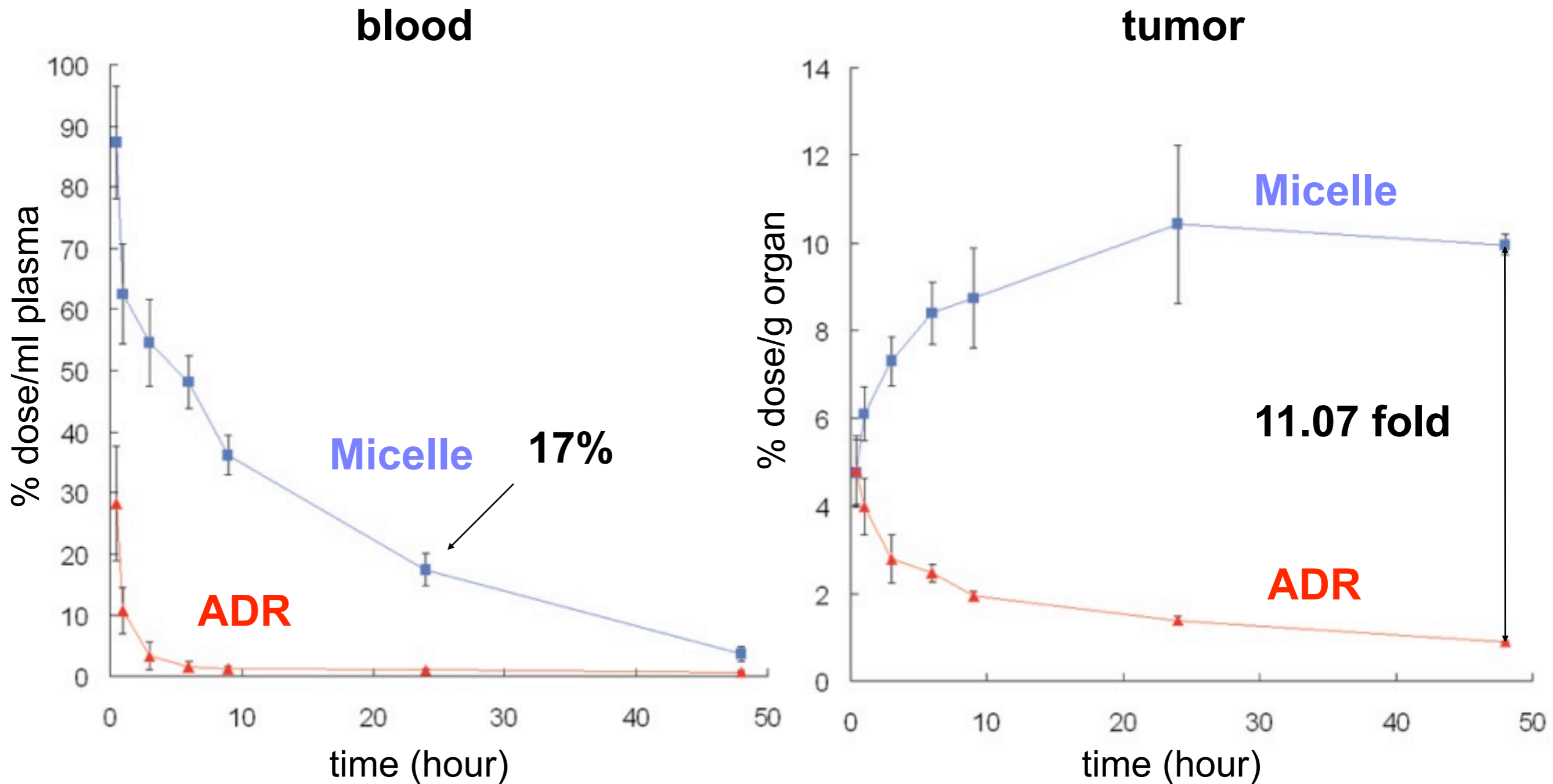
Intracellular distribution of ADR



Intracellular distribution of ADR



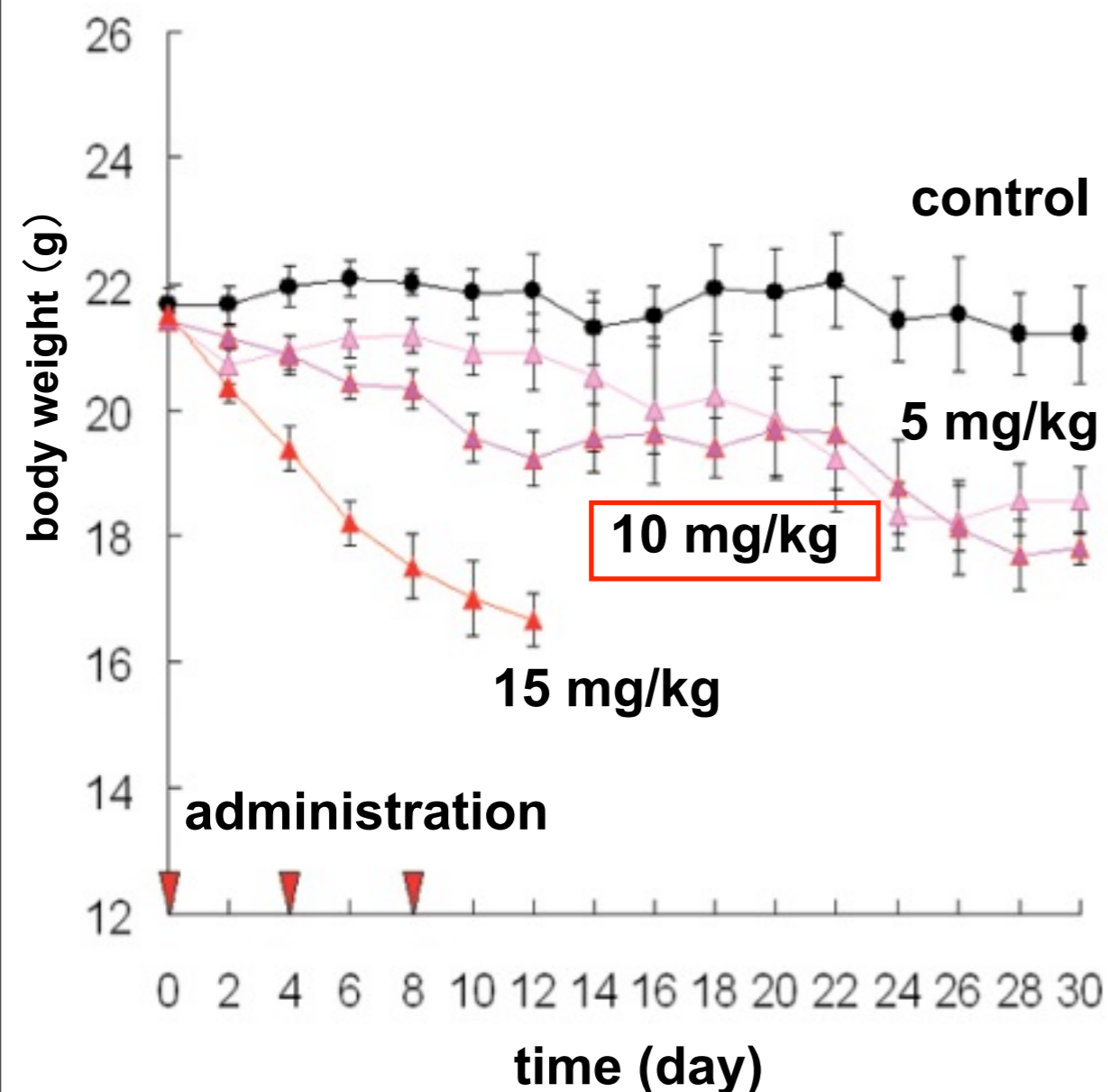
Biodistribution of free and micellar ADR



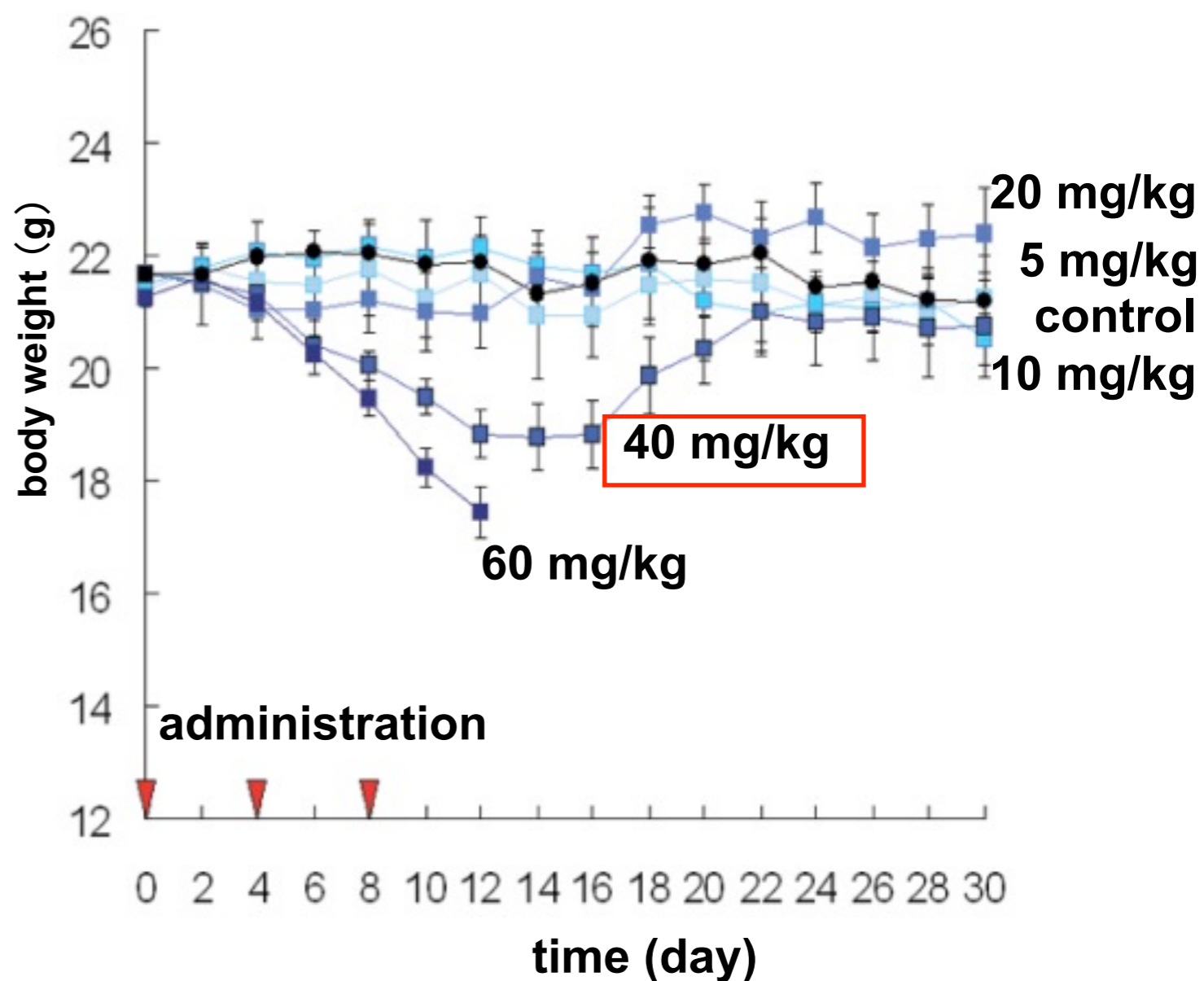
Prolonged circulation and tumor specific accumulation of micellar ADR

In vivo toxicity (body weight change) of free-ADR and micellar-ADR

Free-ADR



Micellar-ADR



Micellar-ADR exhibited more than 4 times higher MTD compared to free-ADR

In vivo antitumor activity

sample	dose (mg/kg) ^a	body weight change on day 30 (%) ^b	toxic death	duration days of tumor growth ^c	complete cure
control	0	-2.18±1.74	0/6	3.74	0/6
ADR	5	-13.35±0.59	0/6	4.21	0/6
	10	-16.84±1.26	0/6	14.59	1/6
	15	—	6/6	—	—
Micelles	5	-0.89±1.68	0/6	3.88	0/6
	10	-4.51±1.44	0/6	3.97	0/6
	20	3.13±1.60	0/6	22.05	2/6
	40	-4.07±0.92	0/6	27.83	3/6
	60	—	6/6	—	—

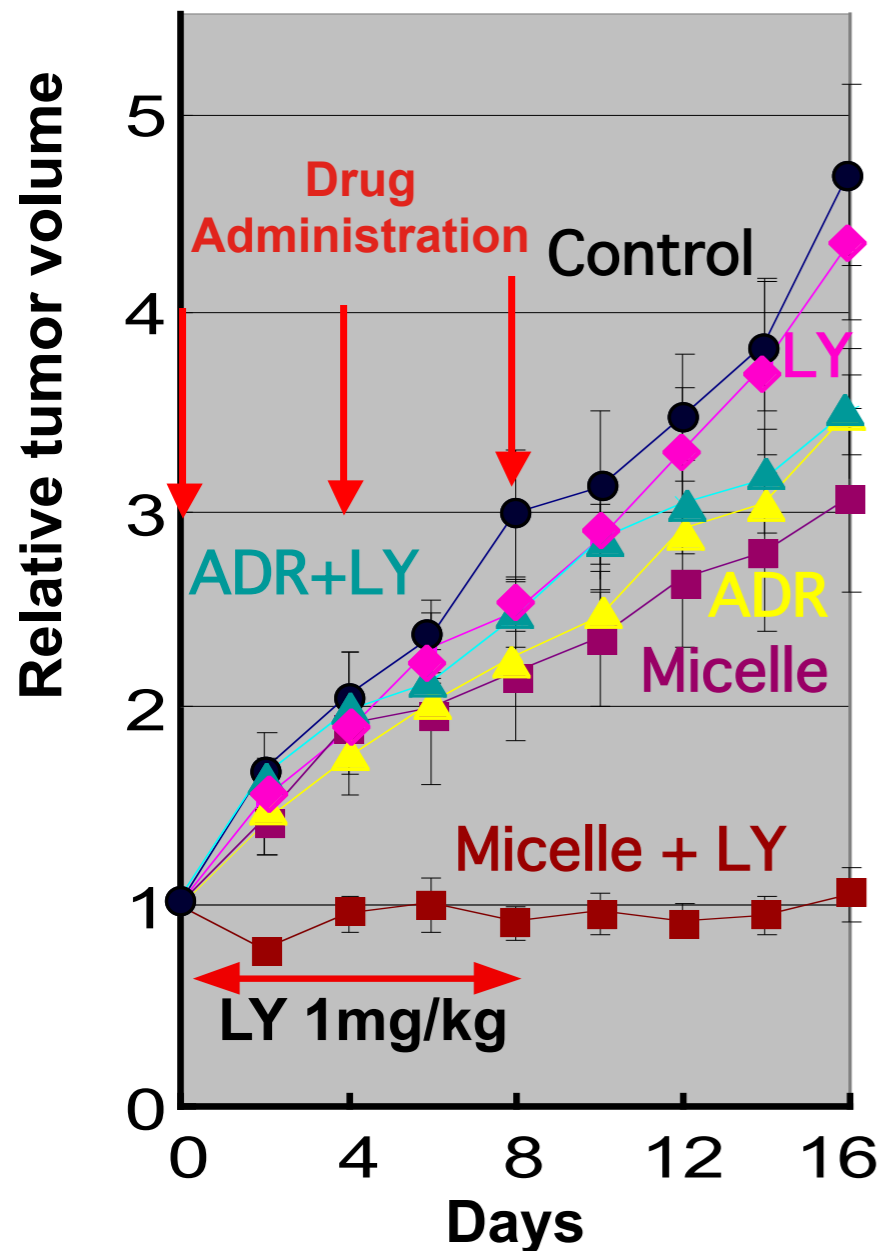
^aAdministrations were carried out three times with a 4-day interval, and doses were determined in free ADR equivalents.

^bBody weights were measured on day 30 after the first injection to compare long-term toxicity between ADR and the micelles. Values are expressed as mean±SEM.

^cDuration to reach 5-fold initial tumor volume.

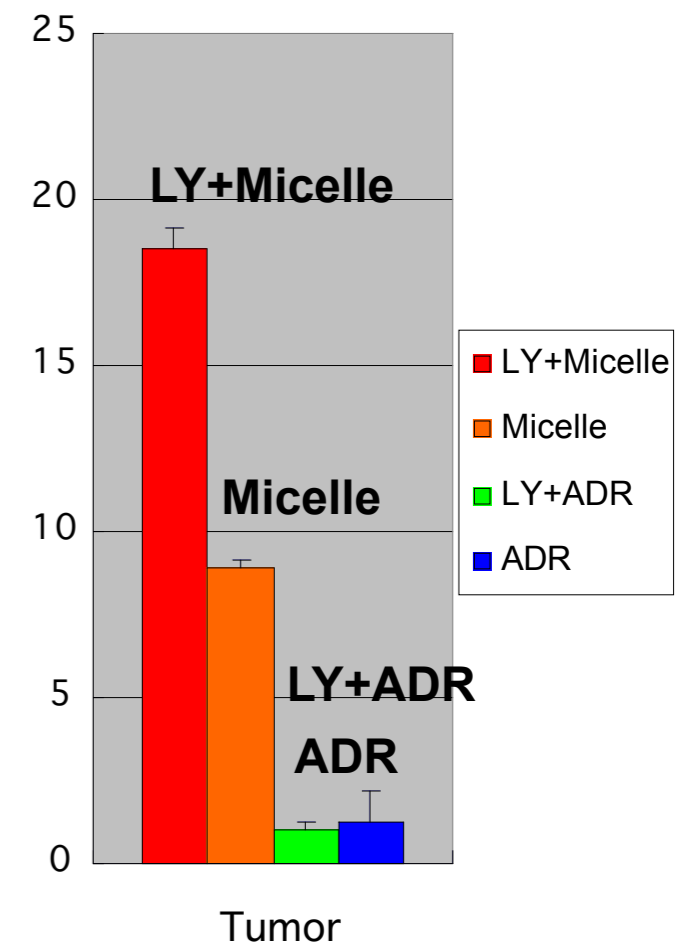
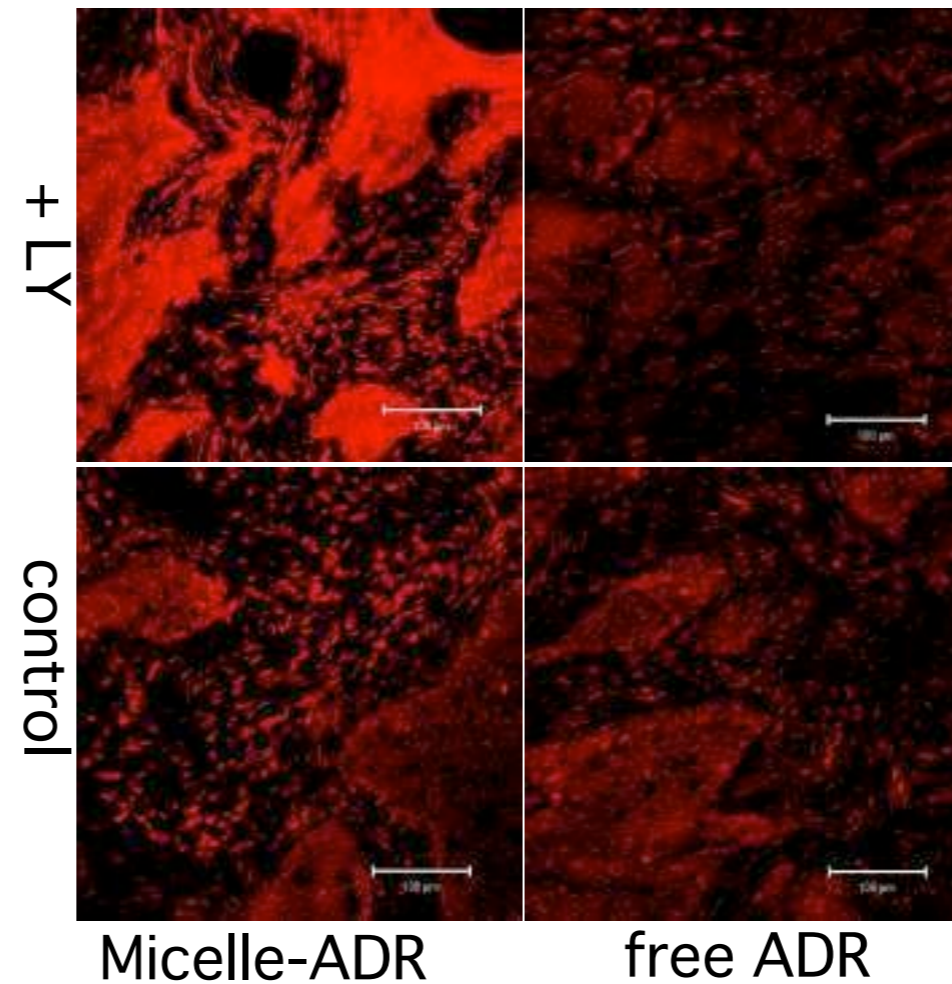
Treatment of intractable pancreatic cancer by pH-sensitive polymeric micelles

Human pancreatic cancer(BxPC3)
(characterized by hypovascularity
and thick fibrosis)



LY: TGF- β inhibitor
(Reagent to transiently increase
the permeability of tumor capillary)

Accumulation of Micelle-ADR into BxPC3

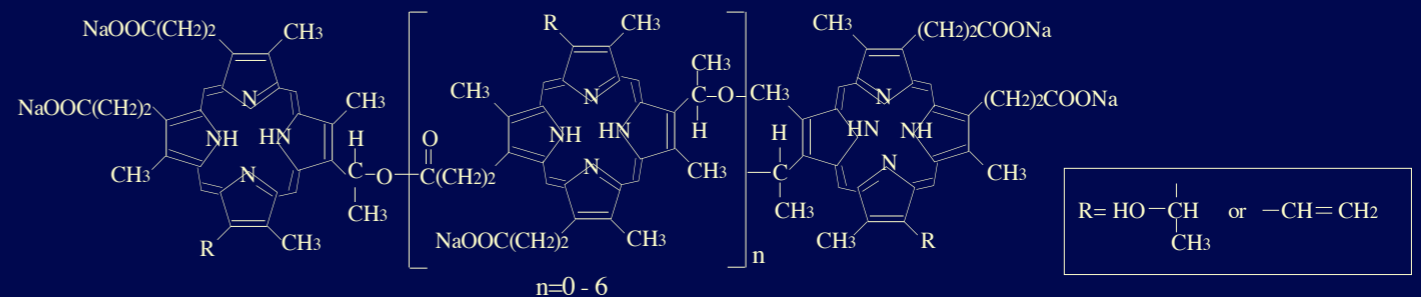


Photodynamic therapy (PDT)

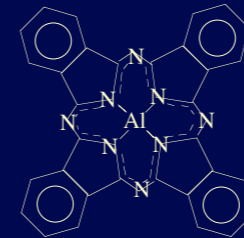
esophageal

i.v. administration of photosensitizer

(A) Photofrin (PII)



(B) metallo-phthalocyanines (MePc)



tumor

lung

gastric

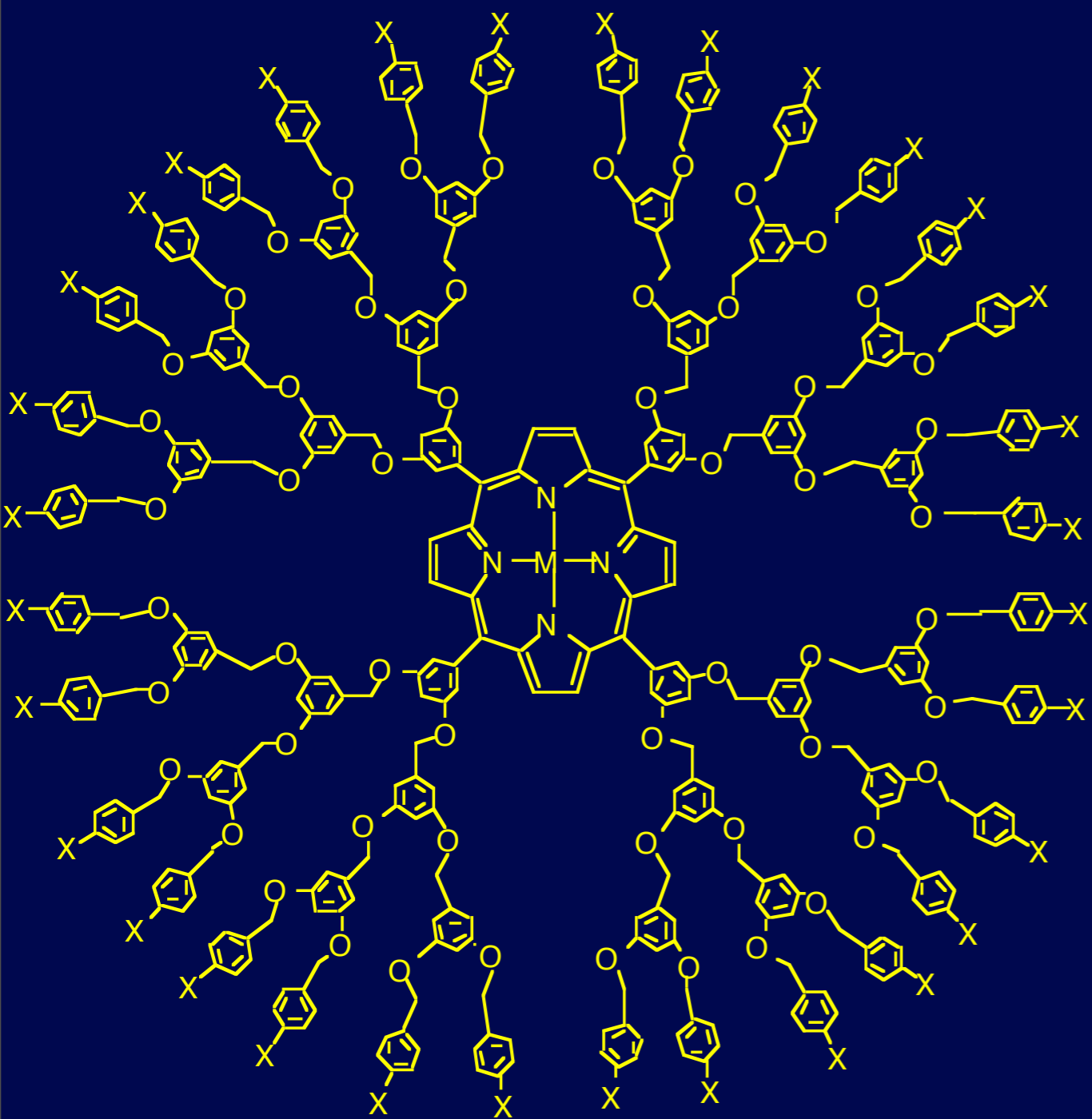
selective irradiation of light

activation of photosensitizer

generation of highly reactive oxygen species

selective toxicity in tumor

Ionic dendrimer porphyrins (DP) as a novel type of photosensitizer



5 nm

- **P32(+)**DP**Zn:**

$X = \text{CONH}(\text{CH}_2)_2\text{NMe}_3^+\text{Cl}^-$ 1)

or $\text{CONH}(\text{CH}_2)_2\text{NH}_3^+\text{Cl}^-$ 2)

M=Zn

- **P32(-)**DP**Zn:**

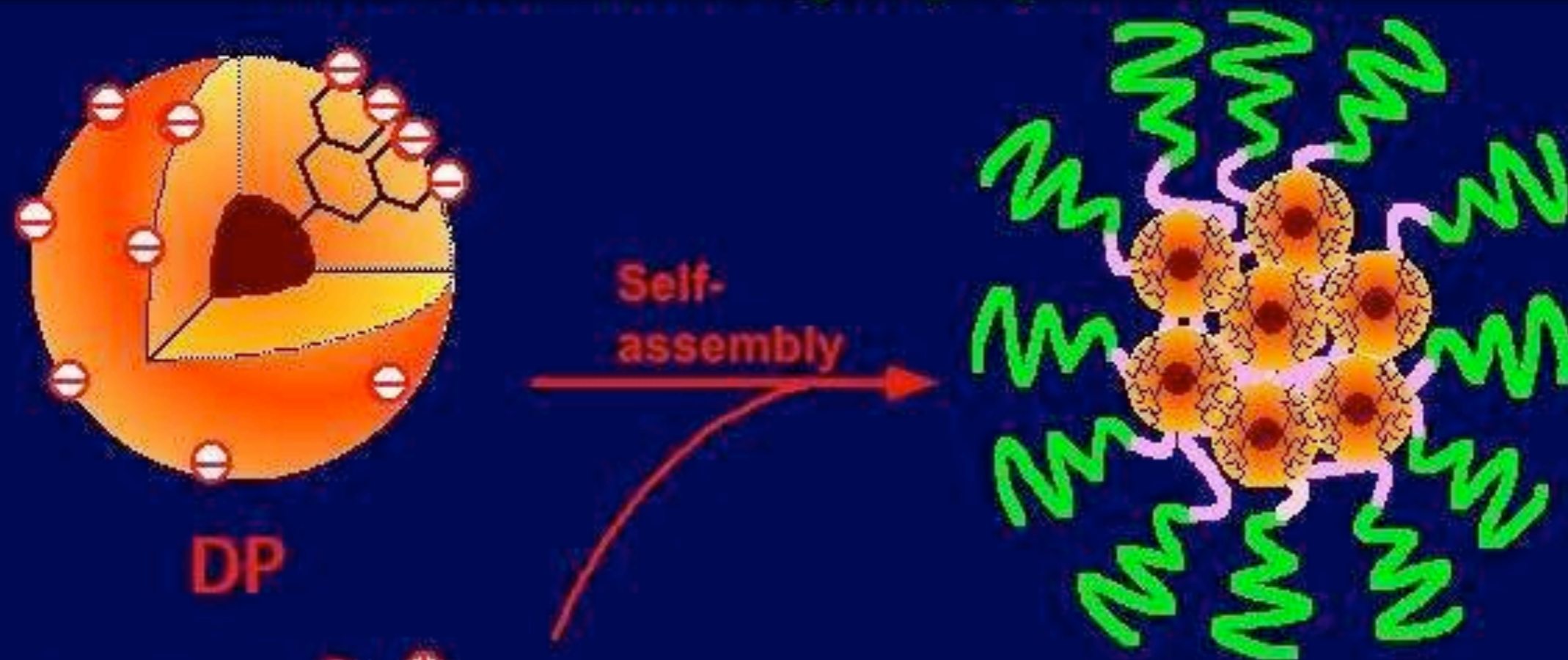
$X = \text{COO}^-\text{K}^+$ 1)

M=Zn

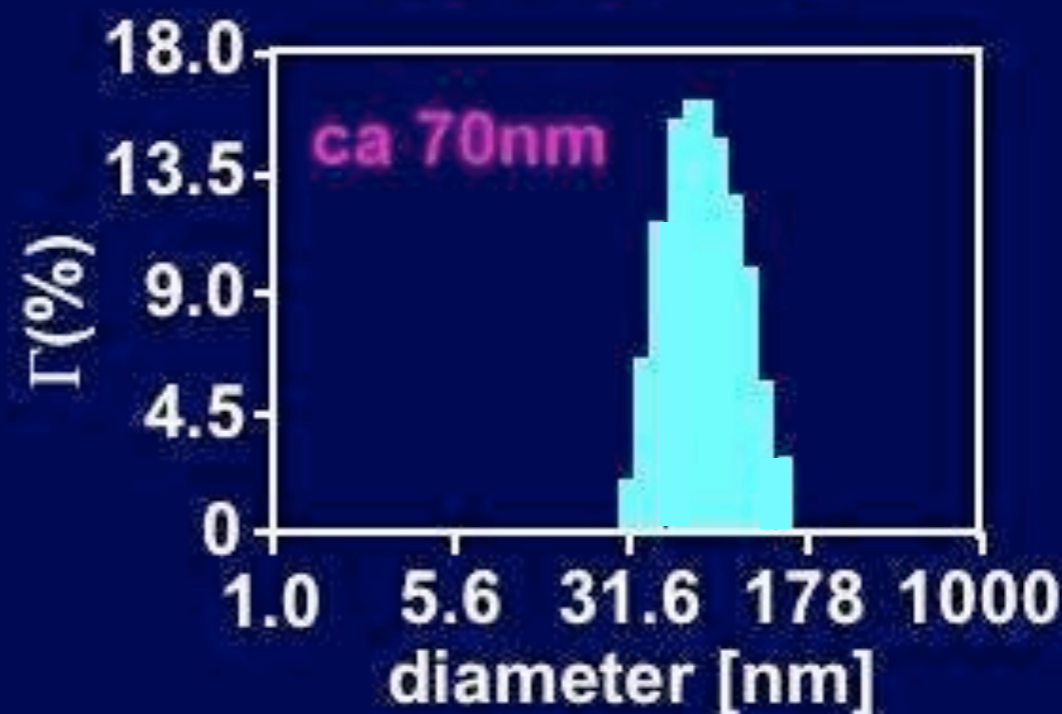
1) Sadamoto, R.; Tomioka, N.; Aida, T. *J. Am. Chem. Soc.* 1996, *118*, 3978-3979

2) Zhang, G.; Kataoka, K.; et al, *Macromolecules*, 2003, *36*, 1304-1309

Polyion complex (PIC) micelles incorporating ionic dendrimer porphyrin (DP)

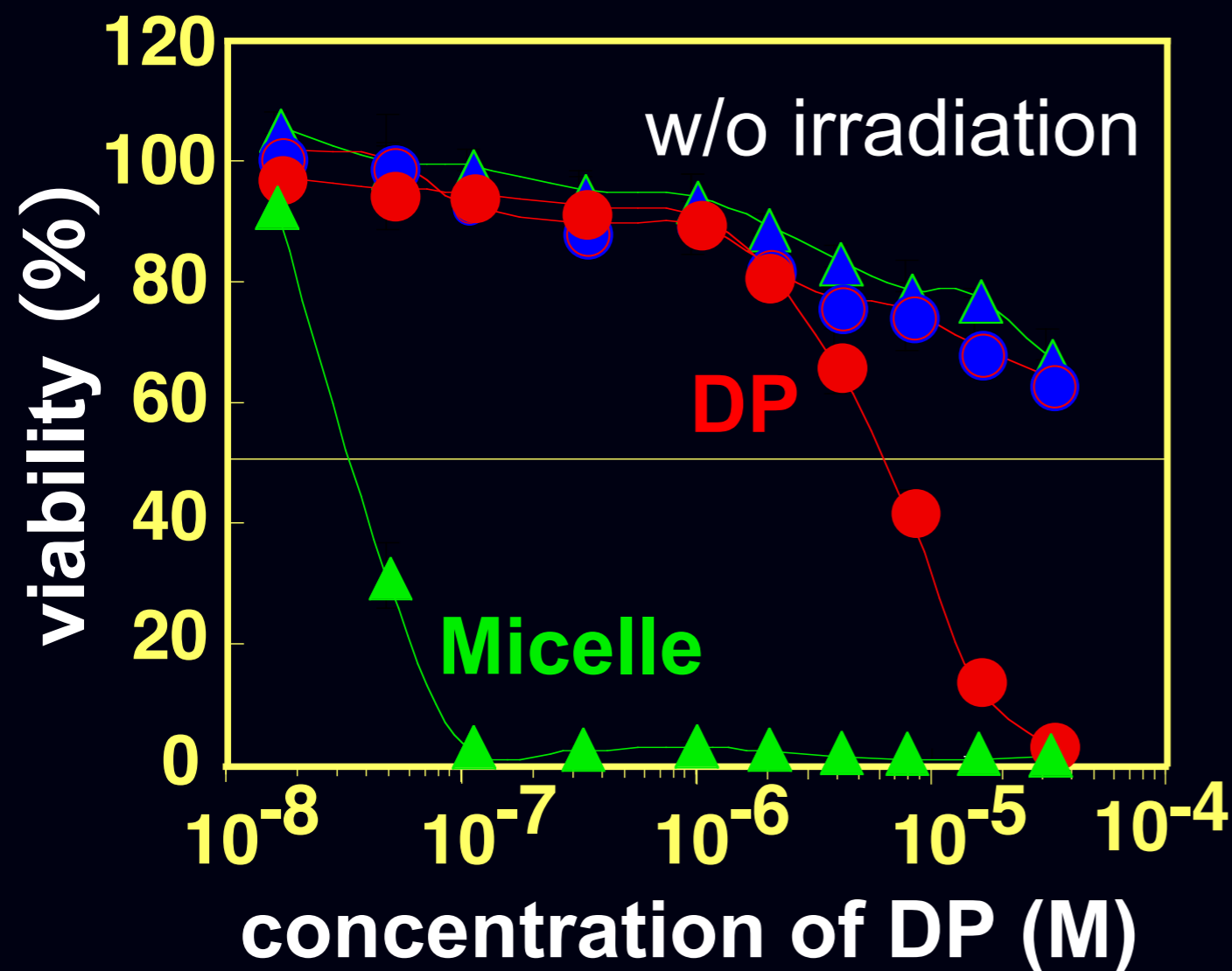


High stability against salt concentration (>300mM) and pH (6 - 8.5)



Photocytotoxicity of DP and DP-incorporated micelles

photocytotoxicity (LLC cells)



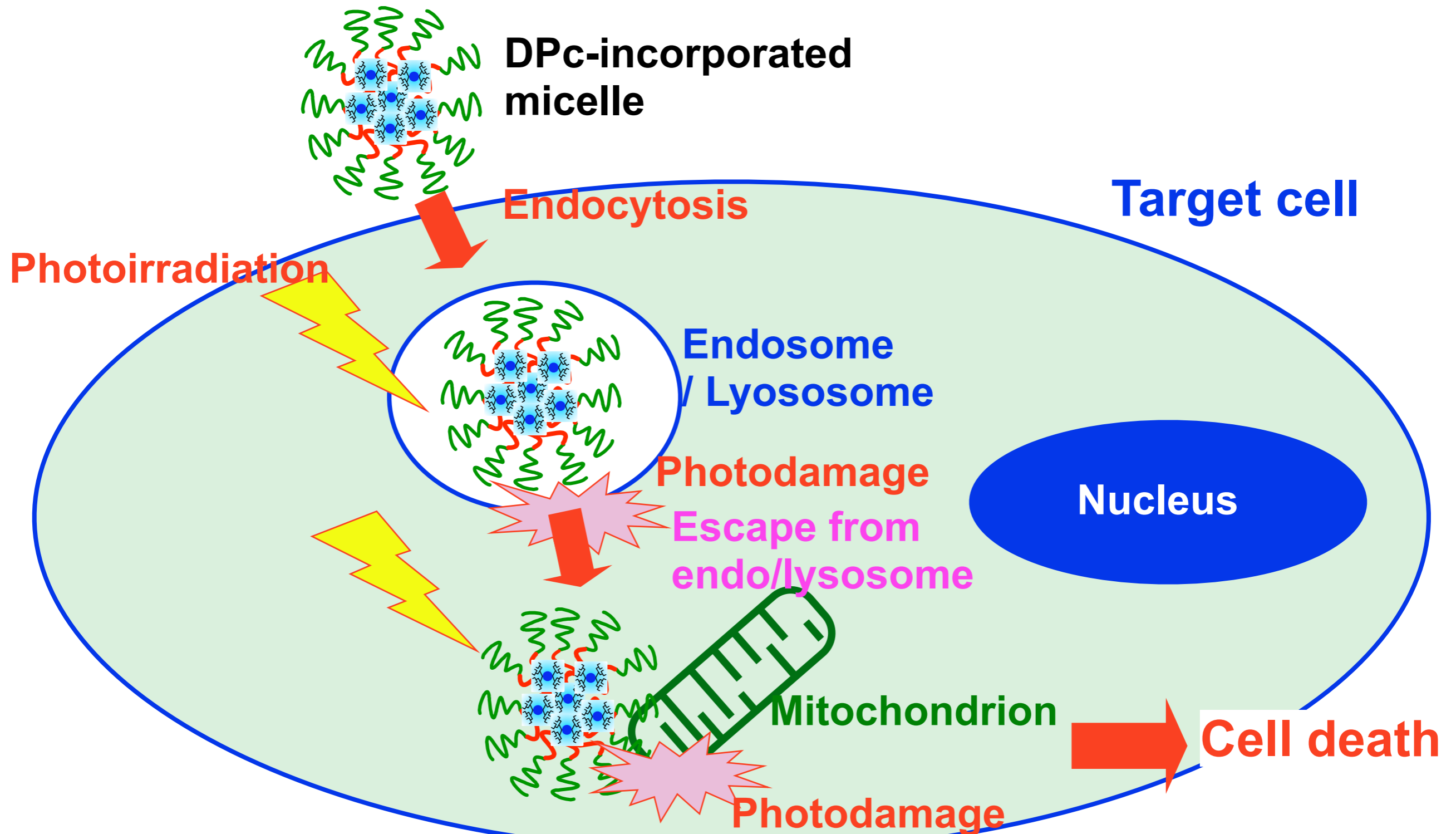
Incorporation of DP into the micelle achieved approximately 280-fold increase in photocytotoxicity.

This result ensures safety after PDT, because the micelle is assumed to dissociate finally.

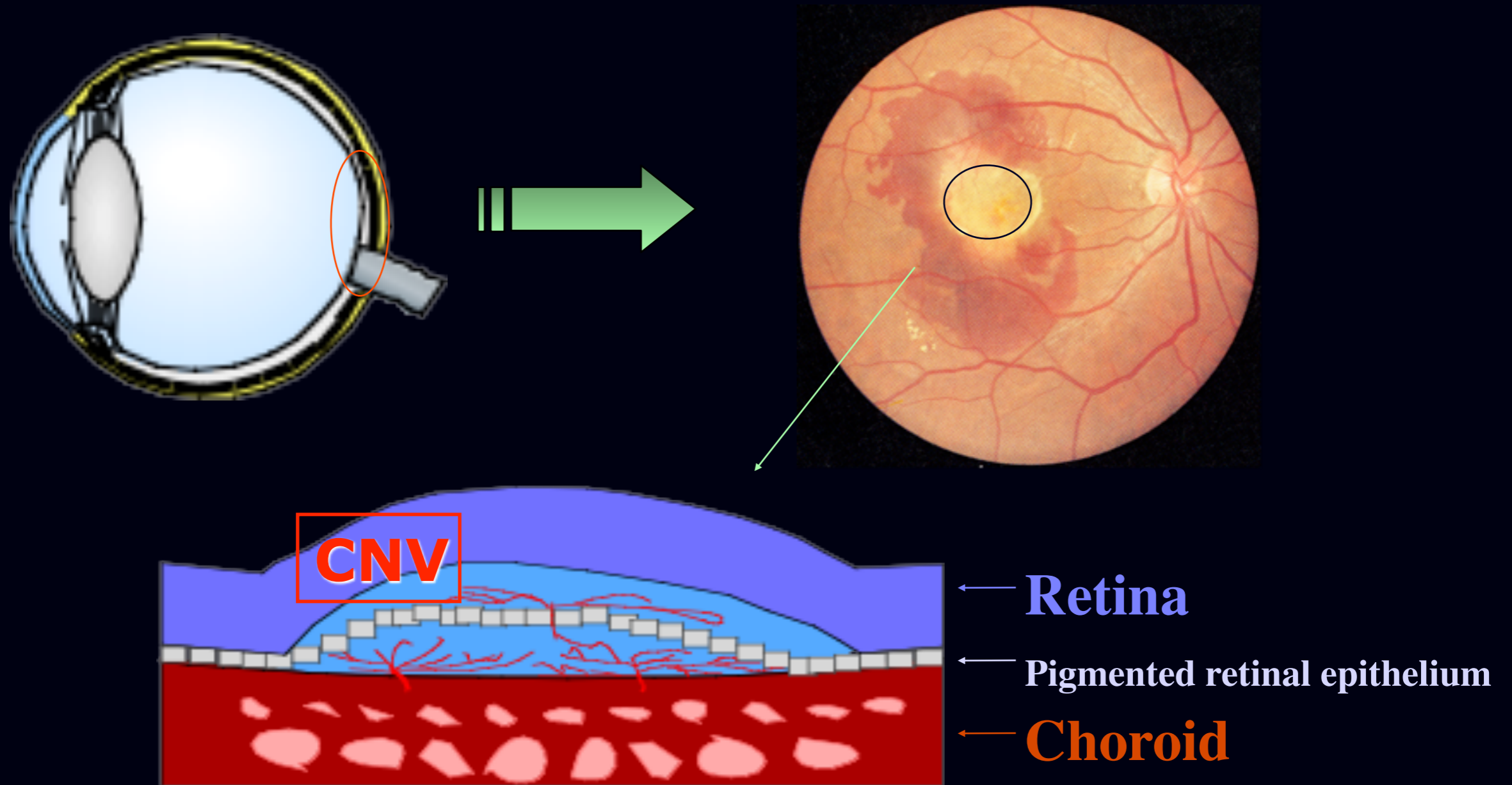
6hr incubation → wash with PBS
→ irradiation → 48hr incubation

Hypothetic Mechanism of Cell Death

endocytic uptake → photochemical disruption of endosomal membrane
→ endosomal escape — interactions with mitochondrial membranes and their photochemical disruption



Exudative age-related macular degeneration (wet AMD) is characterized by choroidal neovascularization (CNV), and is a major cause of visual loss in developed countries.



% of CNV Occlusion

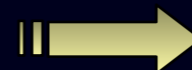
CNV Occlusion [%]

Laser Intensity (J/cm ²)	1 day after PDT		7 days after PDT	
	PIC micelle	Visudyne*	PIC micelle	Visudyne*
5	63.6	--	81.8	--
10	75.0	31	81.3	6
25	88.8	83	83.3	33
50	73.3	54	80.0	36
100	90.9	42	81.8	44

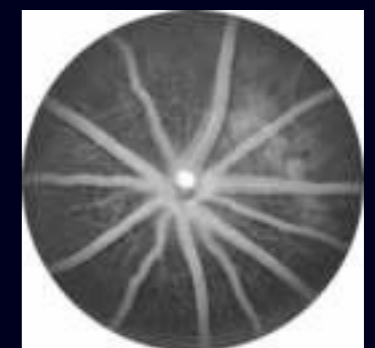
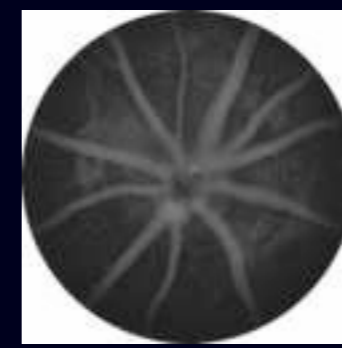
*Zacks et al. IOVS, 2002

Fluorescent imaging of eyeground

Before PDT



After PDT

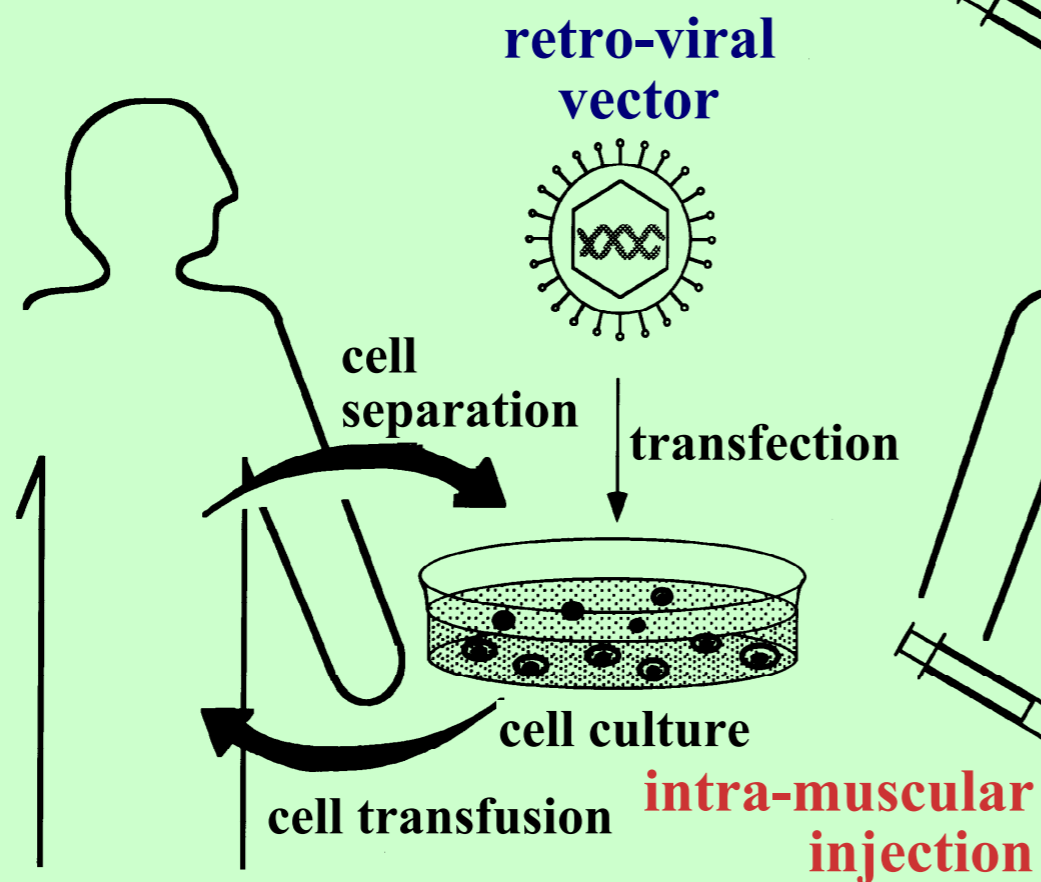


R. Ideta, et al, *Nano Lett.*, 5(12), 2426 (2005)

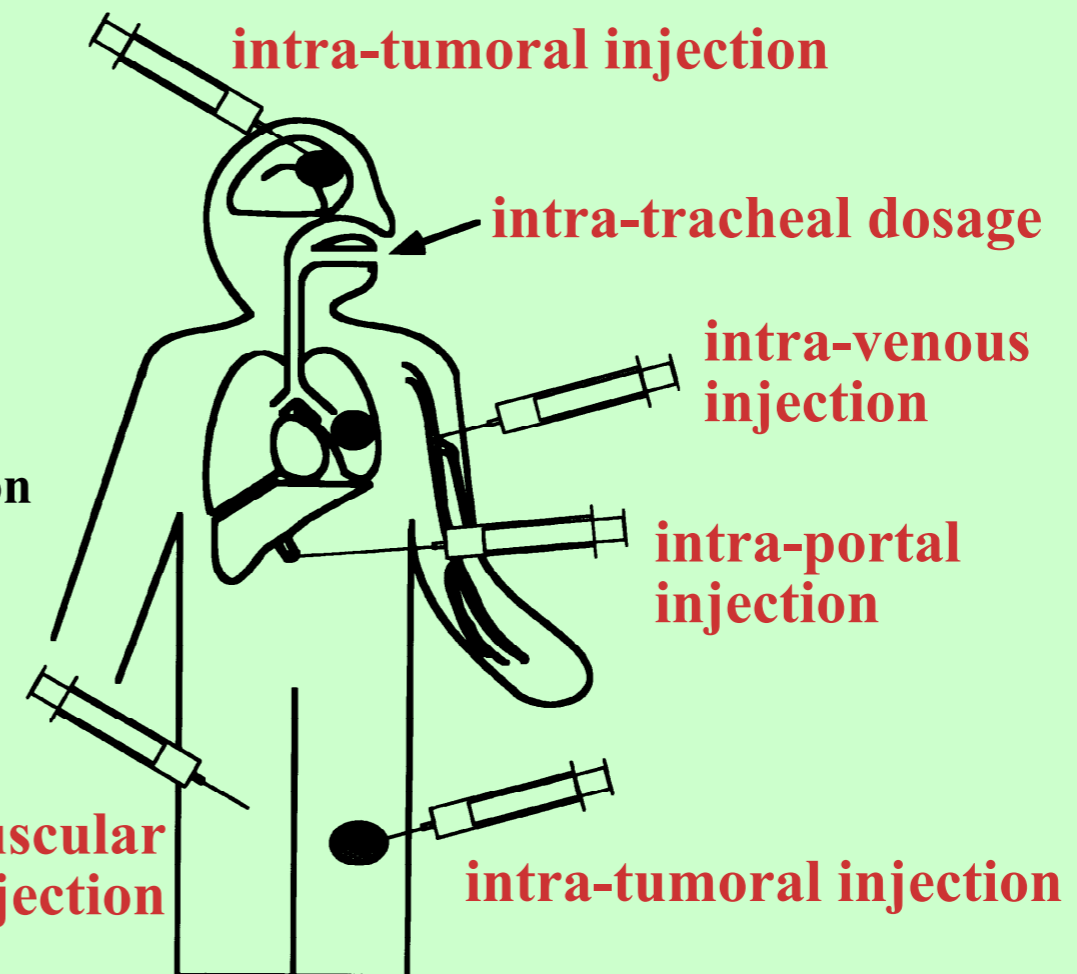
Target diseases for gene therapy

Cancer, Enzyme-deficiency, AIDS, Cardiovascular diseases, Diabetes, Tissue regeneration, etc.

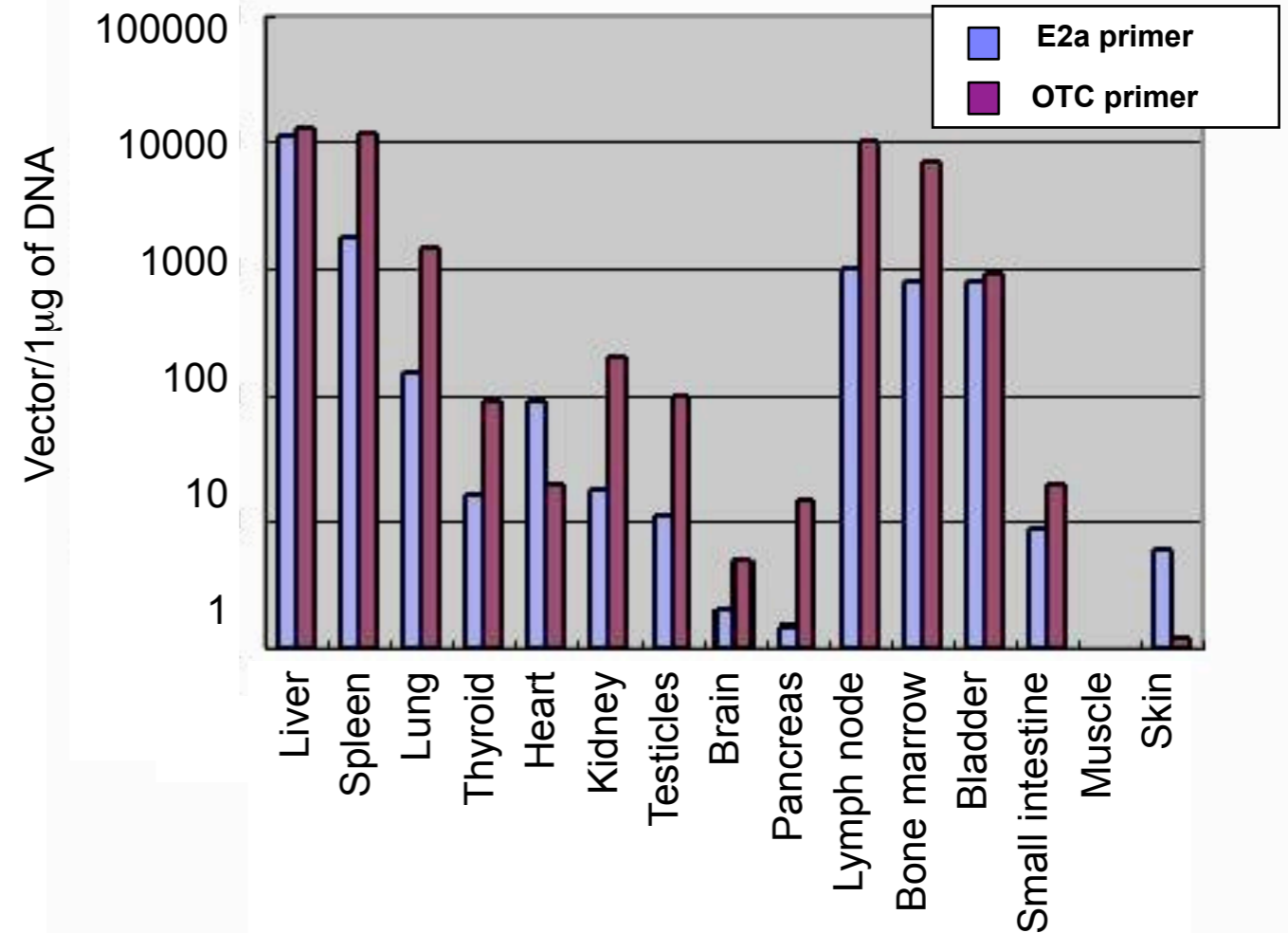
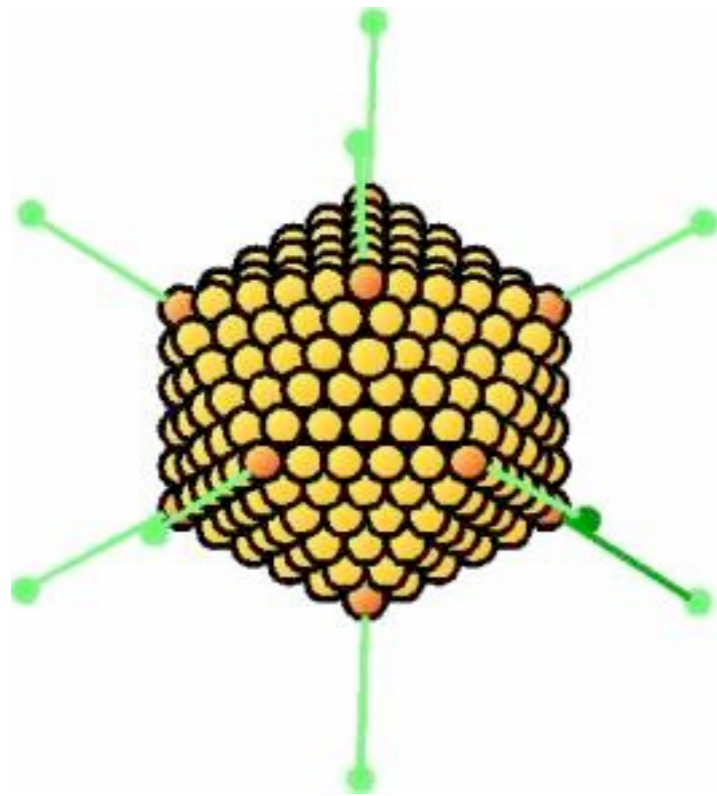
Ex vivo method



In vivo method

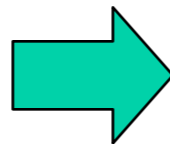


Gene Therapy Death Prompts Review of Adenovirus Vector



Traces of adenovirus DNA (E2a) and a curative gene (OTC).
Patient's target organ is the liver

- Inherent antigenicity
- Limited size in encapsulated gene
- Difficulties in large-size production

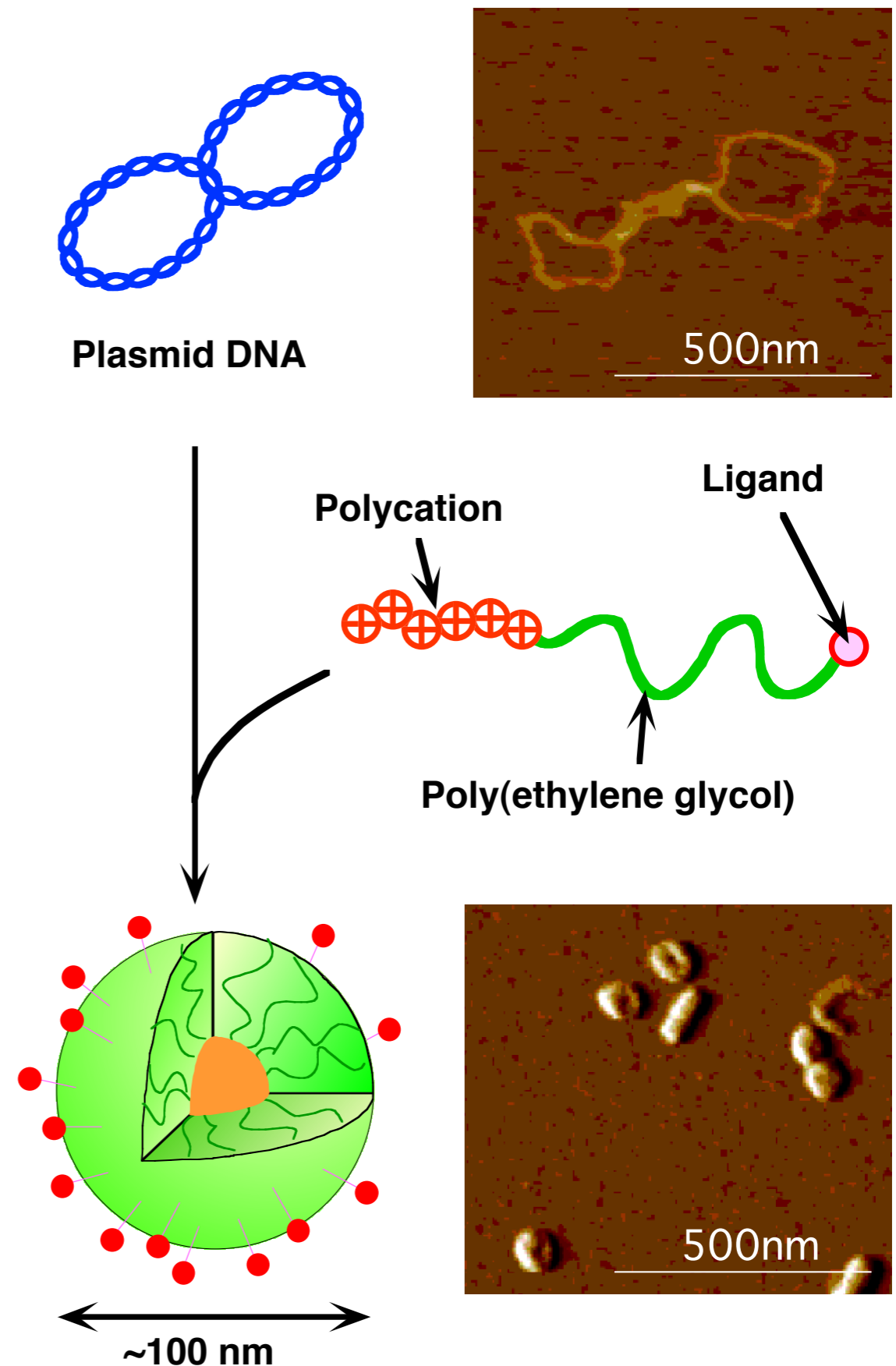
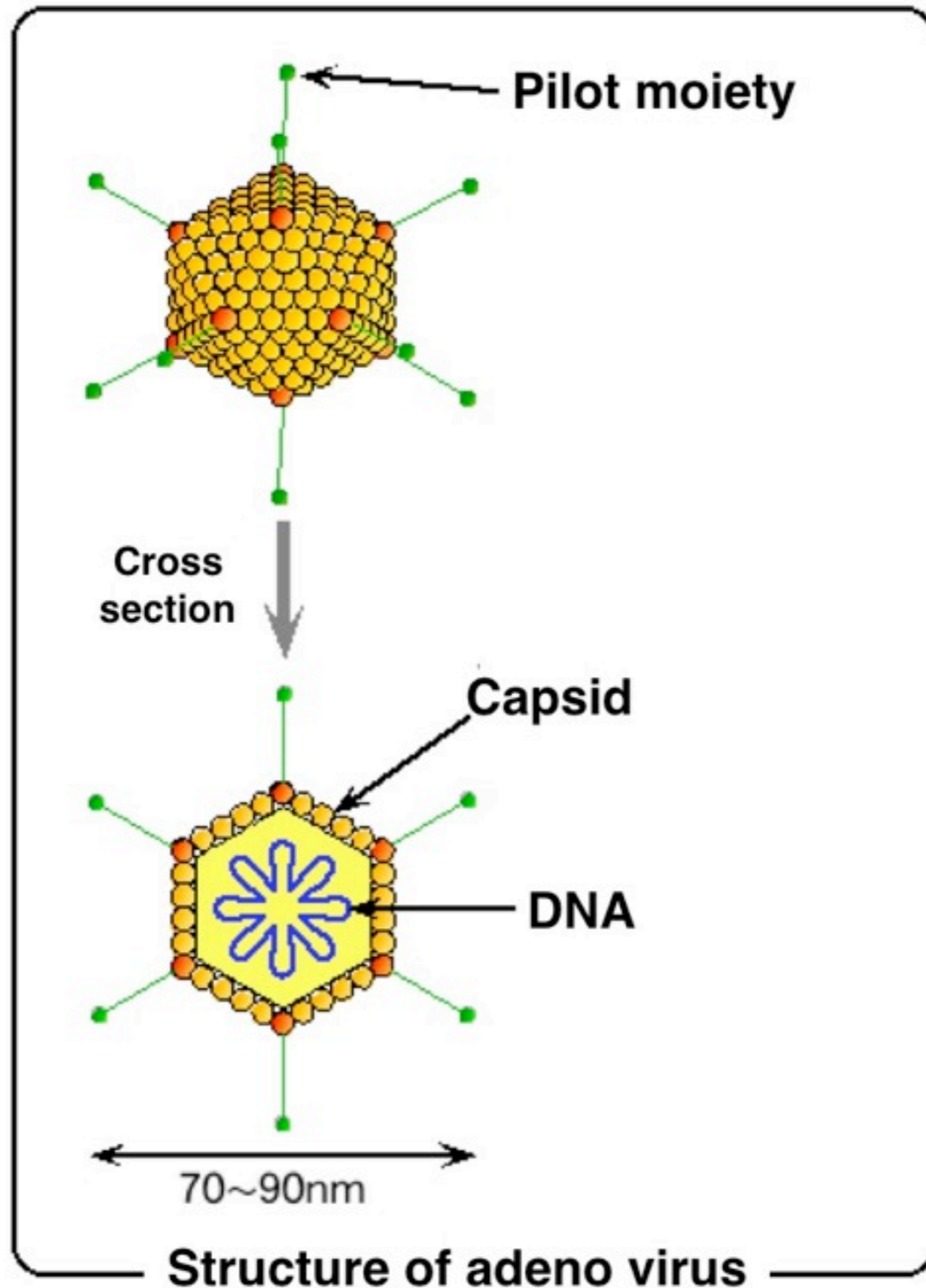


Gene therapy death of patients at University of Pennsylvania on September, 1999

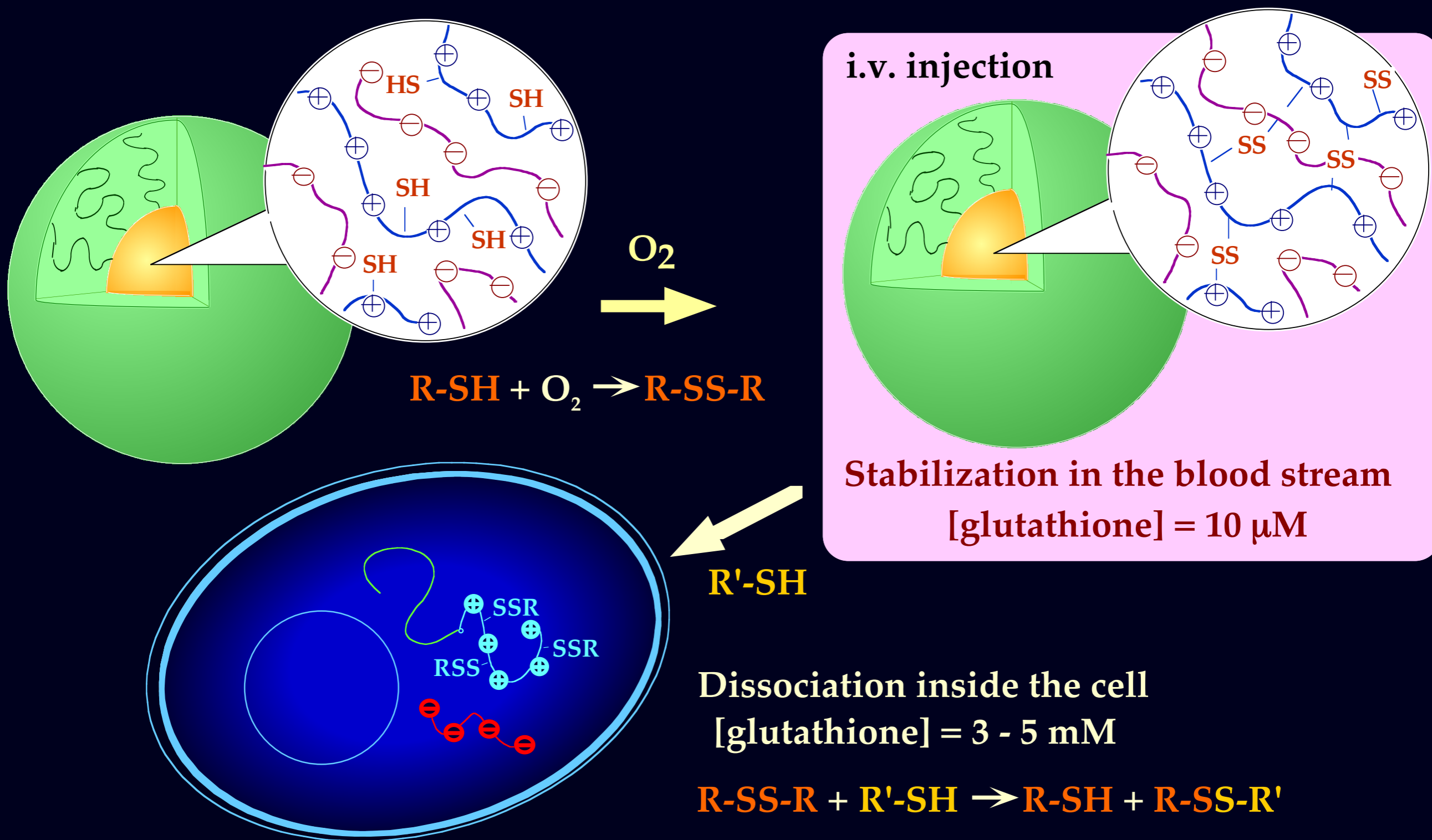
→ 38 trillion virus particles were dosed through i.v. route, yet only 1% of the transferred genes reached the target cells

→ **Restricted clinical use of adenovirus vector**

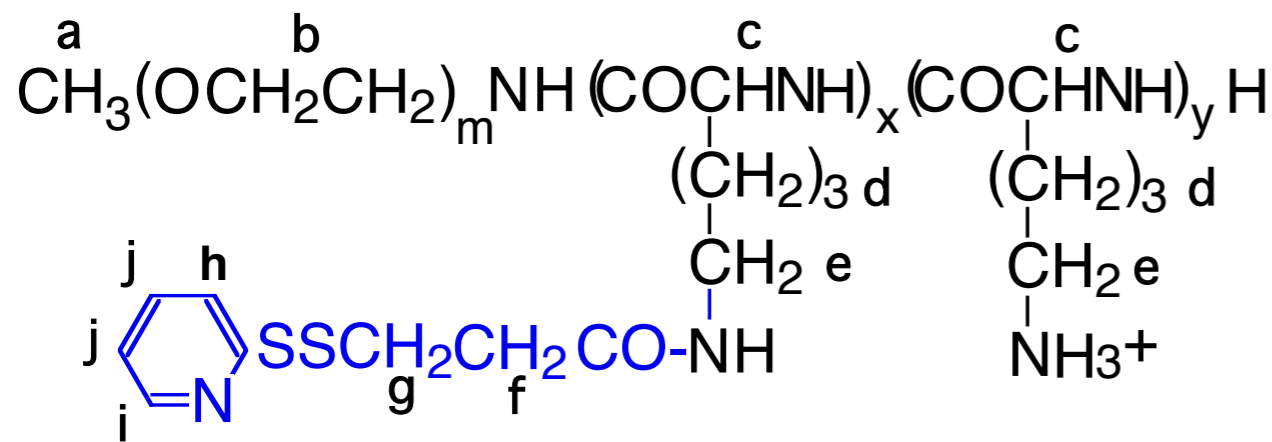
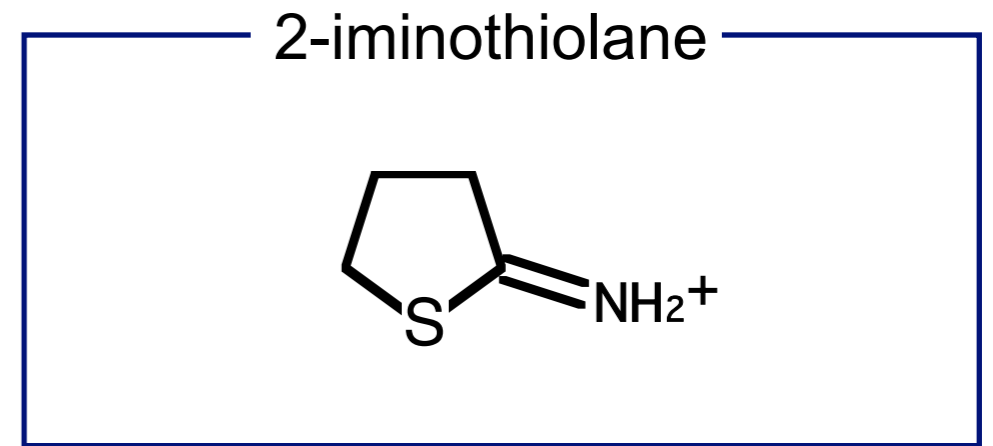
pDNA entrapped polymeric micelle for gene delivery



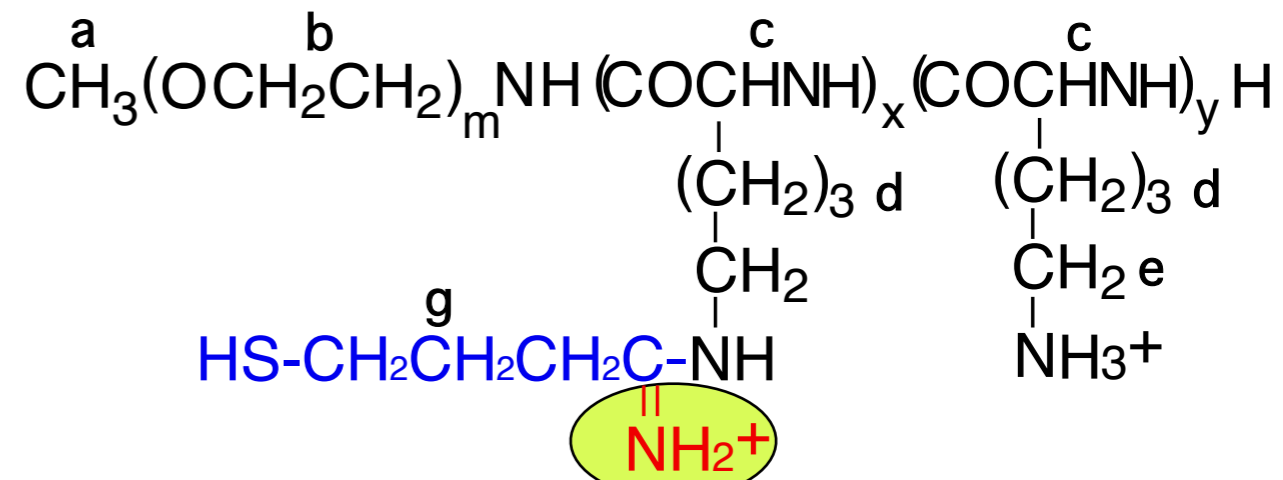
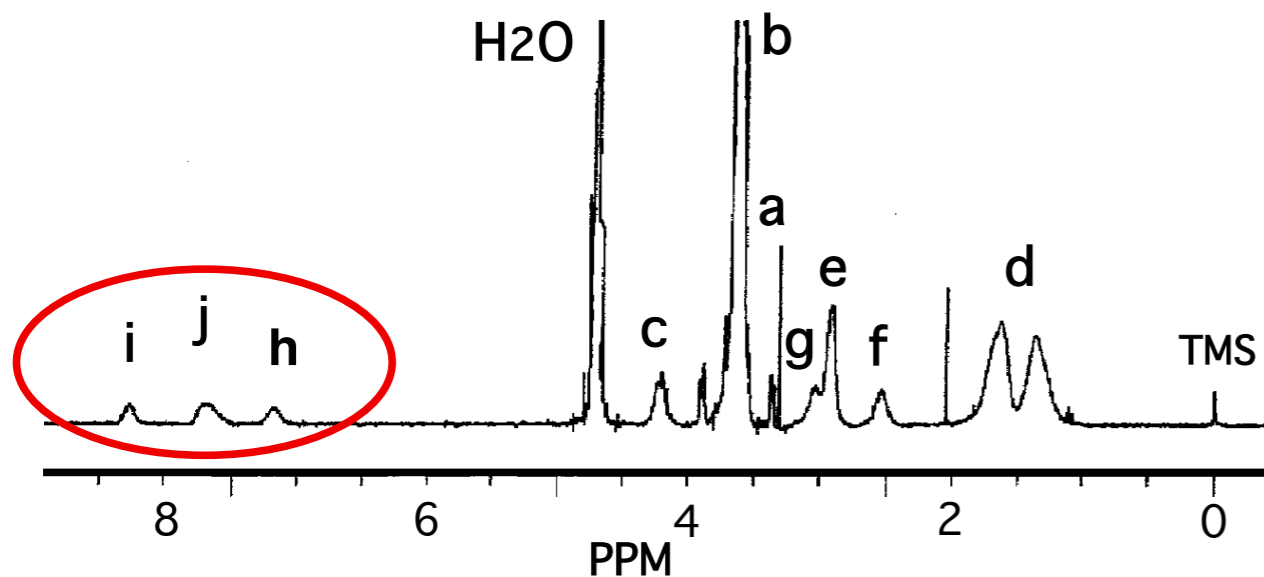
Environment-sensitive stabilization of core-shell structured PIC micelle by reversible cross-linking of the core through disulfide bond



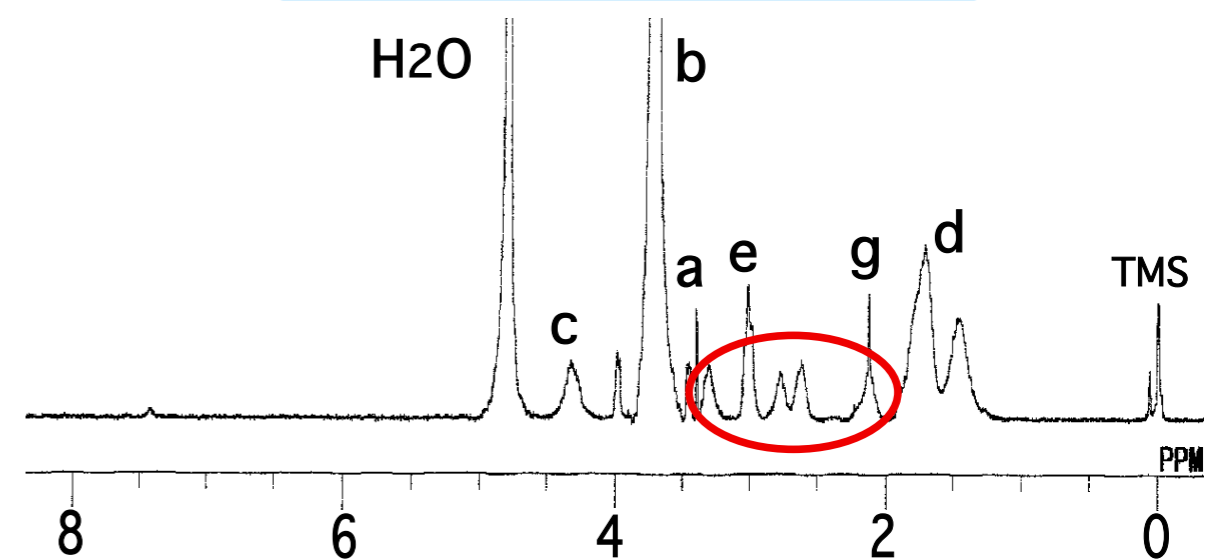
Preparation of thiolated PEG-PLL with controlled charge density



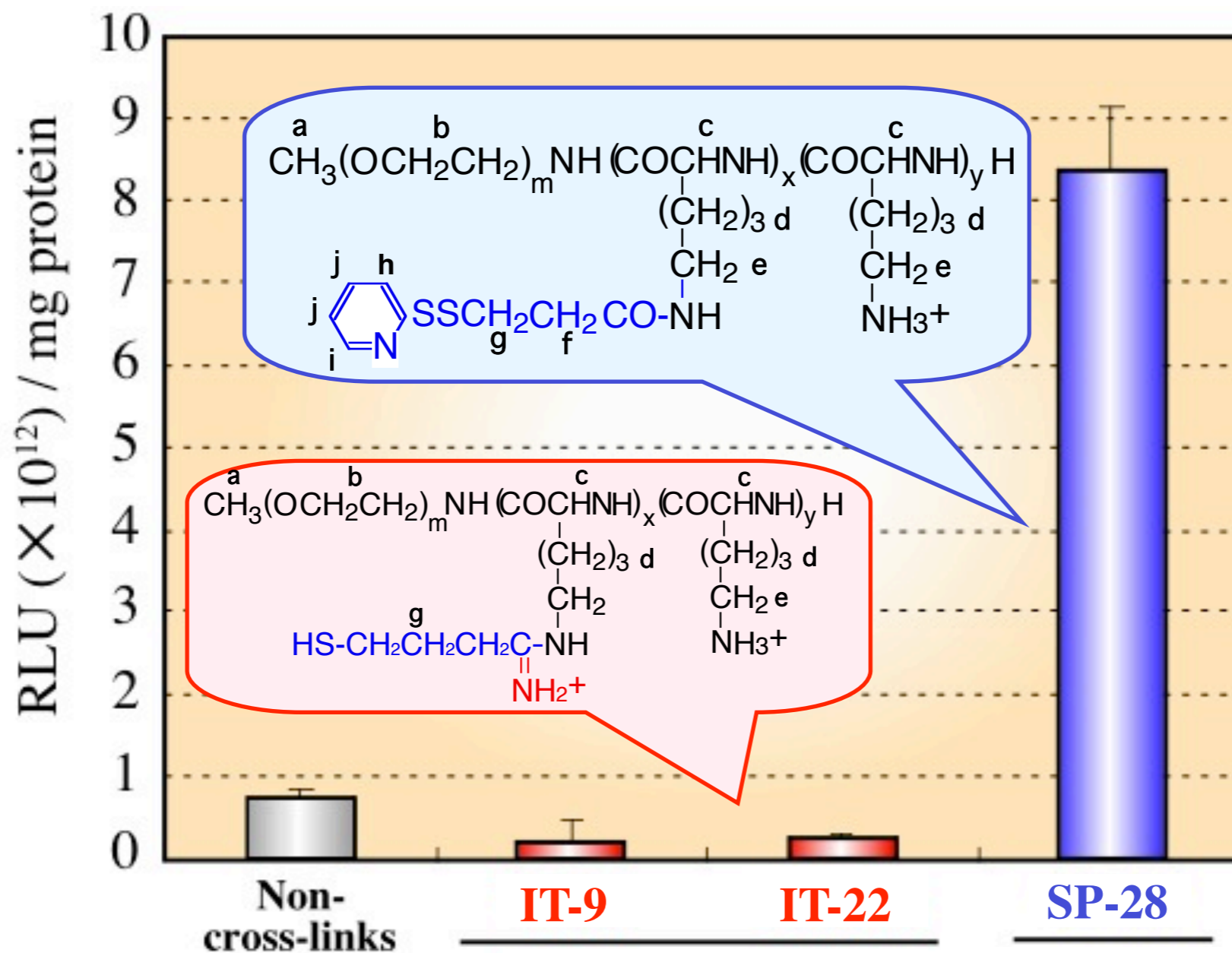
SP-X (X: SS mol%)



IT-X (X: SH mol%)



Improved Gene Transfection by SS Crosslinked Micelles



293T cells

Improved stimuli sensitivity through charge compensated introduction of SS crosslinking

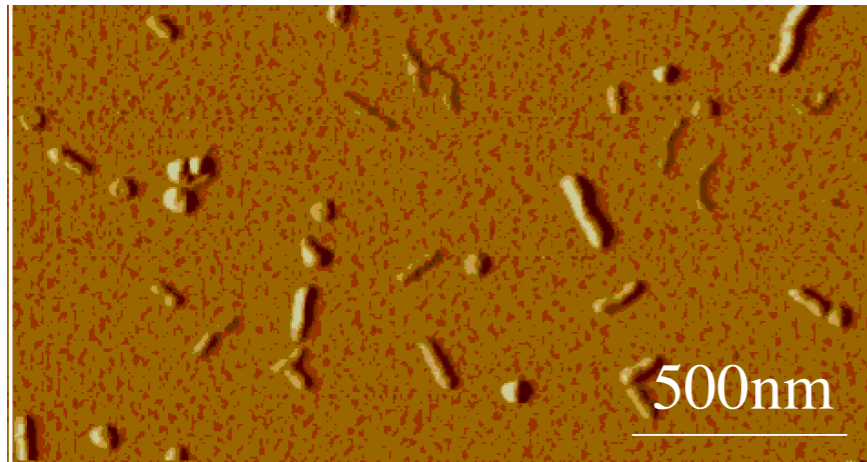


Remarkable increase in transfection efficiency

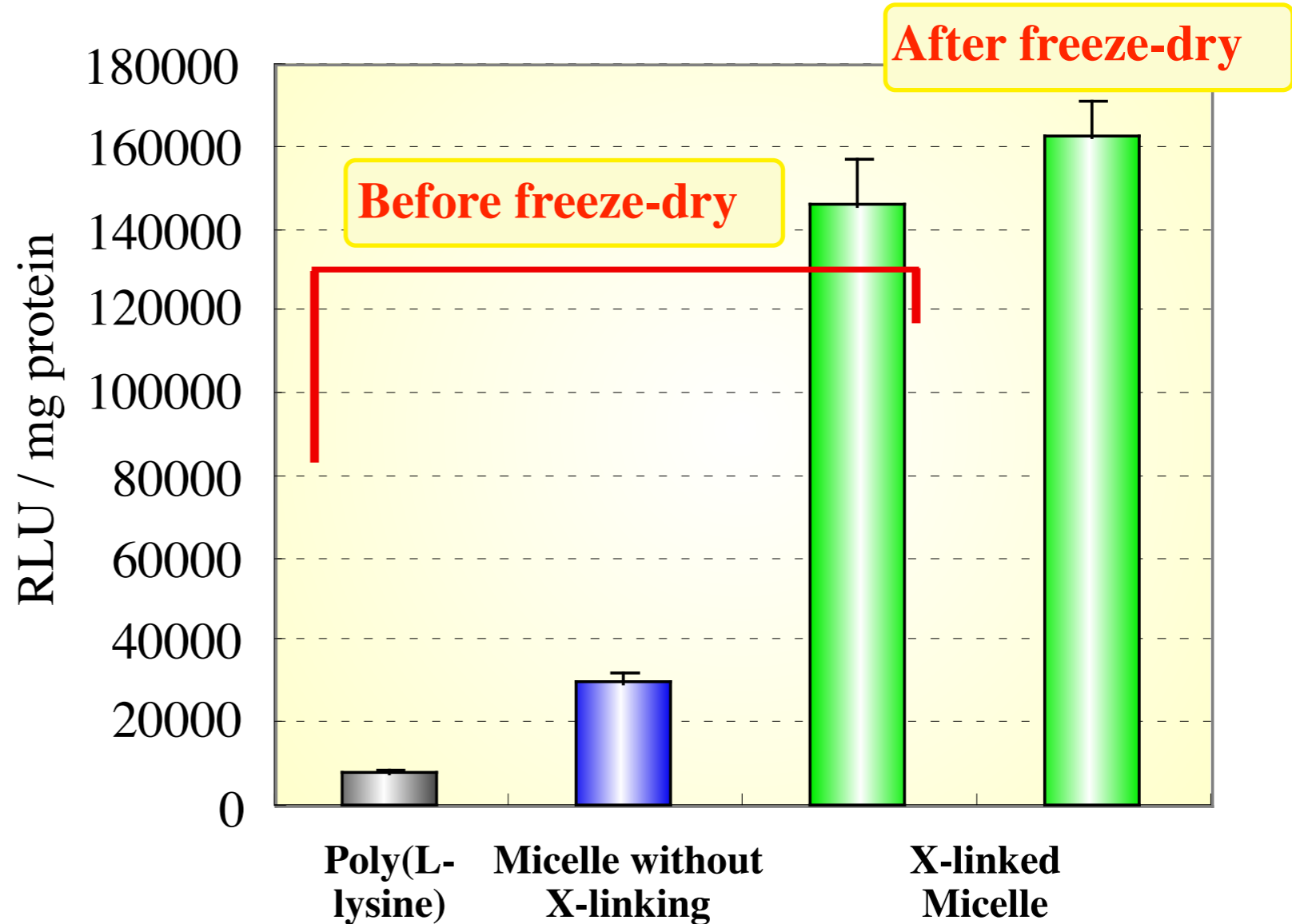
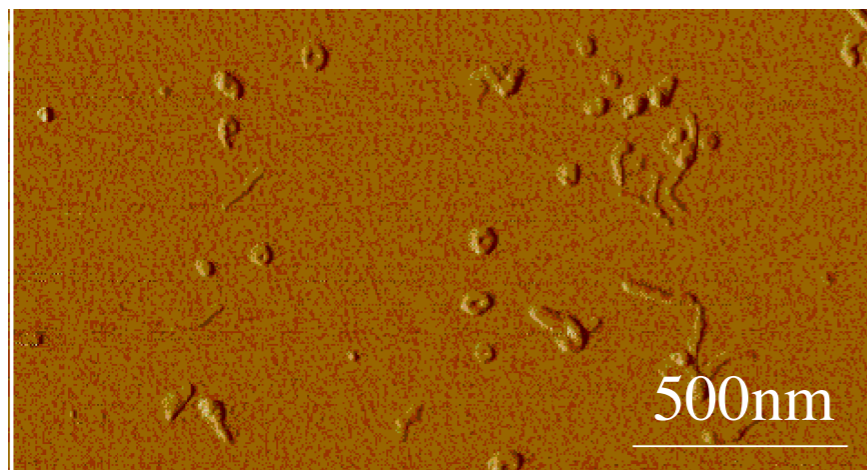
Enhanced gene transfection by freeze-dryable cross-linked micelle vector

	Poly(L-lysine)	Micelle without X-linking	X-linked Micelle
Size before freeze-dry (nm)	105.9	98.1	114.3
Size after freeze-dry (nm)	(1744.8)	(2176.5)	127.2

AFM of X-linked micelle

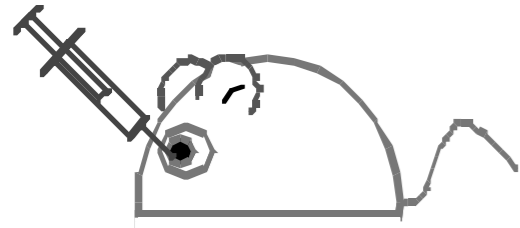


↓ After freeze dry



Liver transfection by systemic injection of cross-linked micellar vector

i.v. injection via
orbital vein

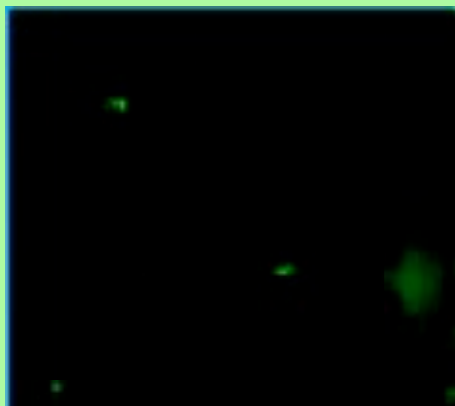


Liver was excised
at a defined day

The excised liver was treated with OCT
compound, and sliced with cryostat.

YFP gene expression in liver

Day 0



Day 1



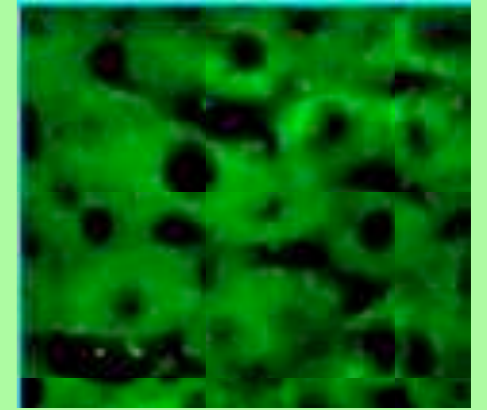
Day 2



Day 3

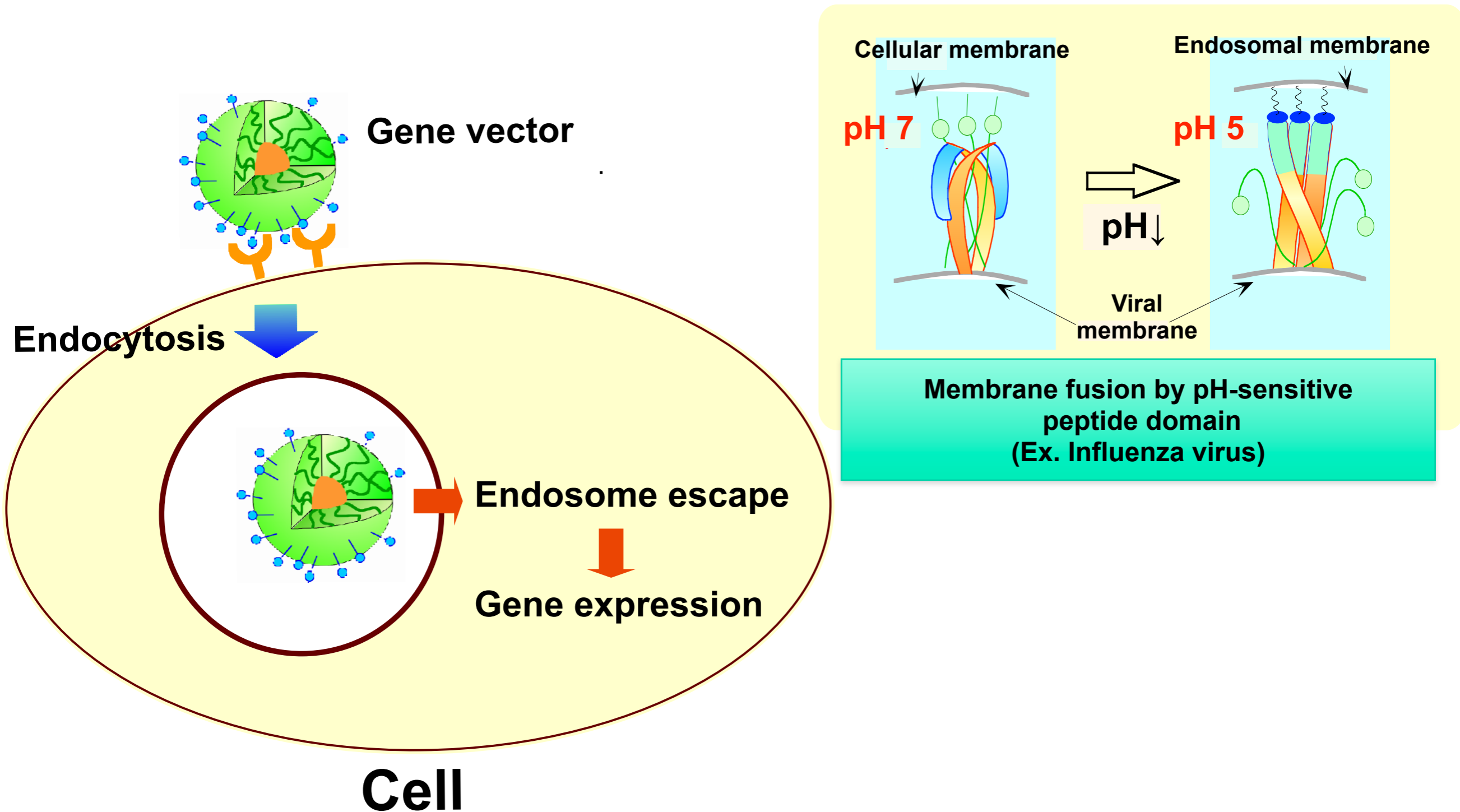


Day 5



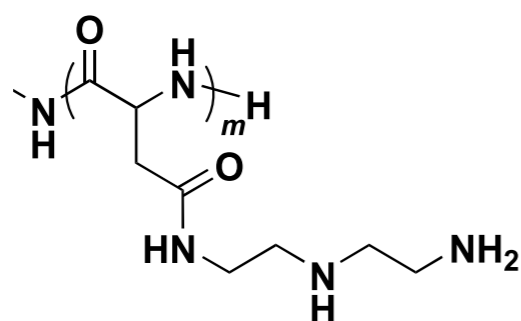
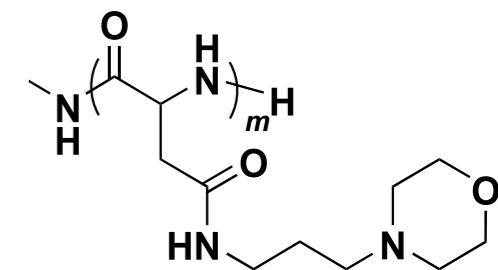
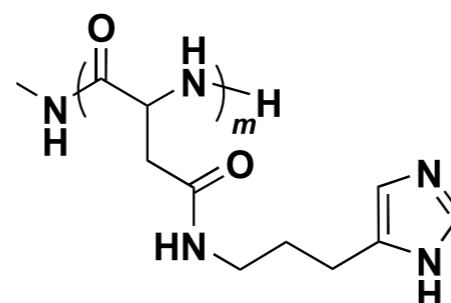
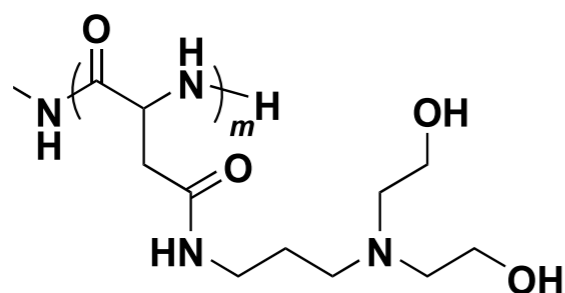
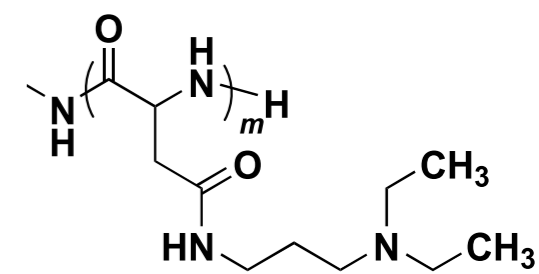
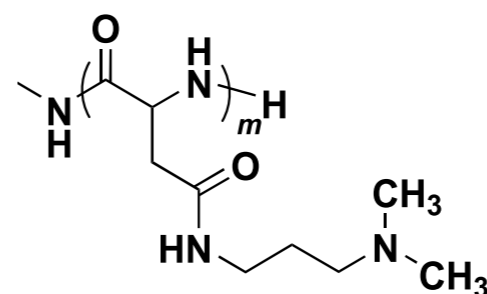
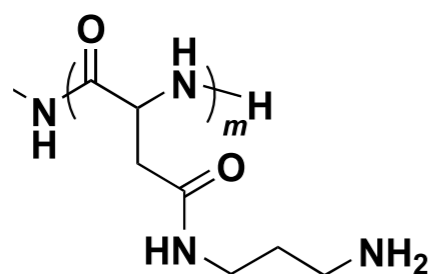
Homogeneous YFP gene expression was observed in liver parenchymal cells
5 days after i.v. injection of cross-linked polyplex micelles.

Endosomal escape: A key issue in intracellular gene and nucleic acid delivery

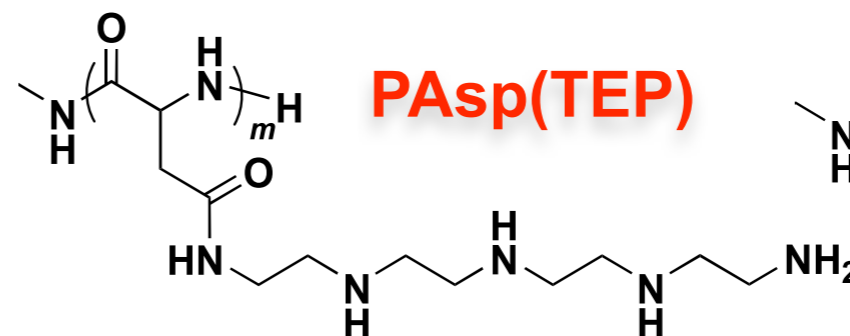
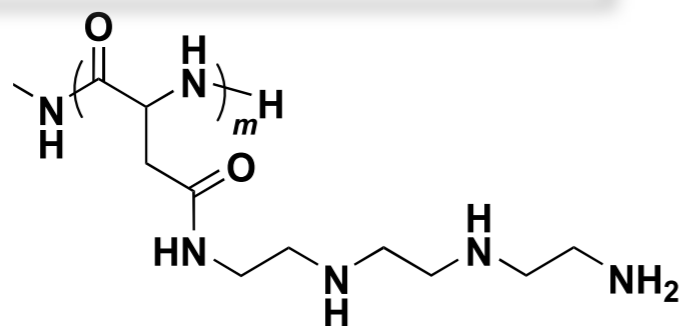
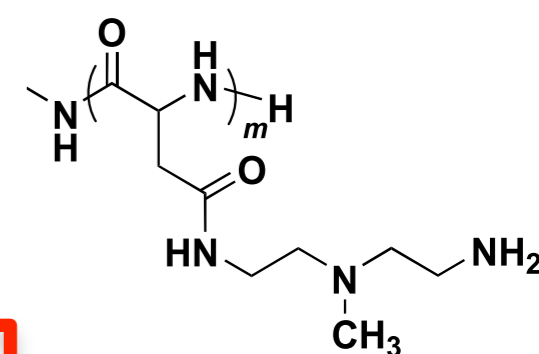
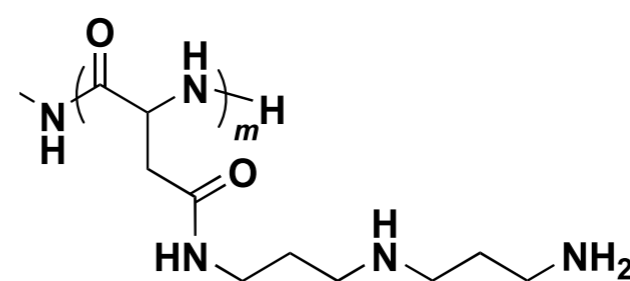


Challenge: Integrating endosome escaping units with minimum cytotoxicity into polyplex nanocarrier

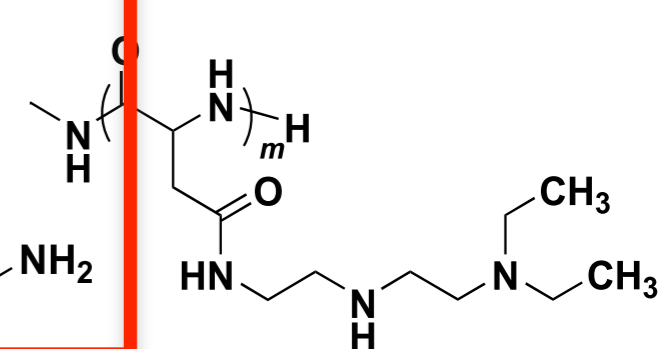
Preparation of a Series of Cationic Polyaspartamides through Aminolysis Reaction of Poly(beta-benzyl aspartate)



PAsp(DET)



PAsp(TEP)



Preparation of a Series of Cationic Polyaspartamides through Aminolysis Reaction of Poly(beta-benzyl aspartate)

Observation of endosomal escape

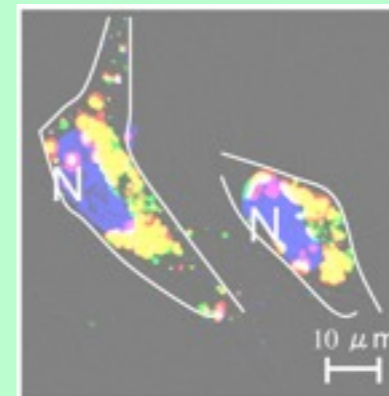
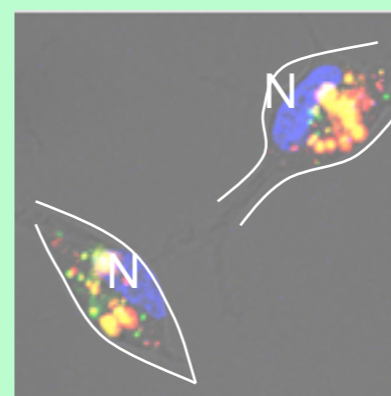
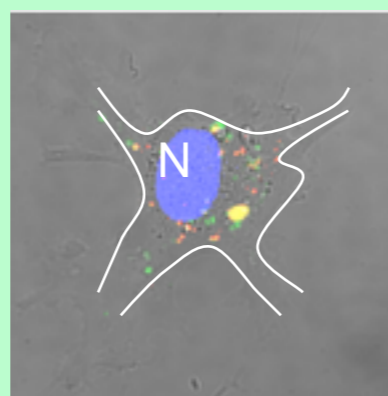
Incubation Time

3hr

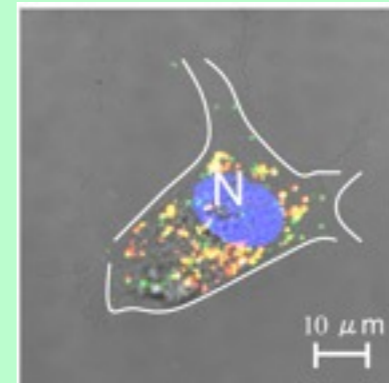
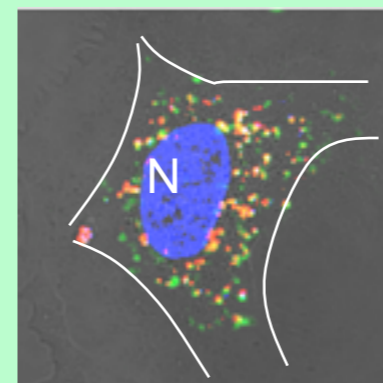
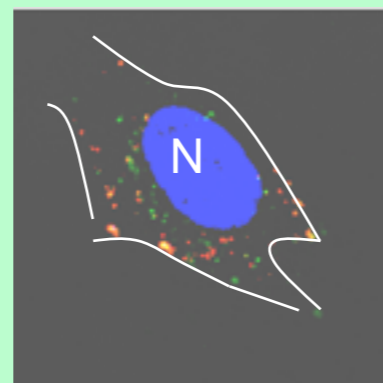
12hr

24hr

PAsp(DET)



P(Lys)

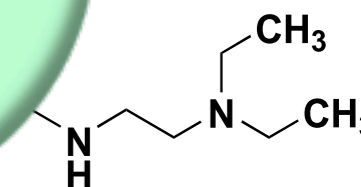
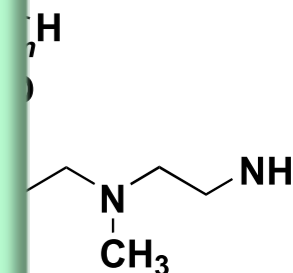
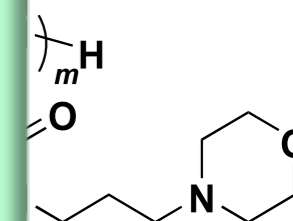
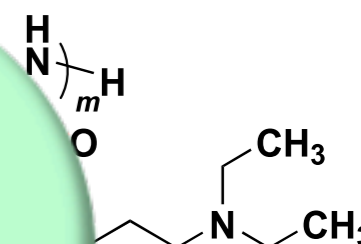


Green: Alexa-labeled dextran (endosome marker)

Red: Cy5-labeled pDNA

Blue: Hoechst 33258-stained nucleus

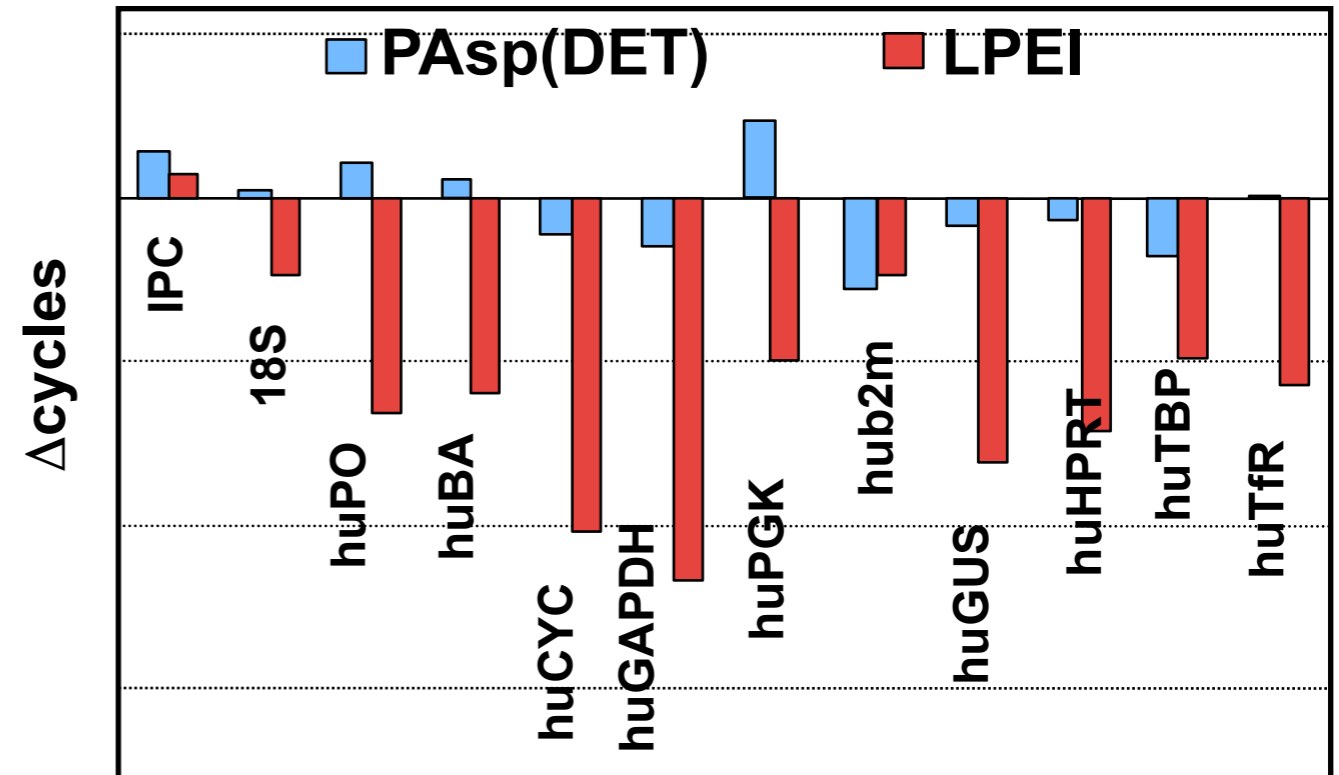
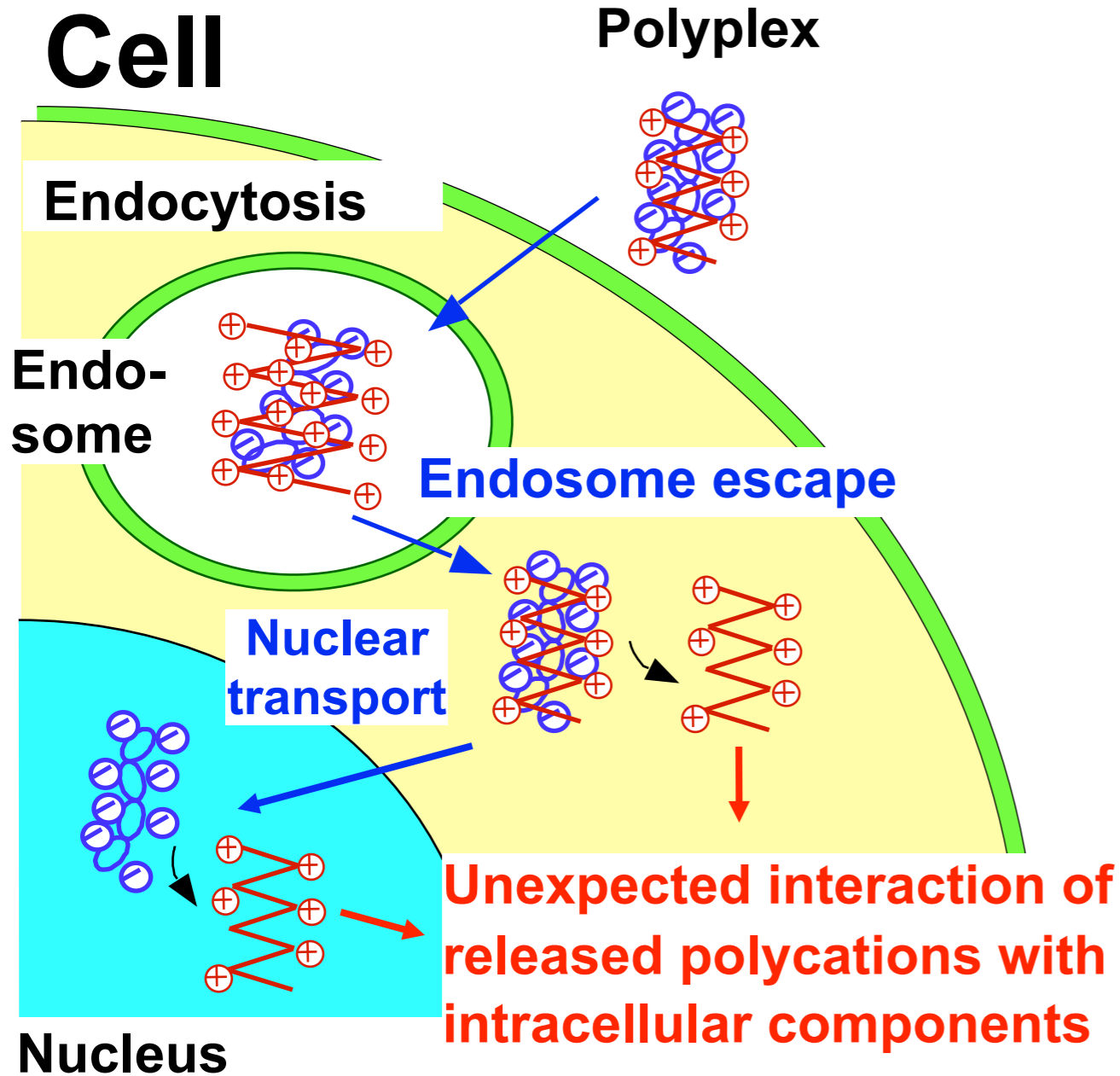
K. Miyata, et al, *J. Amer. Chem. Soc.*, 130, 16287-16294 (2008)



Biocompatibility assay of polycations by materials genomics

Adverse effect of polycations in polyplex due to the non-specific interaction with intra-cellular components

Change in the expression of house-keeping genes with polyplex transfection (Evaluation by real-time PCR)

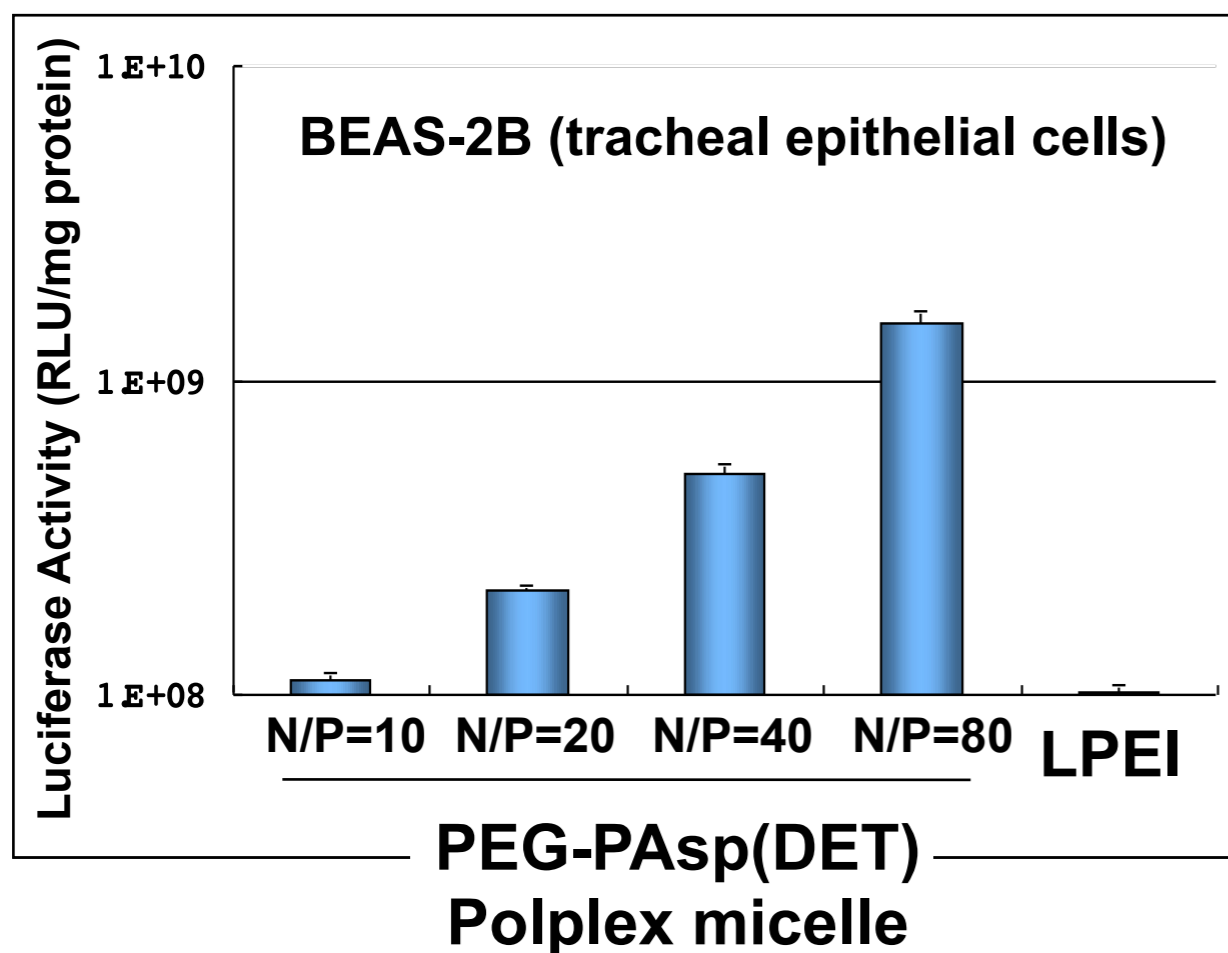


Significant decrease in the house-keeping gene expression for LPEI, yet no significant change for PAsp(DET)

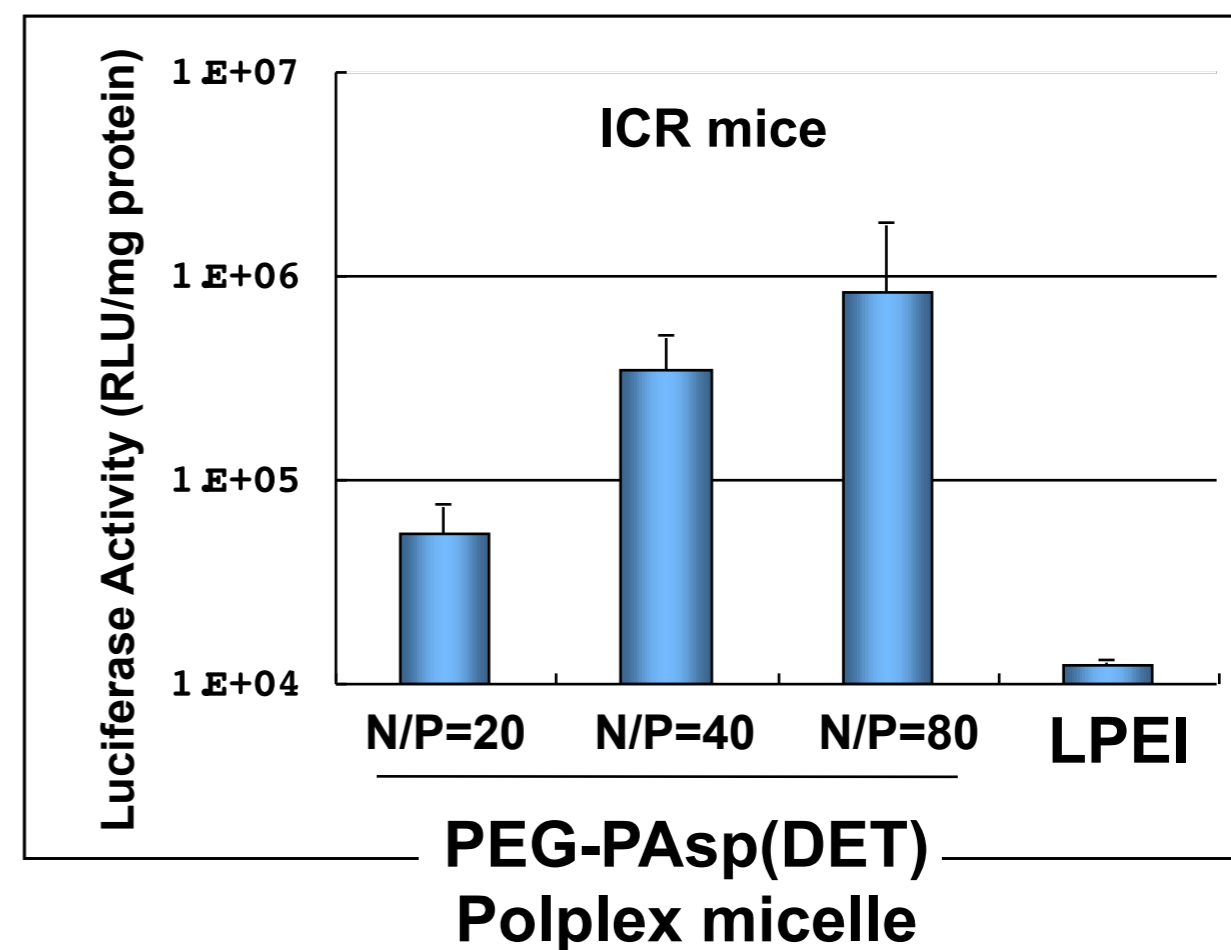
PAsp(DET) as biocompatible gene carrier from the standpoint of materials genomics

Gene Transfer to Lung by PEG-PAsp(DET) Polyplex Micells

Luciferase gene transfection to tracheal epithelial cells (in vitro)

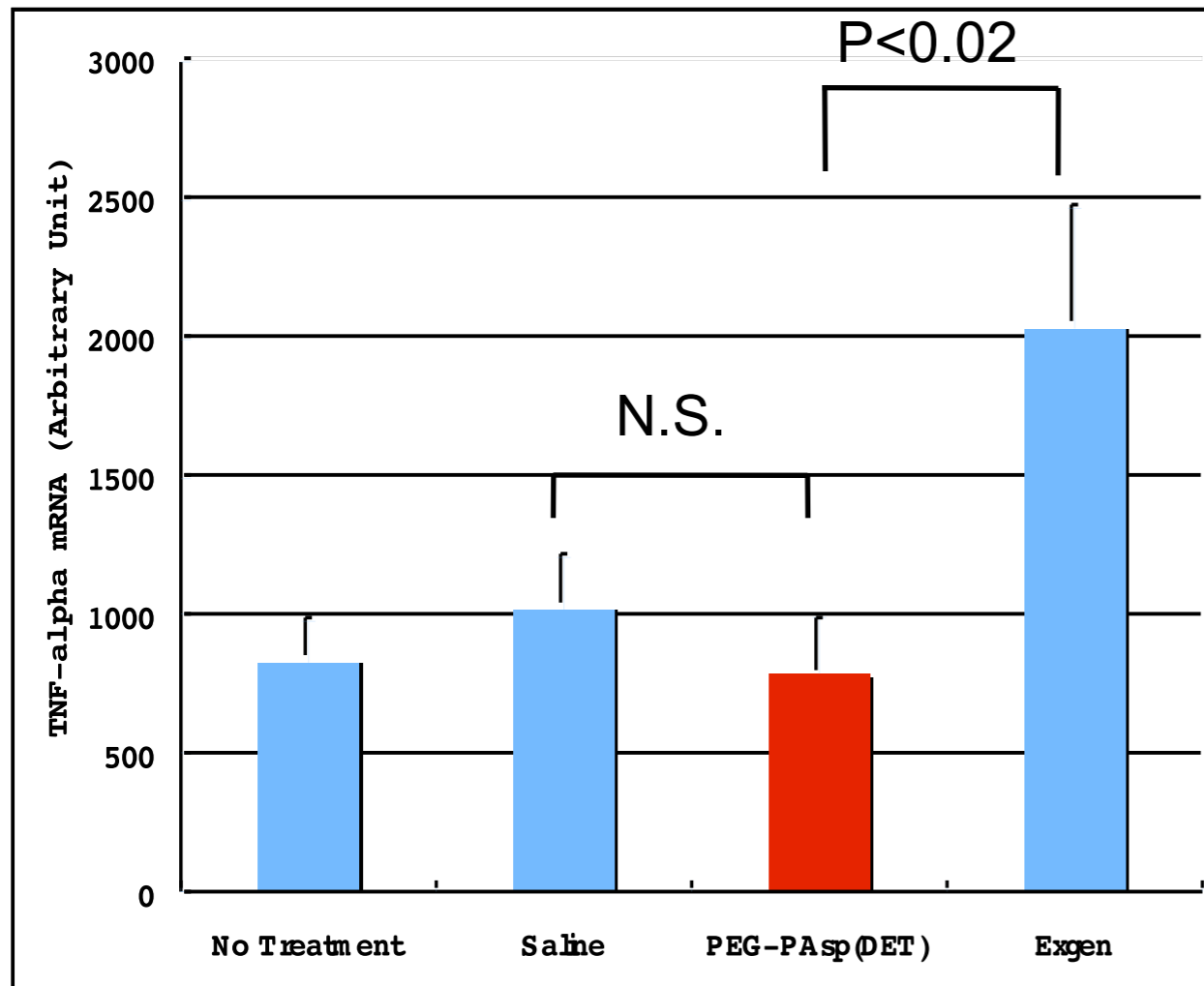


Luciferase gene transfection to lung via intratracheal administration (in vivo)

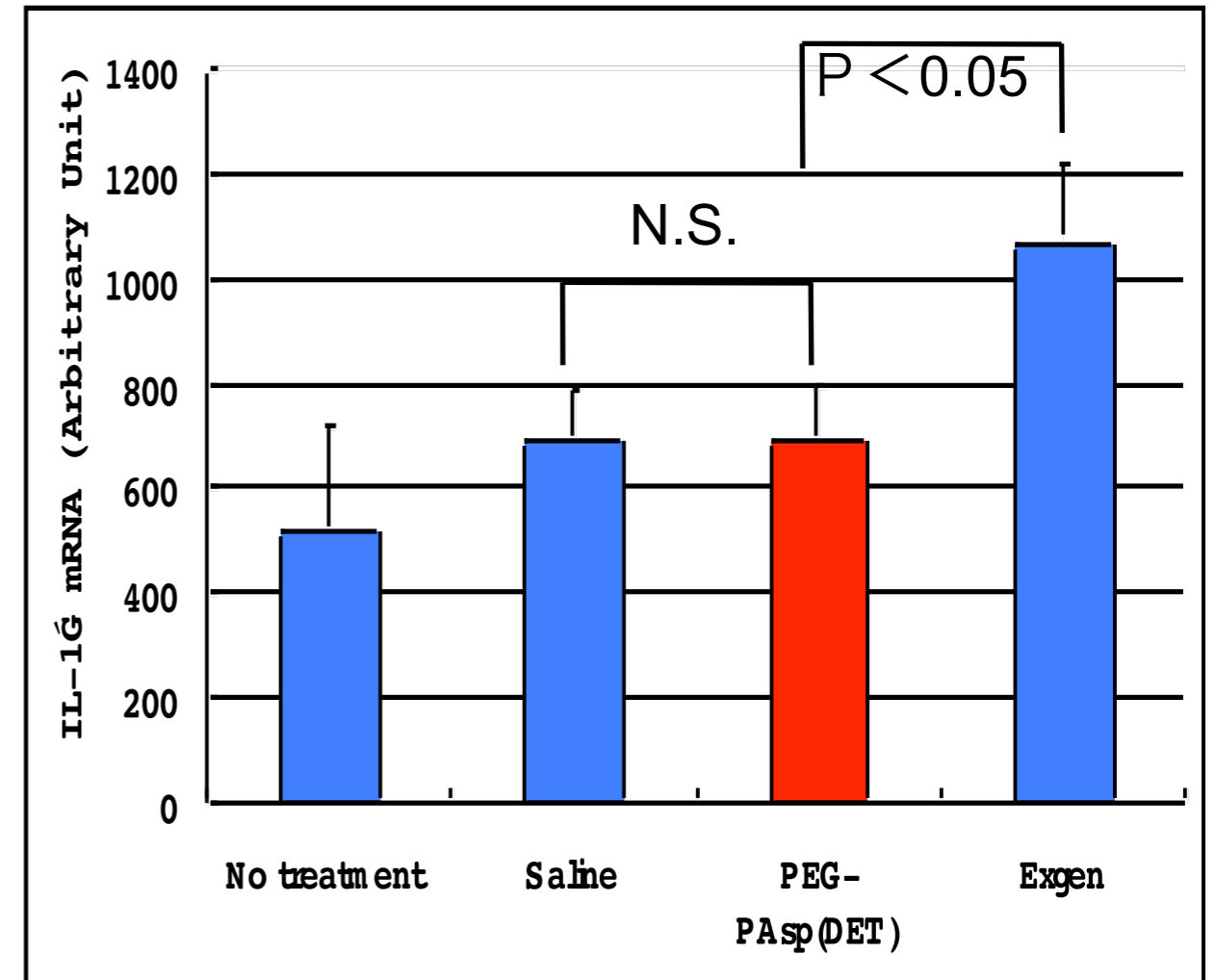


mRNA expression of inflammatory cytokines (TNF- α and IL-1 β) in the lung 1 week after the administration of polyplexes

TNF- α



IL-1 β



Adrenomedullin Gene Transfer by Intratracheal Administration of PEG-PAsp(DET) for the Treatment of PAH

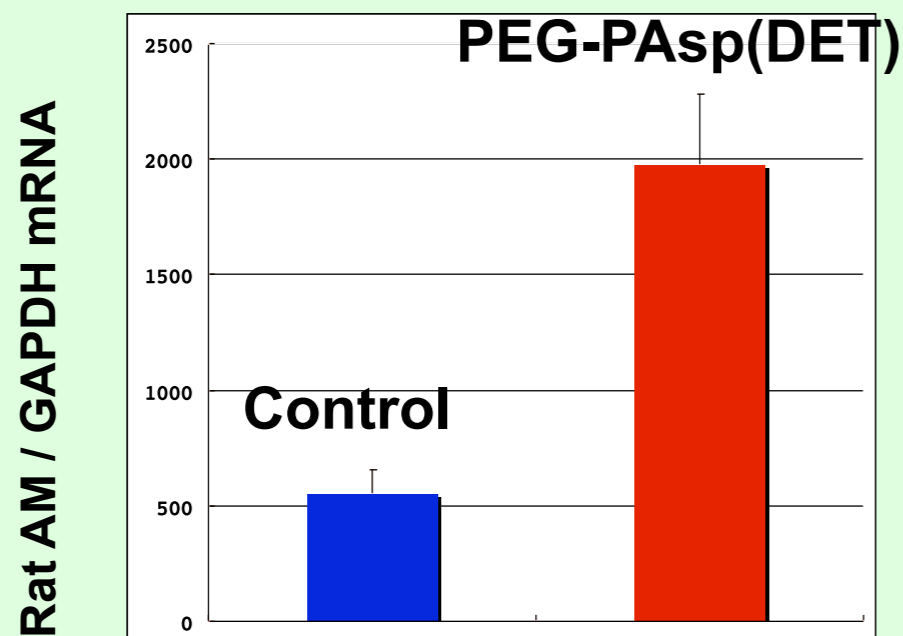
Model Animals for Pulmonary Hypertension

- Day 0** • Subcutaneous injection of monocrotaline
- Day 25** • Measurement of right ventricular pressure by catheter
- Gene transfer of AM gene by intratracheal administration
- Day 28** • Measurement of right ventricular pressure by catheter again and remove of the lung to measure RNA

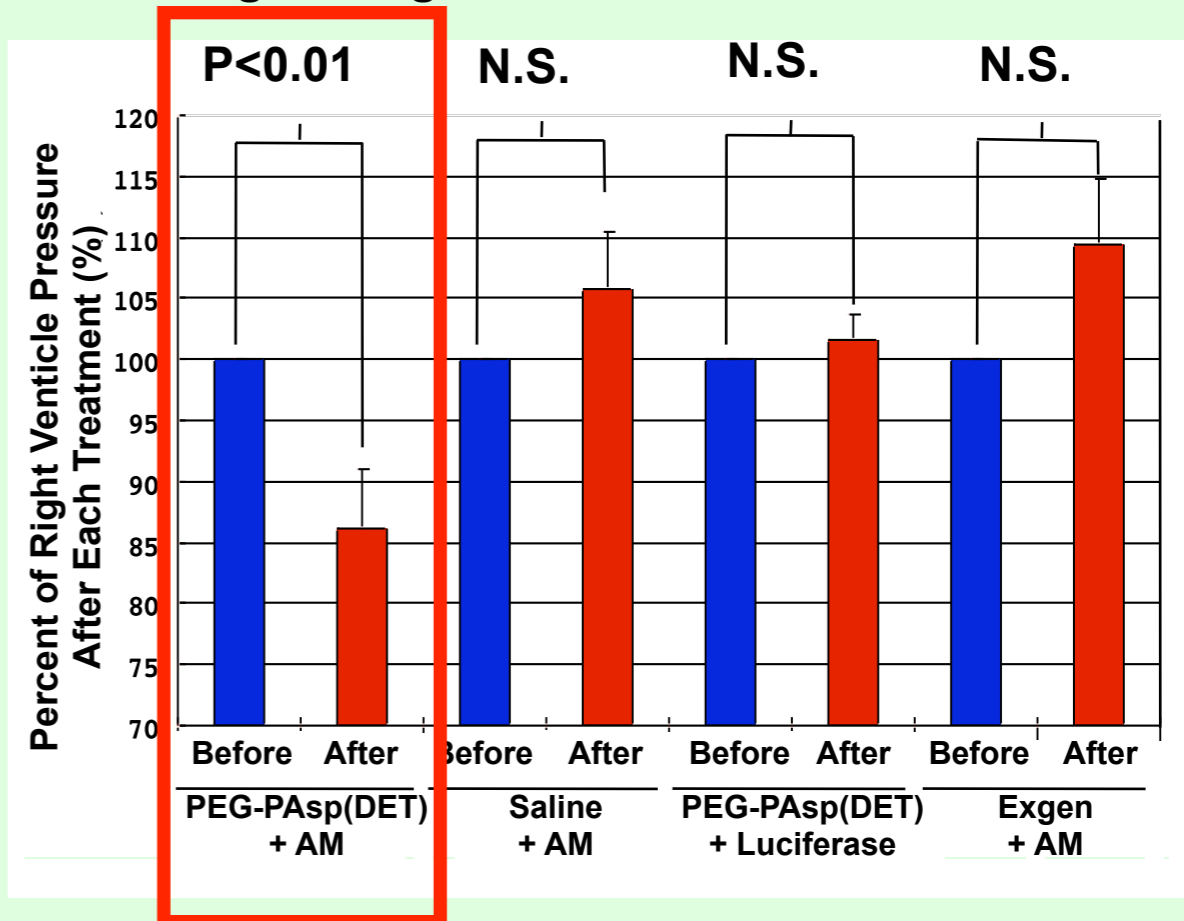
Pulmonary Arterial Hypertension

- Life-threatening disease characterized by progressive pulmonary arterial hypertension
- Death after 2 to 10 years of diagnosis.

Measurement of adrenomedullin mRNA by Real Time RT-PCR



Change in Right Ventricular Pressure



M. Shiba, et al, *Molecular Therapy*, 17(7) 1180-1186 (2009)

Trinity in Regenerative Medicine

Cell

- ES cell
- MSC cell
- iPS cell

Differentiation Control

- Drug
- Gene, siRNA
- Bioactive substance

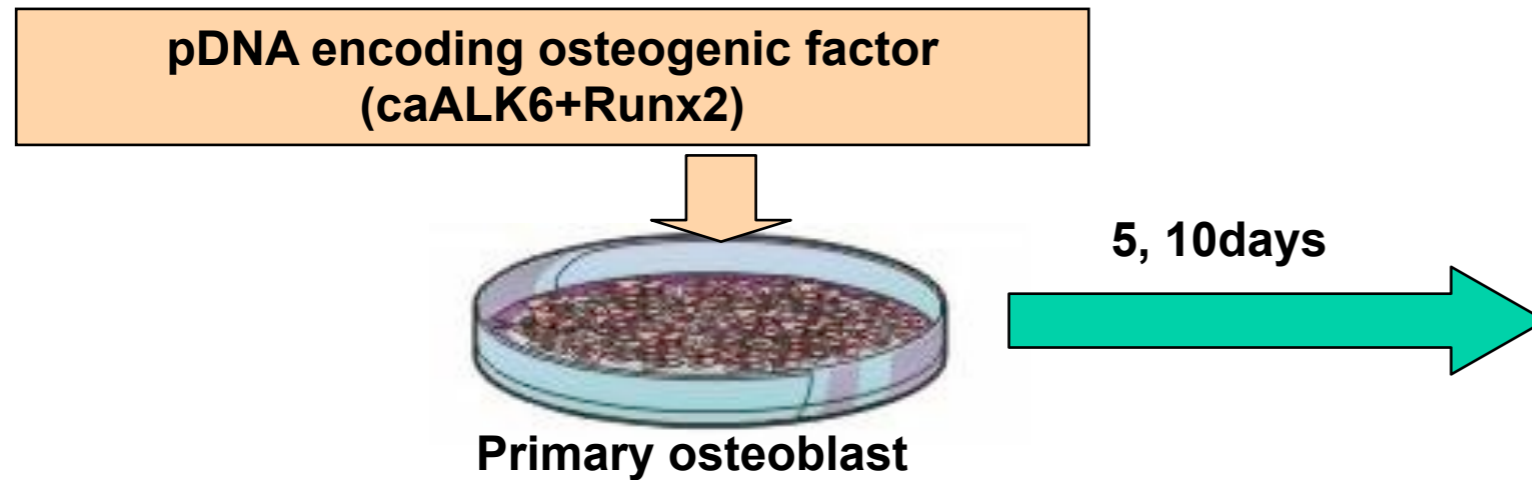
Scaffold

- PLLA, PLGA
- Calcium Phosphate
- Collagen

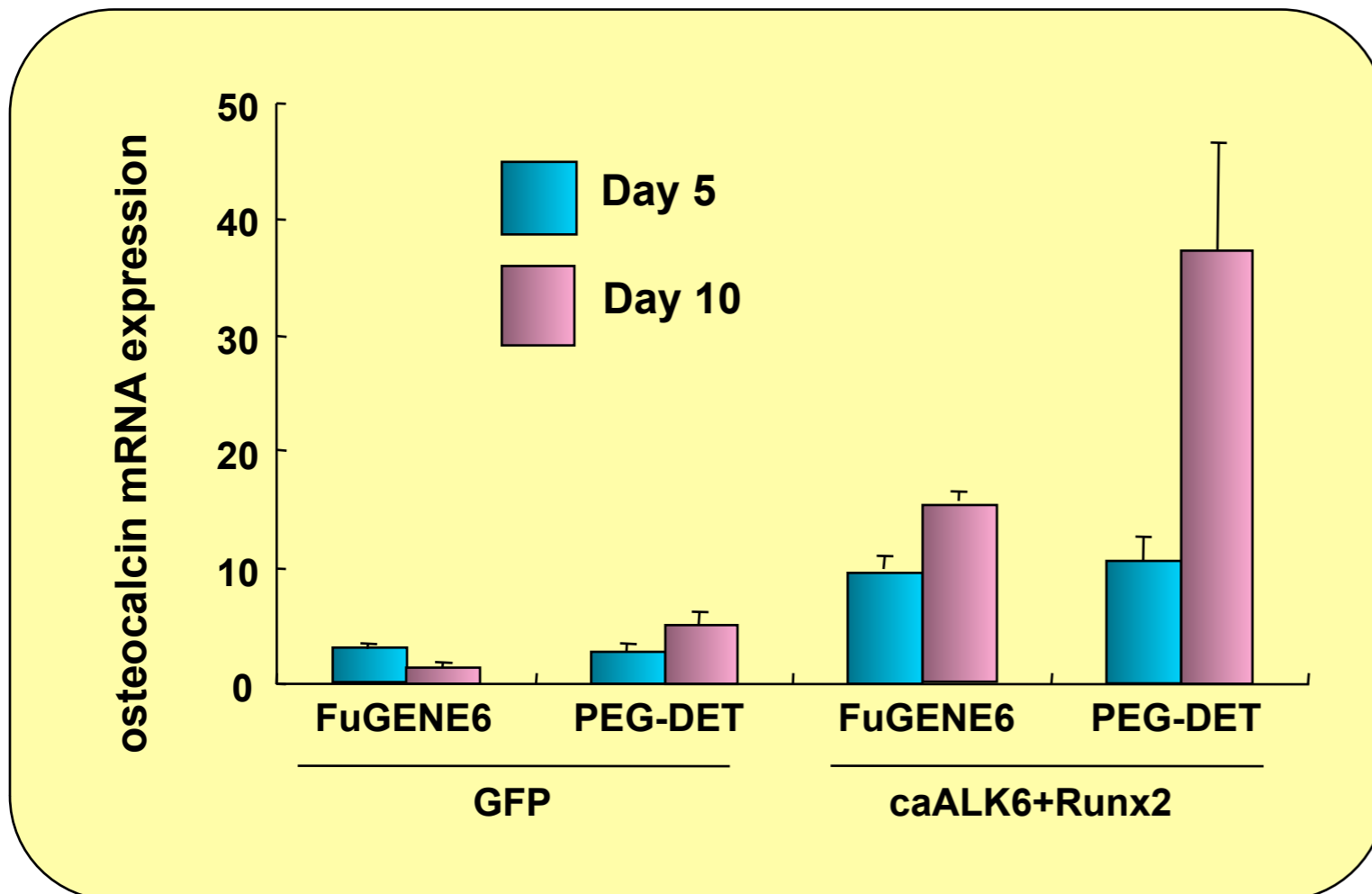


Need for drug and gene delivery systems

Induction of cell differentiation by delivering genes encoding osteogenic factor with polyplex micelles

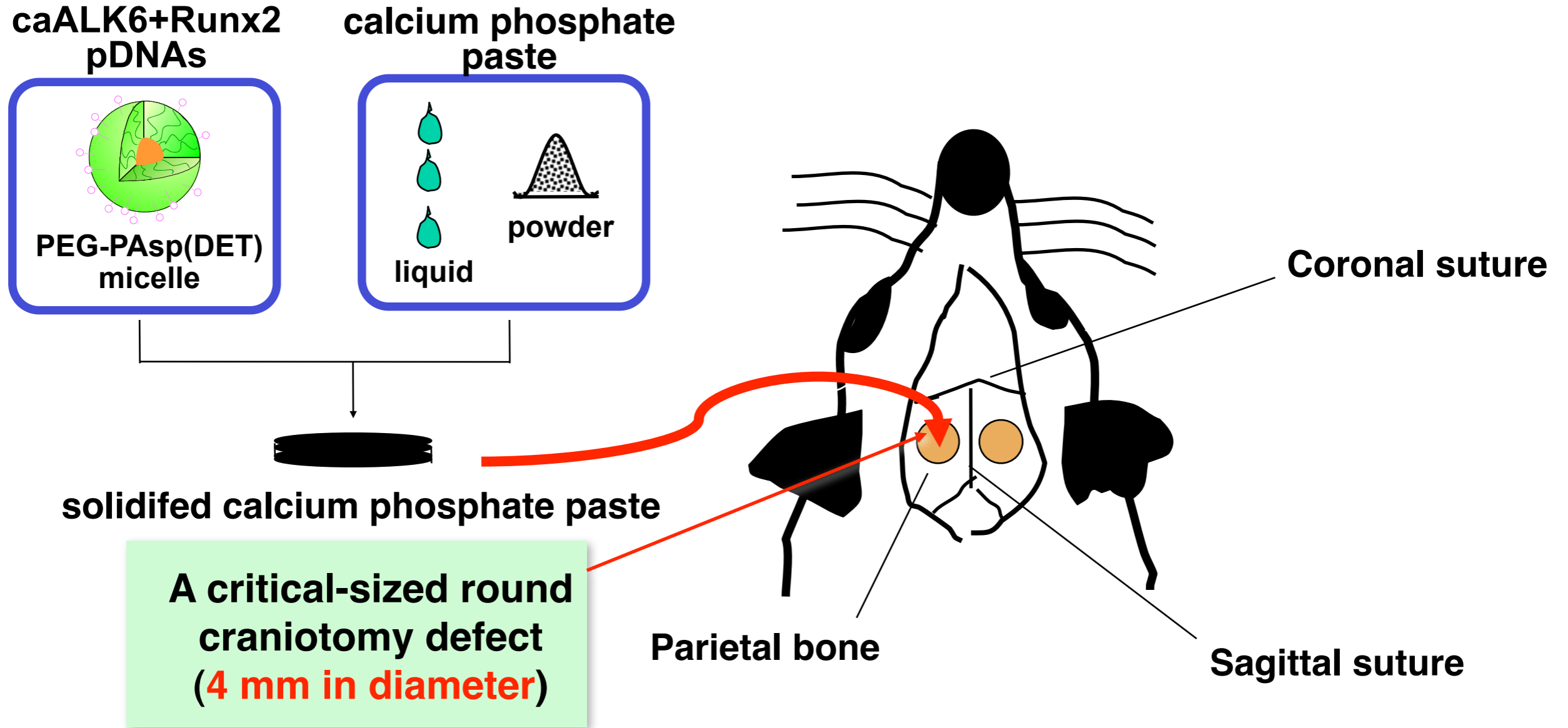


Estimation of osteocalcin (osteoblast differentiation marker) mRNA expression by real-time RT-PCR



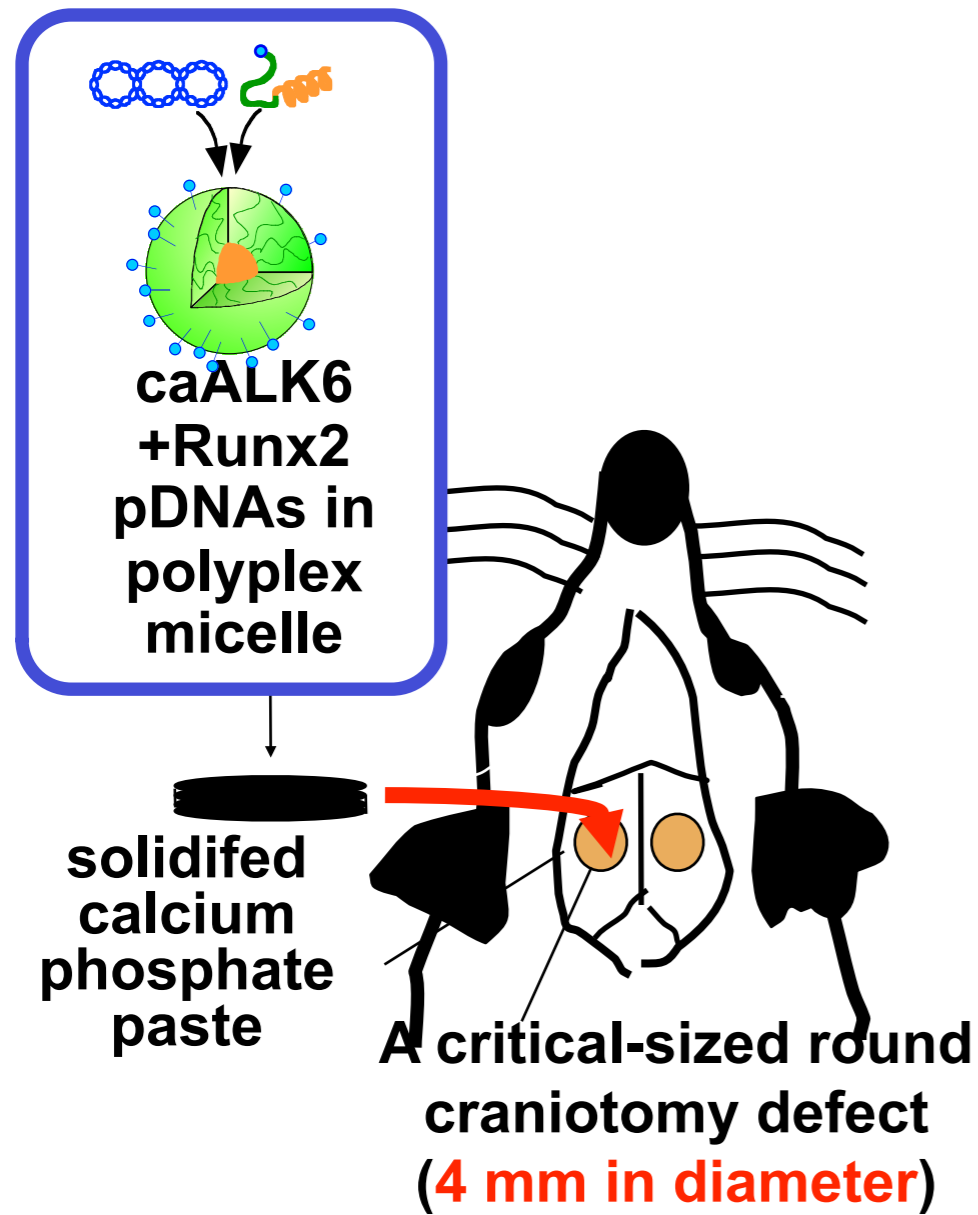
Only polyplex micelles successfully induce the cell differentiation.

Bone regeneration based on *in vivo* transduction without cell source

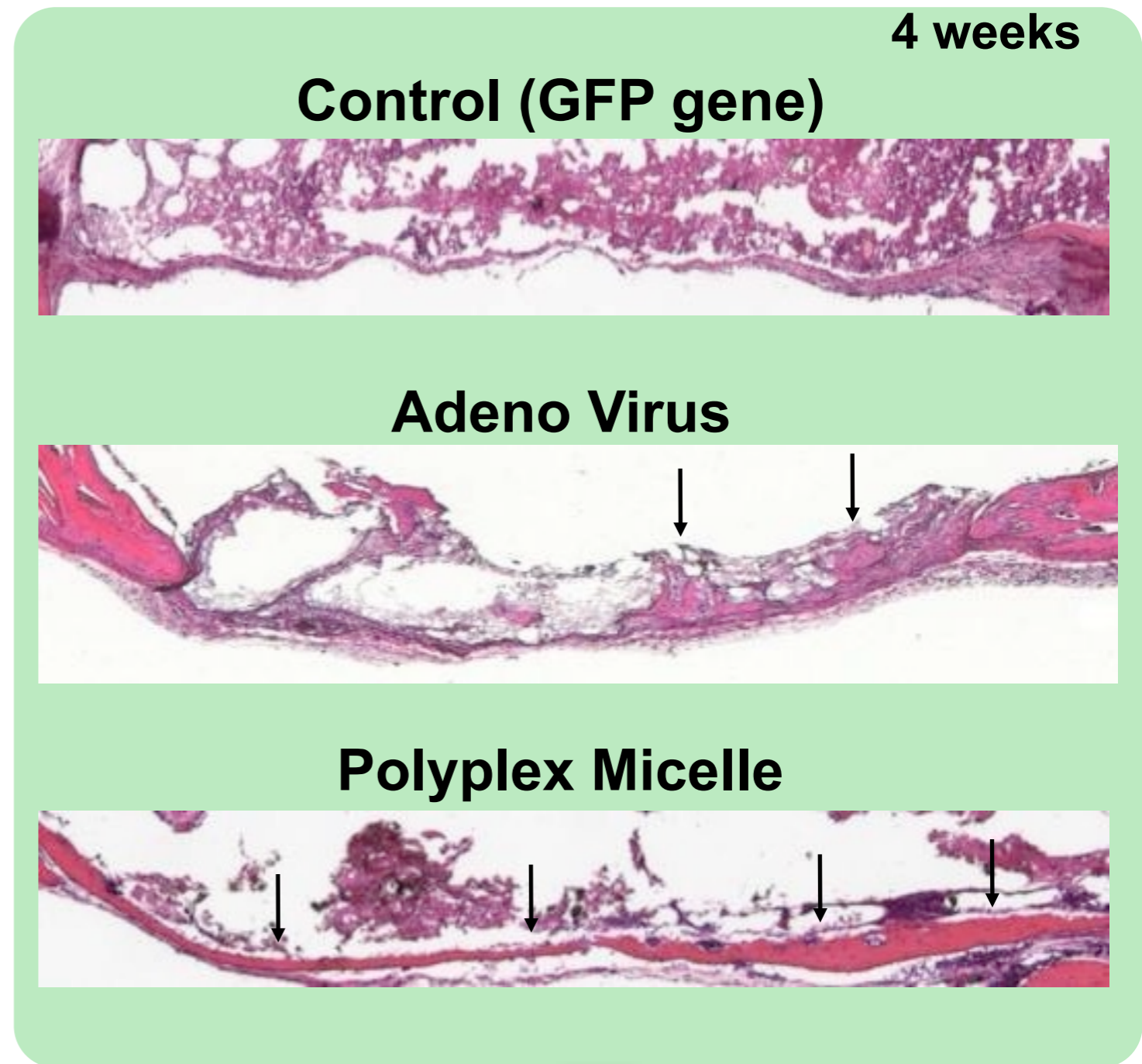
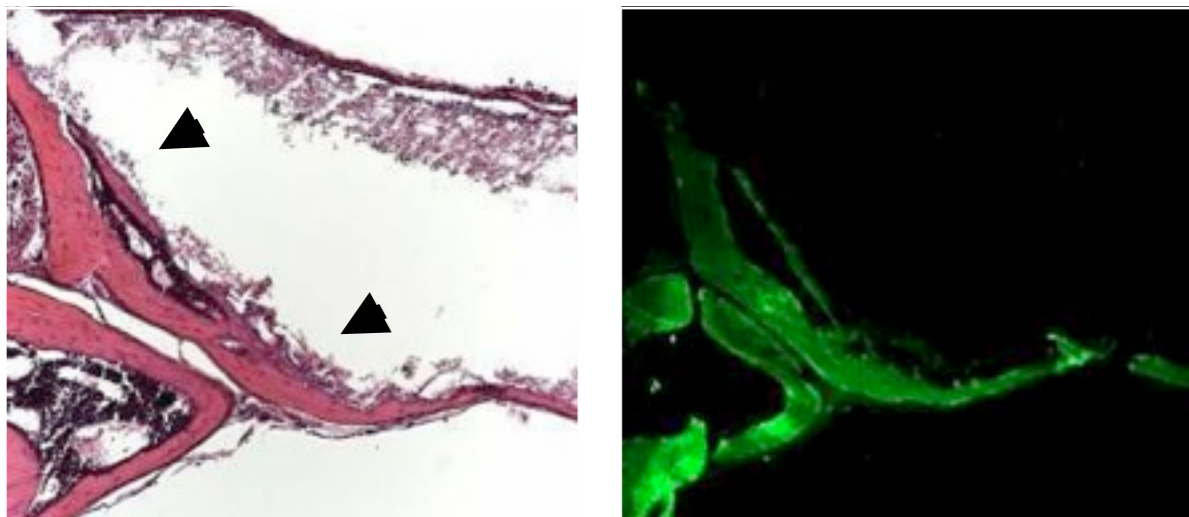


- **Solidified calcium phosphate paste containing Runx2 and caALK6-expressing pDNAs (1.3 $\mu\text{g}/\text{mouse}$)** were placed to cover the defects.
- The mice were sacrificed at 2, 4, 6 weeks after the operation for histological analyses.

Bone regeneration based on *in vivo* transduction without cell source



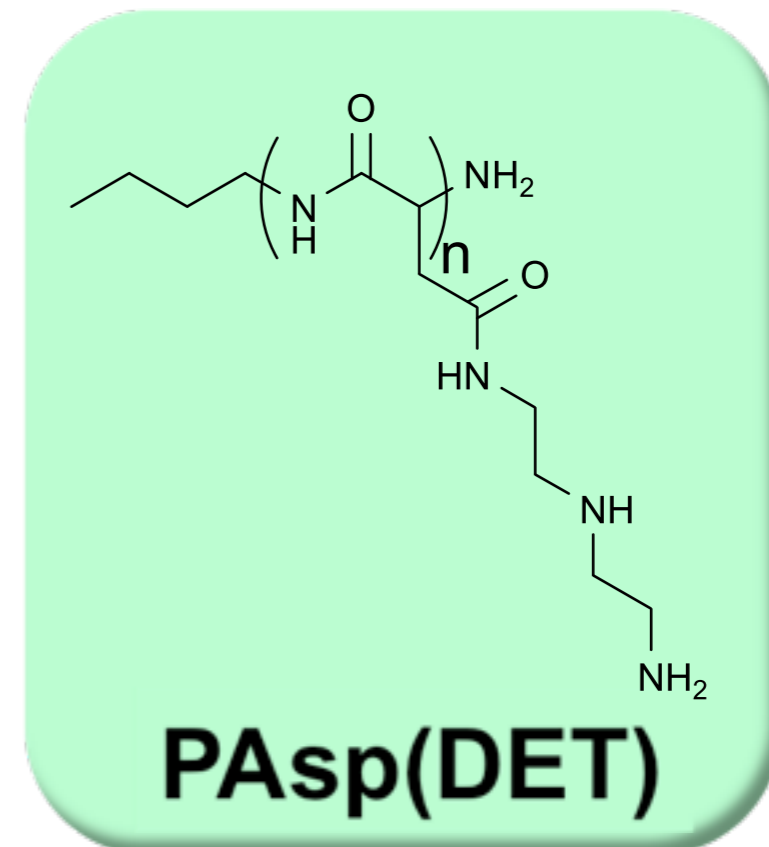
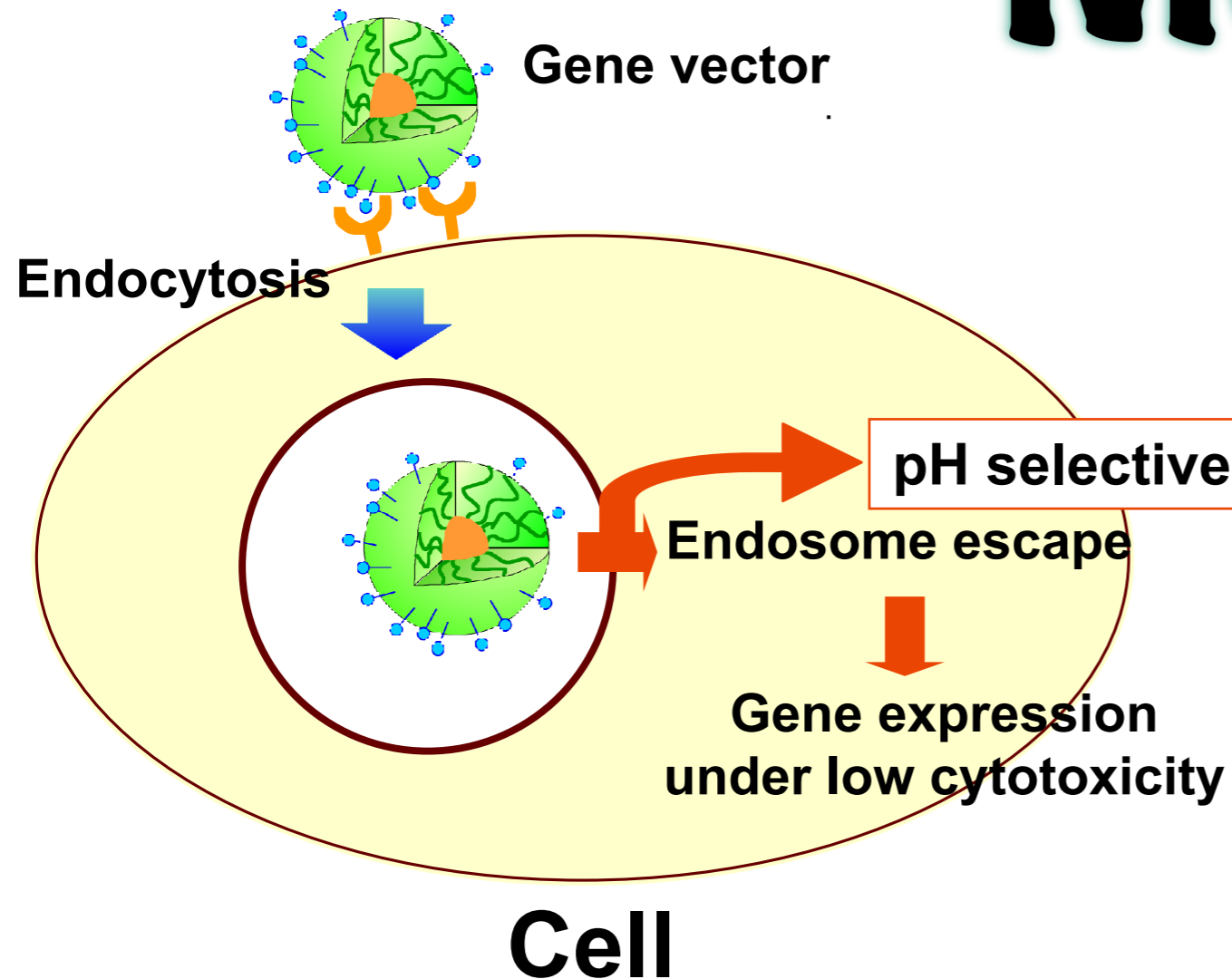
Immuno-staining of Type I collagen



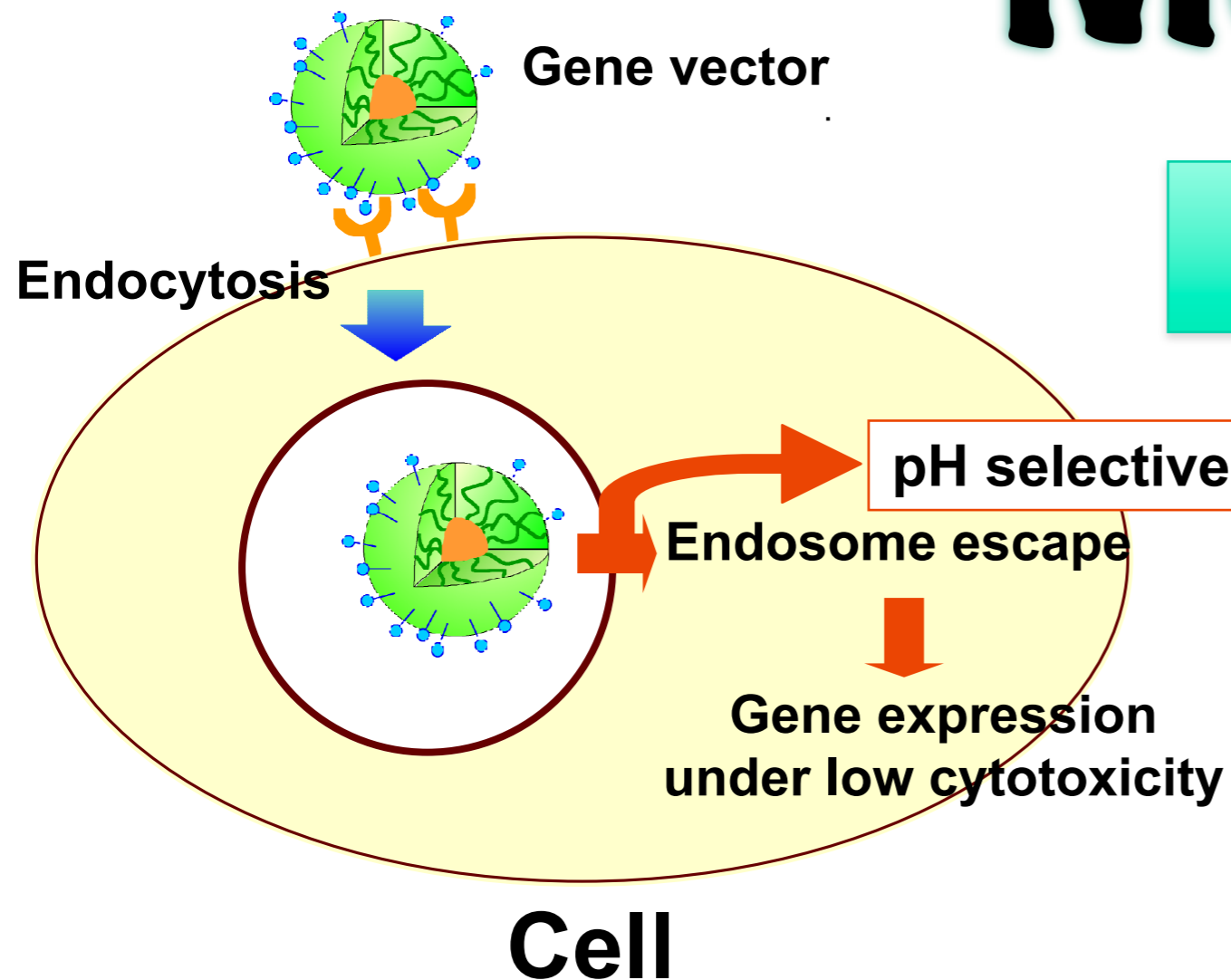
Polyplex micelles exceeded adeno virus to reveal substantial bone formation without inflammation

K. Itaka, et al, Molecular Therapy
15(9), 1655-1662 (2007)

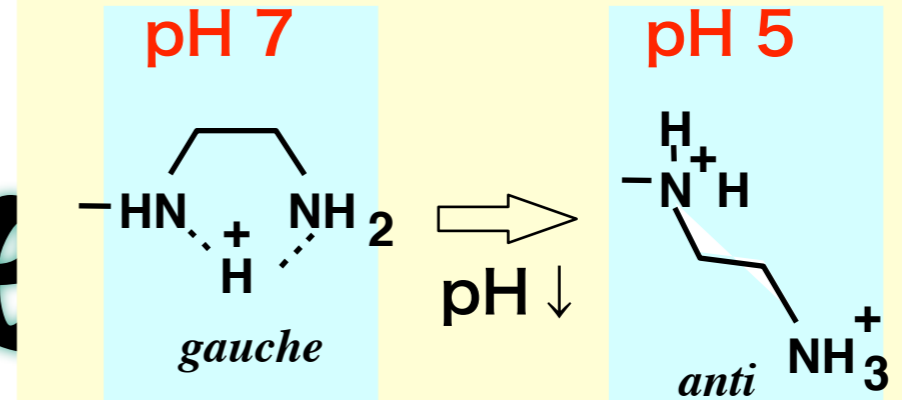
Mechanism?



Mechanism of Endosomal Escape

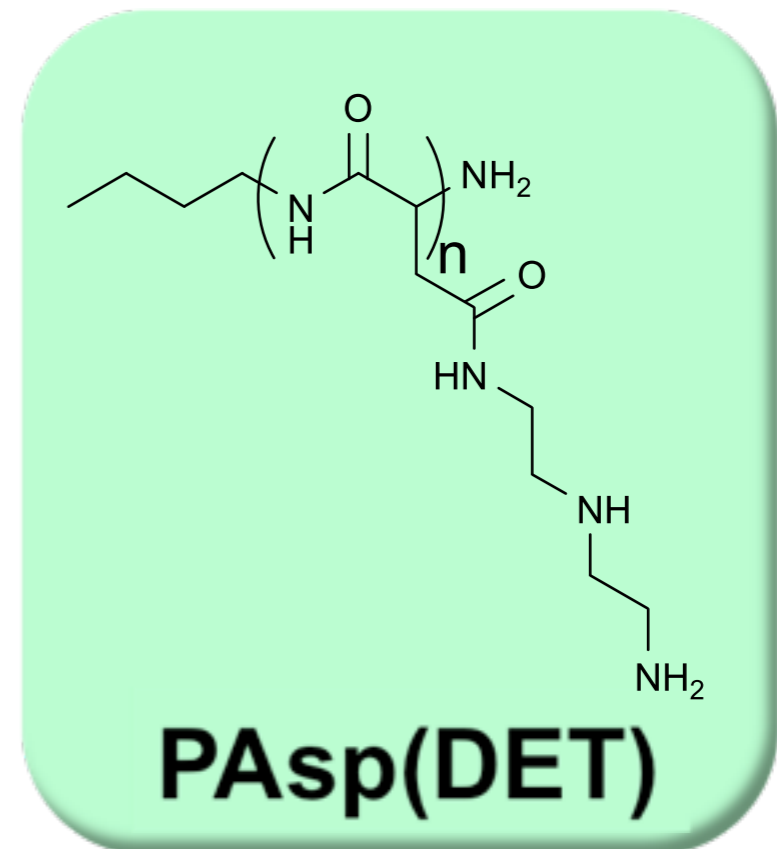


Me

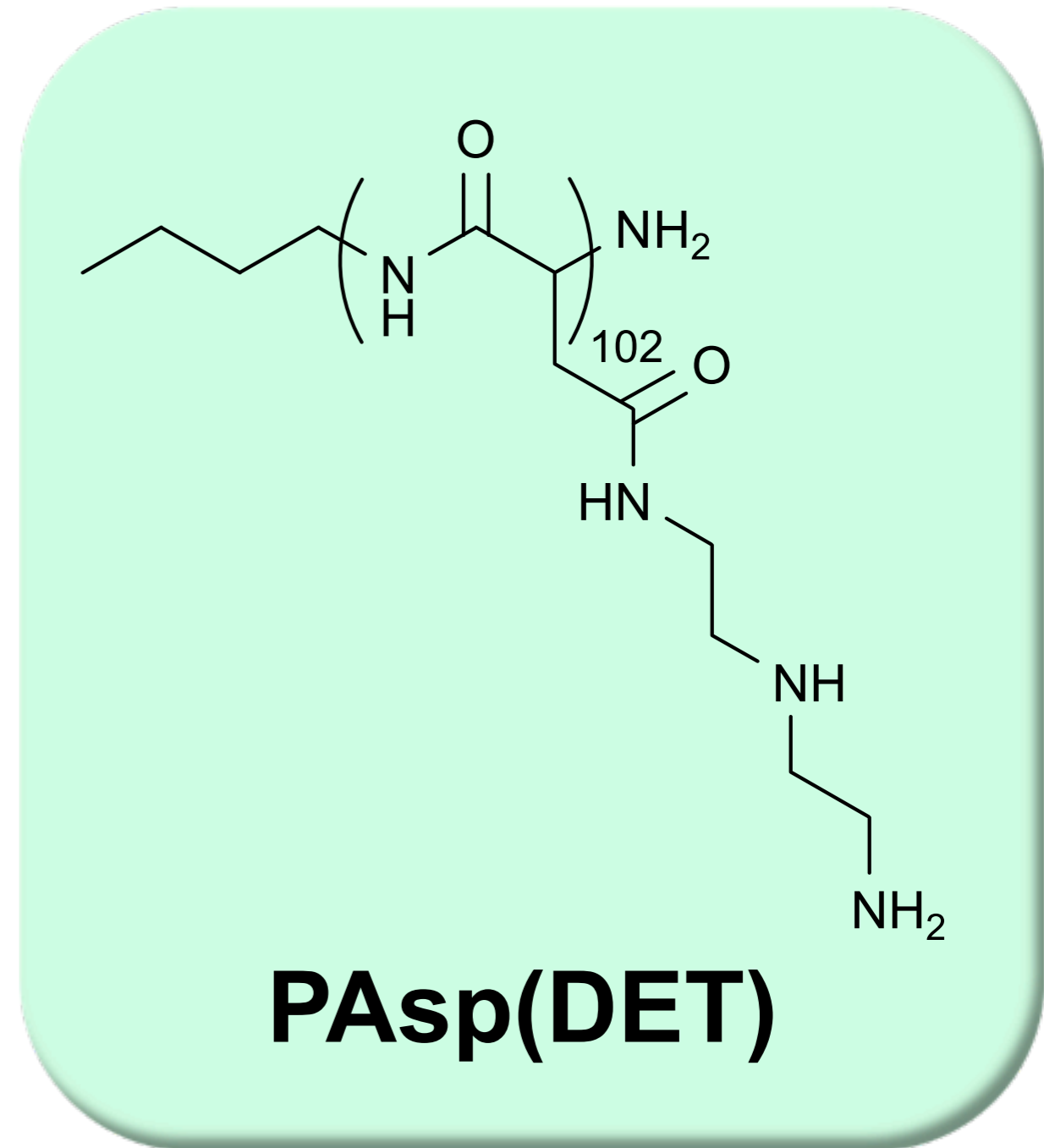
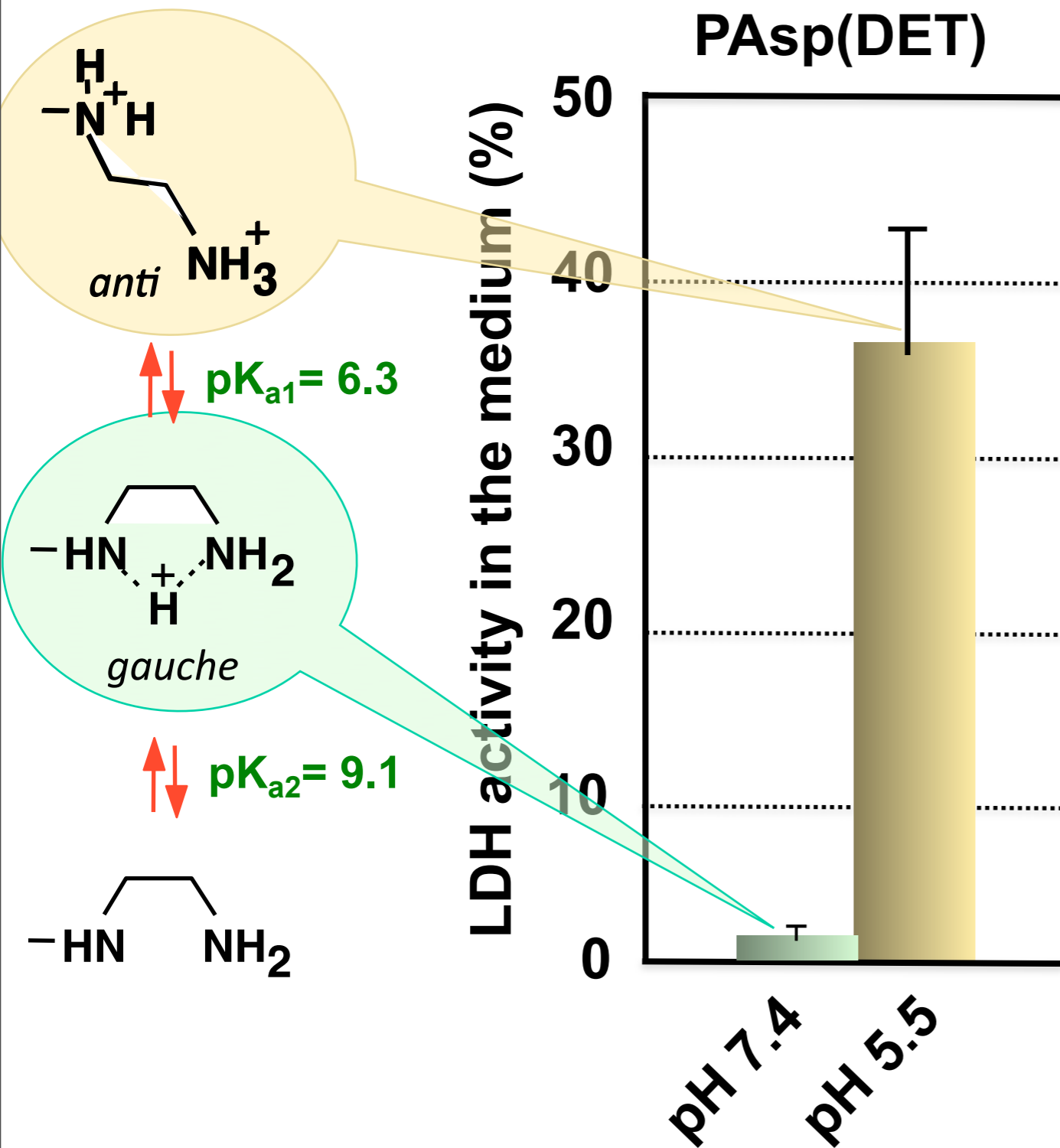


Membrane disruption induced by the protonation of diaminoethane units

?

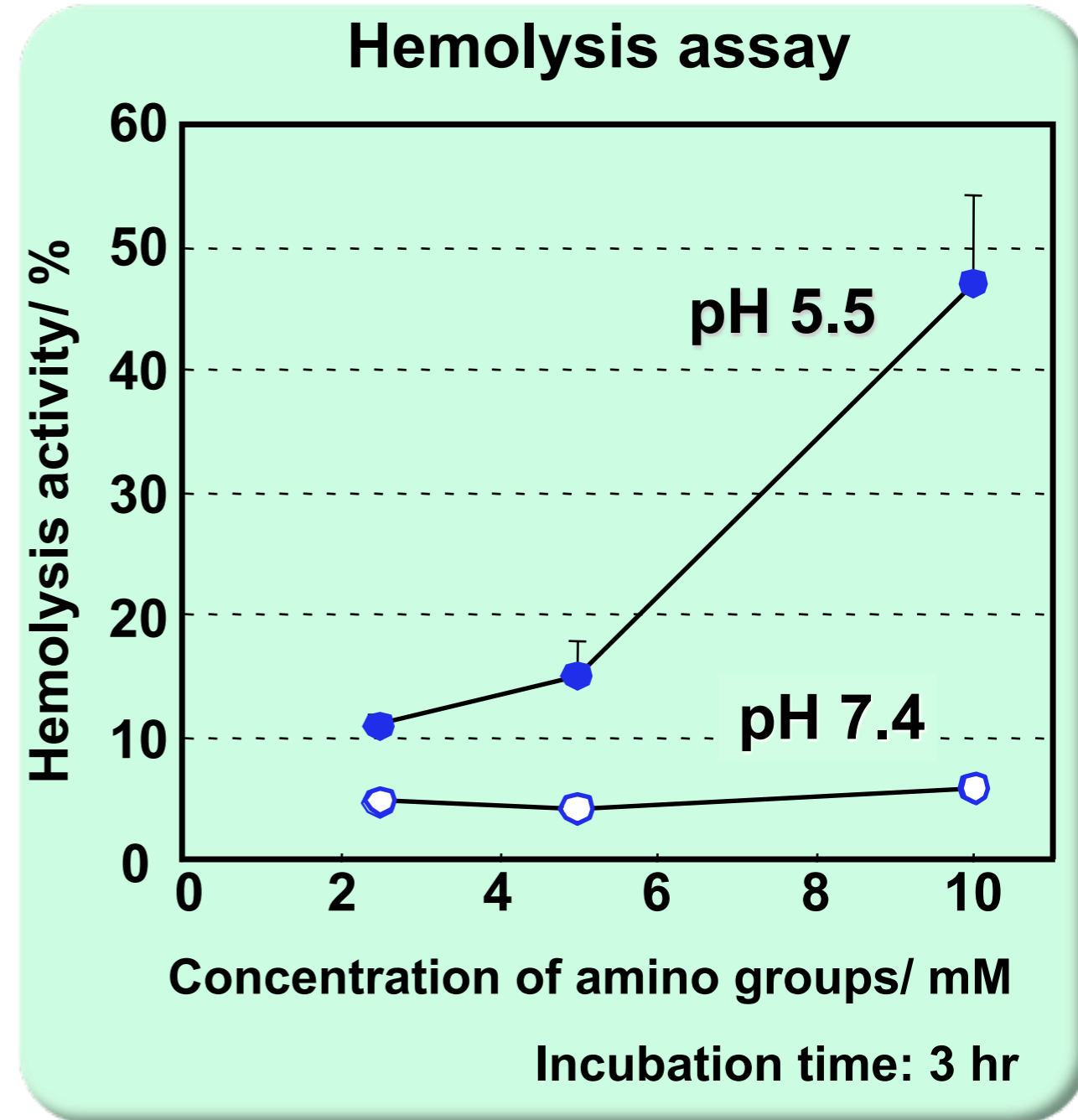
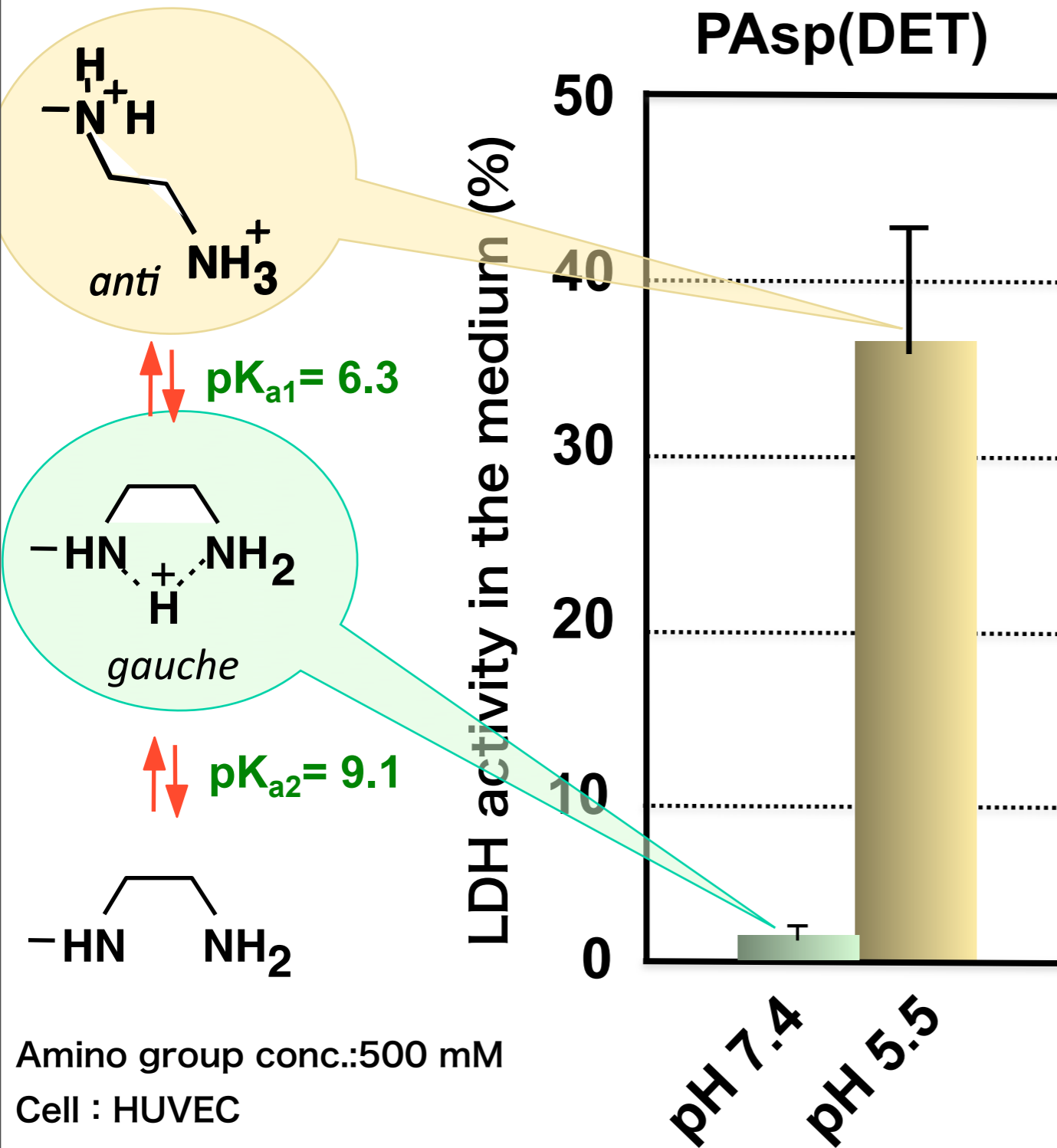


Destabilization of endosomal membrane: Assay by the leakage of cytoplasmic enzyme (LDH)



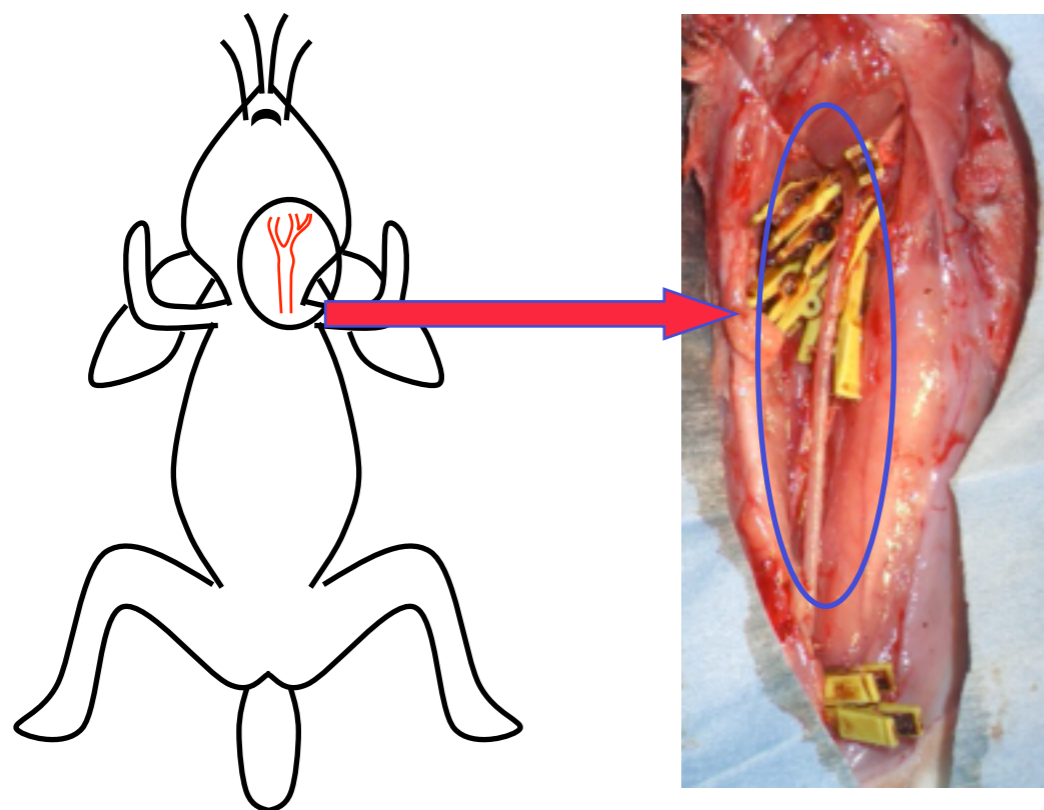
Amino group conc.: 500 mM
Cell : HUVEC

Destabilization of endosomal membrane: Hemolysis Assay



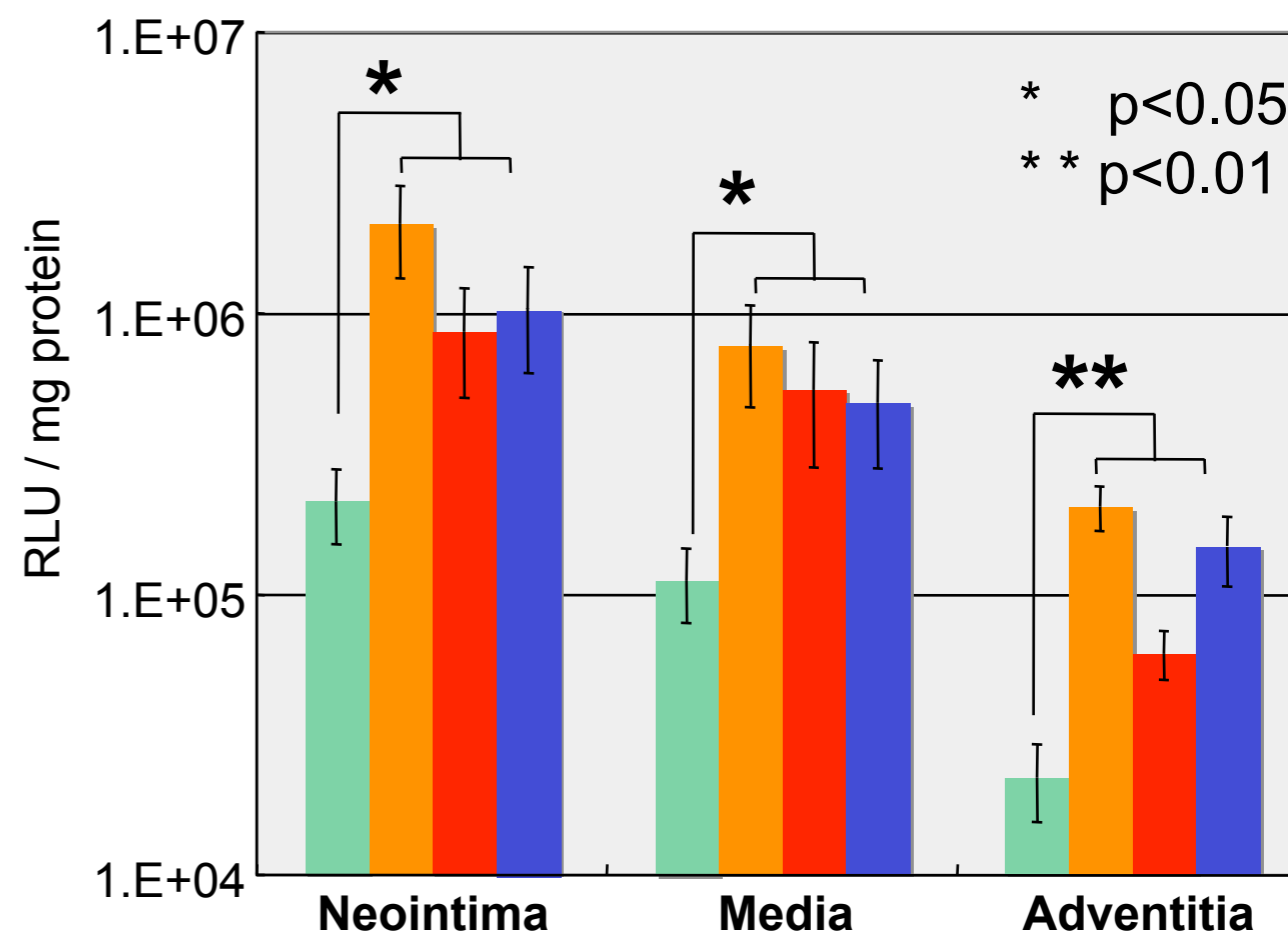
PAsp(DET) exerts membrane destabilization selectively at pH 5.5 to facilitate endosomal escape of polyplex micelles

Gene expression to rabbit carotid artery by micellar nano-vector



- Naked pDNA
(100% patency)
- BPEI polyplex N/P10
(62.5% patency)
- P[Asp(DET)] polyplex N/P 40
(50% patency)
- PEG-*b*-P[Asp(DET)] micelle N/P 40
(100% patency)

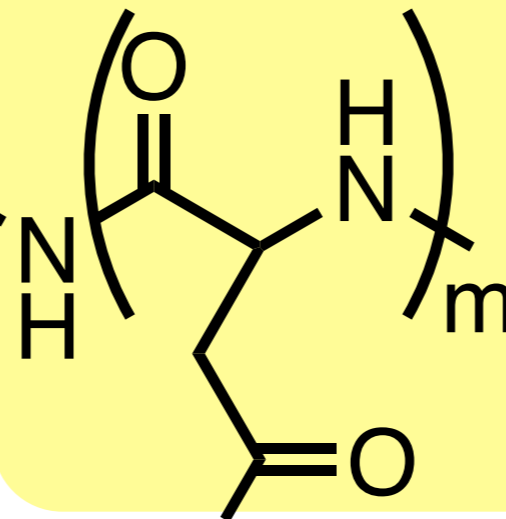
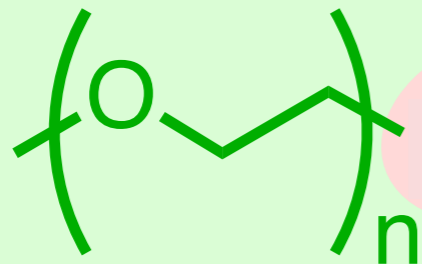
FLAG tag gene expression



Micellar nanovector achieved efficient gene transfer to carotid artery with neointimal hyperplasia without any vascular occlusion by intravascular method

Polymer Design for PEG-Detachable micelle

PEG

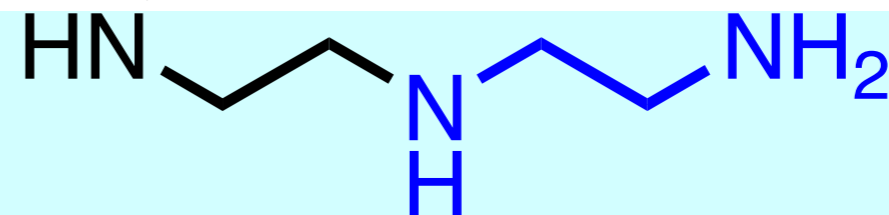


Polyaspartamide

PEG shell layer contributes to biocompatibility and colloidal stability of polyplex micelles

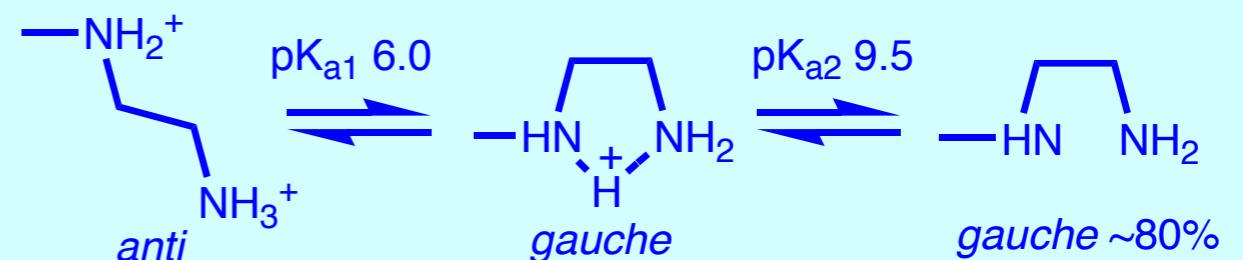
BUT

Often reducing transfection efficacy due to steric effect



<Ethylenediamine unit>

The two step protonation permits DNA condensation at pH 7.4 (mono-protonated) and high membrane disruptive ability in endosomal pH (di-protonated) to induce endosomal escape.



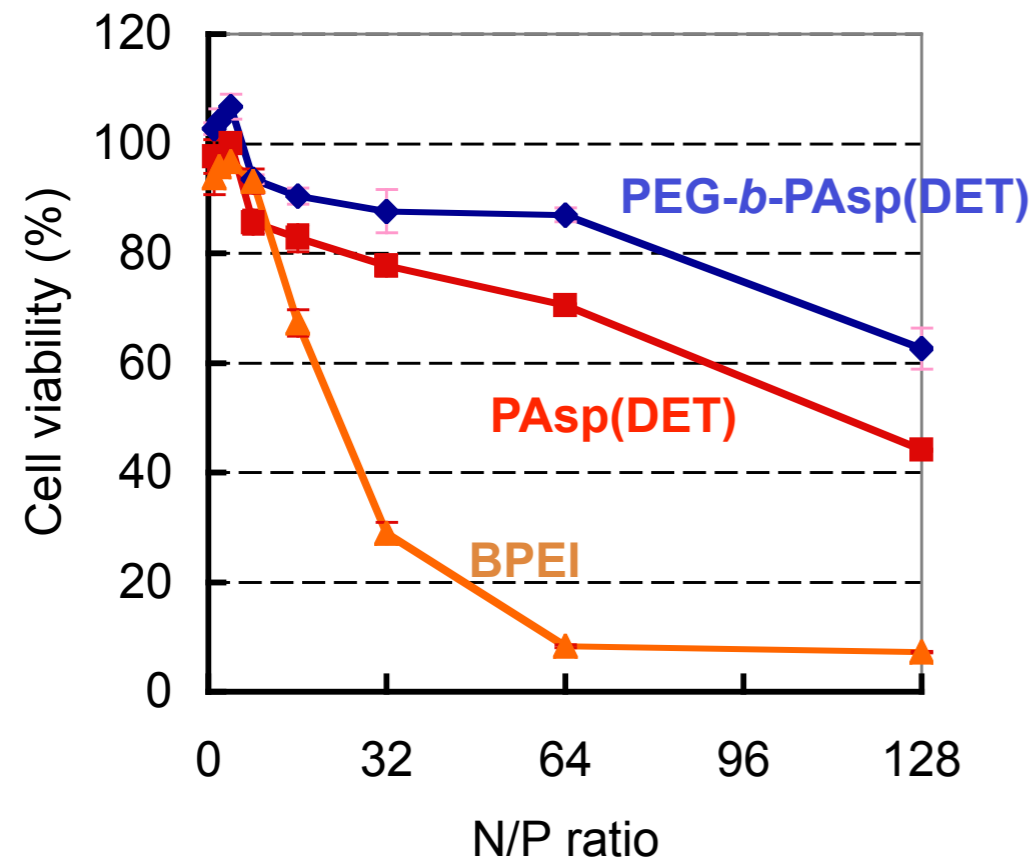
Kanayama, et al *ChemMedChem*, 2006, 1, 439-434

Transfection efficiency and cytotoxicity against vascular smooth muscle cells (SMC)

PAsp(DET)(98mer): polycation without PEG block and forming polyplex with plasmid DNA

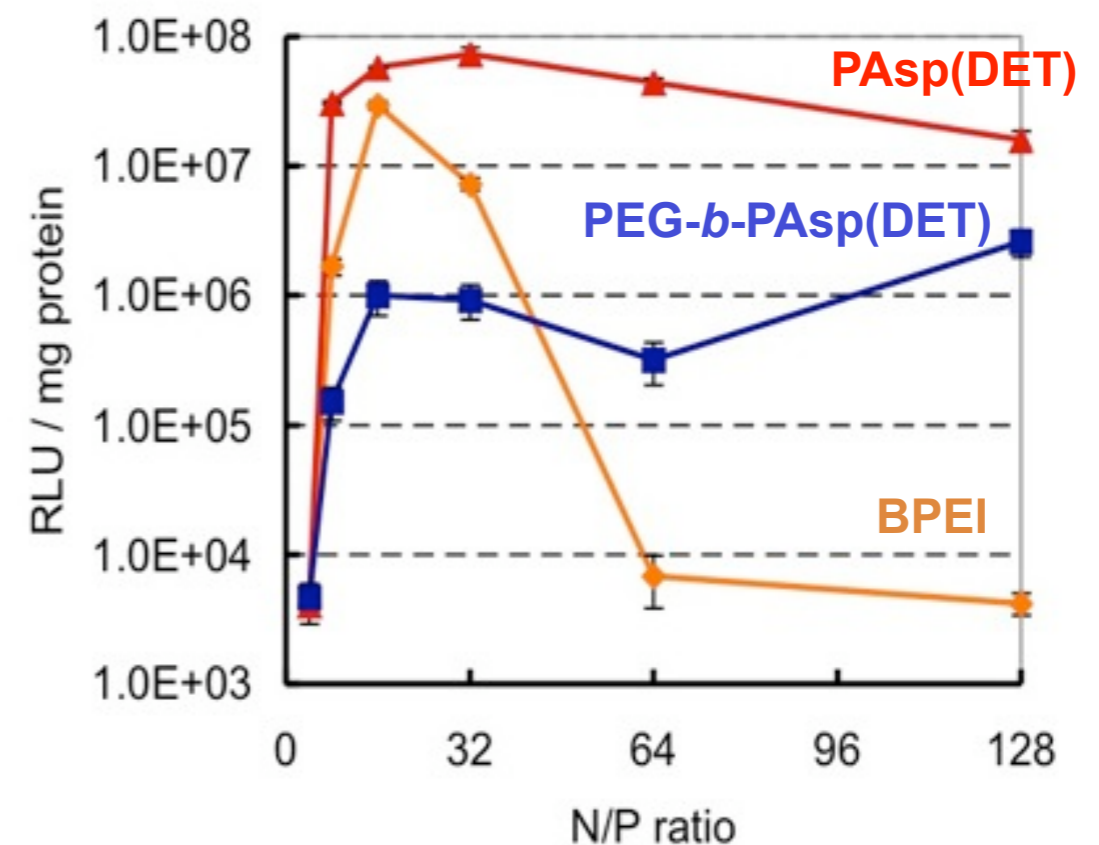
BPEI: branched polyethyleneimine ($M_w=25\text{KDa}$)

Cytotoxicity assessment (MTT assay)



Lower cytotoxicity of PEG-*b*-PAsp(DET) and PAsp(DET) than BPEI.

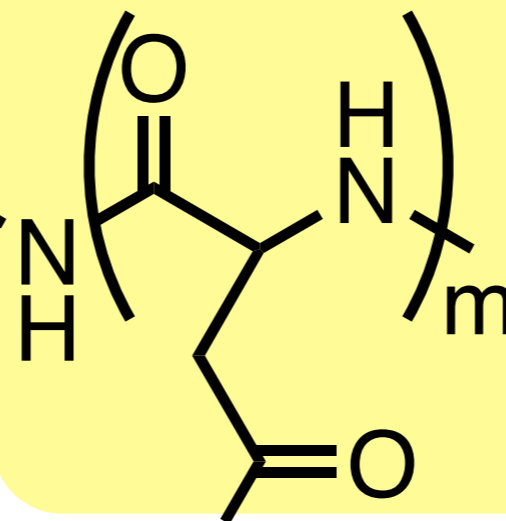
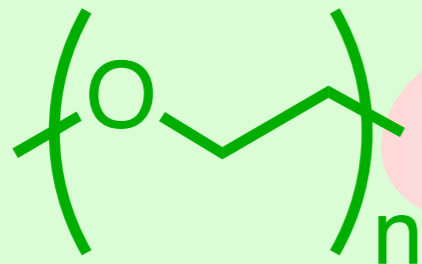
Transfection efficiency (luciferase assay)



Higher transfection efficiency of PAsp (DET) and BPEI polyplexes than PEG-*b*-PAsp(DET) micelles.

Polymer Design for PEG-Detachable micelle

PEG



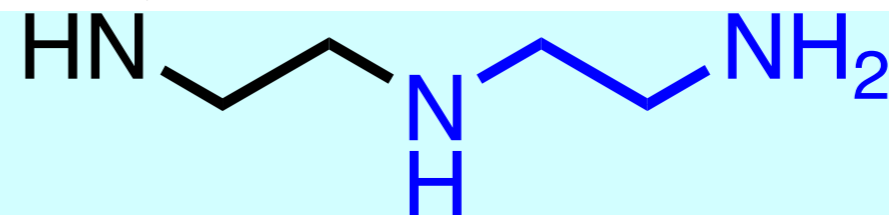
Polyaspartamide

Disulfide linkage
(SS linkage)

Cleavable under intracellular
reduced environment

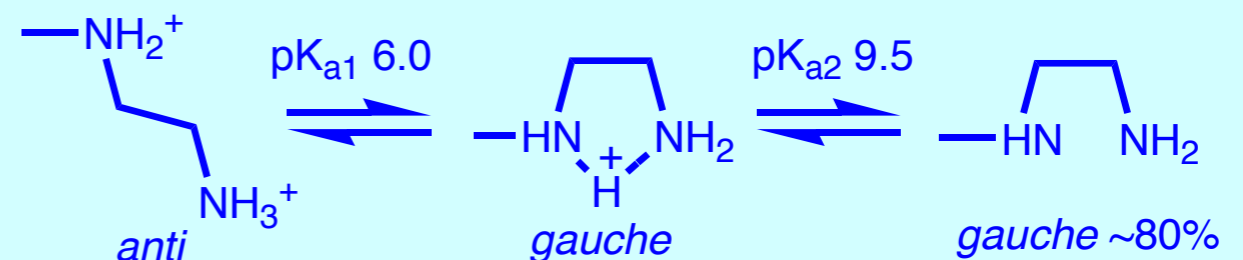
PEG-SS-P[Asp(DET)]

S. Takae, et al, *JACS*, 130(18)
6001-6009 (2008)



<Ethylenediamine unit>

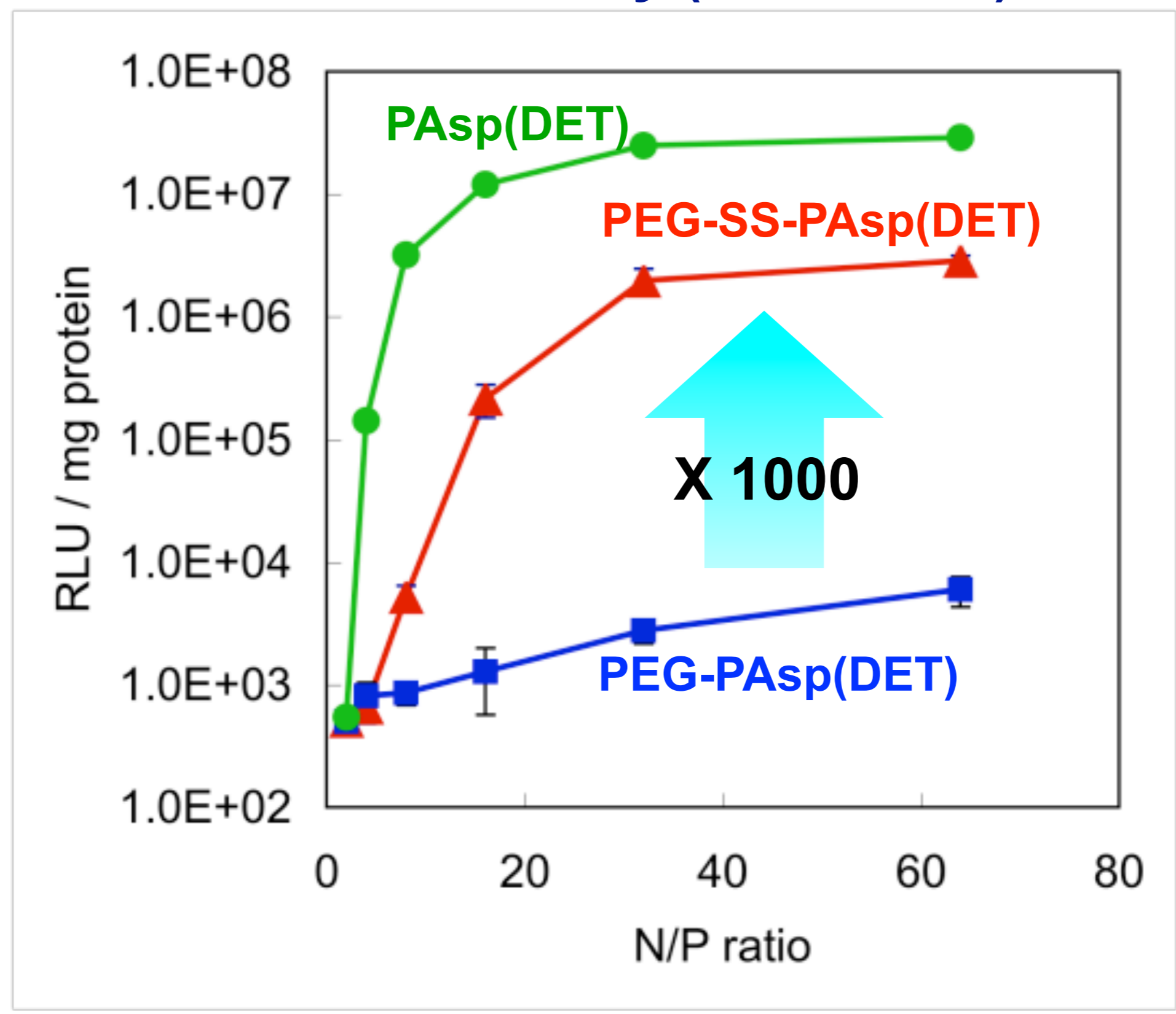
The two step protonation permits DNA condensation at pH 7.4 (mono-protonated) and high membrane disruptive ability in endosomal pH (di-protonated) to induce endosomal escape.



Kanayama, et al *ChemMedChem*, 2006, 1, 439-434

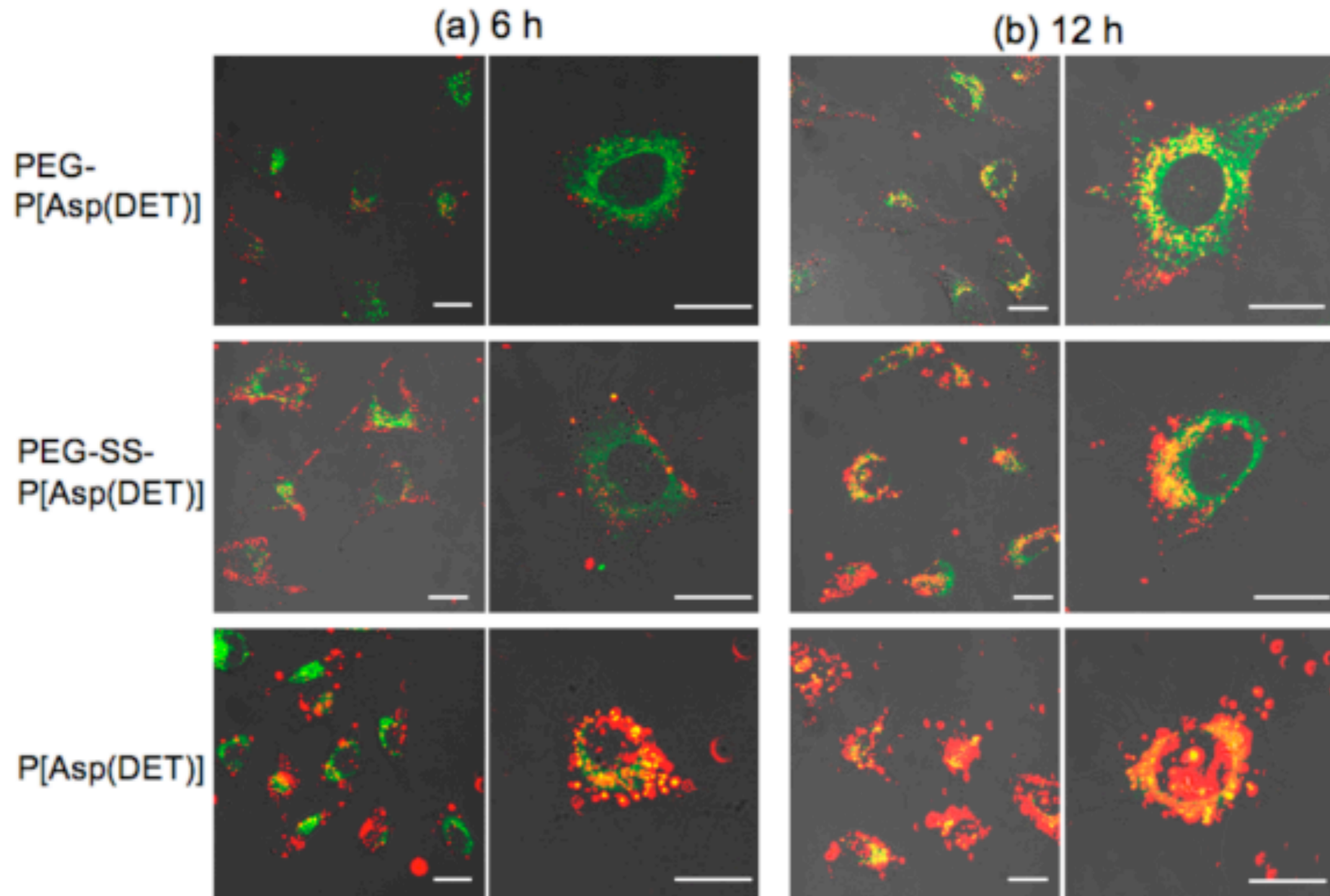
Transfection by PEG-detachable polyplex micelles

Luciferase assay (HeLa cells)



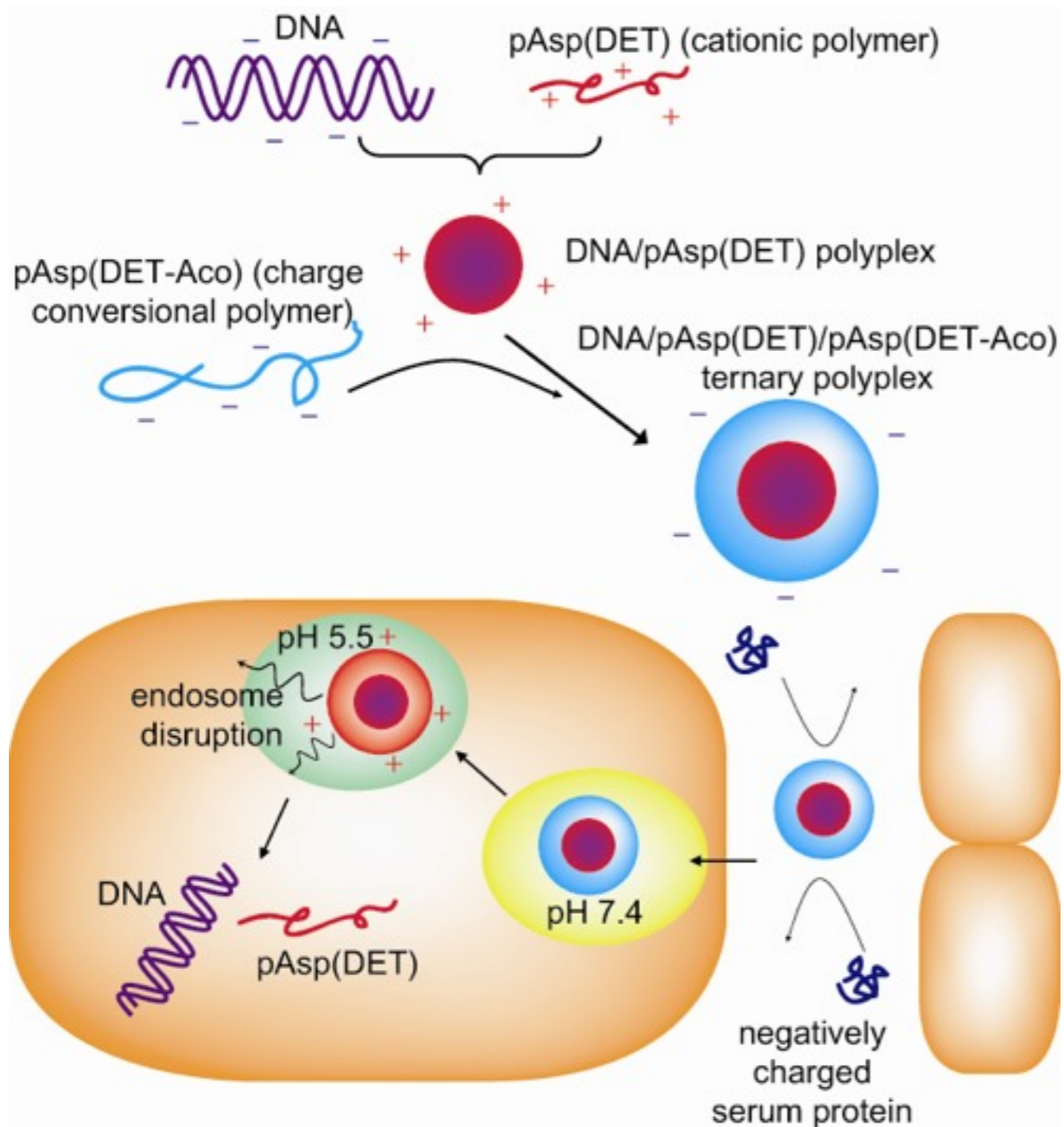
Transfection by PEG-detachable polyplex micelles

Time dependent change in intracellular distribution of pDNA



Cy5-labeled pDNA (Red), LysoTracker (Green)

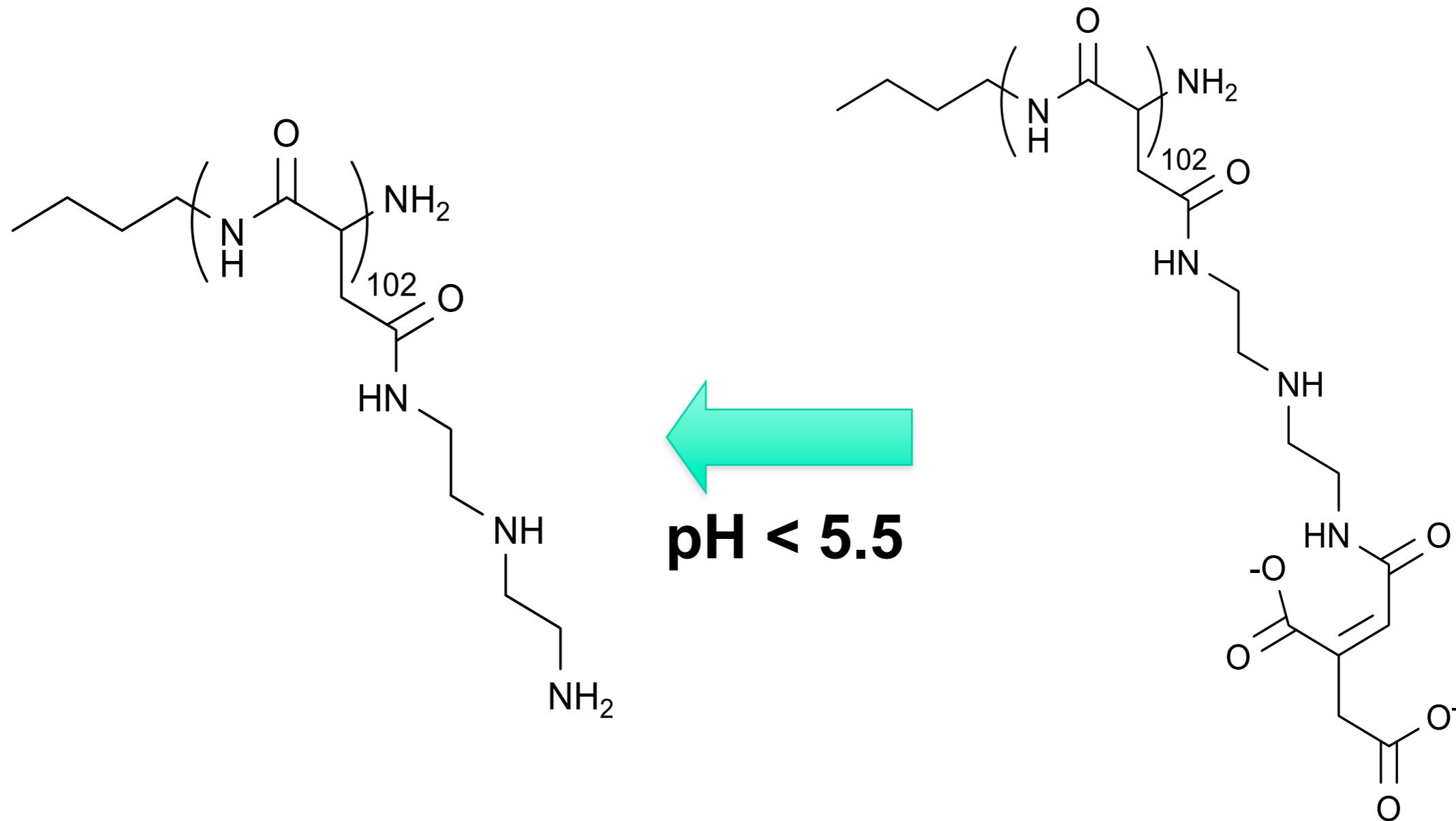
Charge-conversional polyplex system



If the polyplex had negatively charged in the cell exterior, it could reduce the toxicity.

If the charge of the polyplex turned to positive after internalization into the cell, it could disrupt endosome effectively.

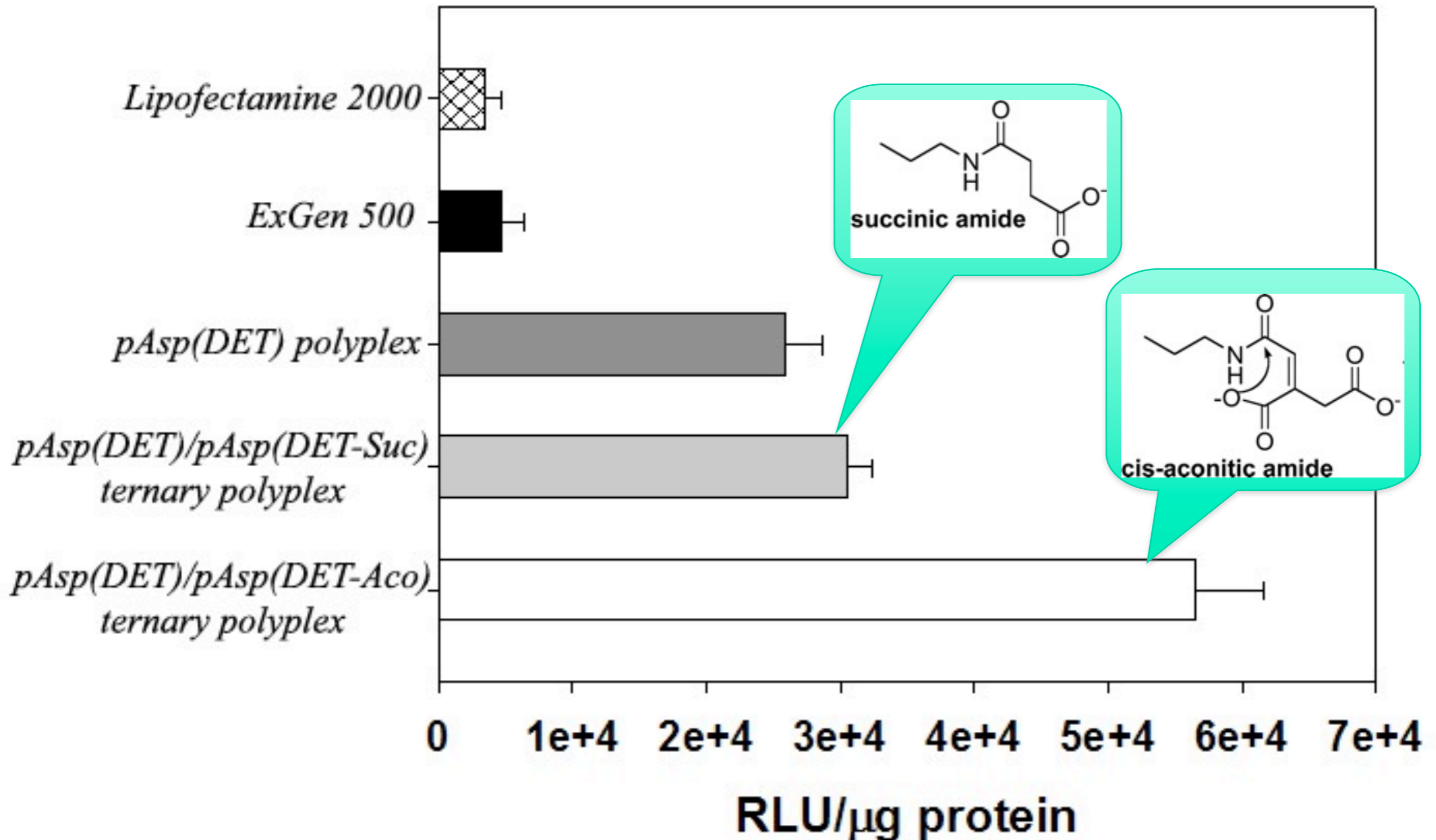
pAsp(DET)/pAsp(DET-Aco)



pAsp(DET) :
cationic polymer
with endosome
disruption moiety

pAsp(DET-Aco) :
charge-
conversional
polymer

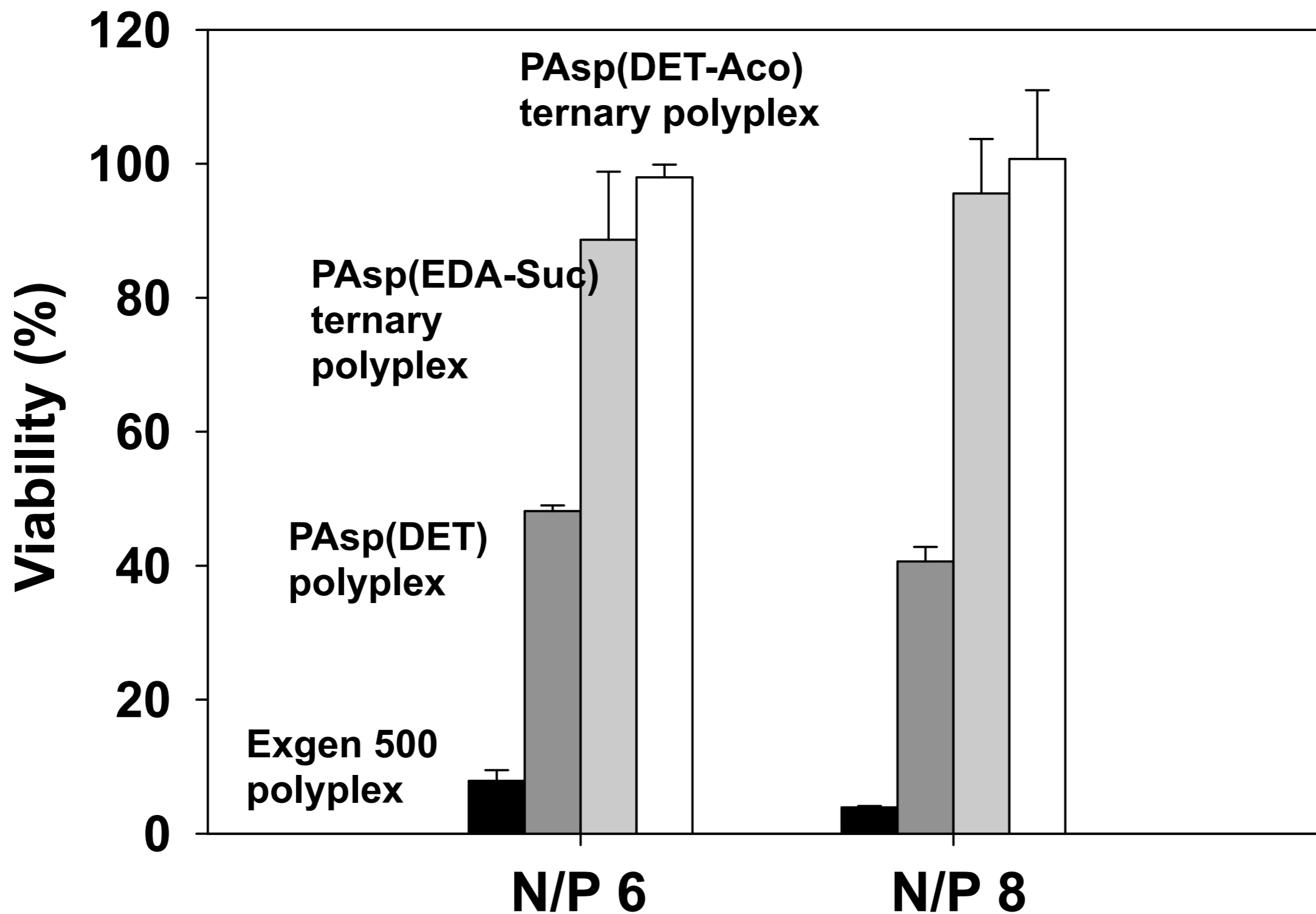
Transfection efficiency of ternary polyplex on HUVEC



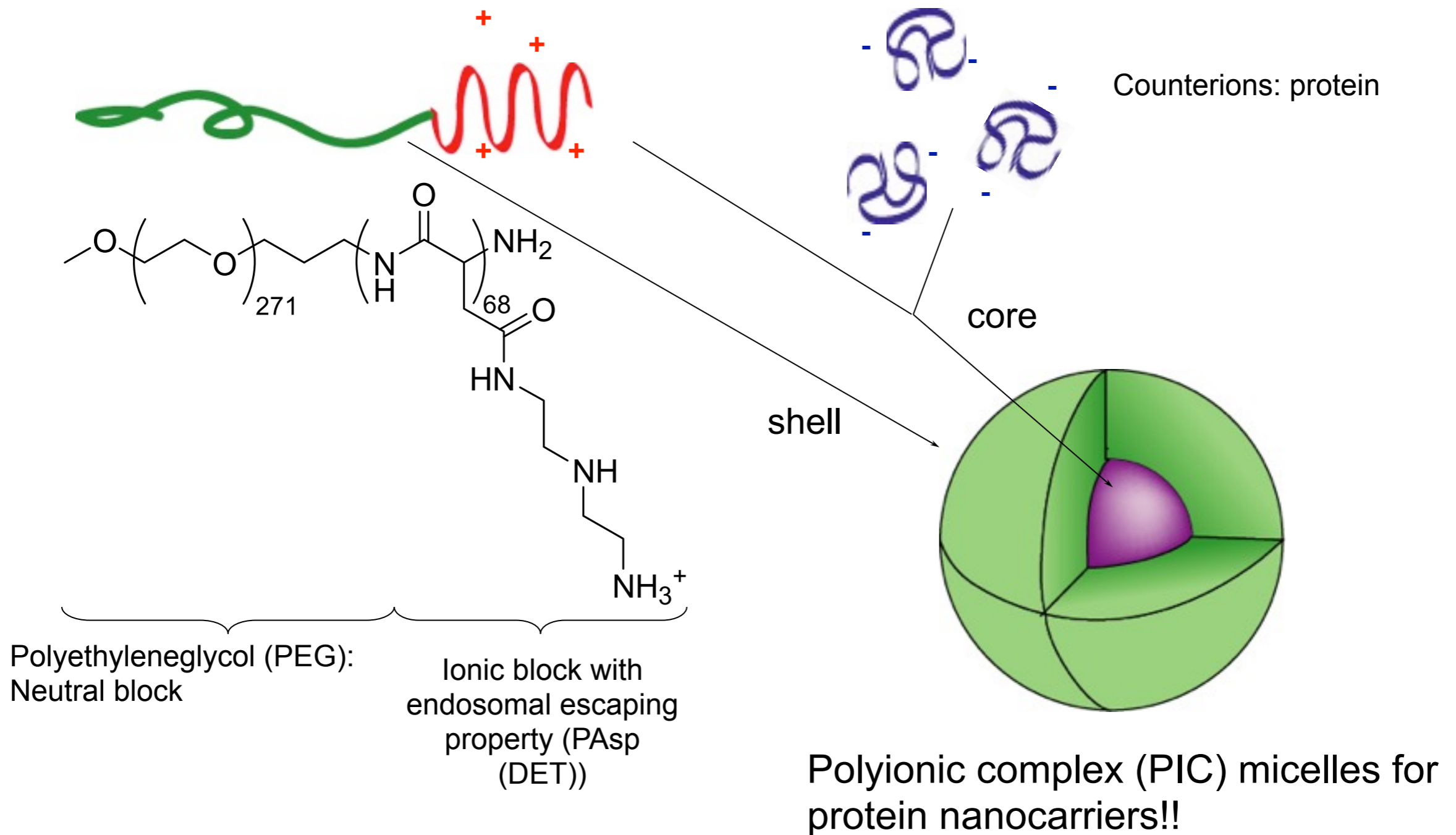
***HUVEC (Human umbilical vein endothelial cells)** are difficult to be transfected and sensitive to toxicity.

*The charge-conversional ternary polyplex (white) showed high transfection efficiency in this primary cells.

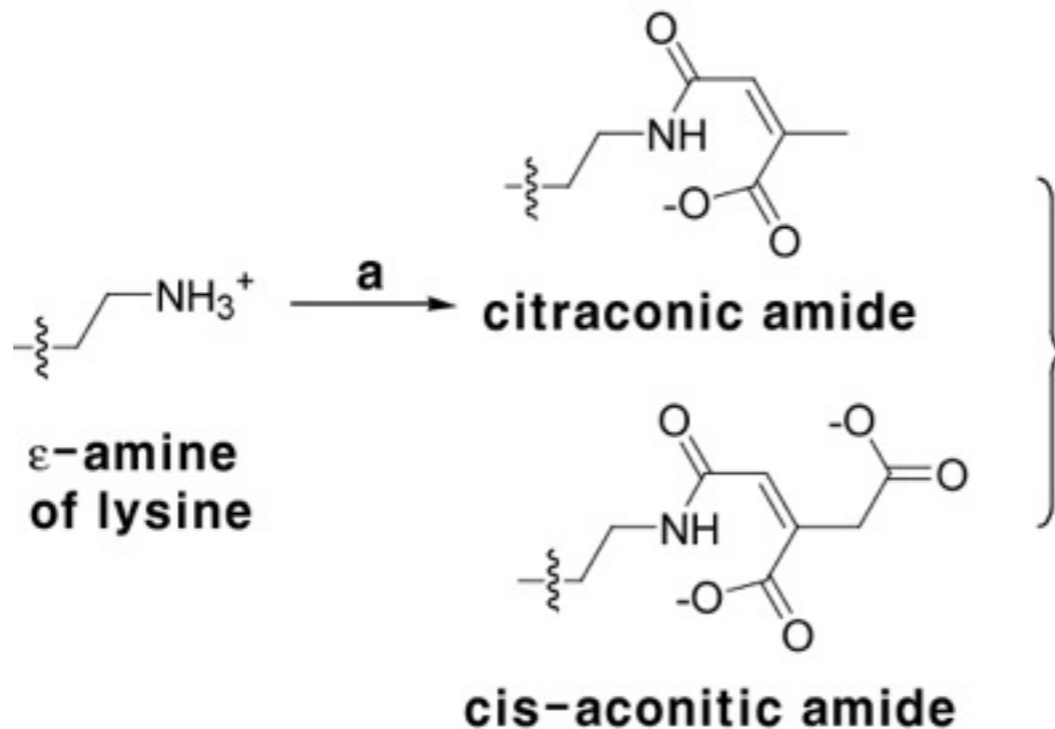
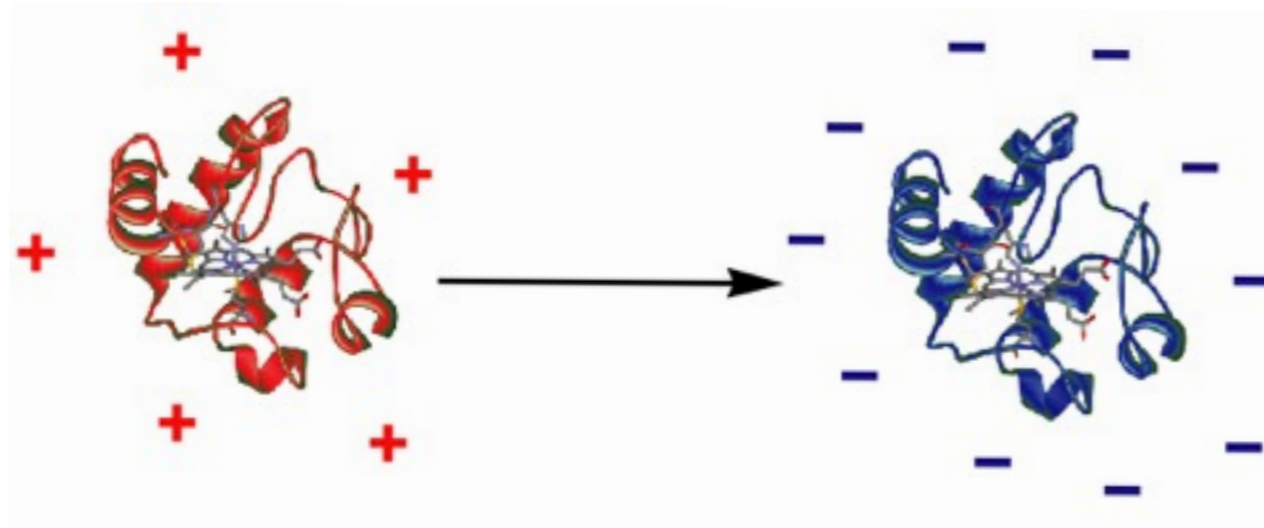
Cytotoxicity of ternary polyplex against HUVEC



PIC micelles: an efficient protein delivery system into cytoplasm



Charge-conversional modification of protein (Cytochrome C)

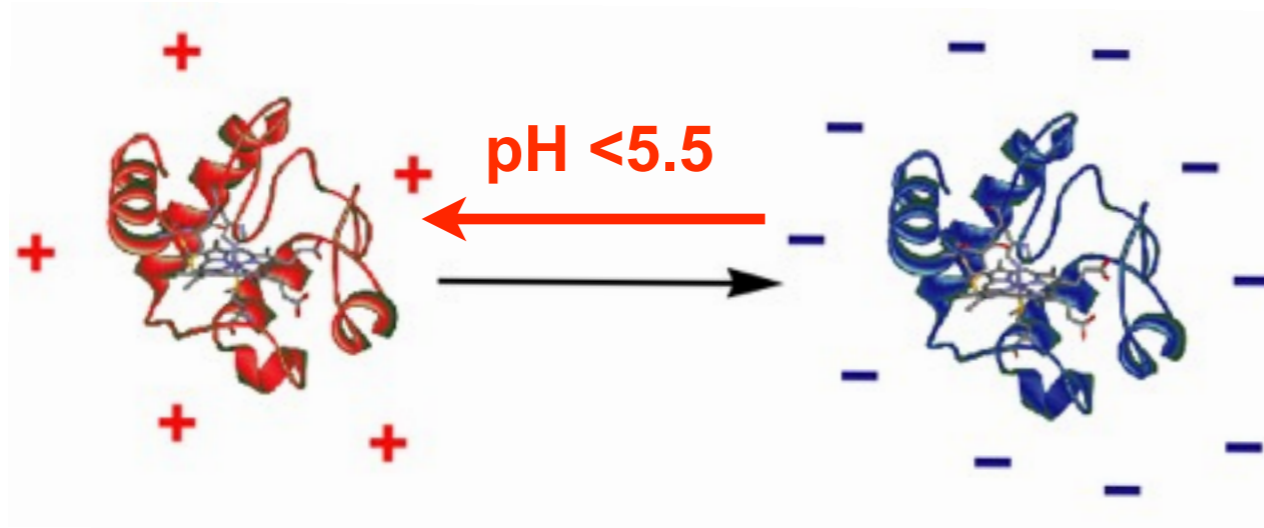


a: citraconic anhydride or cis-aconitic anhydride

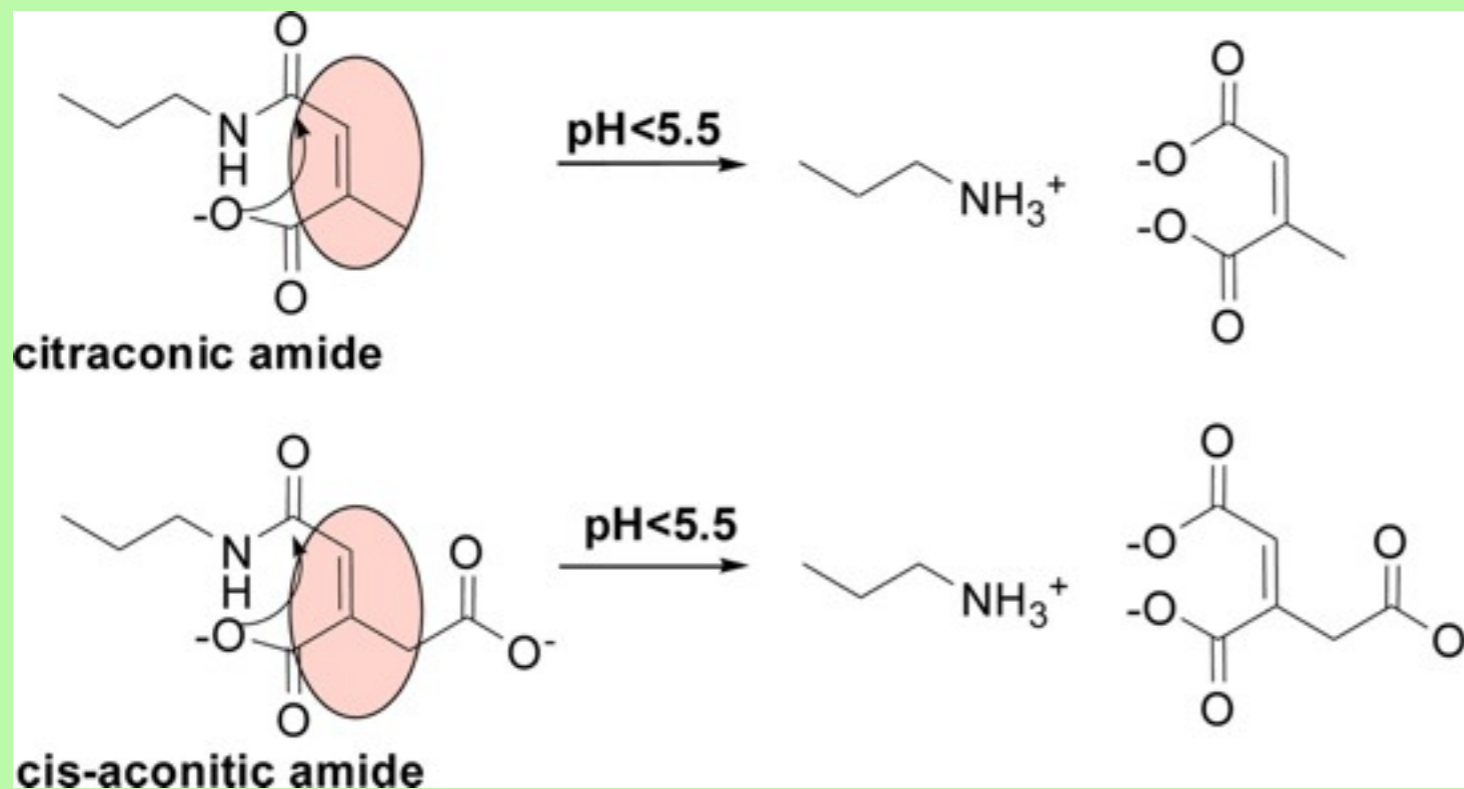
Protein	Charge density (Da/charge)
CytC	+1391
Cyt-Cit	-501
Cyt-Aco	-320

Charge-density can be increased by the charge-conversion!

Charge-conversional modification of protein (Cytochrome C)



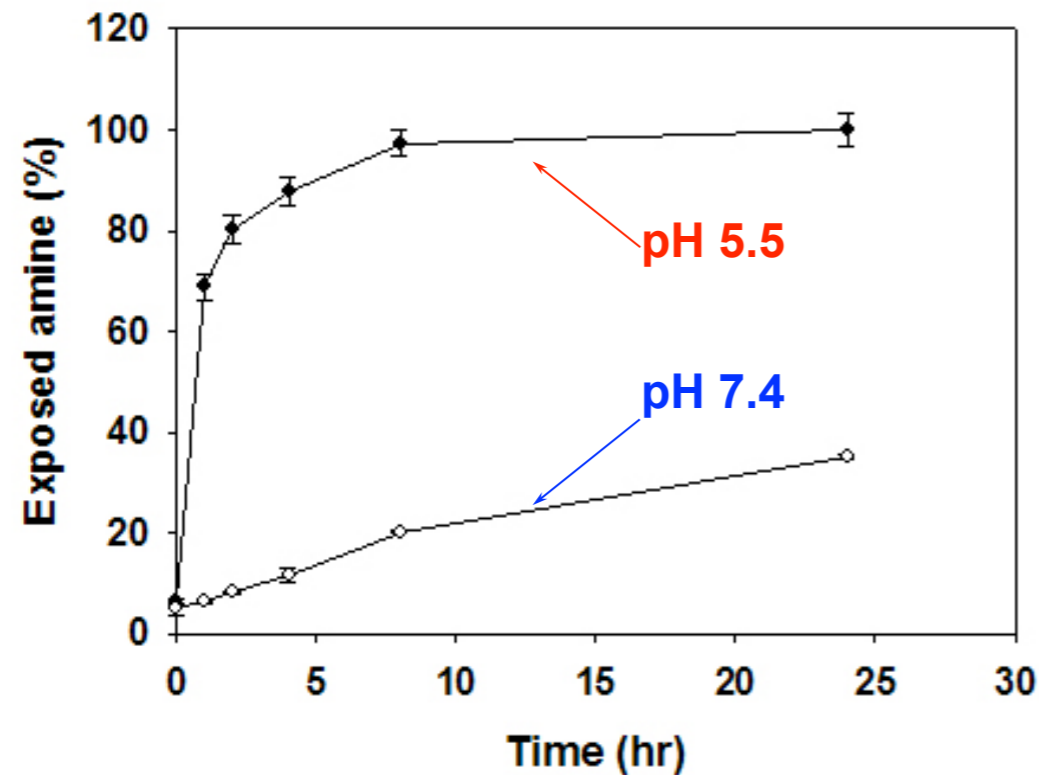
Protein	Charge density (Da/charge)
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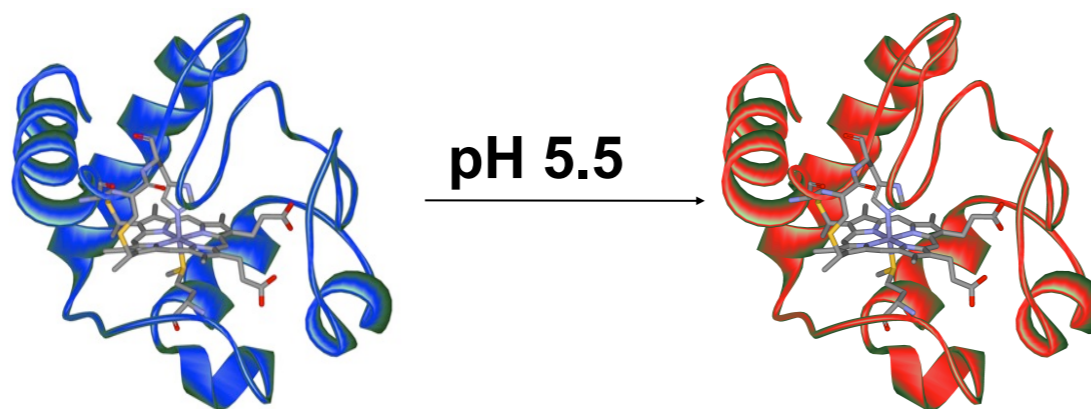
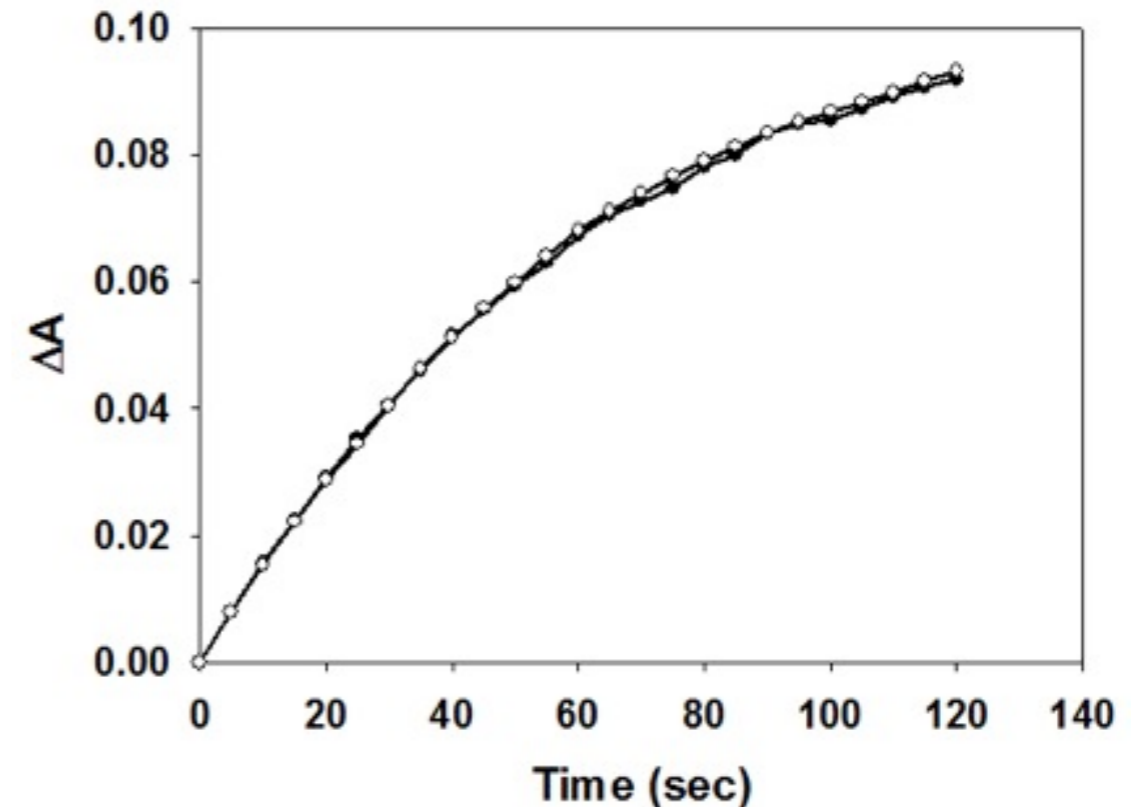
Charge-density can be increased by the charge-conversion!

Reversibility of the charge-conversion

pH-sensitive reversal



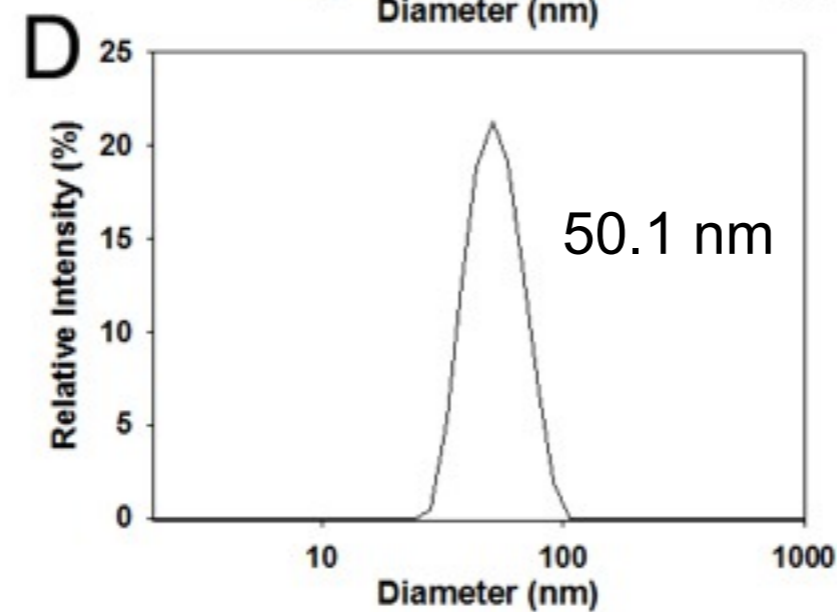
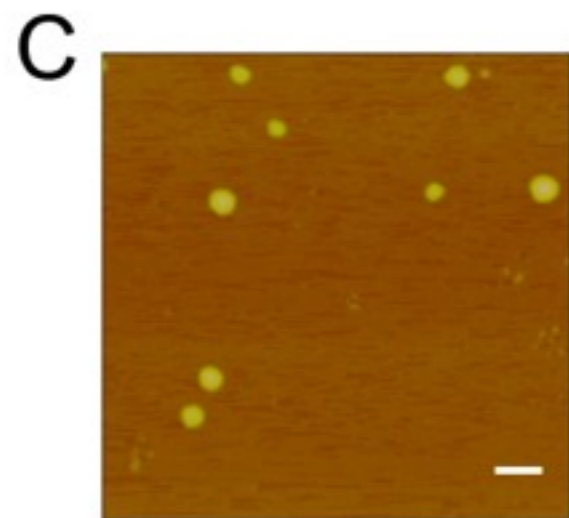
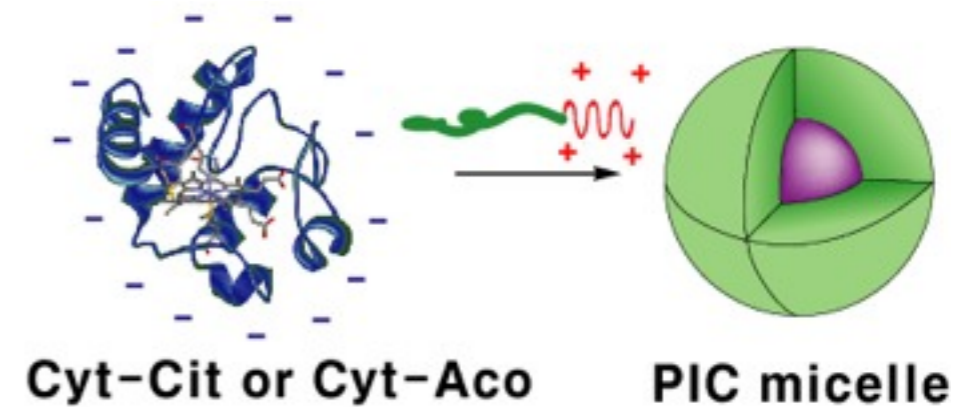
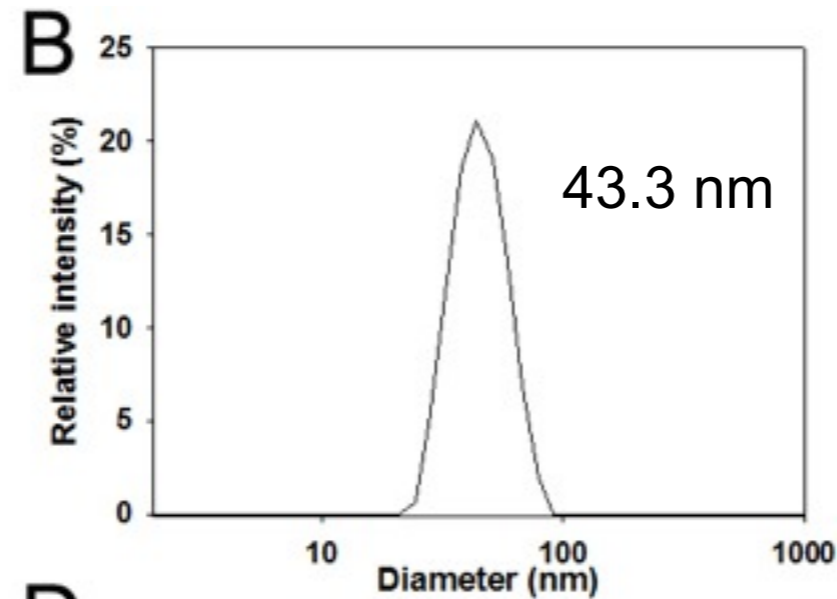
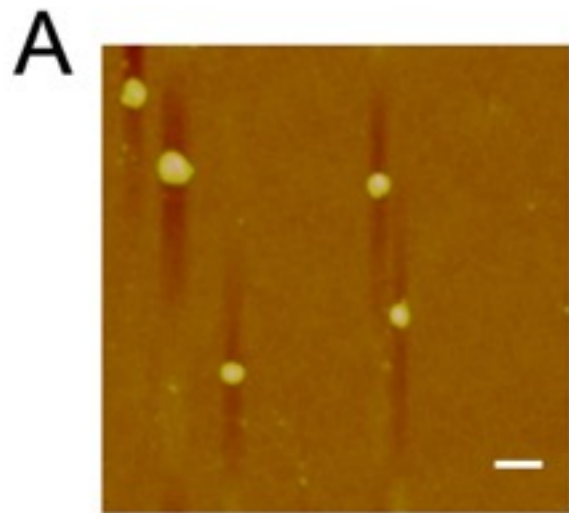
protein activity



The charge-conversion can be reversed rapidly at endosomal pH 5.5.

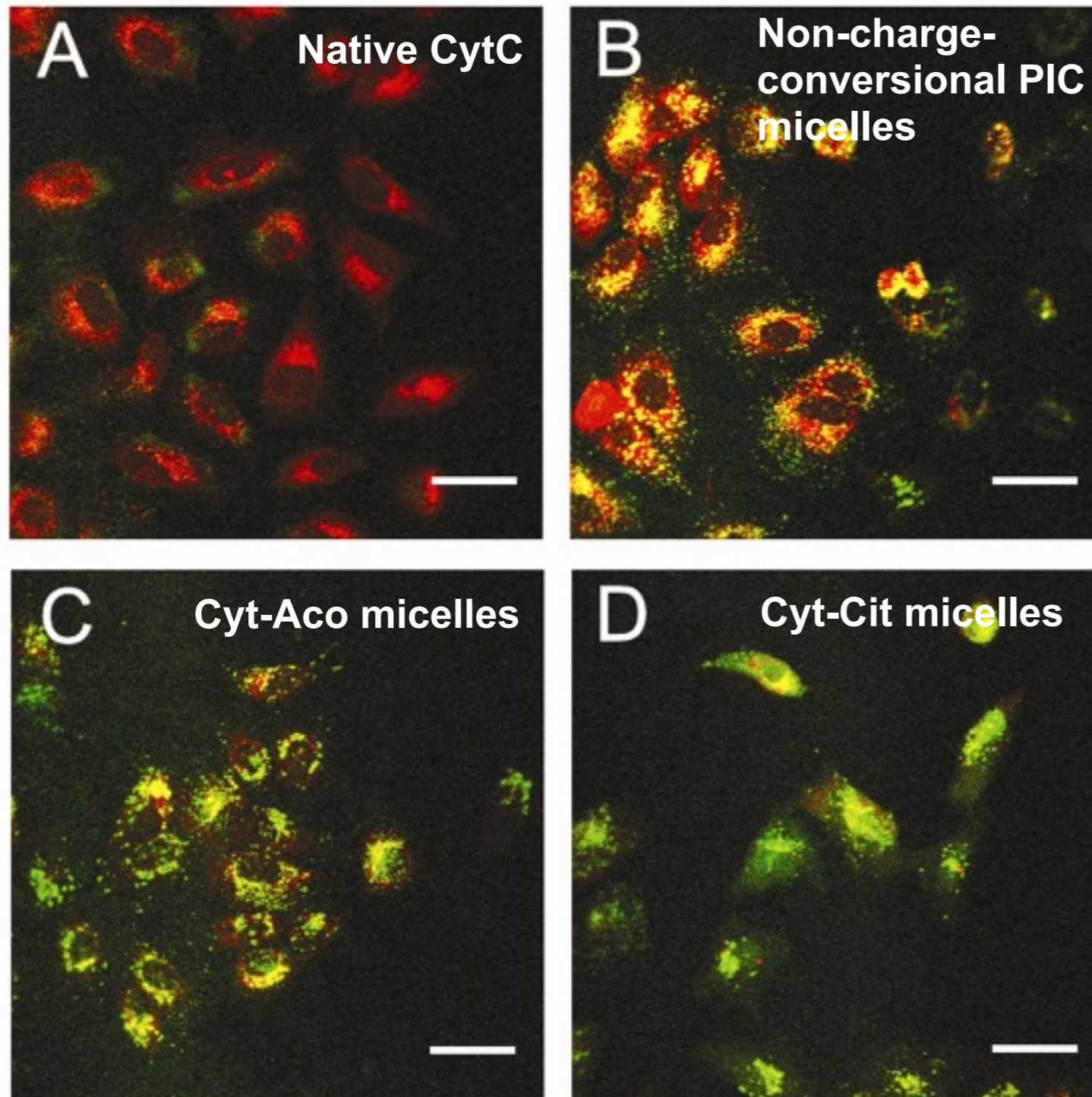
The modification-reversion process does not affect on the protein activity.

Formation of the PIC micelles at physiological salt condition



**Stable
micelles at
150mM NaCl!**

Intracellular protein delivery by charge-conversional PIC micelles



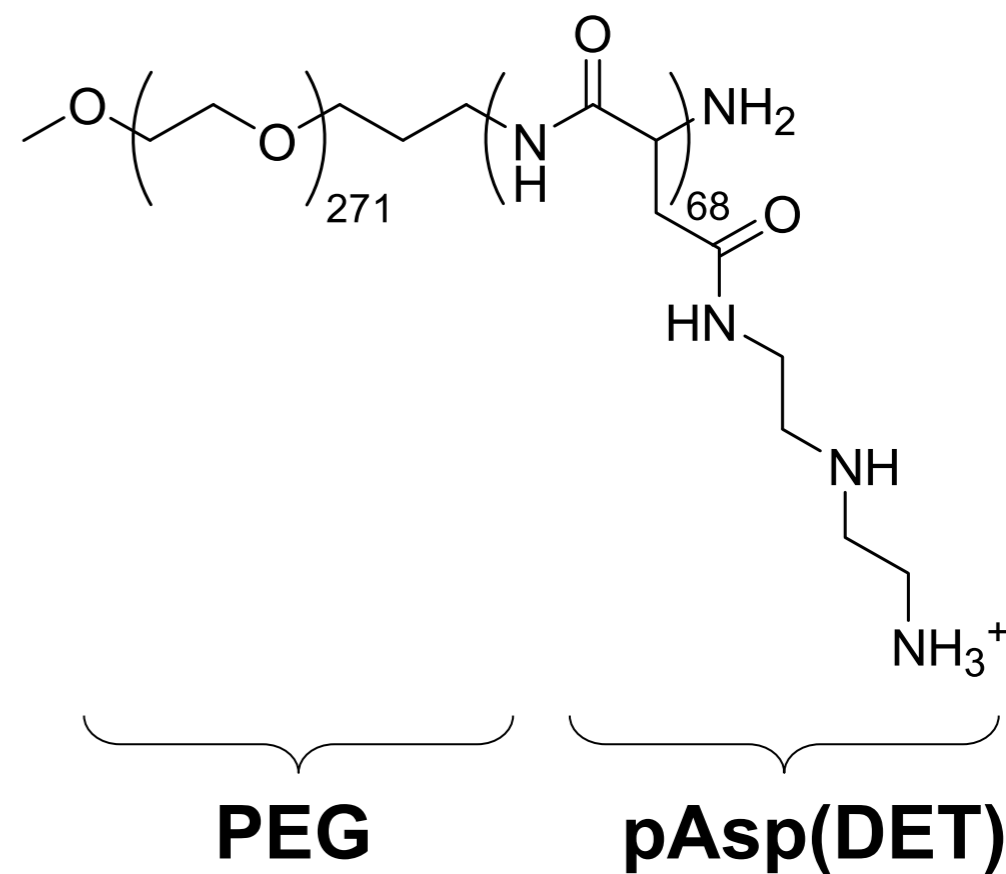
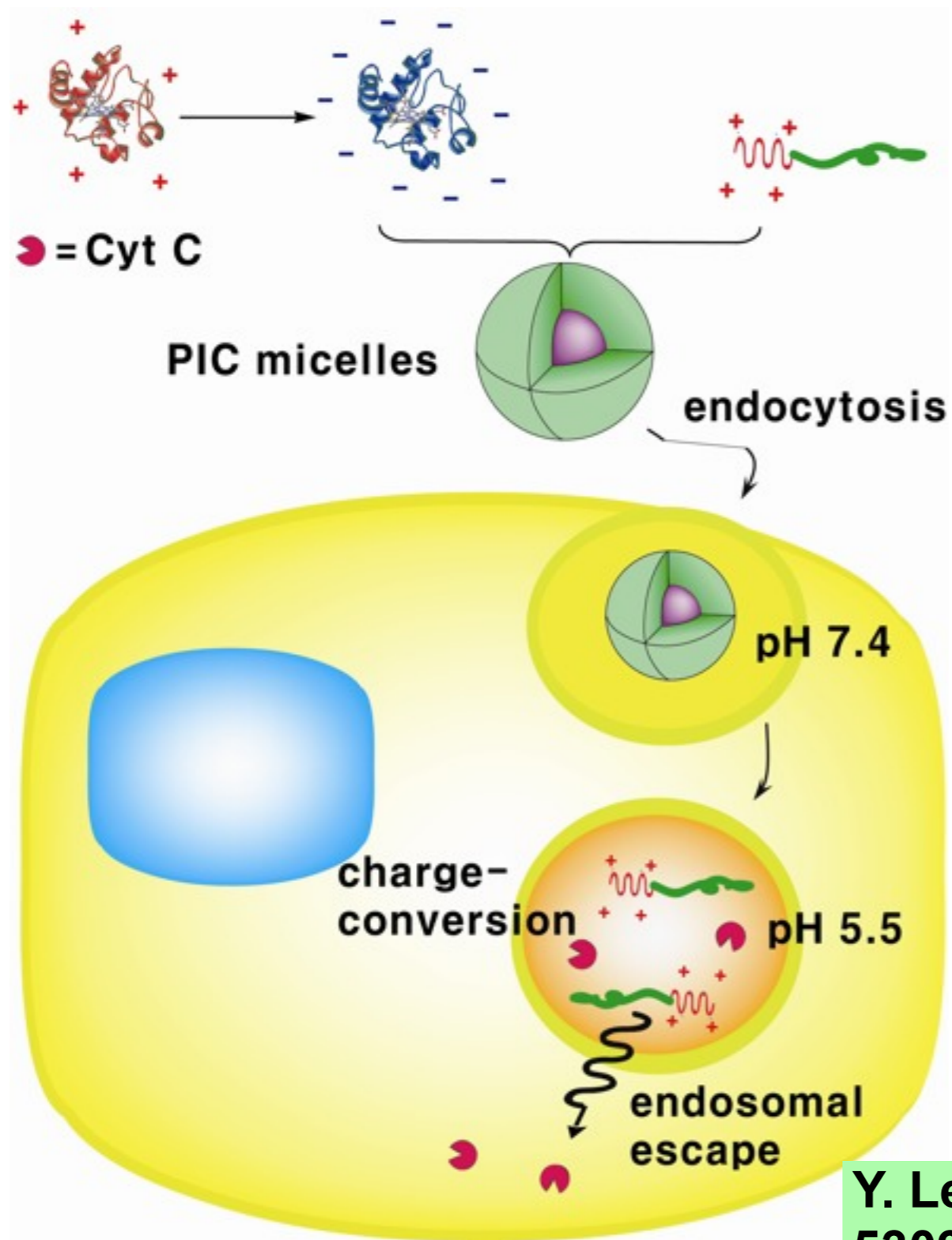
- Cyt-Alexa 488 (protein escaped from endosome)
- Endosome-Lysotracker Red (endosome)
- Co-localization of green and red (Cyt in endosome)

Cyt C: no internalization

Non-charge-conversional PIC micelles: efficient internalization (yellow) but no escape

Charge-conversional PIC micelles: efficient internalization and efficient escape (green)

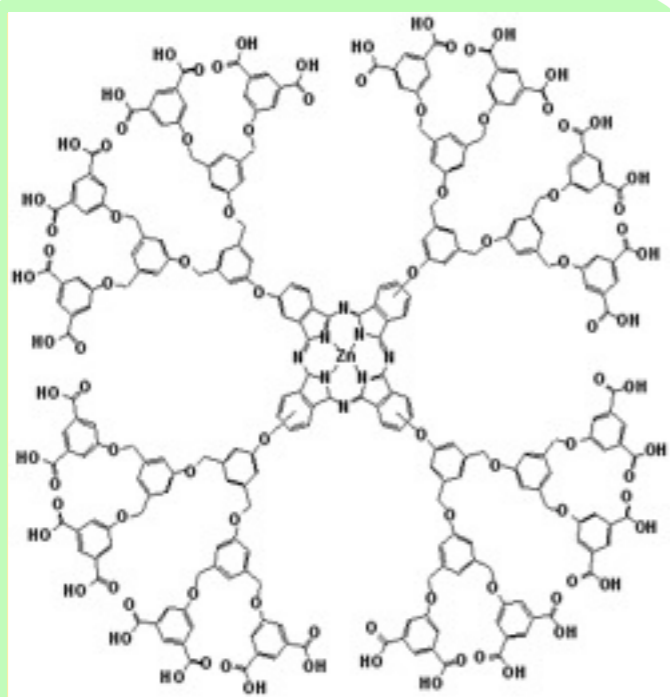
Endosomal escape accelerated by PEG-pAsp(DET) polymer



The released PEG-pAsp(DET) helps the endosomal escape.

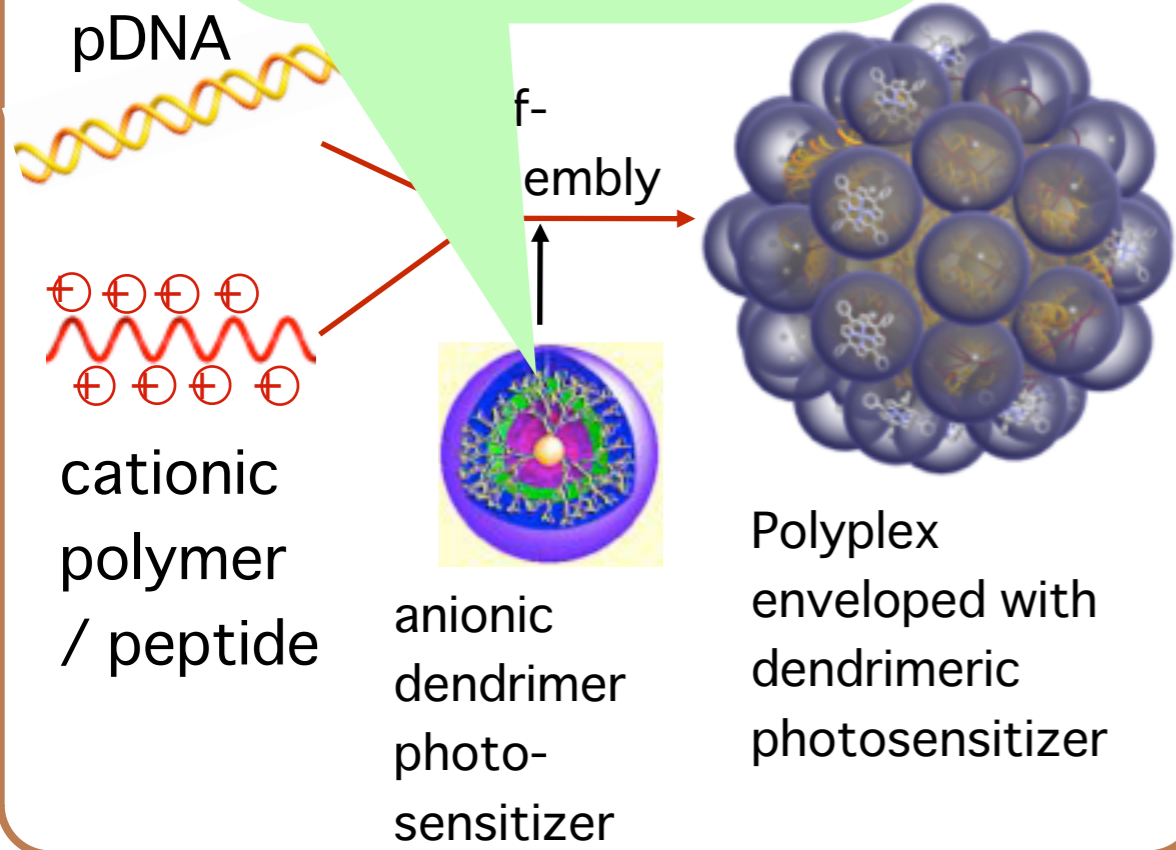
Y. Lee, et al, *Angew. Chem. Int'l. Ed.* 48(29) 5309 (2009) (Highlighted as inside cover story)

Endosomal escape: A key issue in intracellular gene delivery

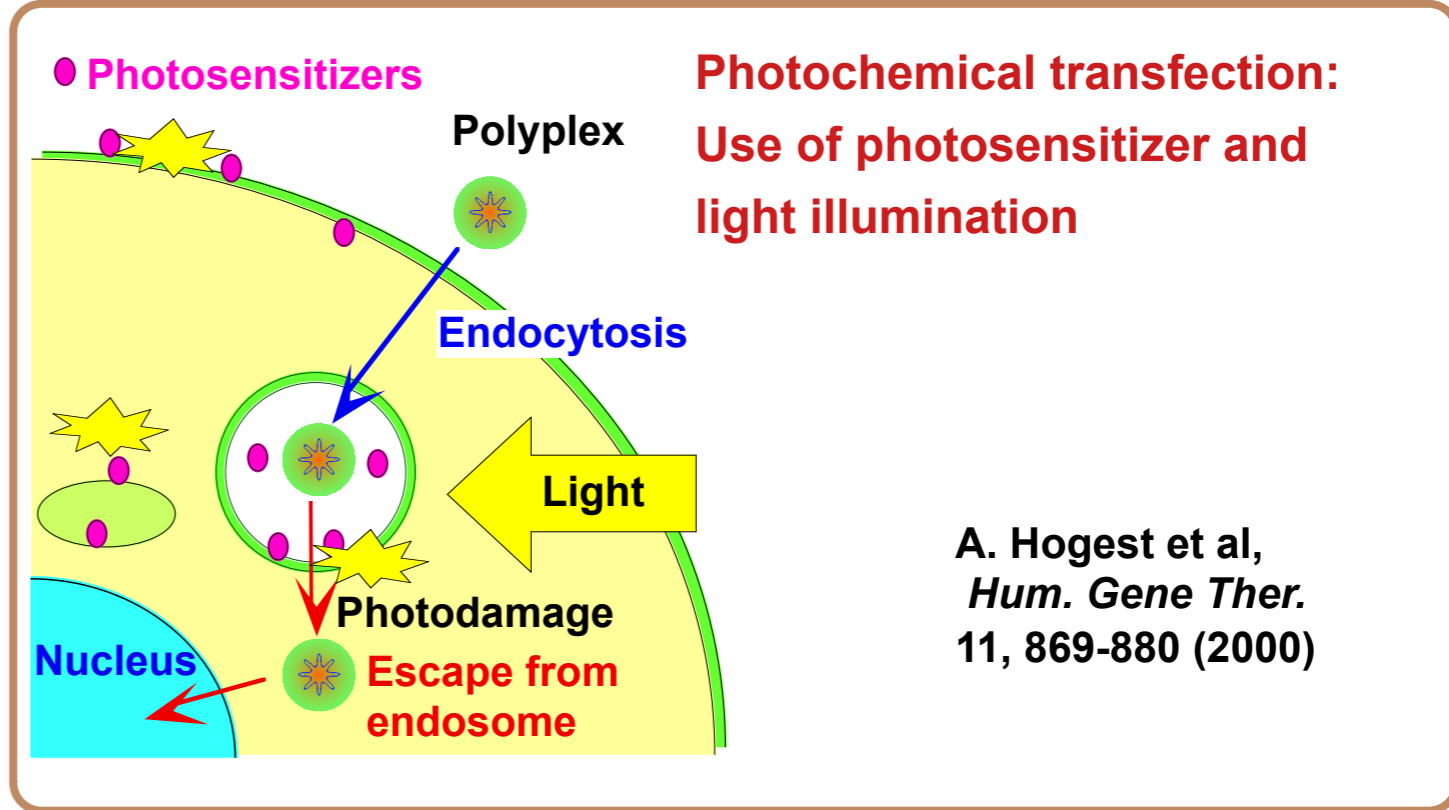


Ca. 3nm

Dendritic Photosensitizer



Challenge: Design of photosensitive polyplex with low cytotoxicity and high photochemical efficiency for site-directed gene transfer *in vivo*

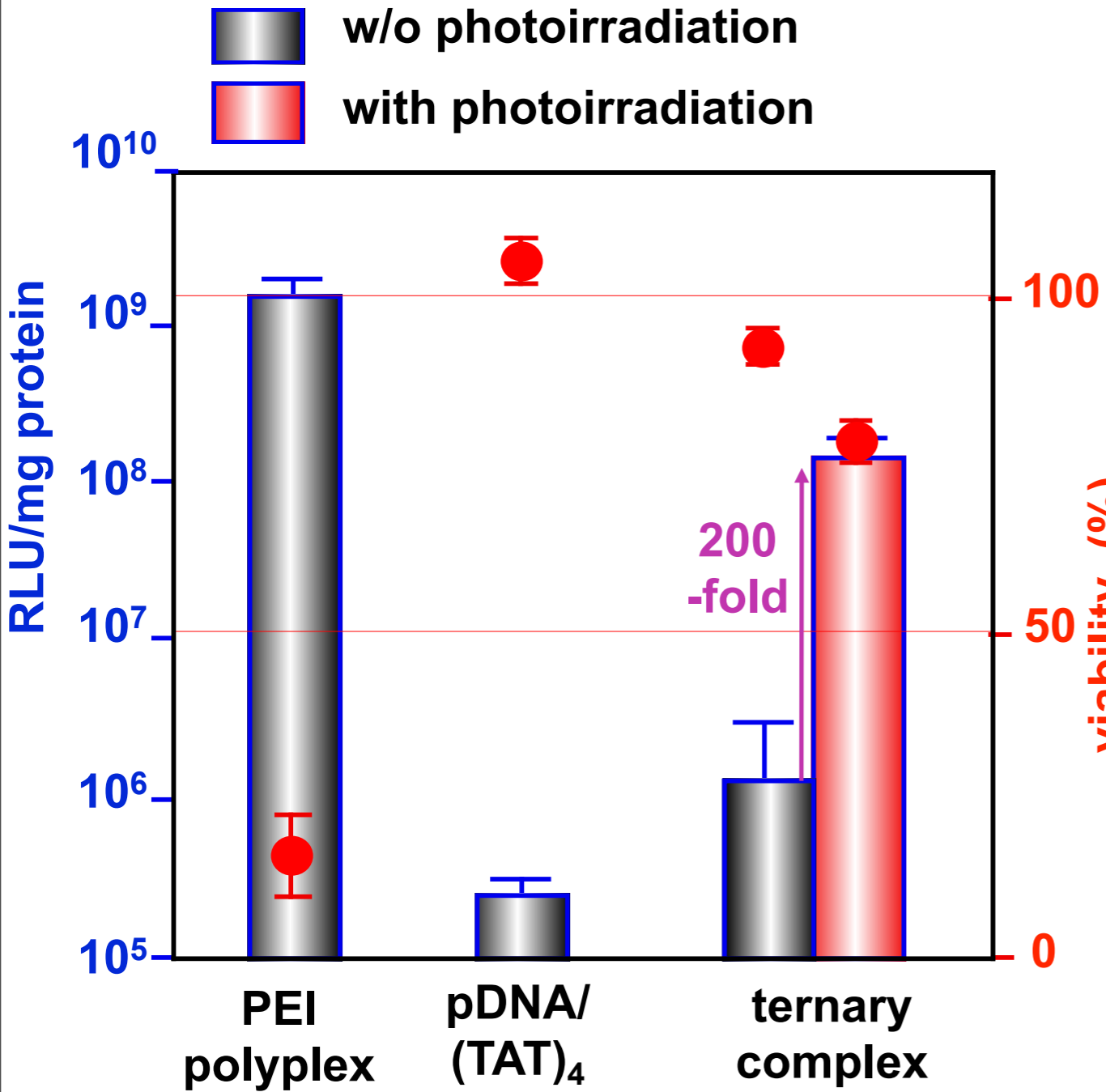


Photochemical transfection: Use of photosensitizer and light illumination

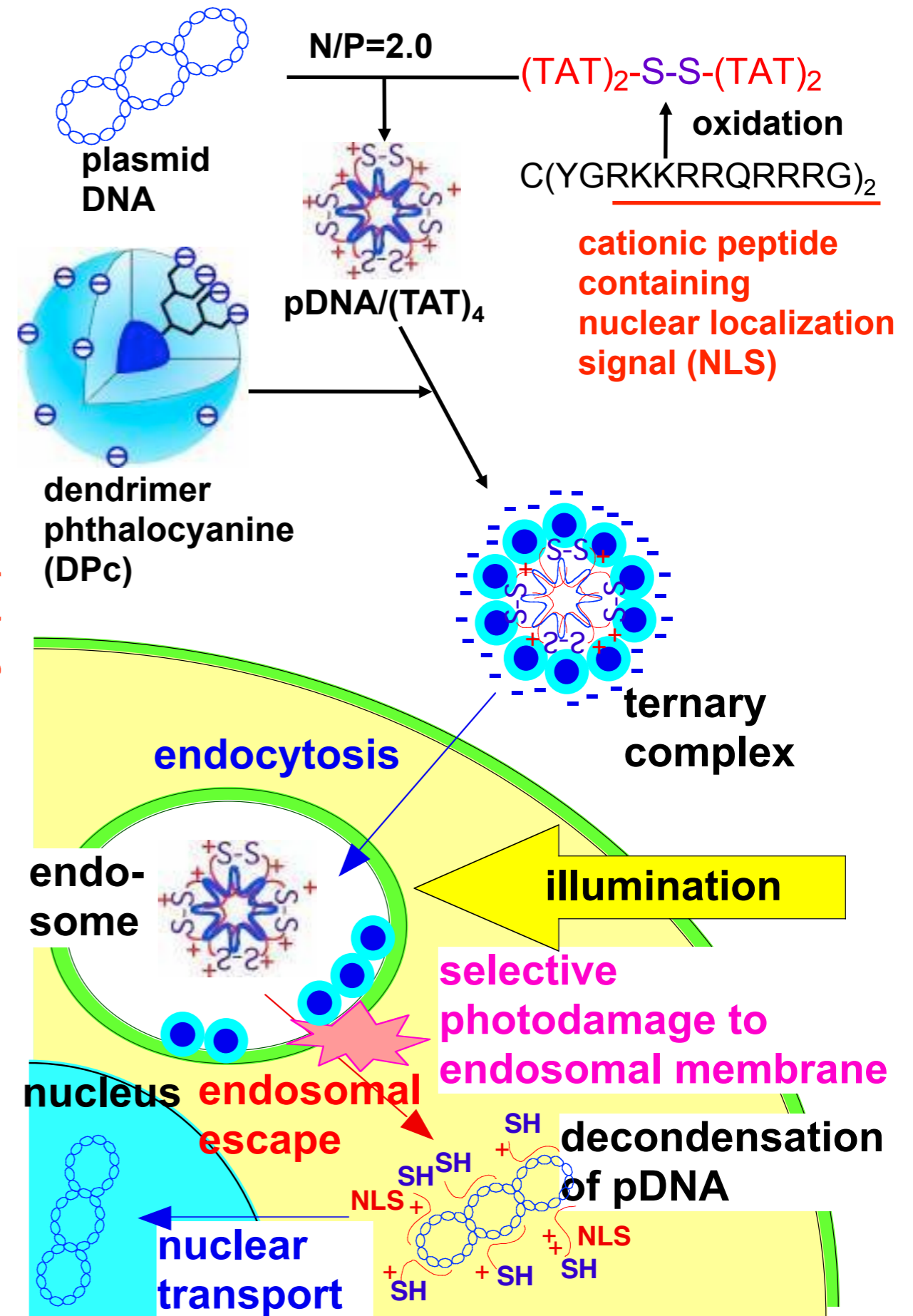
A. Hogest et al, *Hum. Gene Ther.* 11, 869-880 (2000)

Temporal and spatial control of the transgene expression by light-responsive gene carriers

Transfection efficiency and photocytotoxicity of the ternary complex (incubation time:48 h)



Remarkable photochemical enhancement of the gene expression was achieved with reduced photocytotoxicity

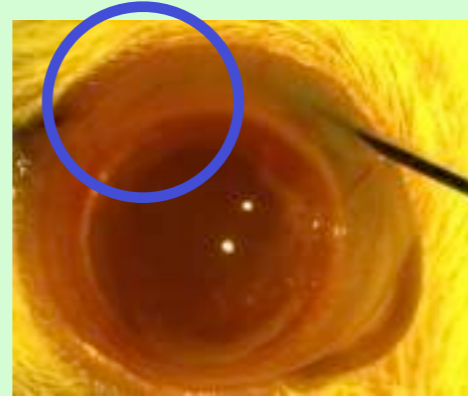


Intelligent gene carrier for temporal and spatial control of gene transfer in vivo

—Site-directed transfection using light-responsive gene carriers—

A part of conjunctiva in a rat eye was photoirradiated 2 h after subconjunctival injection of the ternary complex (150mL)

The fluorescent image of the YFP expression in a rat eye was observed by a stereoscopic microscope



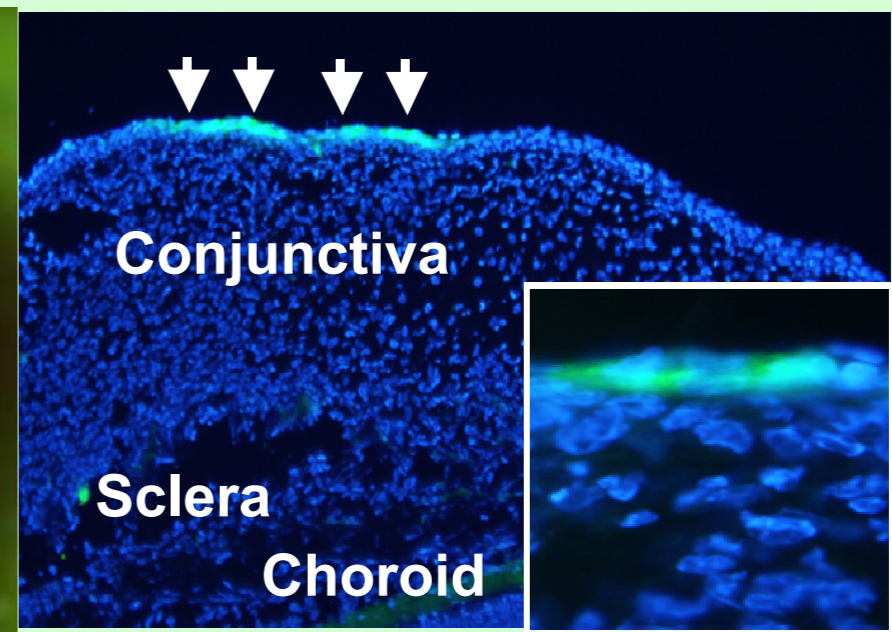
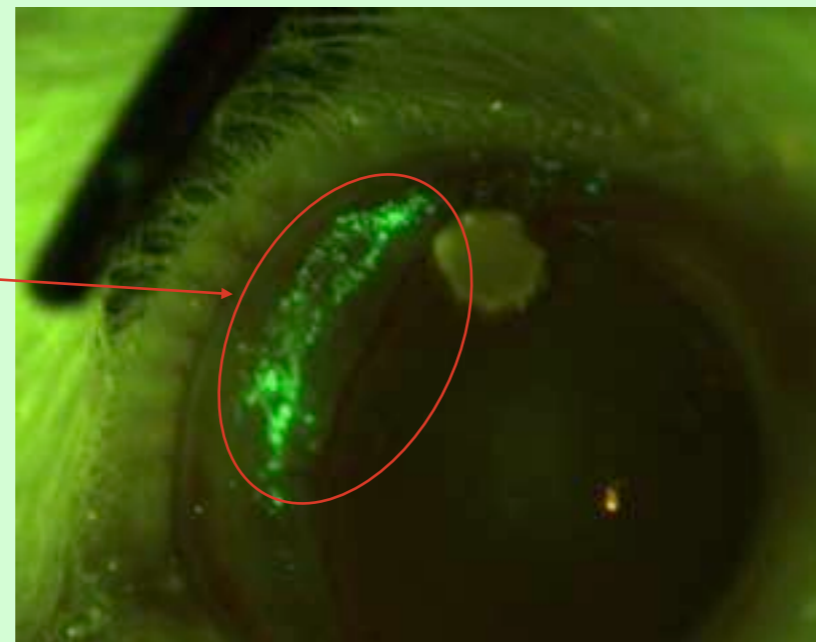
Light-induced, site-directed transfection of the YFP gene (Collaboration with Dept. Ophthalmology, the University of Tokyo Hospital)



Applications for gene therapy of ophthalmic diseases such as AMD

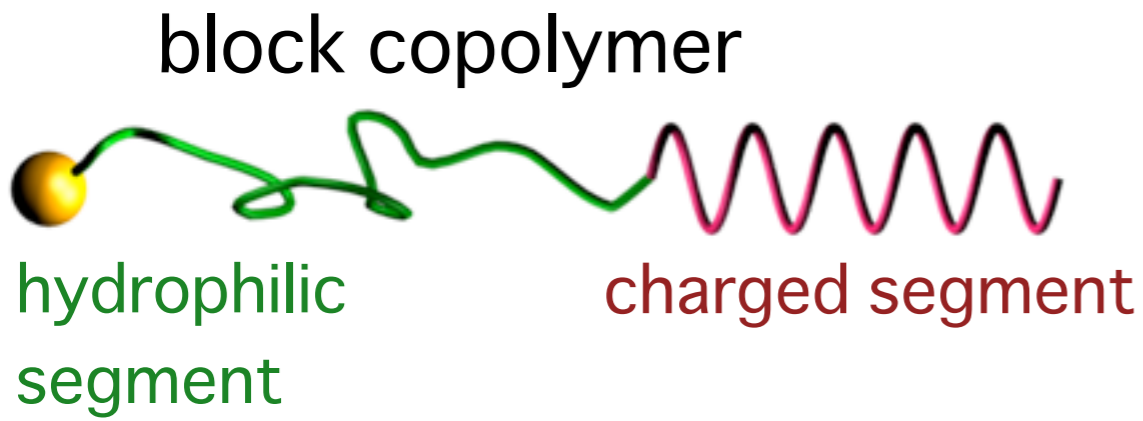
YFP expression only at the laser-irradiated site

laser irradiation

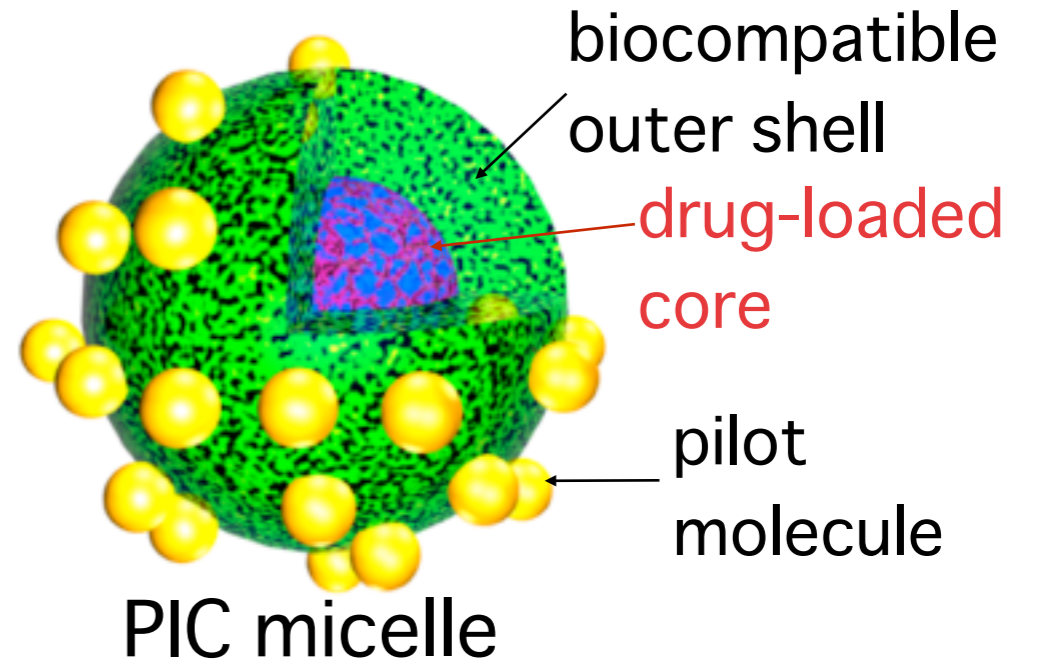



2 days after

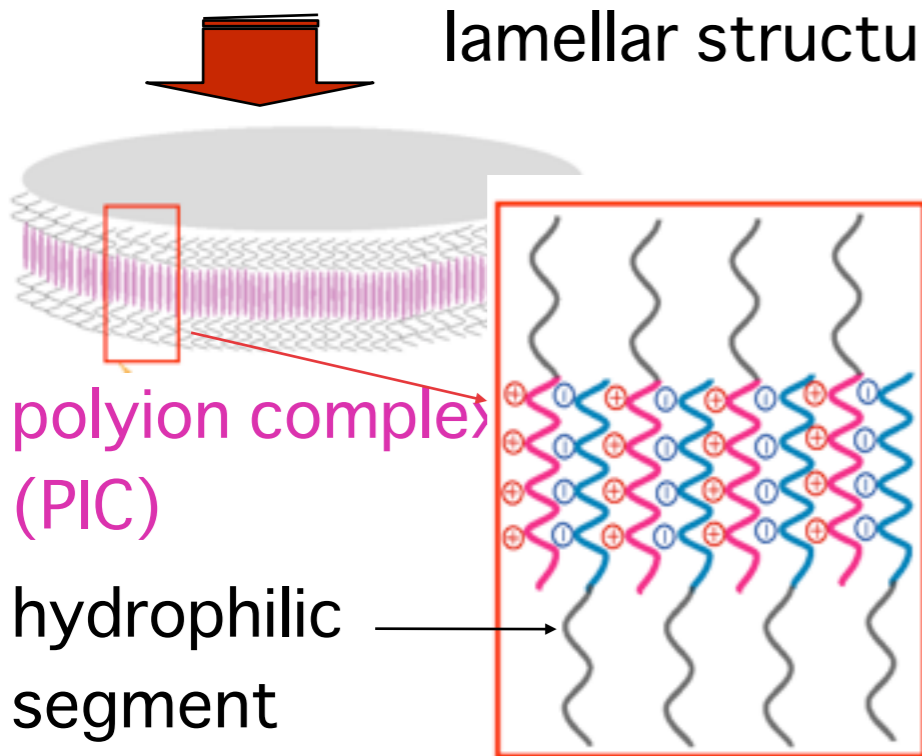
Supramolecular nanocarriers based on polyion complex formation



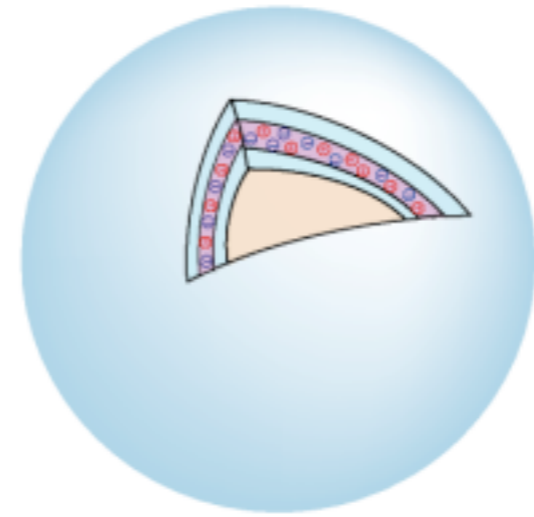

self-assembly



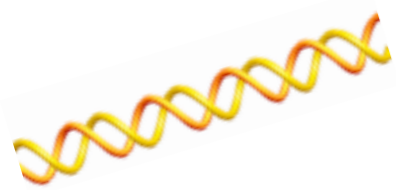
lamellar structure



self-assembly

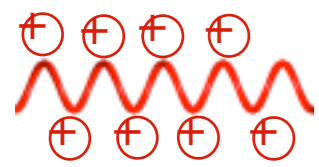


polymeric vesicular nanocarrier (PICsome)

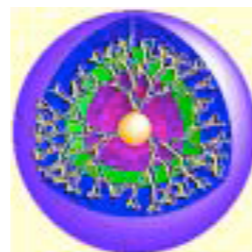


DNA

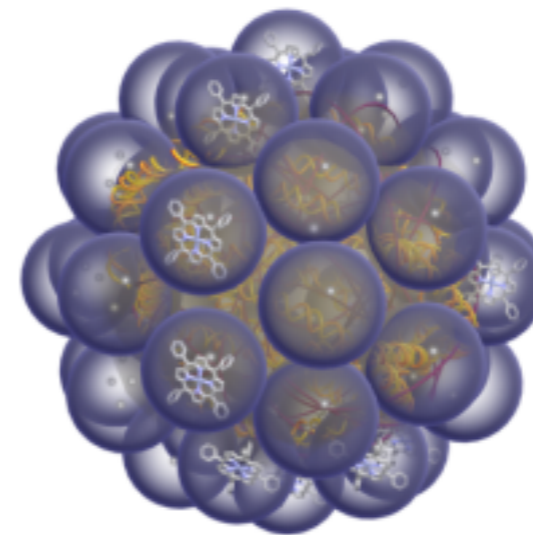
self-assembly



cationic polymer / peptide



anionic dendrimer photosensitizer



Polyplex enveloped with dendrimeric photosensitizer

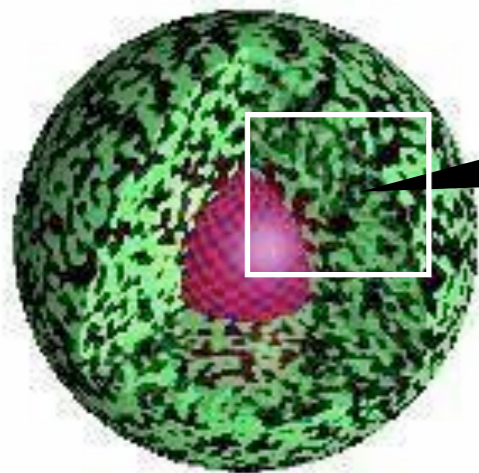
Molecular Strategies for PICsome Formation

* Stabilize lamella phase to prevent micelle formation

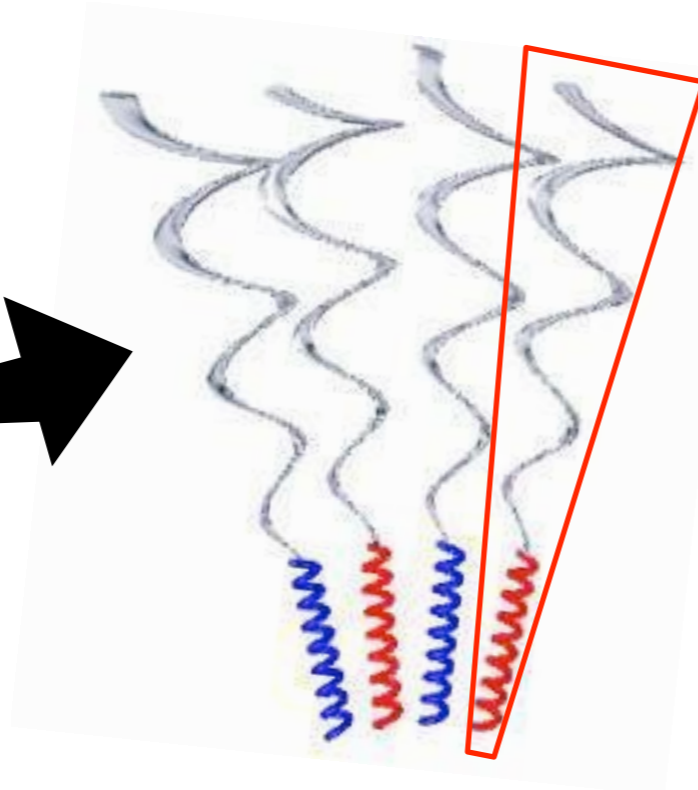
DP of PEG (DP_{PEG}) = 270

DP of Polyion Segments (DP_{PI}) = 70

➡ Formation of Micelles



PIC Micelle



Curved Interface
between
PEG and PIC Layer

Lowered ratio of
 DP_{PEG} to DP_{PI}



More
Planar?

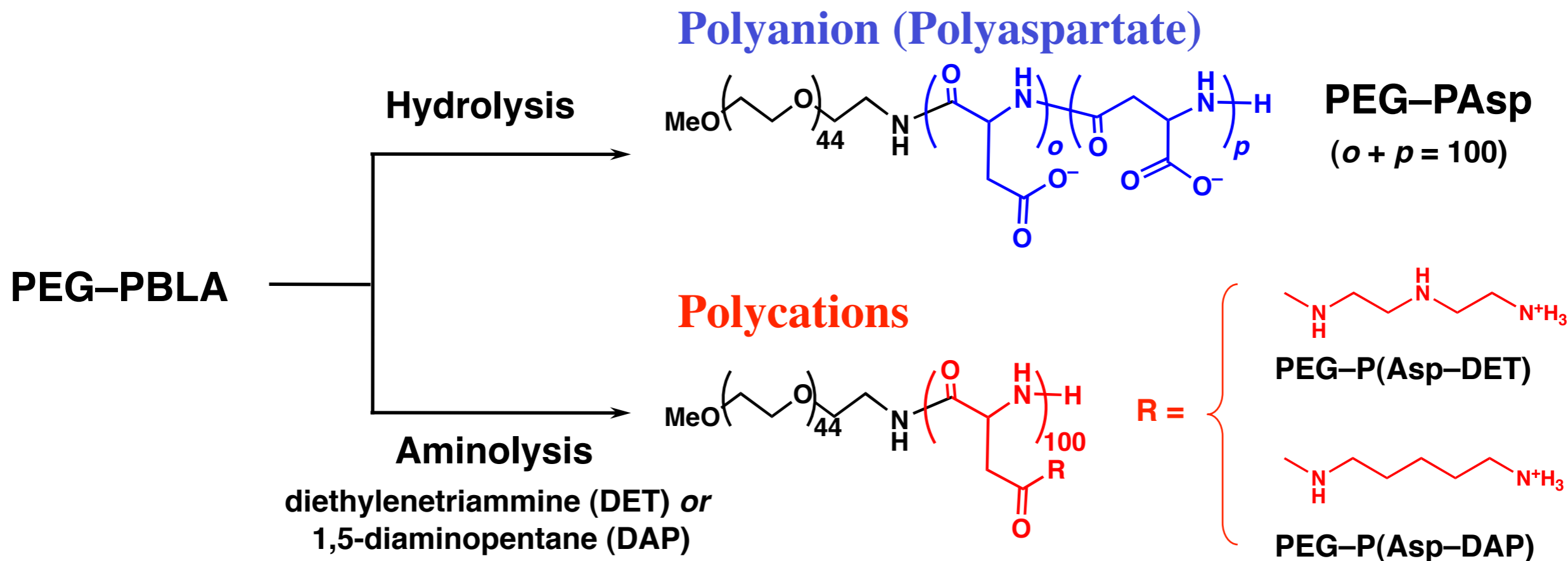
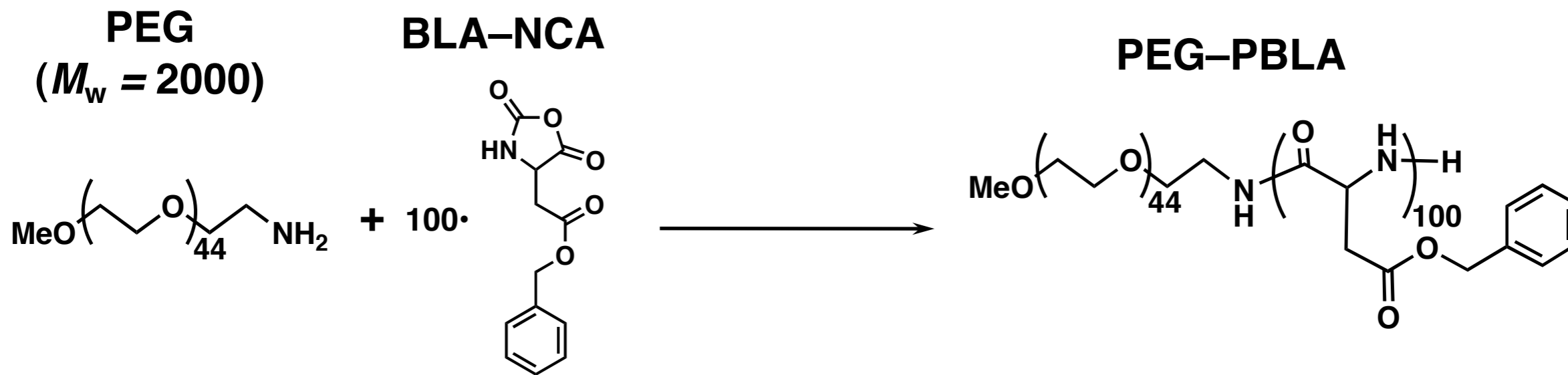
This Work

$DP_{PEG} = 45$

$DP_{PI} = 100$

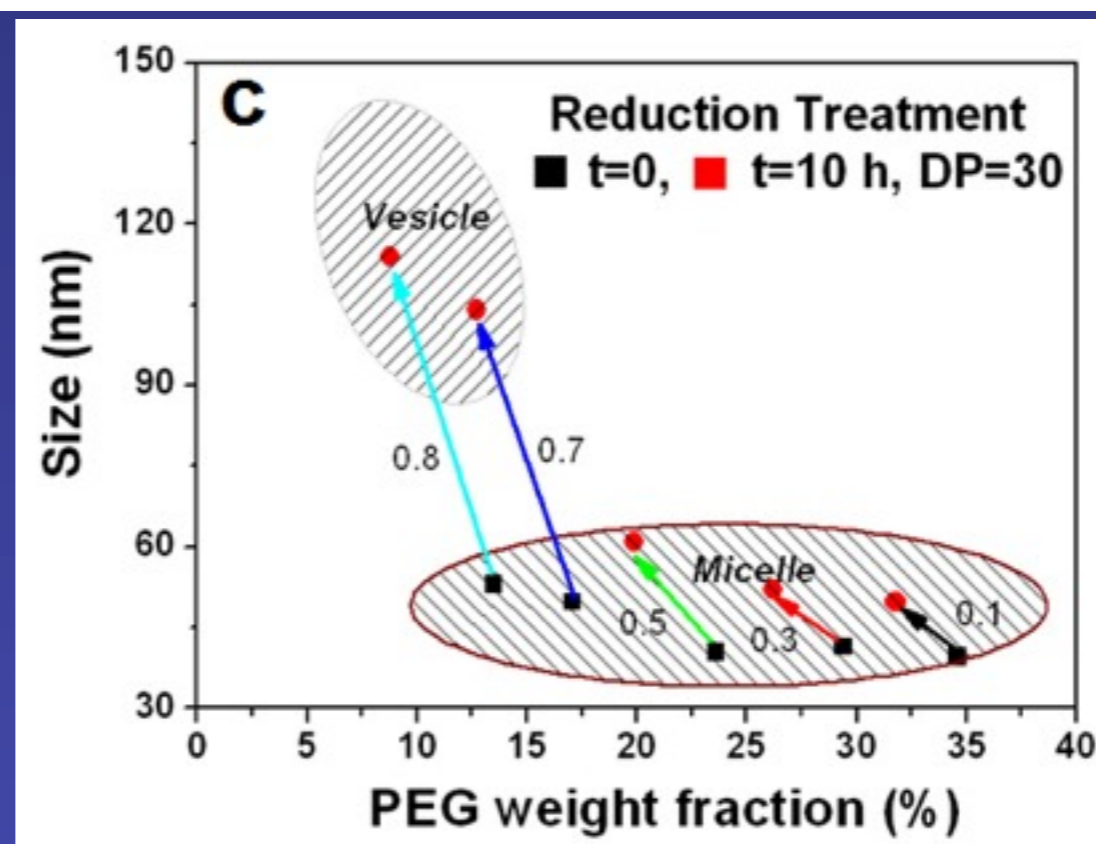
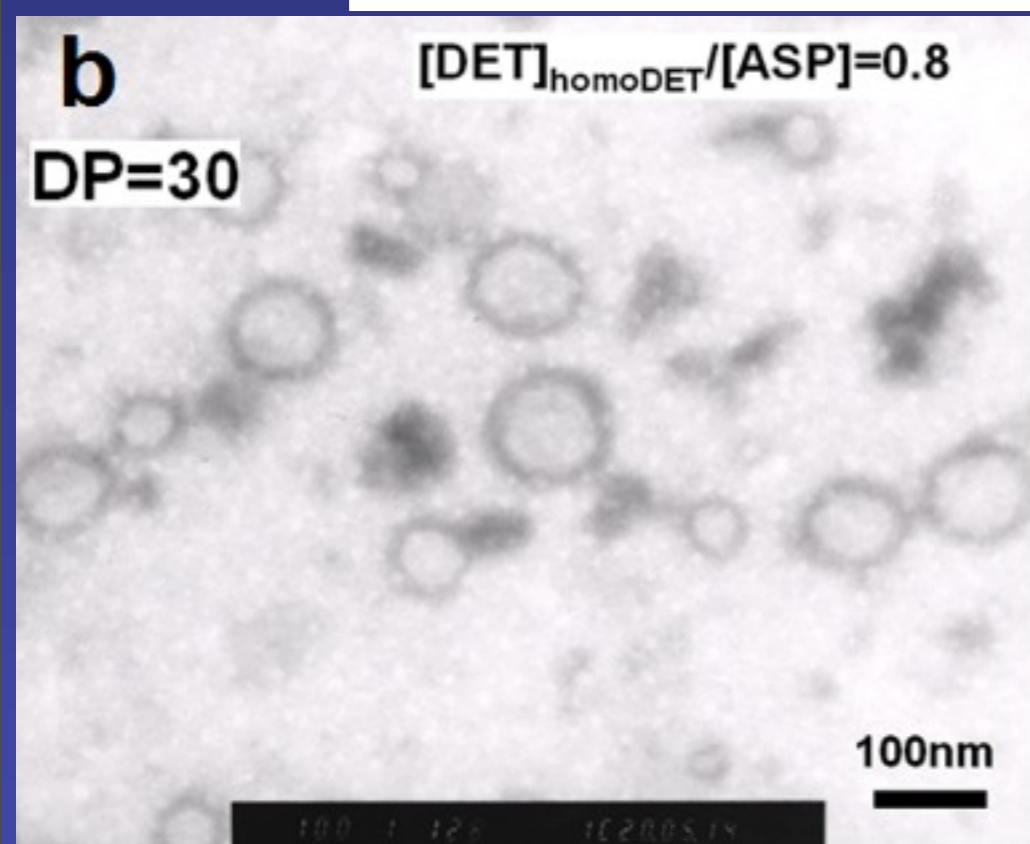
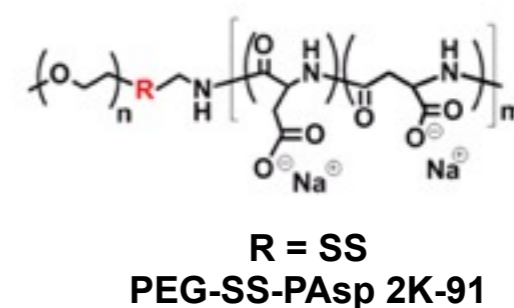
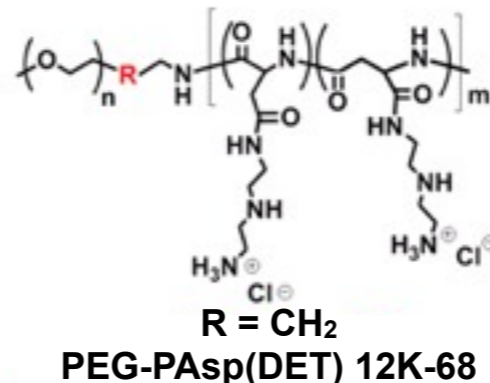
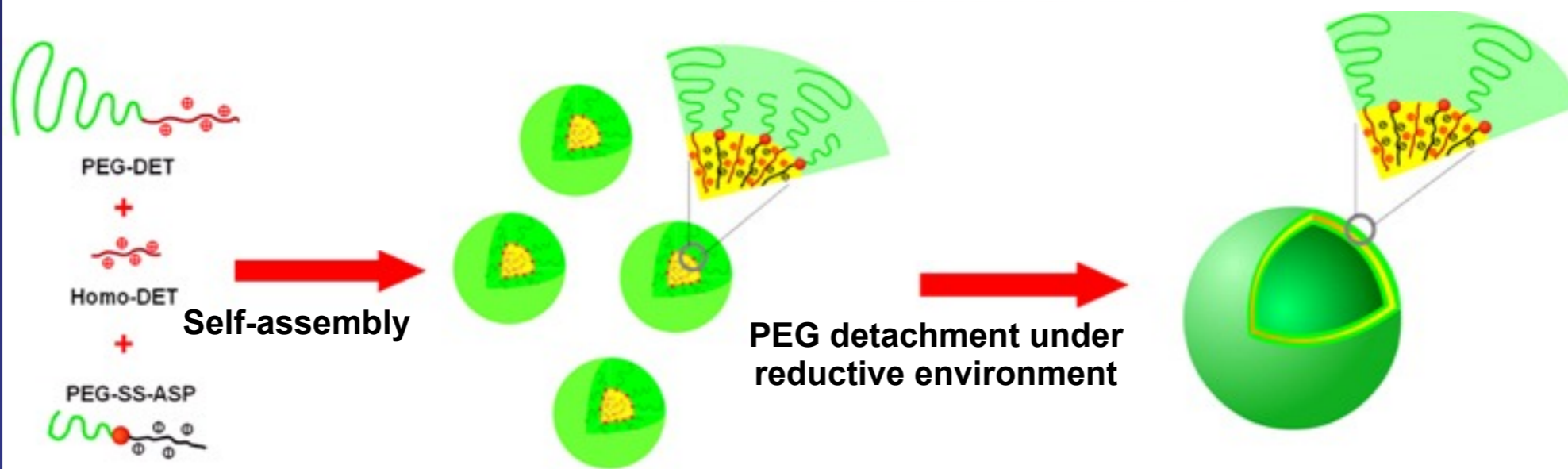
Synthetic Scheme of Block Copolymers

- Chain length matching of a pair of oppositely charged segments



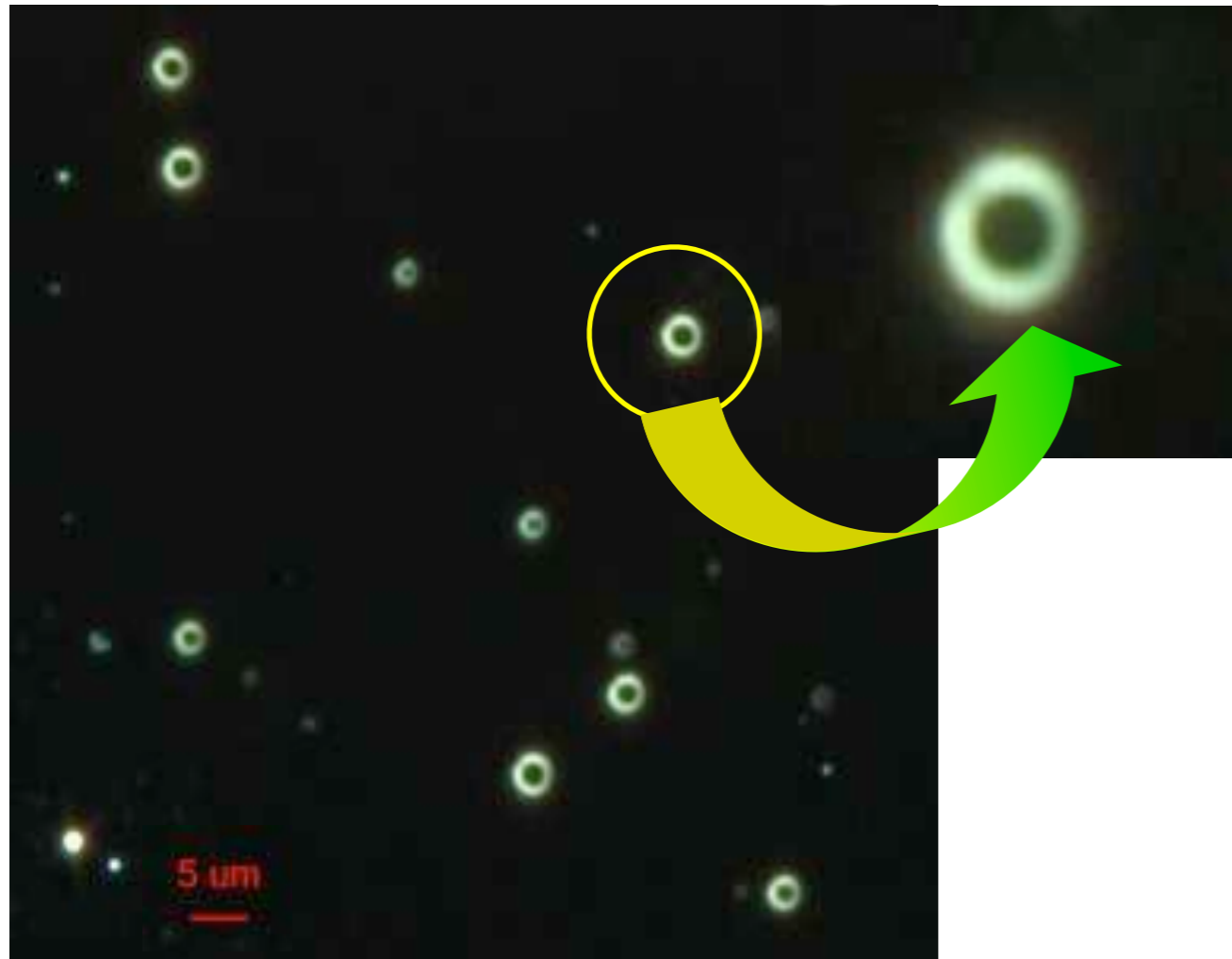
"Self-templating" strategy for hollow nanocapsule preparation

PEG chains
Polyion complex cores

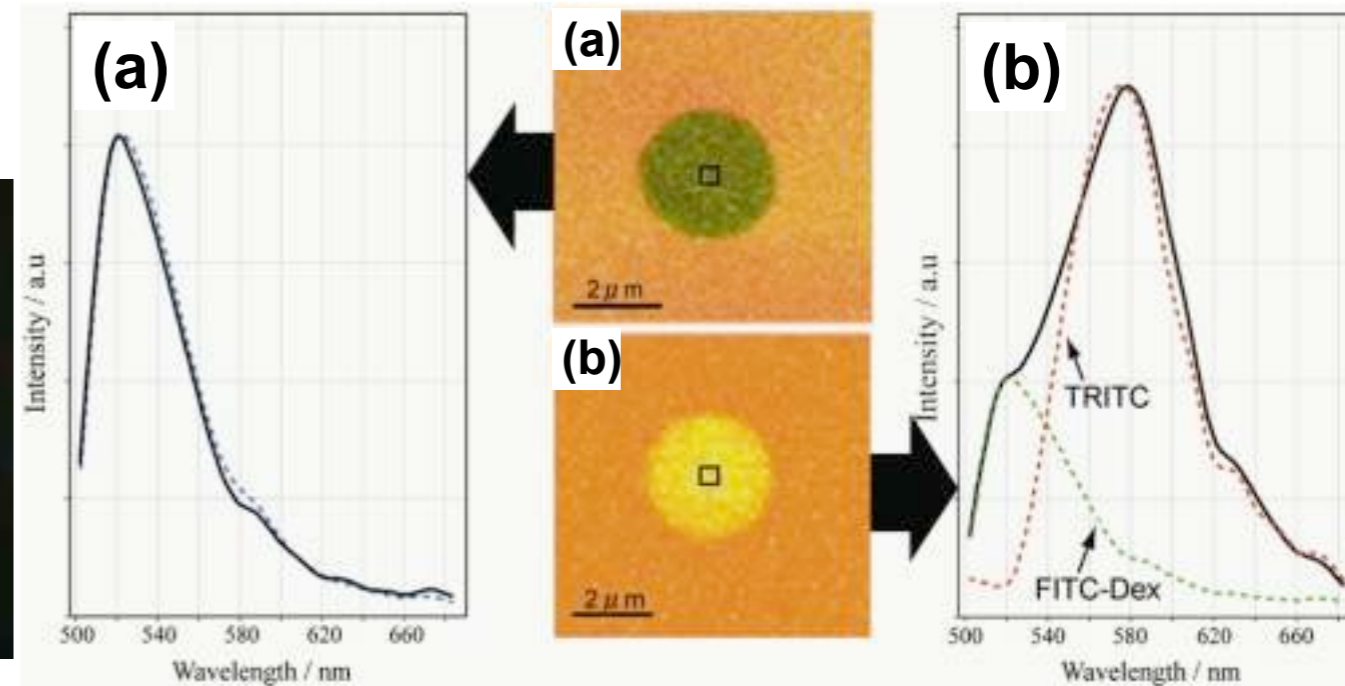


PEG weight fraction is a crucial factor for micelle-to-vesicle transition

Observation of Hollow Structure of PICsome



Dark-field microscopic image of PICsome



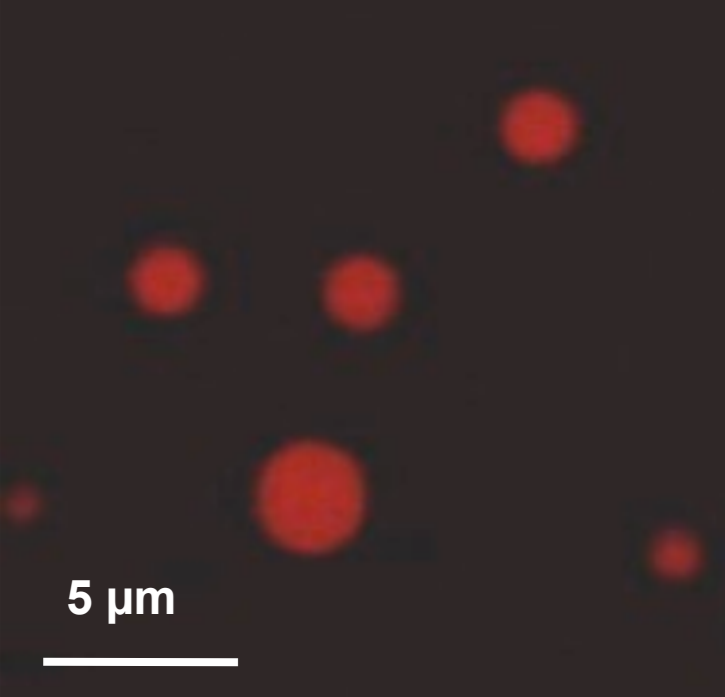
- (a) FITC-encapsulated PICsome + TRITC-dextran ($M_n=65,000\sim76,000$)
- (b) FITC-encapsulated PICsome + TRITC ($M_w=443$)

 Semi-permeable nature of PIC membrane

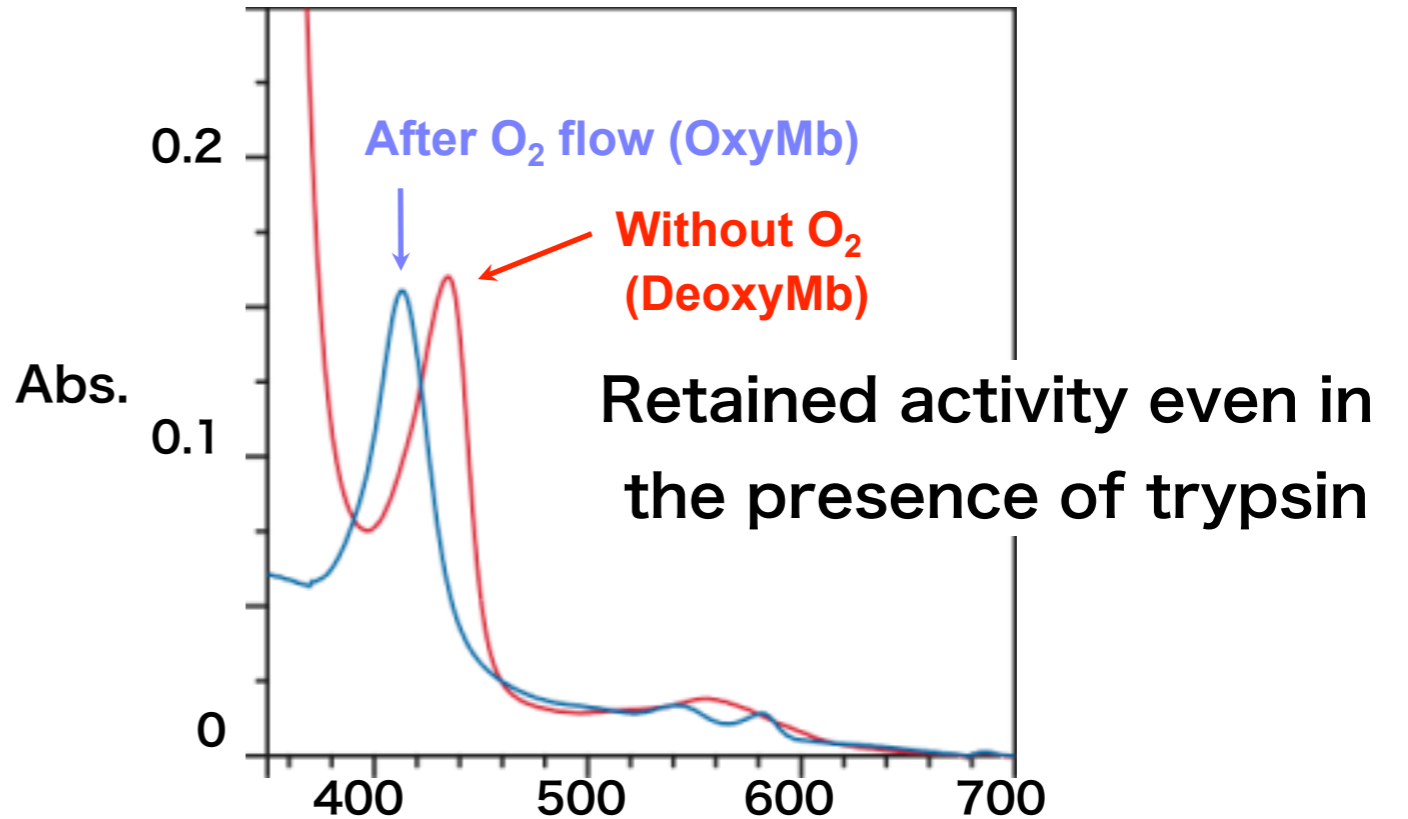
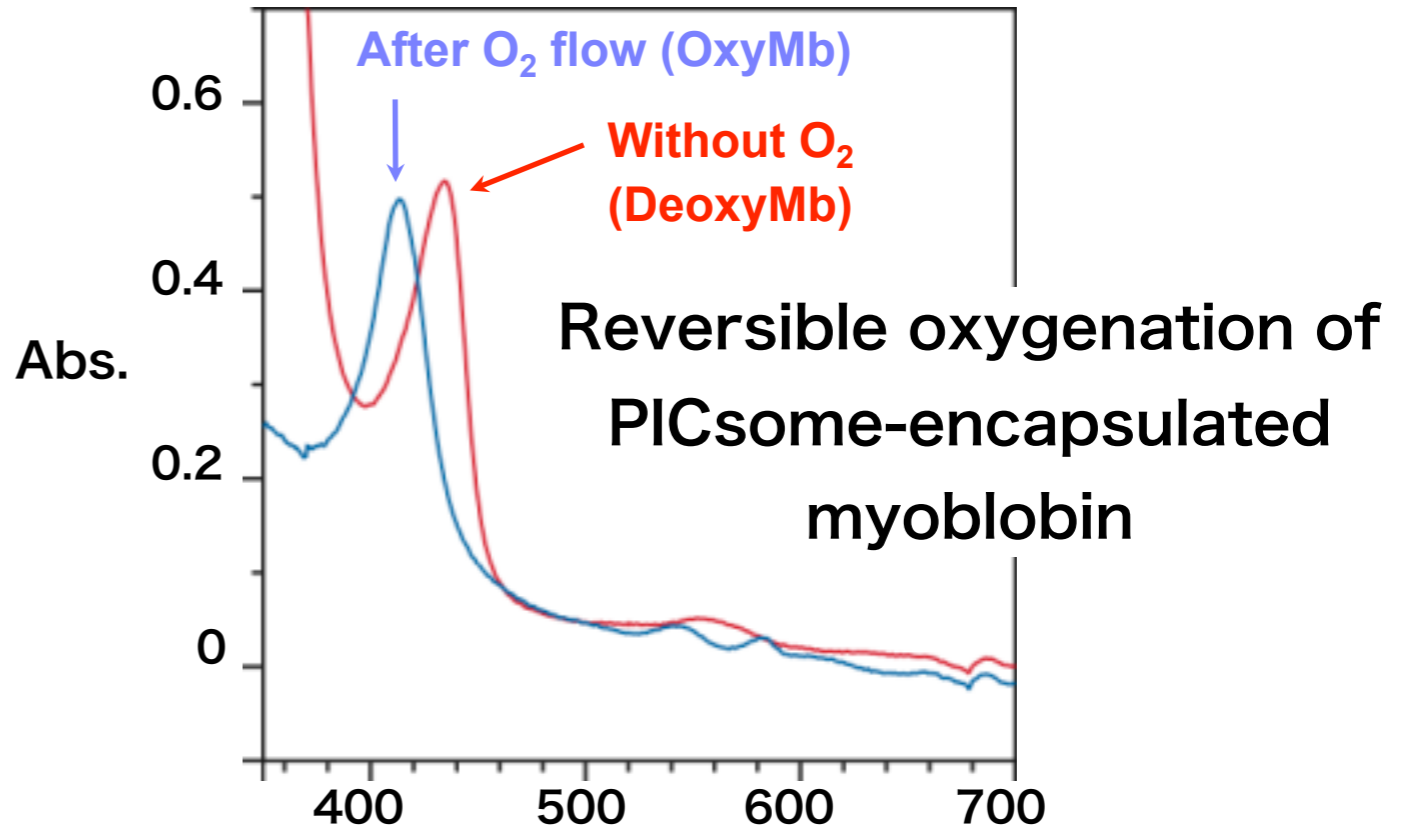
Confocal laser scanning microscopic image of PICsome with entrapped FITC-dextran

Myoglobin-encapsulated PICsome as Nanobio-reactor

Encapsulation of oxygen carrier protein (myoglobin) (Mw = 17,800)

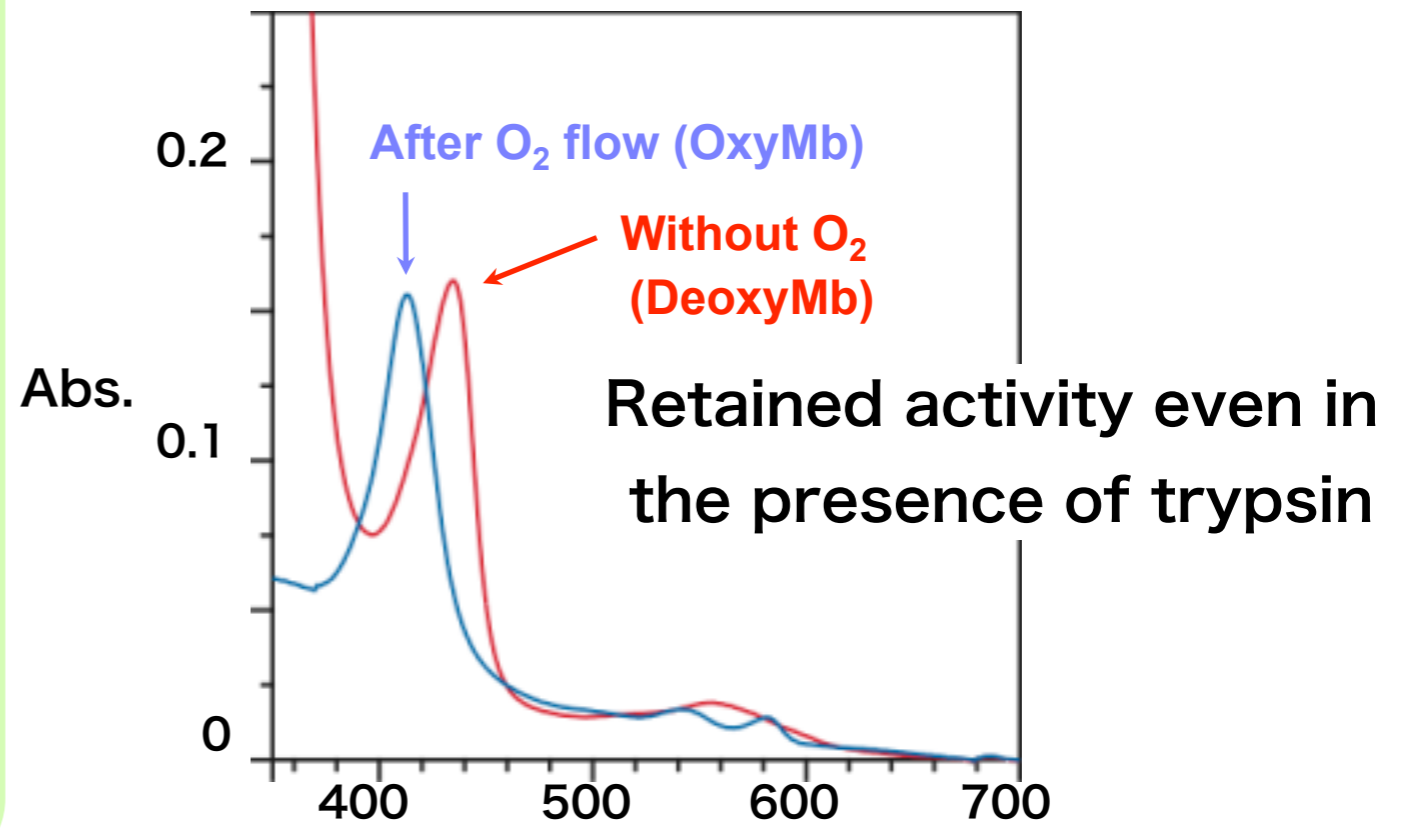
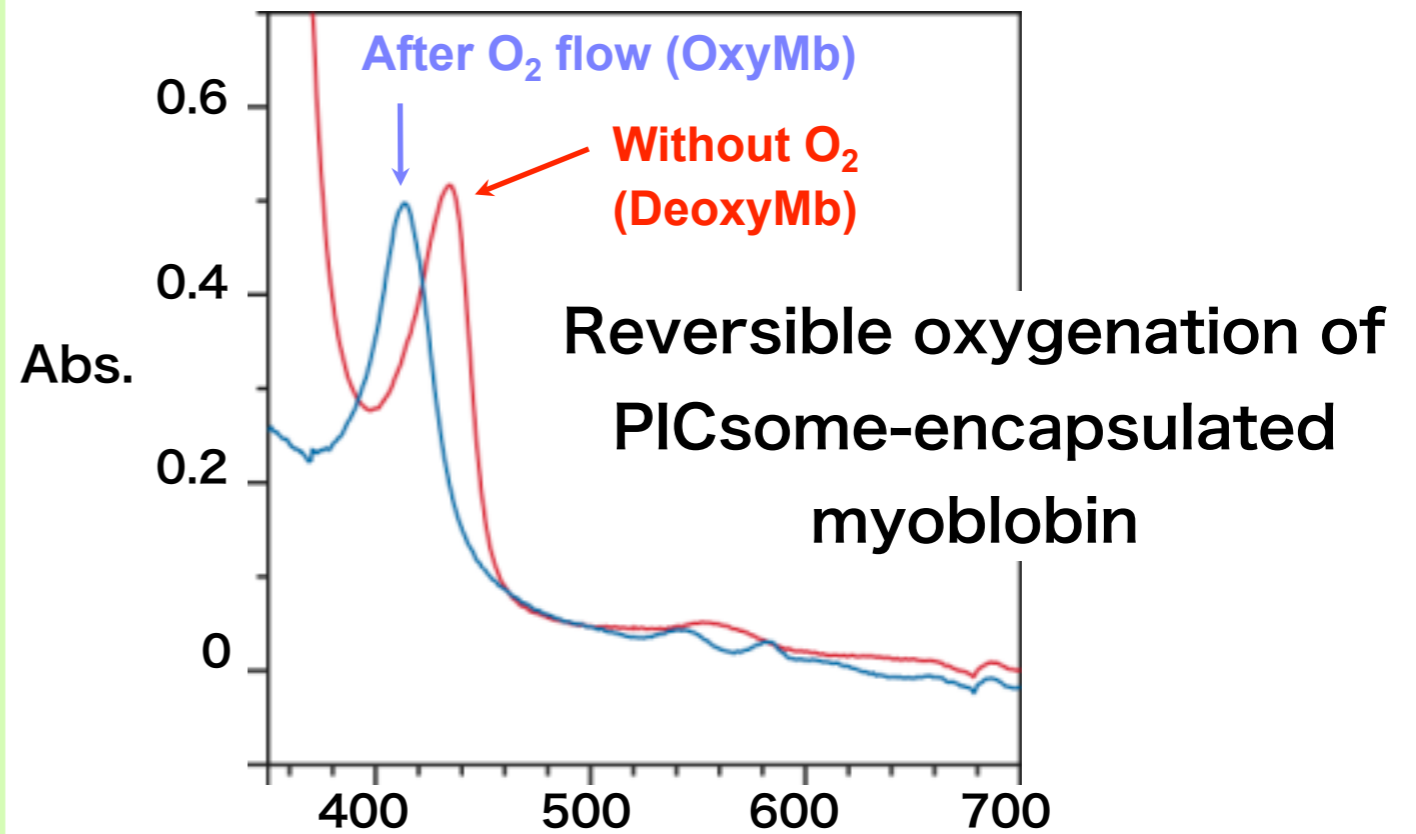
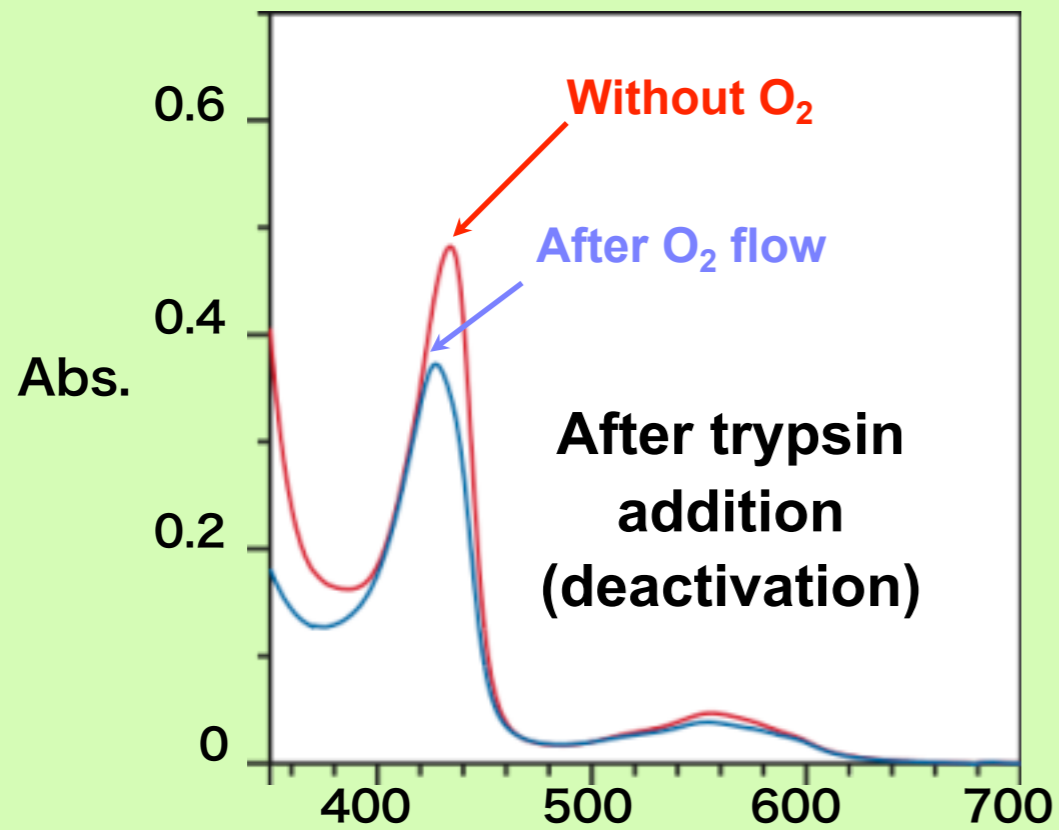
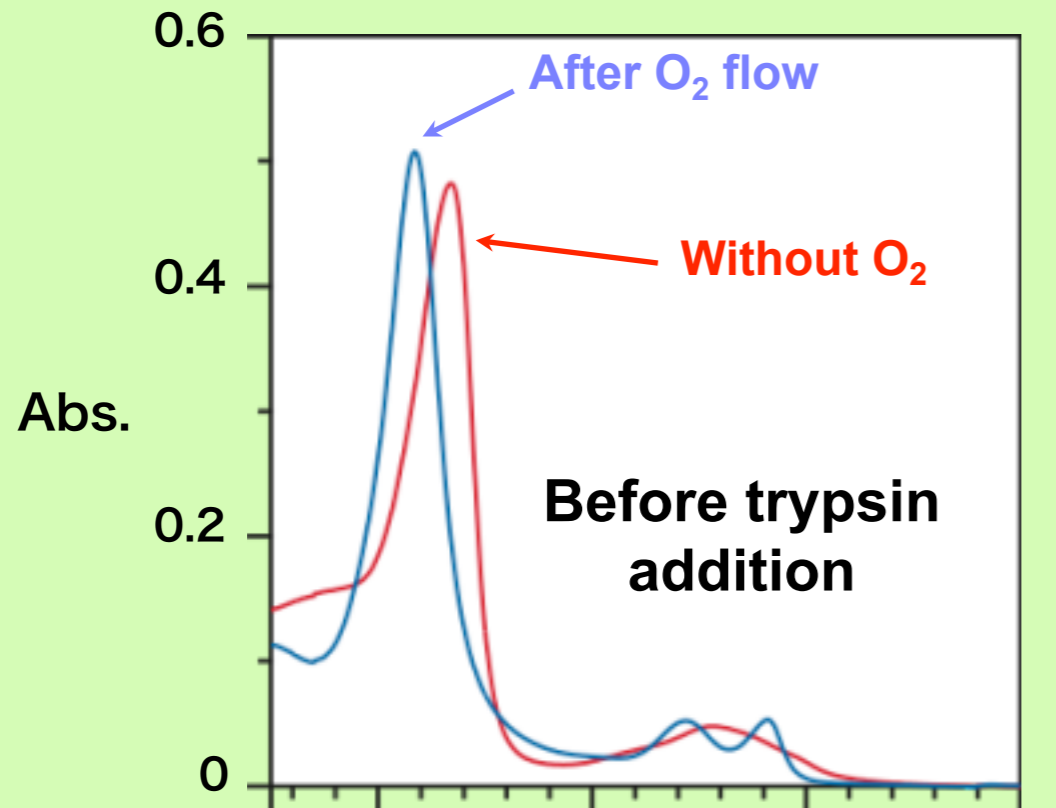


CLSM image of rhodamin-labeled myoglobin in PICsome

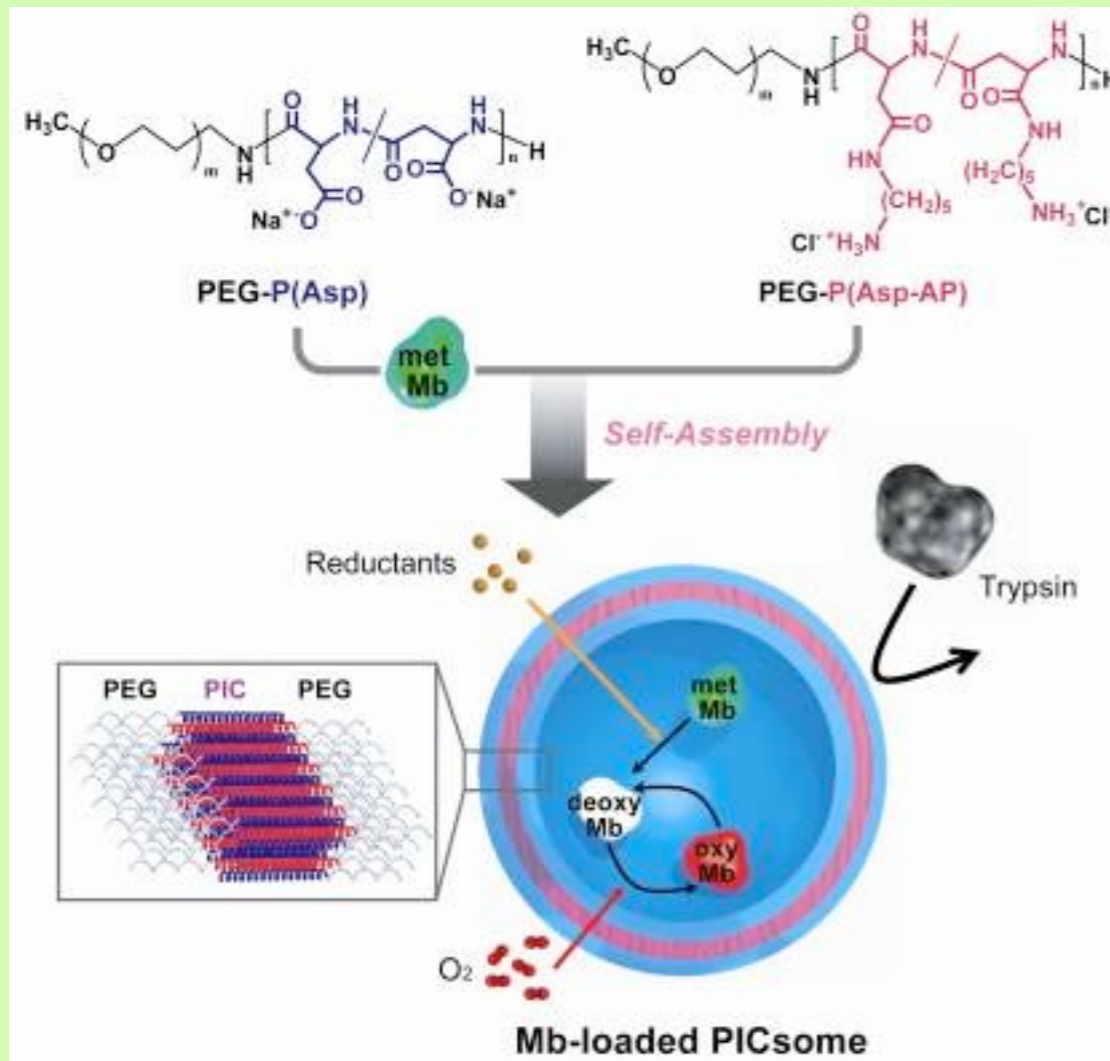


Myoglobin-encapsulated PICsome as Nanobio-reactor

Free myoglobin



Myoglobin-encapsulated PICsome as Nanobio-reactor

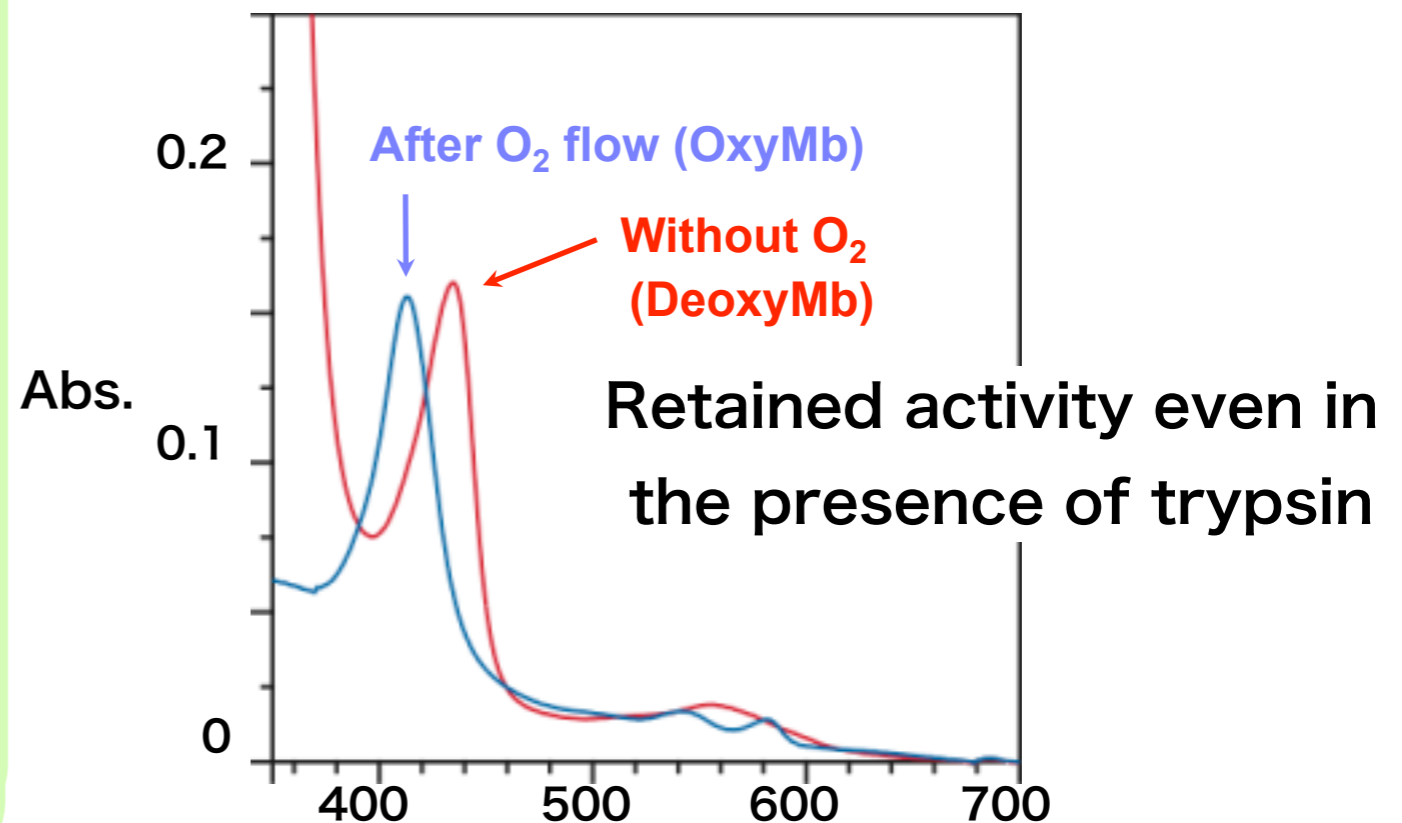
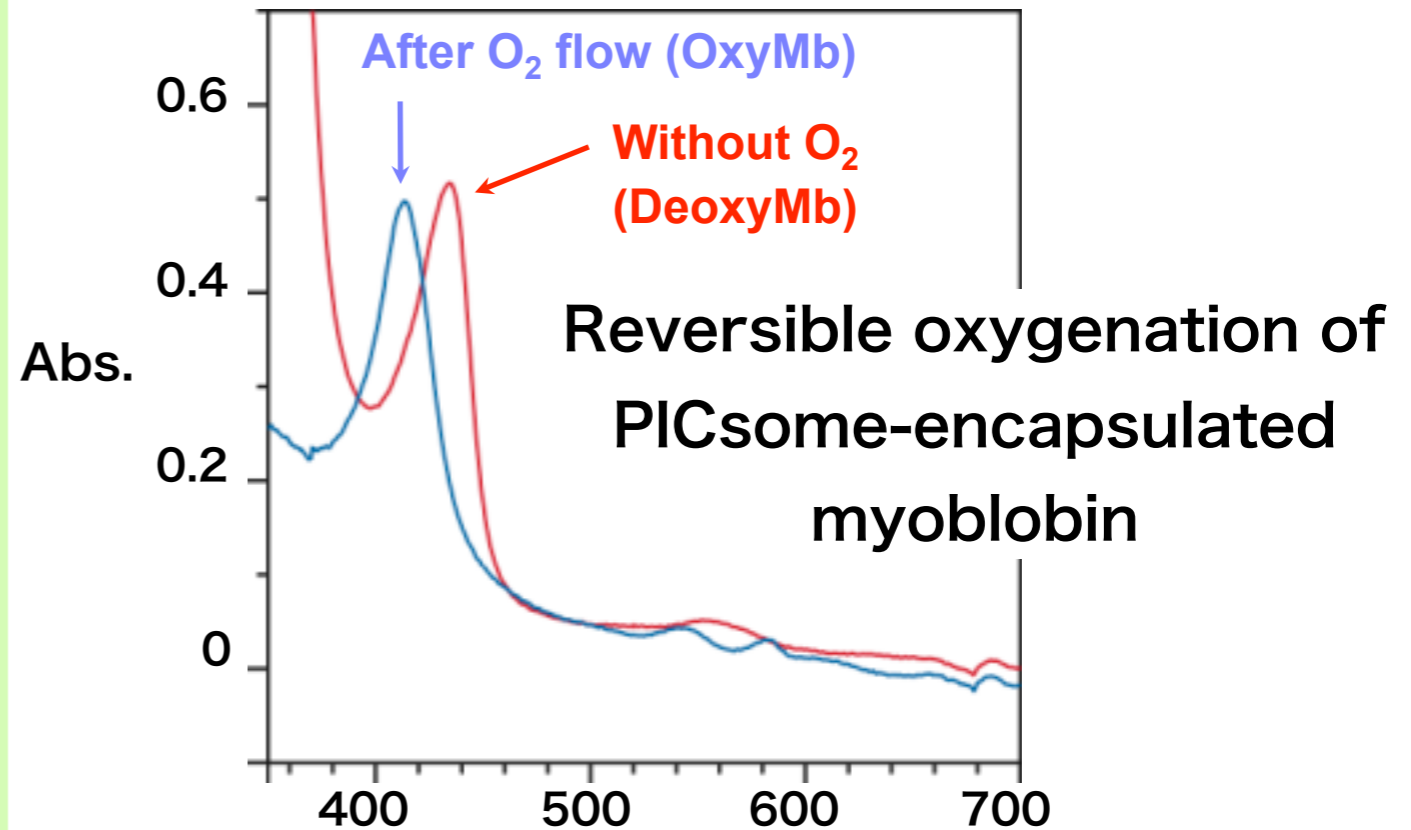


***Reversible O₂-binding**

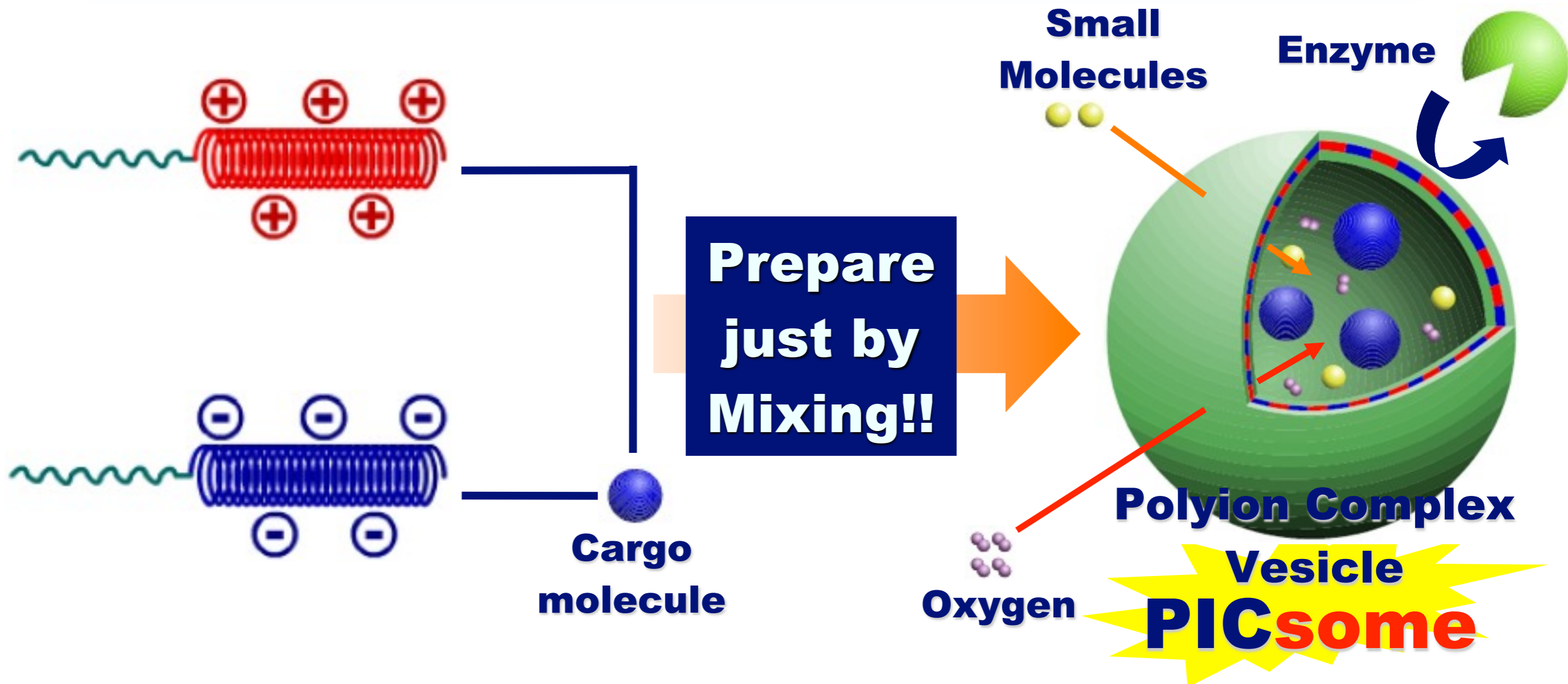
***High Proteinase Resistance**

➔ Promising Carrier for Protein Delivery

A. Kishimura, et al,
Angew. Chem. Int'l. Ed., 46, 6085-6088 (2007)



PICsome as Functional Nano-container



Utilities

- Encapsulating Macromolecules
- Selective Permeability
- Proteinase Resistance
- pH Sensitivity

Applications

- ★ Bio-reactor
- ★ Artificial Organelle
- ★ Artificial Cell
- ★ **Delivery Carrier**